Characterization of Whip Targeting Kinematics in Discrete and Rhythmic Tasks

by

Camille Henrot

Submitted to the
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in Partial Fulfillment of the Requirements for the Degree of
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ABSTRACT

Robotic control of complex objects is inferior to that of humans despite superior communication, sensors and actuators. Therefore, studying human control of complex dynamic objects, in particular a bullwhip, should reveal how humans may achieve superior dexterity.

An expert whip-cracker performing two distinct targeting tasks, discrete and rhythmic, was observed using the Qualisys 3D motion capture software. The objective was to investigate the kinematics of the whip, the kinematics of the subject’s arm while controlling the whip and the differences between discrete and rhythmic tasks.

The subject was able to expertly perform both targeting tasks with excellent targeting accuracy. The study confirmed the existence of a wave propagating down the whip as stated in prior work. Furthermore, a distinct difference between discrete and rhythmic tasks was observed in the reproducibility of position profiles, reproducibility of phase profiles, and the waveforms of elbow and wrist angles. Finally, the whip trajectory was substantially confined to a plane. In contrast with claims made in prior work, this plane was found to be distinct from the parasagittal plane and slanted with respect to it.

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1. Introduction

A challenge of robotic control is understanding and emulating the simplicity by which humans do what they do. How can a robot or a piece of machinery imitate human dexterity? The paradox remains that human communication, computation, and actuation are vastly slower than most modern robots, yet humans achieve dexterity superior to robots. Studying human control of complex dynamic objects should reveal how humans achieve superior dexterity.

Some theories of human neural control state that when humans come into contact with objects, the central nervous system back-calculates a kinematic model and predicts the exact mathematical behavior of the object [1]. Hogan and Sternad, on the other hand, suggest that this dexterity, instead, arises from encoding motor commands as dynamic primitives [1]. Dynamic primitives suggest a different neural representation of complex object manipulation. Two such primitives are rhythmic and discrete motions: a rhythmic motion is periodic while a discrete motion is a stand-alone motion in time.

One particularly complex dynamic object is a bullwhip. The bullwhip varies in both diameter and flexibility along its length and the physical phenomenon of cracking a whip requires parts of the whip to exceed the speed of sound. However, experts can reliably ‘crack’ a whip or use it to strike small targets from large distances.

This project studied the performance of an expert whip user striking an object of 5cm diameter from a distance of 1.8m, which was done for both rhythmic and discrete execution.

Most historical research regarding bullwhips explores mathematical modeling and the exact motion of the whip; however, we found no discussion of the interaction between the human and the bullwhip [2,3]. Prior work has studied the character of the crack of the whip and the trajectory of the whip during a crack. This study instead focused on the targeting task analyzing control, consistency, and reproducibility of the whip trajectory. The characterization of the motion of an expertly controlled whip can be used as a foundation for further work in the study of complex dynamic object control.

2. Background

2.1 Cracking a Bullwhip

According to Goriely, the representation and use of whips is widely misunderstood not only in research circles but in broader communities as well [2]. In fact, the bullwhip is one of the most interesting objects from the standpoint of complex object manipulation. The main purpose of the bullwhip is to produce a distinct, loud cracking sound, used initially to direct animals as well as for communication purposes. Nowadays bull-whip manipulation has become a source of entertainment for wide audiences.

A common bullwhip is made out of a heavy, robust material such as leather or nylon. A detailed schematic is shown below in Figure 1. The whip is made of two parts: the handle and the thong. The handle is the widest and most rigid part of the whip, while the cracker, on the tip of the thong, is the thinnest and most flexible. The crack occurs as the cracker reaches supersonic speed.
Figure 1: Construction of a bullwhip (drawing from Conway [4]). The handle is rigid, the thong is flexible and the cracker, at the end of the whip, is responsible for the distinctive cracking sound.

Goriely and Bernstein both focus specifically on the production of a cracking sound in their studies. The most common explanation of whip motion is that an abrupt change in tension creates an initial waveform propagating down the length of the whip from the handle to the tip of the cracker [2,3]. As the bullwhip diameter decreases down the length of the whip, the velocity increases and eventually exceeds the speed of sound [5].

Goriely points out that most studies explaining the cracking phenomenon of whips assume a specified shape of the whip over time [2]. The model for the shape of the whip is fairly complex and depends on many factors such as the initial formation of a loop, boundary conditions (initial handle velocity and subsequent free-end velocity), whip construction (the effects of tapering) and tension in the whip. Furthermore, for each distinct whip-cracking or targeting technique there exists a different transient whip shape though each technique still produces the cracking sound.

There are several techniques for whip cracking, however the two most common are the forward crack and the cut or overhand technique, often used for targeting [2]. Both techniques are visualized below in Figure 2. The forward crack is neither the most intuitive nor the most efficient technique to crack the whip but it is the technique showing the most obvious wave propagation down the flexible thong. The cut or overhand technique, generally used for targeting, is based upon a change of direction of the whip at the top of the arm motion. The whip-cracker swings the whole whip up off the ground and suddenly changes direction of the handle to produce a rolling shape that propagates as a wave [4]. This project singled out targeting tasks using the cut overhand technique.
Figure 2: Examples of two common whip techniques (drawing from Conway [4]). (A) forward crack technique and (B) cut overhand technique. The cut overhand technique was used in all experiments in this project, the subject swings the whip of the ground (i), reverses arm motion (ii), and the whip cracks over the hand and forward (iii).

2.2 Assumptions of Bullwhip Kinematics

The body of prior bullwhip research focuses heavily on the cracking phenomenon. It would appear that the cracking sound is simultaneous with the targeting task. In this regard, the assumptions made in the study of whip-cracking are relevant to targeting tasks.

One kinematic assumption of whip-cracking research is that all whip motion remains planar. This means that at any point in time the trajectory of the whip in 3D space can be reduced to a two dimensional kinematic system [6]. Generally, the plane is assumed to be in the parasagittal plane, the vertical plane beside the body, or the overhead plane depending on the technique being used.

An excellently crafted whip is constructed with fine cross-hair braiding such that it is possible for an initial planar shape to remain planar as it propagates down the whip [4]. Of course, this behavior is dependent on the skill and dexterity of the manipulator along with the construction of the whip. For example, it may be more difficult to maintain a planar whip trajectory with a poorly constructed whip, in the same way that it may be more difficult for a novice whip user to maintain whip planarity. This project explored planarity in whip targeting.
tasks for an expert whip user. It defined the degree of whip planarity as well as the plane that described the trajectory of the whip.

2.3 Introduction to Dynamic Primitives

Recent work has shown that there is a large distinction in neural control between discrete and rhythmic motions that support the need for the theory of dynamic primitives [7]. It is highly unlikely that the central nervous system computes an exact internal model of human motion when in contact with a complex object for example, a whip. If this were not the case, then the human would be able to control the same object in the same way regardless of discrete or rhythmic tasks. This is the motivation for dynamic primitives.

A study by Schaal shows that discrete and rhythmic motions elicit not only different cerebral activation but that, in fact, there are distinctly measurable transitions that occur between discrete and rhythmic motions as the speed of a discrete task is increased [8,9]. This project explored the differences between discrete and rhythmic motion.

Hogan and Sternad propose that the human interactive behavior is composed of at least three dynamic primitives: submovements, oscillations and mechanical impedances [10]. Of the three, impedance is specifically relevant to the use of tools. These dynamic primitives need not be mutually exclusive and, in fact, it is their simultaneous existence that allows for such complex movements to be so easily performed and retained by the user [10]. It is important to note that humans can voluntarily control all three types of dynamic primitives.

Though this project is not specifically focused on dynamic primitives, the final goal of this study is to gain an empirical understanding of the dynamic primitives at play with whip use. The existence and subsequent definition of dynamic primitive interaction and superposition in whip use is useful in further defining the observed dexterity of humans and to eventually apply such primitives to the field of robotics.

2.3.1 Submovements

Submovements are like discrete movements in that, alone they are movements that begin and end at rest. However, in the case of human dexterity these submovements are stand-alone motions that can then be superimposed in time with other dynamic primitives. Hogan and Sternad define a submovement as “a smooth sigmoidal transition from one value to another with a stereotyped time-profile” and that “each coordinate’s speed profile has the same shape which is non-zero for a finite duration” [1].

2.3.2 Oscillations

The oscillatory primitive is described as an almost periodic-motion. The main distinction is that oscillations are not made up of many overlapping submovements in opposite directions. Though amplitude and exact behavior of the oscillation may vary over time due to fluctuations of biological systems, the average time course of oscillatory behavior is periodic. This periodic behavior should have the same shape for it to be considered an oscillatory dynamic primitive [1].
2.3.3 Mechanical Impedance

Mechanical impedance is the dynamic primitive that deals most with contact and interaction that humans encounter in their daily activities. Fundamentally, cracking a whip requires a mechanical interaction between the manipulator and the whip itself. This interaction is generally an impedance, a generalized stiffness, that specifies the force response to the motion of the object or environment [11]. It should be noted that control of interaction and contact with objects can drastically change the dynamics of a system, often changing its order and complexity. However, mechanical impedance is solely a result of the neuro-mechanical system and is not changed by the presence of contact or interaction, making it an extremely robust method of motor control [10].

3. Experimental Setup

Two experiments were performed to assess the position, velocity, and planarity of both the subject’s arm motion as well as the whip trajectory when using the whip to hit a target. Using the Qualisys 3D motion capture system, three-dimensional positions were recorded for markers along the whip and markers on the subject’s arm for each targeting task.

3.1 Overview of Subject and Experiments

3.1.1 Subject

One male right-handed expert whip-cracker with more than 15 years of whip-cracking experience participated in experiments 1 and 2 after giving informed consent. All experimental protocols were approved by the Institutional Review Boards (IRBs) of the Massachusetts Institute of Technology on the use of human subjects in research. Extensive work in target-oriented whip tricks as well as national and international competitions made this subject representative of controlled whip motion and expert whip manipulation.

3.1.2 Experimental Setup and Marker Placement

The subject performed two whip-cracking tasks: discrete and rhythmic execution. The goal of both tasks was to hit or touch a spherical target mounted on a spring with the tip of a 6ft bullwhip. As shown in Figure 3, the subject was positioned six feet, 1.83m, away from the target to ensure that the end of the whip would hit the target. The target was oriented at the center of the subject’s chest at 60% of the subject’s height, such that the target was in line with the subject’s hand.

The position of the target was calibrated before trials began, namely (x, y, z) of the target was determined before any targeting attempts. In some cases, the fast velocity of the end of the whip displaced the marker from the target making the target unmeasurable (the marker was no longer in the measurable volume of the motion system cameras) for the rest of the session. Through target calibration, success of each trial was assessed by verifying the distance between the calibrated target position and the position of the last marker on the whip.
Figure 3: Experimental setup showing placement of subject and target. The subject is positioned 1.83m from the target. The target is positioned at 60% the subject’s height. The x direction is across the subject’s body, the y direction is towards the target and the z direction is vertically upward from the ground.

To measure position of the subject and the whip, retro-reflective markers were attached to the subject’s dominant arm (right arm), trunk, and head using double-sided adhesive tape designed to be applied directly to the skin. Smaller markers were attached along the length of the whip in six positions. Each position along the whip had two markers placed opposite to each other on the circumference of the whip. This was done to maximize the probability of measurement at every location. No markers were attached to the very end of the cracker of the whip, as there was no physical support available and it would have drastically changed the kinematics of the very thin cracker string. The marker placement on the arm and whip can be seen in Figure 4 below.

The handle of the whip, in this case, was considered rigid while the rest of the markers were attached to flexible portions of the whip. Due to the construction of the whip, the flexibility of the whip increases down its length. As a consequence, marker R6 is located on a more flexible area of the whip than marker R1.
3.1.3 Experimental Description

The goal of each task was to hit or touch the spring target with the end of the whip. In the discrete case, the subject was instructed to perform 5 sessions of 20 discrete whip targeting attempts, totaling to 100 discrete trials over all sessions. The subject was verbally cued to begin each discrete attempt with a “go” signal and proceeded to choose the speed with which he manipulated the whip. Once the subject finished one attempt (trial) he was instructed to come to rest until another cue was given. In rhythmic execution, the subject was instructed to perform 2 sessions of 50 continuous whip trials. However, in the second session the subject did 51 continuous attempts, totaling to 101 rhythmic trials over all sessions. In these sessions, the
subject was cued to begin with a “go” signal and was self-paced in 50 continuous trials without rest. On the fiftieth trial the subject was cued to stop.

In both executions the subject was considered successful if he hit the target. There was visual feedback as the target would oscillate when it was hit. In discrete execution, if the subject was successful, he was instructed to stay at rest until the target oscillation was fully damped. In rhythmic execution, if the subject was successful, the target was not damped and the subject continued to attempt to hit the target. In some cases, the cracker of the whip got caught on the target (discrete: 10 trials out of 100, rhythmic: 1 trial out of 101). These trials were recorded but the data was not included in subsequent analysis. In total, there were 90 valid discrete trials and 100 valid rhythmic trials used in our data analysis.

3.2 Qualisys 3D Motion Capture

Data acquisition consisted of two main parts. The first was 3D motion capture, using the Qualisys motion capture system. The second was identifying markers in each trial using Qualisys Track Manager Software.

3.2.1 Data Acquisition

Traditionally, whip dynamics are studied by means of two-dimensional data acquisition systems such as high-speed video and high-speed shadow photography [2,3]. High-speed video is a robust method to measure and understand transient behavior of complex objects; however, this project explored a new method of 3D data acquisition.

The Qualisys motion capture system is a series of 12 infrared optical cameras. The cameras emit a ray of infrared light which is then reflected by the retro-reflective markers attached to the subject and the whip. The information from these markers is then used for 3D reconstruction of the markers in space [12].

The system must first be calibrated to determine the field of view of this composite camera where marker position can be measured. The calibration process used the Qualisys calibration wand and an axes frame on the ground of the space. The x axis was the direction across the subject’s body, the y-axis was direction between the subject and the target and the z-axis was vertical from the ground. Calibration took about 20 to 30 seconds. The field of view of the experimental space was swept with the calibration wand. The Qualisys Track Manager Software automatically determined whether the calibration was successful or if another calibration process is required.

Once the system was calibrated, the subject and whip marker positions could be measured. Data were recorded with a sampling rate of 200 Hz for up to 3 minutes, so about $3.6 \times 10^4$ time samples per trial. Once recording began the movement of the subject and the whip was recorded until the recording was stopped manually.

Figure 5 below shows an example of the raw data captured in a trial. Initially the data is unidentified, meaning all data are raw position measurements, not linked to any particular marker.
Figure 5: An example of one time sample of raw unidentified data in Qualisys Track Manager Software. The red points in space are unidentified markers corresponding to the markers on the subject and the whip. The x axis is denoted by a red arrow, y axis, light blue and z axis dark blue. The two rectangles on the ground are force pads that were not used for this experiment.

3.2.2 Data Processing and Point Identification

While the track manager software can accurately measure all markers in the field of view, the software does not automatically define what each marker is, i.e. shoulder vs. RI. In order to extract data for each marker, one must identify the measured markers with useful headings or names. This point and click data processing technique is prone to human error.

The fill level of a marker refers to the percentage of time relative to the whole trial the particular marker is seen by the cameras. If a point is obscured during the trial this will be shown in a lower fill level. At any time when a marker is obscured the marker must be re-identified.

In the case of the markers on the subject, the fill level was generally 100% and relatively simple to identify. However, in the case of the markers on the whip, many were obscured due to the kinematics of the whip in space, resulting in a much lower fill level. Over the course of each trial most whip markers required some amount of re-identification. This is where the redundancy of markers became helpful.
Figure 6: An example of one time sample of identified data in *Qualisys* Track Manager Software. The colored points in space are examples of identified data. Green points correspond to markers on the subject, while the other colors correspond uniquely to a whip marker R1, R2, ..., R5. Visual distinction in the identification process is useful to decrease possible error. The x axis is denoted by a red arrow, y axis, light blue and z axis dark blue. The two rectangles on the ground are force pads that were not used for this experiment.

Once markers were identified, the data was segmented into individual trials. Subsequent data processing was performed in *Matlab*.

4. Experimental Methods

The data acquired in the two experiments required several analysis techniques to characterize controlled whip motion. Through the following experimental methods whip and arm kinematics were characterized through position profiles, velocity profiles, joint angles, and planarity studies.

4.1 Data Structure and Integrity

Part of this project explored a new method of data acquisition to study whip motion. Through multiple data acquisition and troubleshooting trials, we developed a robust data capture methodology. This particular set of data required specific processing and restructuring to enable the analysis.
4.1.1 Data Integrity

Though the Qualisys system is a highly sophisticated system, it still requires manual processing to ensure the integrity of the data, particularly in the case of capturing whip motion. The markers used on the whip were small retro-reflective spheres that were attached to the whip with adhesives. These markers are quite fragile and due to their small size can easily be obscured during data acquisition. One objective of this experiment was to design a data acquisition protocol such that the data of whip motion would be adequate to sufficiently describe the motion in the experiment.

An important design feature was marker redundancy. On each measurement point along the whip, two Qualisys markers were attached. This was to increase the probability of measurement of that particular point on the whip during each trial. For this reason, for each sample in a trial there are four distinct cases of marker data, detailed in the Table 1 below. An entry of 1 represents the existence of data for that sample, while an entry of 0 represents no data for that sample.

Table 1: Data occurrence cases. A 1 represents that marker data existed for that sample. A 0 represents that marker data did not exist for that sample.

<table>
<thead>
<tr>
<th>Case</th>
<th>Marker 1</th>
<th>Marker 2</th>
<th>Analysis</th>
</tr>
</thead>
<tbody>
<tr>
<td>Case 1</td>
<td>1</td>
<td>1</td>
<td>The resulting whip point data for time point t is the arithmetic mean in x, y and z position of the markers.</td>
</tr>
<tr>
<td>Case 2</td>
<td>1</td>
<td>0</td>
<td>The resulting data for time point t is the raw x, y and z position data from marker 1.</td>
</tr>
<tr>
<td>Case 3</td>
<td>0</td>
<td>1</td>
<td>The resulting data for time point t is the raw x, y and z position data from marker 2.</td>
</tr>
<tr>
<td>Case 4</td>
<td>0</td>
<td>0</td>
<td>There is no data available thus, the resulting whip point data for time point t, is not a number (NaN) and results in a hole in 3D position data for that trial.</td>
</tr>
</tbody>
</table>

Table 2 shows the percentages of case occurrences for each whip marker over all trials in both rhythmic and discrete tasks. It shows which points on the whip were most measured and which points on the whip were least measured. Whip point R6 did not result in a full data set in either discrete or rhythmic tasks. For this reason R6 data in particular was discarded in the analyses.
Table 2: Whip marker case occurrence percentage for all discrete and rhythmic trials.

<table>
<thead>
<tr>
<th>Whip Marker</th>
<th>Case 1</th>
<th>Case 2</th>
<th>Case 3</th>
<th>Case 4</th>
</tr>
</thead>
<tbody>
<tr>
<td>R1</td>
<td>8.17%</td>
<td>19.43%</td>
<td>72.66%</td>
<td>9.06%</td>
</tr>
<tr>
<td>R2</td>
<td>2.75%</td>
<td>16.71%</td>
<td>88.96%</td>
<td>2.81%</td>
</tr>
<tr>
<td>R3</td>
<td>31.53%</td>
<td>58.99%</td>
<td>47.27%</td>
<td>20.30%</td>
</tr>
<tr>
<td>R4</td>
<td>2.34%</td>
<td>11.32%</td>
<td>60.33%</td>
<td>1.07%</td>
</tr>
<tr>
<td>R5</td>
<td>8.47%</td>
<td>27.68%</td>
<td>40.98%</td>
<td>8.89%</td>
</tr>
<tr>
<td>R6</td>
<td>0.00%</td>
<td>0.00%</td>
<td>7.92%</td>
<td>0.00%</td>
</tr>
</tbody>
</table>

In retrospect, marker redundancy was quite useful to ensure data integrity. As can be seen the occurrence rate for Case 1 in all whip points is much lower than the combined occurrence of Case 2 and Case 3, showing that at any time point t, it is quite unlikely for both markers to be measured by the Qualysis system. When identifying points in the track manager system, there is no practical way to distinguish between marker 1 or marker 2, one can only distinguish if the point is R1, R2, R3 etc. In this sense, Cases 2 and 3 are examples of a similar case where only one marker is visible.

Clearly, there are improvements to be made in this procedure. Firstly, the positioning of the cameras makes a great deal of difference and therefore should be optimized for future whip experiments, particularly for the trajectory swept out by markers further down the length of the whip. However, due to the nature of this data acquisition method, the processing of data is critical to the analysis. Redundancy of measurement points, organization and processing of case occurrences are all integral to the data integrity required for characterization of the whip motion.

4.1.2 Data Structure and Segmentation

For clarity in subsequent sections, the structure and format of the data are detailed in Figure 7 below. Each task, rhythmic and discrete, has a set of data. These data were separated into trials, each trial being a whip attempt to hit the target. For the discrete task, the data included 90 trials and for the rhythmic task, the data included 100 trials. Within each trial there are two main data subsets. The first is the full whip and the second is the arm. The arm data includes position data of the shoulder, elbow, wrist, and hand. While the full whip includes position data for markers R1, R2, ..., R6. However, R6 was discarded for reasons explained above.

The data were initially organized by each individual trial or whip attempt. For each whip attempt (x, y, z, t) were stored in a data set. Using Visual3D software, each trial for each marker was pipelined such that each marker had a data structure of n trials and each trial had (x, y, z, t). Each trial was cut manually in Qualysis Software using a reference position to define initial and final sample of each trial. However, as the subject controlled the speed of each trial, the lengths of the trials were usually different.
Most data analysis was applied horizontally across trials, that is that the analysis was applied to each individual trial and then averages were taken over collections of trials. An alternative approach was to analyze a subset of trials and average across all subsets.

4.1.3 Testing Statistical Significance

To test hypotheses of possible relationships between discrete and rhythmic tasks as well as between neighboring whip markers, one-tailed t-tests were used with an alpha value of 0.05. Statistical significance was calculated on large data sets of average values to test the probability of a relationship between two data sets.

This method was used to estimate the probability that the observed relationships were due to random occurrence. If the probability is calculated to be below the alpha value, the null hypothesis—there is not relationship between data sets—is rejected and the experimental hypothesis accepted [13].

4.2 Characterization of Whip Kinematics

One main objective of both experiments was to characterize the motion of the whip as controlled by the expert whip user. We characterized the kinematic behavior of the whip focusing on reproducibility, performance rating, position and velocity profiles. Discrete and rhythmic executions were analyzed separately in each of the following sections.

4.2.1 Separation and Registration of Whip Trials

In order to analyze position and velocity profiles over many trials, each set of trial data had to be matched to a common reference point and be of the same array length. Figure 8 shows the segmentation and registration process. To compare data across trials, a reference point, $P_m$, the maximum peak value of R1 z-position for each whip trial $n$, and its corresponding time...
index, $I_n$, were used to match trials. Each trial had a length of elements before $I_n$ defined as $L_i$, and a length of elements after $I_n$ defined as $L_f$. The minimum $L_i$ and $L_f$ across all whip trials were chosen as the final matching length for all trials. For each whip trial the start index was calculated as $(I_n - L_i^{\text{min}})$ and the end index was calculated as $(I_n + L_f^{\text{min}})$. In this manner, all whip trials for all markers along the whip were matched at peak point $P$ with equal array length.

![Figure 8: Illustration of registration and segmentation process. (A) raw trials before registration, (B) trials after registration.](image)

4.2.2 Whip Throwing Profile

To further compare discrete and rhythmic tasks, the data was segmented again such that it only included the throwing motion of the whip. The throwing motion was part of both discrete and rhythmic tasks, however, the tasks differed in the rest of each trial. In discrete trials the arm and whip came back to rest at the side of the subject, whereas in rhythmic trials the arm and whip continuously cycled through throwing motions. In order to compare the targeting differences in the two experiments, data was segmented into throwing profiles.

Figure 9 shows a diagram of the throwing profile. A throwing profile was defined to begin when the elbow angle was at a minimum and end at the instant when R5 reached a minimum distance from the target. The minimum distance between R5 and the target is the instant where the success or failure of each trial was determined.
Figure 9: Graphic of throwing profile for rhythmic and discrete trials. The profile begins at the time of minimum elbow angle and ends at the minimum distance between the target and R5 in each trial.

Figure 10 illustrates the profile waveforms of the method above.

Figure 10: Elbow angle and distance between R5 and the target. Black dashed lines designate the beginning and end of the throwing profile.
4.2.3 Whip Velocity Profile

The second characterization of whip kinematics is the average velocity profile for all points along the whip over all trials. In most cases, if data was missing the missing portion would be a group of 5-10 time samples, not just one time sample. Therefore, the velocity slope calculation needed a sufficient range of samples. Given a position value at time point \( i \) and a range of position values from time points \( i-5 \) to \( i+5 \), the velocity is calculated as a slope using neighboring points, per Equation 1, to account for any missing data due to earlier point identification. This method maximized the number of velocity estimates available.

Velocity was calculated using the following equation:

\[
v_i = \frac{\sum (t_i - \bar{t}) \times (x_i - \bar{x})}{\sum (t_i - \bar{t}) \times (t_i - \bar{t})}
\]  

(1)

In this case, \( \bar{t} \) and \( \bar{x} \) are the mean values of time and position in the range.

4.2.4 Whip Performance

Another method to characterize whip motion is through a metric of the subject’s whip performance over many trials. The subject’s whip targeting performance was quantified in terms of the position of all whip points measured relative to the calibrated target position.

In each trial, the minimum distance between each point on the whip and the target was calculated to show a performance metric for the whip motion. The minimum distance calculations were unreliable for the performance of R6 as the marker was not measurable in close proximity to the target itself.

As the integrity of target and R6 data was not adequate to get a direct calculation of performance, target accuracy was extrapolated based on the physical distance between R5 and the tip of the whip cracker. Target accuracy for discrete and rhythmic tasks was calculated using the following equation.

\[
\text{Target Accuracy} = \frac{\text{minimum distance R5-Target}}{\text{physical distance}}
\]  

(2)

Minimum distance between R5 and the target was calculated by averaging the minimum distance over all trials. Physical distance refers to the measured distance between R5 and the tip of the cracker from the experimental setup.

4.3 Characterization of Arm Kinematics

4.3.1 Elbow and Wrist Angle- Para-sagittal Plane

One of the simplest ways to understand the motion of the arm over time is to analyze elbow angle and wrist angle in the para-sagittal plane. Figure 11 shows how elbow and wrist angles were defined. It may not be the case that the arm is planar in the y-z plane, however, this
approximation should be sufficient to understand the transient behavior of the elbow and wrist during whip trials.

For elbow angle calculation
\[
\cos \theta_1 = \frac{y_s - y_e}{\sqrt{(y_s - y_e)^2 + (z_s - z_e)^2}} \tag{3}
\]
\[
\cos \theta_2 = \frac{y_w - y_e}{\sqrt{(y_w - y_e)^2 + (z_w - z_e)^2}} \tag{4}
\]
\[
\theta_{\text{elbow}} = \theta_1 - \theta_2 \tag{5}
\]

For wrist angle calculation
\[
\cos \theta_1 = \frac{y_e - y_w}{\sqrt{(y_e - y_w)^2 + (z_e - z_w)^2}} \tag{6}
\]
\[
\cos \theta_2 = \frac{y_h - y_w}{\sqrt{(y_h - y_w)^2 + (z_h - z_w)^2}} \tag{7}
\]
\[
\theta_{\text{wrist}} = \theta_1 - \theta_2 \tag{8}
\]

Figure 11: Elbow and wrist angle. The elbow angle $\theta_{\text{elbow}}$, is shown in blue and the wrist angle $\theta_{\text{wrist}}$, is shown in orange. The other angles are required by the calculation process below. Blue and orange circles represent the markers on the subject during experimentation.
4.4 Characterization of System Kinematics

4.4.1 Planarity Data Subsets

For all planarity analysis, the data was organized into subsets of ten whip trials, outlined in Table 3. For discrete and rhythmic tasks, there were 9 and 10 calculation subsets respectively. The subsets of data analyzed were identical in both methods.

Table 3: Data subsets used in two methods of planarity analysis. Sets of ten trials were used for each calculation.

<table>
<thead>
<tr>
<th>Method</th>
<th>Trial Subsets</th>
</tr>
</thead>
<tbody>
<tr>
<td>LMS</td>
<td>Discrete 1-10, 11-20, ..., 81-90</td>
</tr>
<tr>
<td></td>
<td>Rhythmic 1-10, 11-20, ..., 91-100</td>
</tr>
<tr>
<td>PCA</td>
<td>Discrete 1-10, 11-20, ..., 81-90</td>
</tr>
<tr>
<td></td>
<td>Rhythmic 1-10, 11-20, ..., 91-100</td>
</tr>
</tbody>
</table>

4.4.2 Planarity – Least Mean Square Plane

In historical work, the whip trajectory has been assumed but not proven as planar. There are three possibilities for planarity: each individual point’s trajectory is confined to its unique plane, or all point’s trajectories belong to the same plane, or there are multiple planes in the system shared by various groups of points along the whip.

To determine planarity, a plane was fit to the throwing profile for each individual whip trial using the Least Mean Square (LMS) method. This Least Square planar fitting method assumes that the z-component of the data is dependent on the x and y-components. Due to this assumption, planarity was also confirmed using a secondary method.

Given the data set: \( \{(x_i, y_i, z_i)\}_{i=1}^n \)

The plane was parameterized as follows

\[
 z = Ax + By + C
\]  

The values of \( A, B \) and \( C \) are determined to minimize the mean square error

Error is calculated by

\[
 E(A, B, C) = \sum_{i=1}^{n} [(Ax_i + By_i + C) - z_i]^2
\]  

This error function is non negative and its minimum, the least square value, occurs at:

\[
 \nabla E = (0,0,0)
\]  

This leads to a system of equations which can be solved to find \( A, B \) and \( C \).
\[(0,0,0) = \nabla E = 2 \sum_{i=1}^{n} [(Ax_i + By_i + C) - z_i](x_i, y_i, 1)\]  

Which leads to the matrix equation

\[
\begin{bmatrix}
\sum_{i=1}^{n} x_i^2 & \sum_{i=1}^{n} x_i y_i & \sum_{i=1}^{n} x_i \\
\sum_{i=1}^{n} x_i y_i & \sum_{i=1}^{n} y_i^2 & \sum_{i=1}^{n} y_i \\
\sum_{i=1}^{n} x_i & \sum_{i=1}^{n} y_i & \sum_{i=1}^{n} 1
\end{bmatrix}
\begin{bmatrix}
A \\
B \\
C
\end{bmatrix}
= 
\begin{bmatrix}
\sum_{i=1}^{n} x_i z_i \\
\sum_{i=1}^{n} y_i z_i \\
\sum_{i=1}^{n} 1
\end{bmatrix}
\]

(13)

Solved by matrix inversion and subsequent multiplication [14].

By construction, \(A, B, C\) are the coefficients of the plane satisfying the LMS error criterion. Furthermore, the LMS error can serve as a figure of merit for planarity of the whip trajectory.

Each error value was normalized by the total distance travelled for individual whip markers. Larger travelled distances are less likely to fit to a plane, therefore one would expect the error value to increase for each marker down the length of the whip. Normalization allows for an unbiased calculation in this regard.

\[
\text{Normalized Error (\%) = } \frac{\text{RMSE}}{\text{distance travelled}}
\]

(14)

The normalized error is thus a percentage value of the total distance travelled. A smaller percentage corresponds to a higher degree of planarity.

**4.4.3 Planarity – Principal Component Analysis**

Principal Component Analysis (PCA) provides insight into the dimensionality of data. In this case, we are interested in whether the whip trajectory data set is approximately confined to a plane or a line.

PCA consists in determining eigenvectors and eigenvalues of the covariance matrix for a data set. The covariance matrix is a multi-dimensional generalization of the concept of variance. For two dimensions covariance is calculated as follows,

\[
cov(x, y) = \frac{\sum_{i=1}^{n}(x_i - \bar{x})(y_i - \bar{y})}{n - 1}
\]

(15)

For our three dimensional case the covariance becomes a real-valued symmetrical matrix of size 3x3 where the diagonal values are the variances in x, y and z directions.

\[
C = \begin{bmatrix}
cov(x, x) & cov(x, y) & cov(x, z) \\
cov(y, x) & cov(y, y) & cov(y, z) \\
cov(z, x) & cov(z, y) & cov(z, z)
\end{bmatrix}
\]

(16)
For a three-dimensional data set, three eigenvector, eigenvalue pairs are then calculated. Each eigenvector is a direction while the eigenvalue translates the amount of data variability in that direction. As the covariance matrix is real-valued, positive-definite and symmetric, the eigenvectors are orthogonal. The eigenvector corresponding to the biggest eigenvalue (first principal component) provides the direction in which the data shows the highest degree of variability. For a data structure to be considered planar, two eigenvalues would be much greater than the third. For a data structure to be considered linear, one eigenvalue would be much greater than the other two eigenvalues. If all eigenvalues have comparable magnitude, there is no underlying data structure and hence reduction of dimensionality of the data set is not possible [15]. Note that, equal eigenvalues are equivalent to an isotropic distribution of the data in space.

In terms of analyzing eigenvectors, standard deviation of principal component direction was calculated for discrete and rhythmic tasks. For each whip marker the average direction was calculated. Similarly, for all whip markers R1, R2, ..., R5, the average direction was calculated. The angles between the five whip marker direction vectors and the average direction of all whip markers were calculated.

\[
\vec{v} = [x, y, z]_{R1} \\
\vec{w} = [x, y, z]_{R1,R2,...,R5} \\
\theta = \cos^{-1} \frac{\vec{v} \cdot \vec{w}}{||\vec{v}|| ||\vec{w}||}
\]

Standard deviation of each principal component direction was thus the standard deviation of the five calculated angles for discrete and rhythmic tasks.

4.4.4 Describing a Plane in Spherical Coordinates

To compare results from LMS and PCA, the planes were represented in spherical coordinates. By defining the normal of the plane from a (0,0,0) origin, the plane's orientation can be described by what we will define as the attitude, \((\varphi, \theta)\), see Figure 12. \(\varphi\), is generally designated as the azimuthal angle, and \(\theta\) as the polar angle.
Figure 12: Spherical coordinates showing \( \varphi, \theta \) and \( r \). \( \theta \) is defined as the polar angle and \( \varphi \) is the azimuth angle. We will refer to \( (\varphi, \theta) \) as the attitude of the plane. [16].

The para-sagittal plane has an attitude of \( (\varphi, \theta) = (0, 90) \) degrees. Any deviation from these two angles shows a deviation from the para-sagittal plane.

4.4.5 Position vs. Velocity Phase Profile

If the kinematic behavior arises from a state-determined system, it may be represented as \( \dot{q} = \Phi(q) \) where \( q \) is a vector. For a second-order system, a phase plot of \( \dot{q} \) vs. \( q \) displays the system dynamic equations. A position versus velocity plot is similar to a phase plot; a geometric representation of a dynamical system in state space. The use of position versus velocity profiles provides a different way to classify or represent the system.

Using the velocity calculation from above and position data, a position versus velocity plot is easily generated for each marker. The data set of position and velocity is six dimensional, and for convenience we look at \( x, y \) and \( z \) directions separately.

Each marker had a triplet of position vs. velocity curves. However, not all markers moved over the same range of values. To facilitate correlation between markers, it was necessary to normalize the curves based on mean and standard deviation to effectively compare the geometrical shapes. Normalized values were calculated with the following equation:

\[
X_{\text{norm}} = \frac{(x_l - \bar{x})}{\sigma_x}
\]

(20)

This equation was applied to \( x, y \) and \( z \) directions for both position and velocity.

To calculate a measure of variance of each phase profile, a phase thickness was calculated. Each loop was translated to the origin by subtracting the mean of the position-
velocity data set from each point. Each point was converted into polar coordinates using the following equations.

\[ r = \sqrt{p^2 + v^2} \]  \hspace{1cm} (21)
\[ \theta = \tan^{-1}\left(\frac{v}{p}\right) \]  \hspace{1cm} (22)

Where \( p \) is position data and \( v \) is velocity data.

There were 160 thickness calculations, one for every two degrees around the unit circle. Thickness was calculated as follows:

\[ \text{thickness} = r(\theta)_{\text{max}} - r(\theta)_{\text{min}} \]  \hspace{1cm} (23)

Average and standard deviation of phase profile thickness were calculated from this data set.

5. Results

The main results of this study are as follows. The position and velocity profiles are similar in shape between the rhythmic and discrete cases, confirming the existence of a wave propagating down the whip. In both cases the subject demonstrated almost perfect targeting accuracy. The elbow and wrist angles are consistent throw to throw. However, the discrete and rhythmic cases exhibit distinct waveforms. The whip trajectory is reliably confined to a plane. The position versus velocity phase profiles are different between rhythmic and discrete cases, with the rhythmic case exhibiting lower variation than the discrete case.

5.1 Whip Position and Velocity Throwing Profiles

System axes were defined in Figure 3 for reference. Figure 13 shows the position profiles for each of the five markers R1, R2, ..., R5 along the whip. Let us define the thickness of each position or velocity profile curve as the average standard deviation over the set of trials of every time sample. The thickness of each of these curves represents the standard deviation about the average position profile of each of the markers and demonstrates the consistency of these profiles from throw to throw. Initial and final samples are determined by the bounding method described in section 4.2.2.
Table 4 provides the overall thickness for the discrete and rhythmic tasks. This thickness and overall measure of the reproducibility of the profiles is defined as the average over all markers R1, R2, ..., R5 of their individual profile thickness. The thickness of rhythmic task profiles is significantly smaller. This result is statistically significant at the 5% significance level.

**Table 4:** Average thickness of position profiles in discrete and rhythmic whip tasks.

<table>
<thead>
<tr>
<th></th>
<th>X Direction (m)</th>
<th>Y Direction (m)</th>
<th>Z Direction (m)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Discrete</td>
<td>0.083 ± 0.033</td>
<td>0.143 ± 0.093</td>
<td>0.152 ± 0.121</td>
</tr>
<tr>
<td>Rhythmic</td>
<td>0.049 ± 0.018</td>
<td>0.131 ± 0.055</td>
<td>0.050 ± 0.021</td>
</tr>
</tbody>
</table>

**Figure 13:** Position throwing profile for all whip markers in discrete and rhythmic tasks. Each color corresponds to a different whip marker.
Figure 14 below shows the same profiles for velocity over time. In both profiles there is a clear wave propagation with velocity amplitude increasing progressively from R1 to R5 implying an acceleration of whip markers down the length of the whip.

Figure 14: Velocity throwing profile for all whip markers in discrete and rhythmic tasks. Each color corresponds to a different whip marker. All velocity profiles are relatively smooth with the exception of R4\(^1\), in green.

Once again the thickness was calculated for each task shown in Table 5. As compared to position profiles, the velocity profiles show a much higher thickness. This is understandable since velocity is the derivative of position. These results in Table 5 show that the reproducibility of velocity profiles is not statistically different between rhythmic and discrete tasks.

\(^{1}\) In discrete trials, the R4 signal, in green, was not as reliable due to the high occurrence rate of no identifiable data. Resulting velocity signals were therefore not as smooth as whip points that were more easily identified in data processing.
Table 5: Average thickness of velocity profiles in discrete and rhythmic whip tasks.

<table>
<thead>
<tr>
<th></th>
<th>X Direction (m)</th>
<th>Y Direction (m)</th>
<th>Z Direction (m)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Discrete</td>
<td>0.473 ± 0.366</td>
<td>1.307 ± 1.246</td>
<td>0.734 ± 0.665</td>
</tr>
<tr>
<td>Rhythmic</td>
<td>0.469 ± 0.204</td>
<td>1.977 ± 1.273</td>
<td>0.909 ± 0.523</td>
</tr>
</tbody>
</table>

5.2 Target Accuracy

Figure 15 shows the minimum distance from the target for whip points R1, R2, ..., R5 for all trials. Each whip marker is characterized by a cluster of points over all trials which is essentially located in the y-z plane (see axes scale). The spread of these clusters between one another is consistent with the physical distance between markers as measured in the experimental setup.

Minimum distance from Target- Discrete

![Graph showing minimum distance from target in discrete task](image)

Figure 15: Minimum distance between target and whip points in discrete task. Each color corresponds to one whip marker and the clusters show the minimum distance over all discrete trials. The data is essentially located in the y-z plane, take note of the x axis.

Figure 16 below shows the minimum distance between each whip point and the target over all rhythmic task trials. It would appear that the expert subject is equally capable of hitting the target in discrete and rhythmic tasks.
Figure 16: Minimum distance between target and whip points in rhythmic task. Each color corresponds to one whip marker and the clusters show the minimum distance over all discrete trials. The data is essentially located in the y-z plane, take note of the x axis.

Figure 17 below shows the average values and standard deviation for minimum distance over all trials.

Figure 17: Mean and standard deviation of minimum distance between target and whip points. (A) shows these values for discrete tasks and (B) for rhythmic tasks. Error bars show the range of standard deviation for each whip marker.
Table 6 provides the numerical values of the data displayed in Figure 17. The third row shows the physical distance between markers as measured in the experimental setup. As one would expect the physical values are greater than the average values because the whip never reaches full tension during whip targeting tasks.

<table>
<thead>
<tr>
<th></th>
<th>R1 (cm)</th>
<th>R2 (cm)</th>
<th>R3 (cm)</th>
<th>R4 (cm)</th>
<th>R5 (cm)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Discrete</td>
<td>172</td>
<td>153</td>
<td>128</td>
<td>102</td>
<td>71</td>
</tr>
<tr>
<td>Rhythmic</td>
<td>165</td>
<td>148</td>
<td>126</td>
<td>102</td>
<td>72</td>
</tr>
<tr>
<td>Physical</td>
<td>191</td>
<td>167</td>
<td>140</td>
<td>111</td>
<td>78</td>
</tr>
</tbody>
</table>

As the integrity of target and R6 data was not adequate to get a direct calculation of performance, target accuracy was extrapolated based on the physical distance between R5 and the tip of the whip cracker. R6 was 33 cm from R5 and the tip of the cracker was 45 cm from R6. Per the definition of target accuracy in section 4.2.4, the subject achieved an accuracy of 90.12% and 92.53% in discrete and rhythmic tasks, respectively. The difference between discrete and rhythmic tasks in target accuracy was not statistically significant at the 5% significance level, showing that the type of whip technique used does not affect the targeting accuracy of the expert subject.

5.3 Elbow and Wrist Angle

Figure 18 below shows the elbow and wrist angle in succession for three randomly non-contiguous chosen trials. The waveform is highly reproducible, and the wrist and elbow angle have troughs and peaks at similar time samples implying synchronicity of the two joint angles.
Figure 18: Elbow and wrist angle of three trials in discrete task. The blue corresponds to the elbow angle and the orange corresponds to the wrist angle. The black dashed lines separate individual trials or throws.

Figure 19 shows the elbow and wrist angle over multiple cycles during the rhythmic task. These waveforms are clearly periodic.

Figure 19: Elbow and wrist angle of three trials in rhythmic task. The blue corresponds to the elbow angle and the orange corresponds to the wrist angle. The black dashed lines separate individual trials or throws.
Both rhythmic and discrete tasks exhibit a high degree of reproducibility from throw to throw. In contrast, the elbow angle and wrist angles have a smaller range of motion in the rhythmic case.

5.4 Planarity

Historical work involving whip dynamics assumes that whip motion remains planar and more specifically remains in the para-sagittal plane [2,3]. Least mean square plane fitting (LMS) and principal component analysis (PCA) confirmed planarity of whip trajectory. However, the inscribed plane deviates from the para-sagittal plane.

5.4.1 Characterization of Planarity using Least Mean Square and Principal Component Analysis

Both LMS and PCA methods confirm planarity in discrete and rhythmic whip targeting tasks. These two techniques corroborate each other. Figure 20 shows the attitude (φ, θ) for the planes estimated using the LMS and PCA methods.

![Comparison of LMS and PCA Normals in Spherical Coordinates](chart.png)

**Figure 20:** Comparison of LMS and PCA φ and θ values. The blues correspond to φ values in both methods and the green and yellow correspond to θ values.

Table 7 shows a final comparison of whip planarity. In this table the values for full whip analysis (all markers R1, R2, ..., R5) are used to describe the experimental data concisely. It is clear that the whip’s motion is not fully inscribed in the para-sagittal plane and instead in a plane with attitude (φ, θ) slightly tilted about the y-z plane. The small standard deviations shown in the table confirm a high degree of planarity.
Table 7: Full whip (R1, R2, ..., R5) planarity comparison between discrete and rhythmic tasks and comparison of LMS, PCA and para-sagittal planes.

<table>
<thead>
<tr>
<th>Plane</th>
<th>$\phi$ (degrees)</th>
<th>$\theta$ (degrees)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Para-sagittal</td>
<td>0</td>
<td>90</td>
</tr>
<tr>
<td>Discrete, LMS</td>
<td>19.16 $\pm$ 0.47</td>
<td>104.97 $\pm$ 3.78</td>
</tr>
<tr>
<td>Discrete, PCA</td>
<td>17.08 $\pm$ 2.19</td>
<td>97.36 $\pm$ 3.25</td>
</tr>
<tr>
<td>Rhythmic, LMS</td>
<td>11.83 $\pm$ 0.54</td>
<td>105.30 $\pm$ 3.40</td>
</tr>
<tr>
<td>Rhythmic, PCA</td>
<td>12.51 $\pm$ 2.09</td>
<td>103.34 $\pm$ 4.69</td>
</tr>
</tbody>
</table>

5.4.2 Least Mean Square Plane

The Least Mean Square analysis provides a figure of merit by way of a root mean square error. The mean and standard deviation of these error values (refer to Table 3 for trial subsets) were normalized by the distance travelled for each individual whip marker. Figure 21 below shows the normalized error value for each whip marker, as well as all whip markers R1, R2, ..., R5 at once.

The rhythmic task shows a higher degree of planarity by a factor of about 2. The differences in root mean squared error between neighboring whip markers was not found to be statistically significant. However, the difference between rhythmic and discrete tasks was found to be statistically significant at the 5% significance level.
Figure 21: Normalized average root mean square error of LMS plane fit for discrete and rhythmic tasks. Error was normalized by the distance travelled by each whip marker. The error bars are the standard deviation of the mean error for each whip marker.

5.4.3 Principal Component Analysis

PCA offers a detailed look into the shape of whip marker trajectories that is not shown through the LMS method. Figure 22 shows normalized eigenvalues of the three principal components for individual markers, shoulder to R5. The third eigenvalue in the rhythmic case is essentially zero for wrist, hand and whip markers, not quite for the discrete case. It follows that rhythmic tasks were more planar than discrete. In that case, the value of variance accounted for by the first principal component is 80-90% of the total variance, implying a unidimensional trajectory.
Table 8 shows the numerical values of Figure 22 and shows the relative contribution to total variance from each principal component. A smaller percentage of variance in principal component three shows a higher degree of planarity.

Table 8: Relative contribution from each principal component. Values are in percent of total variance for each marker.

<table>
<thead>
<tr>
<th></th>
<th>Variance PC1 (%)</th>
<th>Variance PC2 (%)</th>
<th>Variance PC3 (%)</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>Discrete</td>
<td>Rhythmic</td>
<td>Discrete</td>
</tr>
<tr>
<td>Shoulder</td>
<td>85.3</td>
<td>59.0</td>
<td>13.7</td>
</tr>
<tr>
<td>Elbow</td>
<td>88.8</td>
<td>86.8</td>
<td>10.0</td>
</tr>
<tr>
<td>Wrist</td>
<td>60.9</td>
<td>88.8</td>
<td>34.9</td>
</tr>
<tr>
<td>Hand</td>
<td>60.9</td>
<td>93.7</td>
<td>35.1</td>
</tr>
<tr>
<td>R1</td>
<td>60.0</td>
<td>93.2</td>
<td>37.2</td>
</tr>
<tr>
<td>R2</td>
<td>57.0</td>
<td>97.8</td>
<td>40.2</td>
</tr>
<tr>
<td>R3</td>
<td>58.4</td>
<td>92.6</td>
<td>38.9</td>
</tr>
<tr>
<td>R4</td>
<td>81.6</td>
<td>88.2</td>
<td>18.0</td>
</tr>
<tr>
<td>R5</td>
<td>76.9</td>
<td>80.5</td>
<td>21.6</td>
</tr>
</tbody>
</table>

Figure 23 below shows the average standard deviation in direction of principal components over all whip trials. If a system is planar one would expect only the standard deviation of the direction of the third principal component to be significantly smaller than the first two. In discrete tasks this behavior is clear, with the variation of direction on the order of 30 to 40 degrees. However, rhythmic tasks do not exhibit the same behavior. Instead there is very little variation in direction of the first and second principal component. This further confirms the result that rhythmic tasks show more unidimensional behavior than discrete tasks.
Figure 23: Angle standard deviation of principal component direction from mean direction of all whip points R1, R2, ..., R5.

Table 9 shows the average eigenvectors for all three principal components and all whip markers R1, R2, ..., R5. From Figure 23 above, the principal components of rhythmic tasks approximately stay in the same direction from trial to trial. The average eigenvector of principal component one in rhythmic tasks is very close to the y direction unit vector which is, as expected, the direction of the target.

Table 9: Average eigenvector for each principal component for whip markers R1, R2, ..., R5 in discrete and rhythmic tasks.

<table>
<thead>
<tr>
<th></th>
<th>PC 1</th>
<th>PC 2</th>
<th>PC 3</th>
</tr>
</thead>
<tbody>
<tr>
<td>Discrete</td>
<td>[-0.24, 0.82, -0.07]</td>
<td>[-0.17, 0.17, 0.84]</td>
<td>[0.95, 0.29, 0.12]</td>
</tr>
<tr>
<td>Rhythmic</td>
<td>[-0.16, 0.95, -0.22]</td>
<td>[-0.26, 0.20, 0.90]</td>
<td>[0.95, 0.21, 0.23]</td>
</tr>
</tbody>
</table>

5.5 Position vs. Velocity Phase Profile

Position and velocity data were used to create a phase profile for each individual marker from the shoulder to R5. From there, normalized phase plots were calculated and correlated between neighboring points.

5.5.1 Decomposed Phase Profile

For each task there are a series of three phase profiles in x, y and z directions. Figure 24 shows the original phase profile data sets for all markers in both discrete and rhythmic tasks. In terms of shape, both discrete and rhythmic task phase profiles show similar geometric shapes in x, y and z directions. In discrete tasks there is an extra loop of data at the start of the curve as that is the data that corresponds to setting the whip to rest, a motion that is not present in the rhythmic
trials. These curves begin from the first marker on the whip, R1, and augment in size down the length of the whip to R5.

Figure 24: Position and velocity phase profiles for discrete and rhythmic tasks.

Of course, the motion of the arm and the motion of the whip are relative to the distance that each individual point travels in one trial. For that reason, Figure 25 below shows the normalized phase profiles of each marker from shoulder to R5. Let us define a phase thickness as the width of the phase profile. The thickness of the curve’s outline is a feature that corresponds to the reproducibility of the task.

Furthermore, there is a distinct difference between the shoulder phase profile in both tasks. In discrete tasks, particularly in the x and y directions, there is a loop similar to the ones exhibited in the subsequent whip markers. However, in rhythmic tasks, there is no defined loop in the phase profile. This implies that a different motion strategy is in use between both tasks.
**Figure 25:** Normalized position and velocity phase profiles for discrete and rhythmic tasks.

Figure 26 below shows the variance or *thickness* of the normalized phase profiles. The difference between the phase *thickness* or variance between tasks is statistically significant at the 5% significance level. However, there is not a statistically significant difference in variance between neighboring points within each task. The highest contrast between both cases is in the y direction.
6. Discussion

The subject was able to expertly perform both discrete and rhythmic whip targeting tasks with a targeting accuracy of 90.1% and 92.5%, respectively.

The position and velocity profiles of the whip markers support the existence of a wave propagating down the length of the whip. It is to be noted that the observed acceleration of whip markers down the length of the whip in both discrete and rhythmic tasks had been confirmed in prior work [2,3].

The whip trajectory in both discrete and rhythmic cases is confined to a plane. The data further show that this plane, with an average attitude \((\varphi, \theta) = (15, 102)\) degrees, is not exactly the para-sagittal plane. The whip trajectory of the discrete case exhibits significant transversal range of motion. In the rhythmic case, however, both the second and third principal components are small in absolute value. This implies an almost unidimensional trajectory with a much smaller transversal component.

In general, rhythmic performance appears to be less variable than discrete performance. This is supported by the higher reproducibility of position, velocity, and phase profiles, as well as the higher degree of planarity. All differences in variance between discrete and rhythmic tasks were statistically significant at the 5% significance level.

The differences between discrete and rhythmic tasks may be due to a difference in initial conditions and constraints. In discrete tasks, each whip attempt (cycle) involves a unique set of initial conditions, for example the shape of the whip as it landed or the position of the arm as it ended up resting after the previous trial. However, in rhythmic tasks the subject has to account for initial conditions and constraints only once, on the first attempt (cycle); there is no discrete transition thereafter, rather a smooth kinematic continuity from cycle to cycle requiring a lesser degree of control at the onset of the throw. By virtue of this continuity, since the whip does not come to rest between cycles, rhythmic tasks require significantly less impulse energy to initiate the throw cycle to cycle than discrete tasks do.
We have identified five key characteristics manifesting expert control of the bullwhip in targeting tasks: target accuracy, reproducibility of position and velocity profiles, planarity, reproducibility of elbow and wrist angle, and reproducibility of phase profiles. Both accuracy and reproducibility suggest a high degree of control. High target accuracy is its corollary.

From the perspective of human neural control, the elbow and wrist angle waveforms are core signatures. The repeatability of these waveforms in both discrete and rhythmic cases (Fig. 17 and 18, respectively) may be a necessary condition for the remarkable reproducibility and control of the whip itself. In this case, the waveforms of elbow and wrist angles imply a highly calibrated system or model that interacts with the whip such that target accuracy and system reproducibility are made possible.

This supports the theory that humans run ‘internal models’ to control complex dynamic objects. Both the elbow and wrist angle waveforms and the arm phase profile characteristics imply a very detailed internal model that ensures expert control of the object. In simplest terms, the only input - kinematic and dynamic - to this system is from the subject himself. Therefore, it would follow that the specific waveforms and features of the arm kinematics are precise manifestations of an internal model at play.

7. Further Work

If indeed an internal model exists in the control of complex dynamic objects, the next step is to identify and fully define this model. To investigate a potential internal model, the elbow and wrist angle waveforms could be reproduced using a robot or simple mechanical device. If the behavior of the whip shows the features of control as demonstrated by our expert subject (reproducibility, planarity and target accuracy), one could argue that the internal control model has been confirmed. However, if these features are not present it would suggest that there is another dimension to this internal model yet to be identified, most probably the forces at work during expert manipulation.

Indeed, while the kinematics of the subject’s arm and the bullwhip in discrete and rhythmic tasks have been well defined, the dynamics of the system have not been considered. To continue examining the proposed theory of human dynamic primitives and how it may be involved in control strategies of complex dynamic objects, one would need to investigate the forces at play in the system, particularly the forces of interaction between the hand of the subject and the whip.

Once the model has been defined for the whip, it would be interesting to investigate whether similar models apply to other complex objects. Would the arm kinematics and dynamics be similar with other complex dynamic tools? Furthermore, does a skill with one complex tool allow for better control of other complex tools as compared to a complete novice? Through similar task design and more specific recruitment, complex tool control strategies and possible internal models involved can be further investigated.
References

Appendices

Appendix A: Correlation of Phase Profile in Neighboring Points

The following data analysis and results were also applied to both discrete and rhythmic tasks. A histogram was created from phase profiles by counting the number of points in each grid square of the position versus velocity plane. The frequency of this occurrence was assigned a color density that was consistent across all markers. Once histograms and color bitmaps were created for each marker in all three directions, the histograms of neighboring markers were cross-correlated in Matlab. This function output a correlation coefficient, $r$, that was calculated using the following equation:

\[
    r = \frac{\sum_{m} \sum_{n} (A_{mn} - \bar{A})(B_{mn} - \bar{B})}{\sqrt{\left(\sum_{m} \sum_{n} (A_{mn} - \bar{A})^2\right) \left(\sum_{m} \sum_{n} (B_{mn} - \bar{B})^2\right)}}
\]  

(24)

Where $A$ and $B$ are the $m \times n$ sized matrices of the neighboring marker histograms. Figure A.1 below shows an example of the histograms and bitmaps created in this process.
Figure A.1: Example of histogram and recurrence plot for marker R2 in the rhythmic task.
Figure B.2 below shows the correlation values between neighboring marker’s normalized phase profiles in x, y and z directions.

Figure A.2: Correlation coefficients of position and velocity plots of neighboring points in x, y and z directions.
In general, these results require further investigation to formulate a stronger conclusion that could be applied to the study of human control of complex objects. However, a few observations and potential conjectures have been made in the following text.

Beginning with looking at the z-direction, rhythmic and discrete tasks seem to have a similar pattern of correlation from wrist to R5. This pattern shows a high correlation between wrist and hand markers with a trough in correlation between hand and R1. The correlation value then peaks again between R1 and R2 to then linearly decreases on the remainder of the correlation values.

Though it is not clear what exactly the correlation value may imply between the hand and R1, a potential comparison may be seen in research on percussionists, most specifically passive impedance control to reach higher bandwidth motions. Hajian shows that by allowing a drumstick to bounce loosely in a simple robot’s grasp, the speed of possible motions increases [17]. Applying this to the whip, perhaps how tightly one holds the whip affects the behavior of the whip itself. If this were true, it could suggest, much like expert percussionist, expert whip-crackers hold the whip less tightly when controlling the whip.

In the y-direction, however, rhythmic and discrete tasks have very different correlation features. Discrete tasks show very little or negative correlation between points from the hand onward to the end of the whip, whereas rhythmic tasks show an almost constant correlation value from the wrist on to the end of the whip. Again we are confronted by the differences between discrete and rhythmic tasks, another important takeaway from this project.