

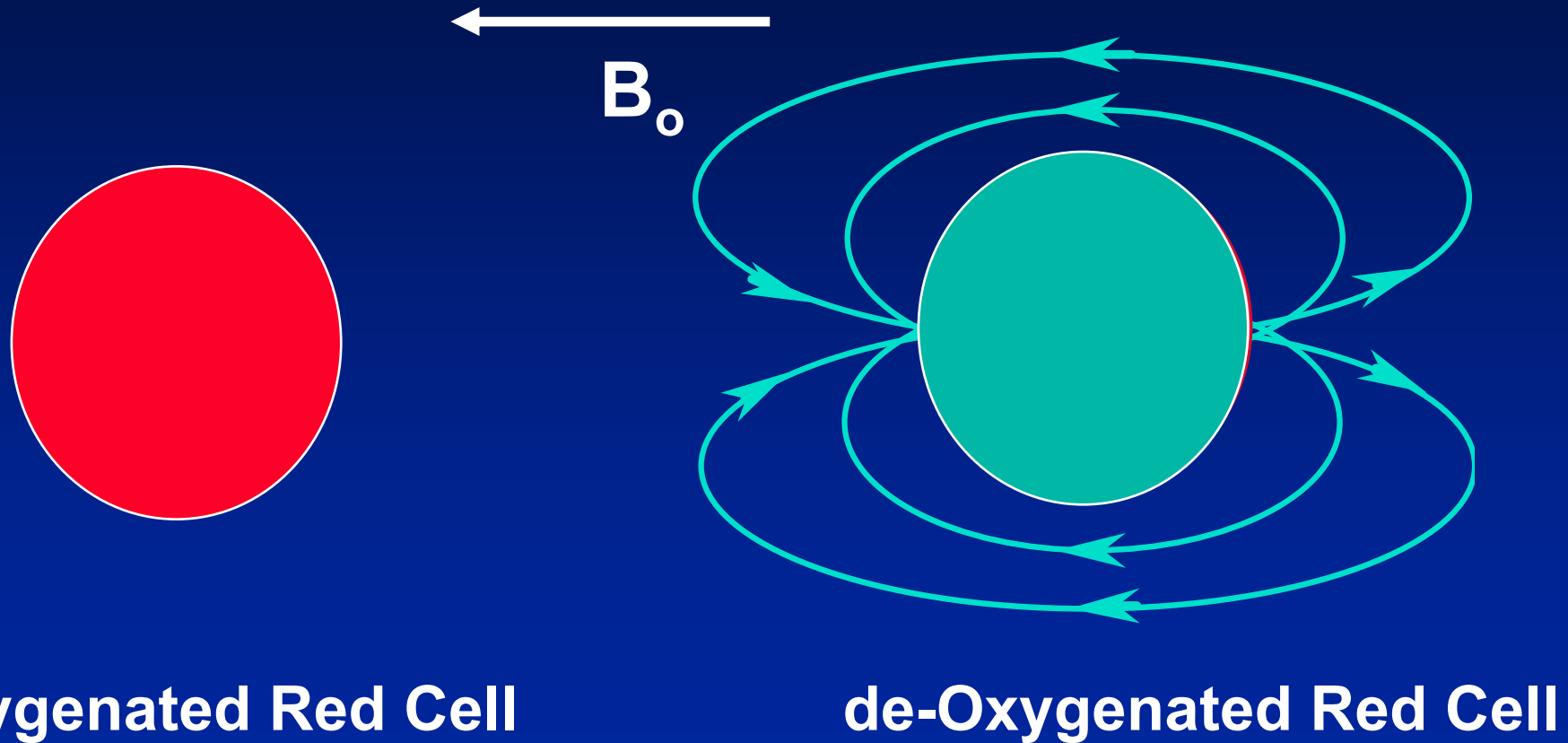
# Noise in fMRI

**MGH-NMR Center**

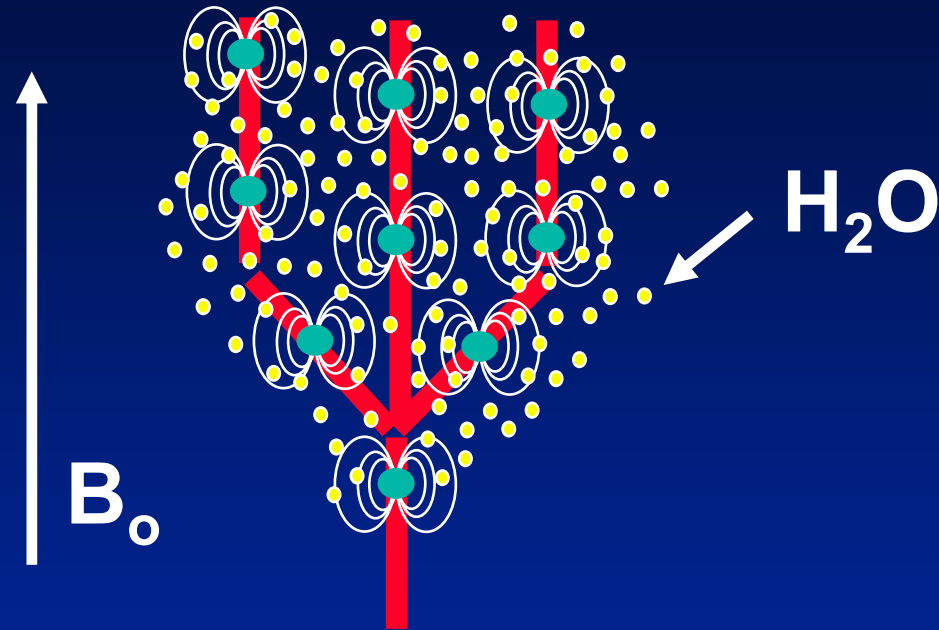
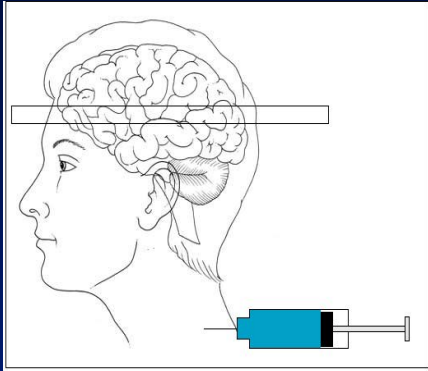
**1) Brief review of BOLD**

**2) Noise sources in the  
BOLD experiment**

# Field Homogeneity and Oxygen State



# Addition of paramagnetic compound to blood



Signal from water is dephased by local fields ( $T_2^*$  shortens), S goes down on EPI  
**Magnetic stuff**  $\uparrow$  **MR signal**  $\downarrow$

# Basis of BOLD fMRI

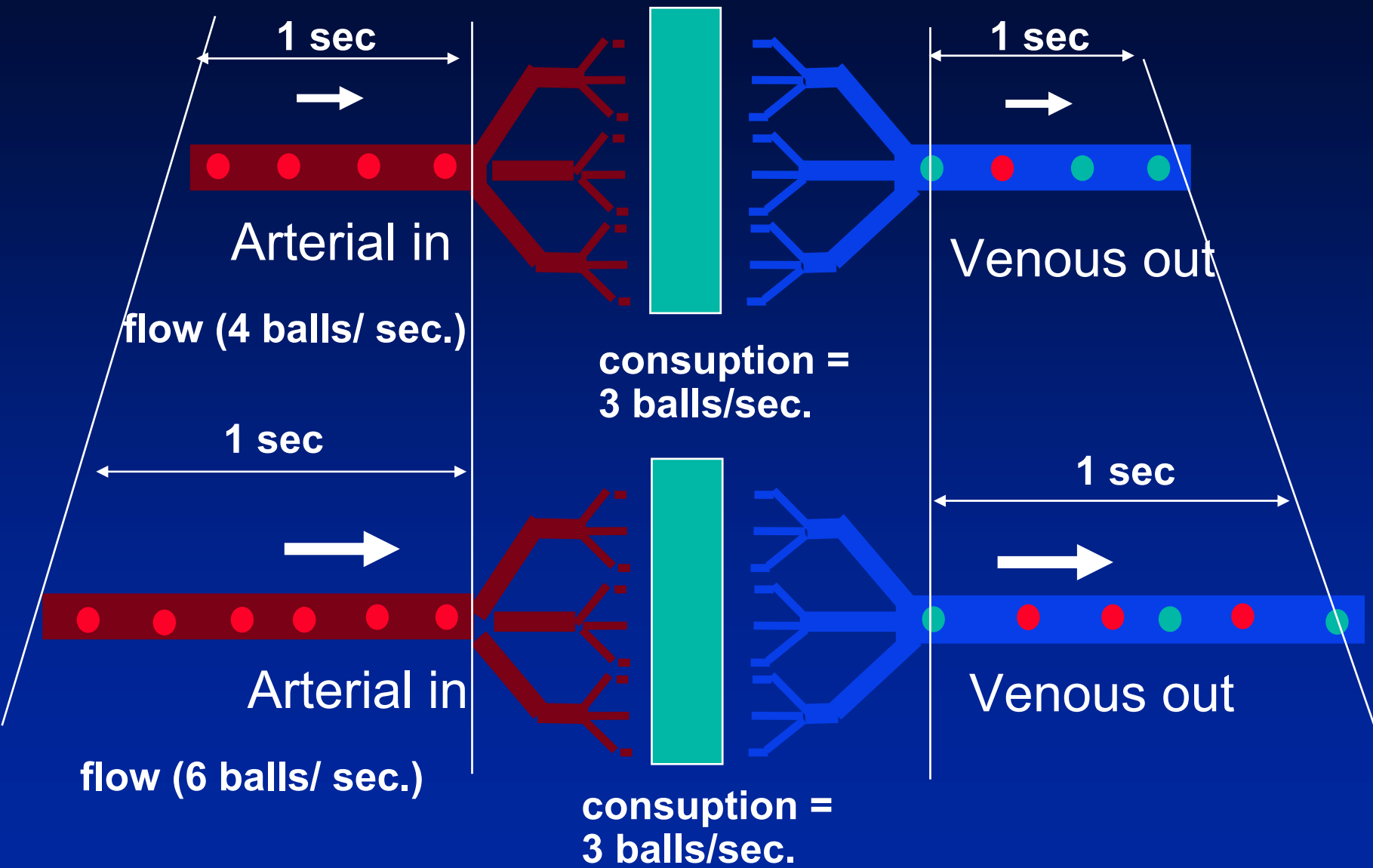
During activation...

Flow  $\uparrow$  but  $\text{CMRO}_2$  only goes up a little

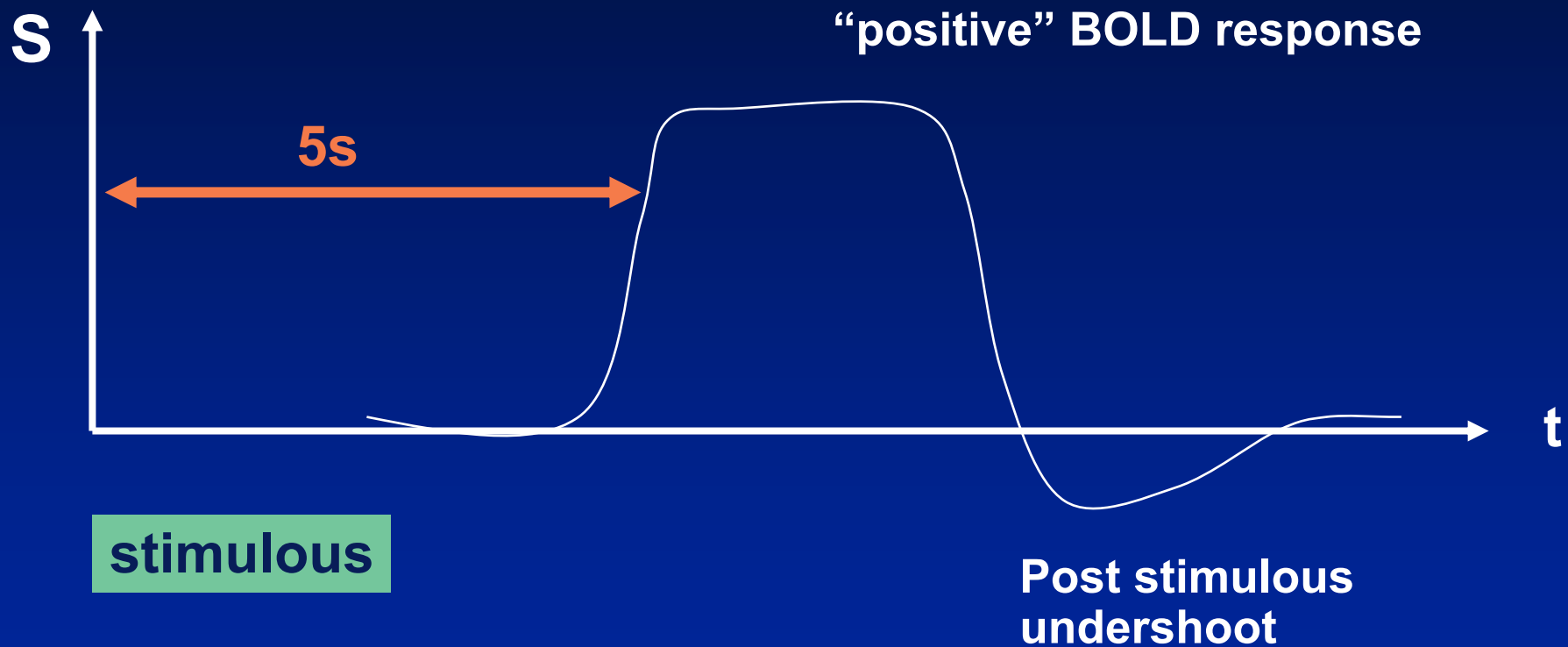
DeOxy Hb in veins  $\downarrow$

As magnetic stuff  $\downarrow$  T2\* weighted MR signal  $\uparrow$

# decrease in deoxygenated red cell concentration



# Time response of BOLD



# Important BOLD considerations

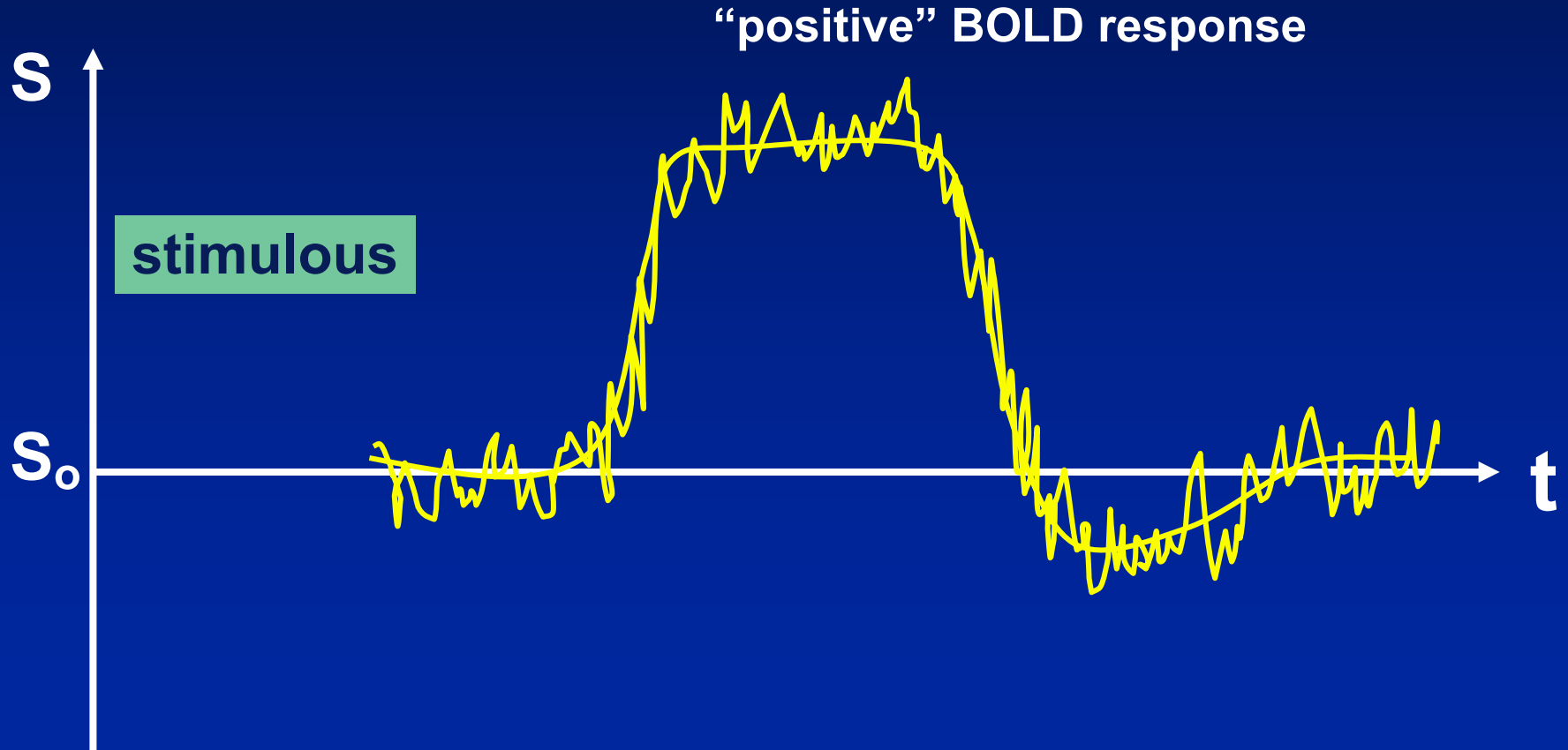
- In 50ms, water diffuses 25 $\mu$ m on average  
thus moves  $\sim$ 4x diameter of capillary...
- Water diffuses readily in and out of RBC.
- Water does not exchange between vascular and tissue pools.
- 20x more water in tissue space, nonetheless, 2/3 of BOLD signal is intravascular at 1.5T.



# Important BOLD considerations

- Diffusion in and around RBC shortens intravascular T2 esp. at high field making intravascular water contribute less to spin echo.
- B-W model shows that spin echo (T2) is more localized to small vessels than grad echo (T2\*).

# BOLD effect modulates signal where does the noise come from?



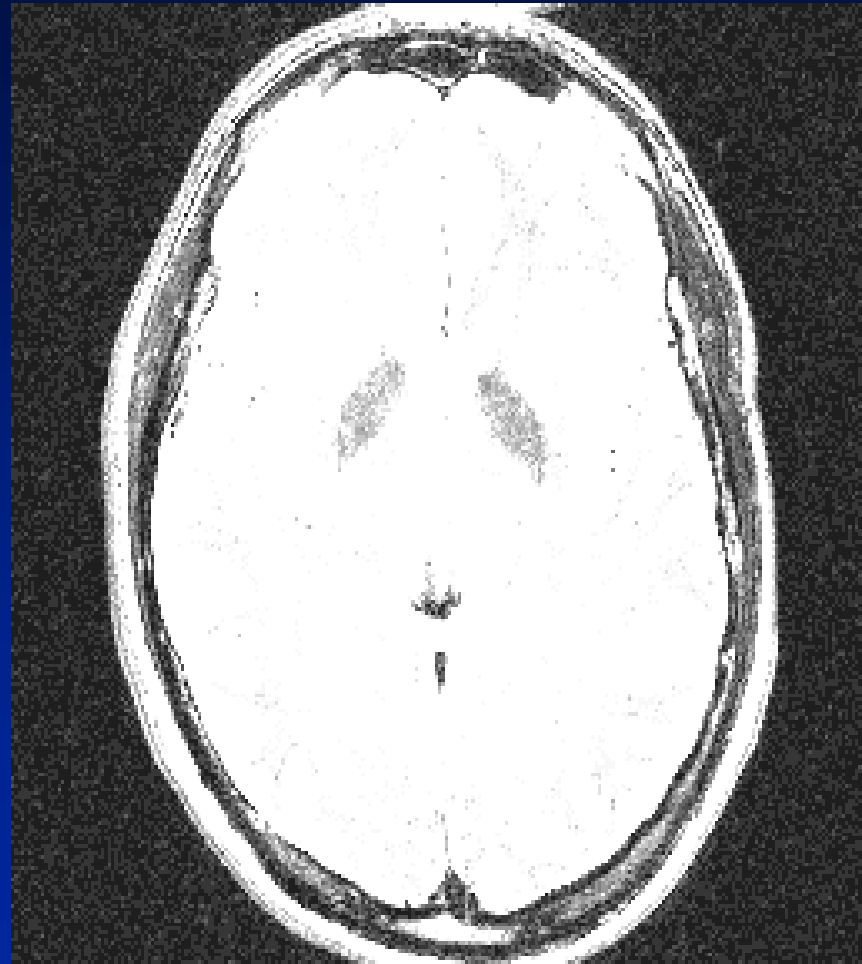
# Thermal Noise in MRI

Thermal white noise in a resistor:

$$P_{\text{noise}} = 4kTRB$$

Noise is flat across freq and is not encoded by gradients.

>> noise voltage due to resistive losses is Gaussian, temporally and spatially uncorrelated.



# Thermal Noise in MRI

Resistive losses from

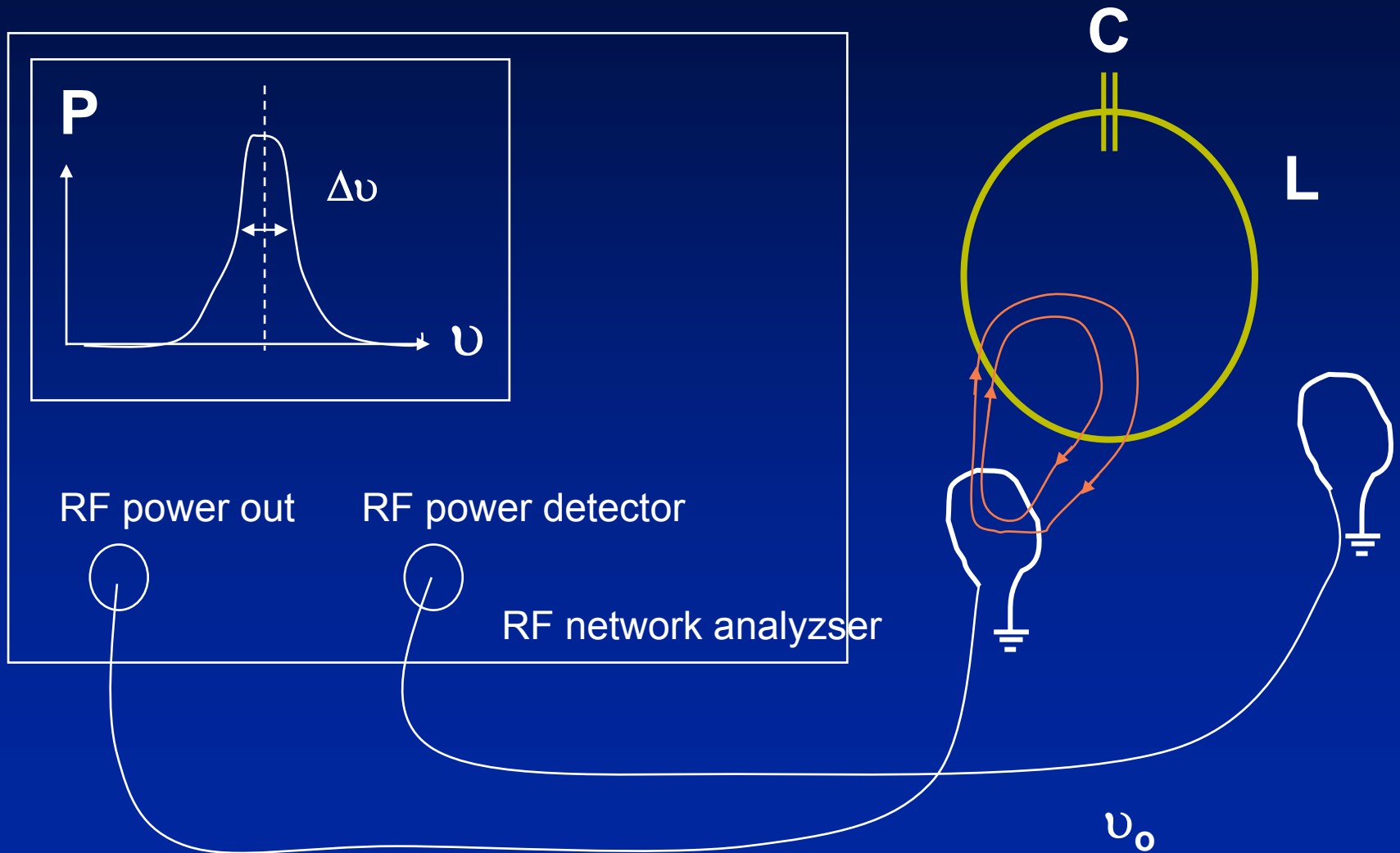
a) wires and components in coil.

b) Driving ionic RF eddy currents in body.

Body losses are generally 5x larger (or more)...

$P_{\text{noise}} \propto R$  means noise scales with volume  
of tissue in coil

# Measuring loss in a coil



# Thermal Noise in MRI

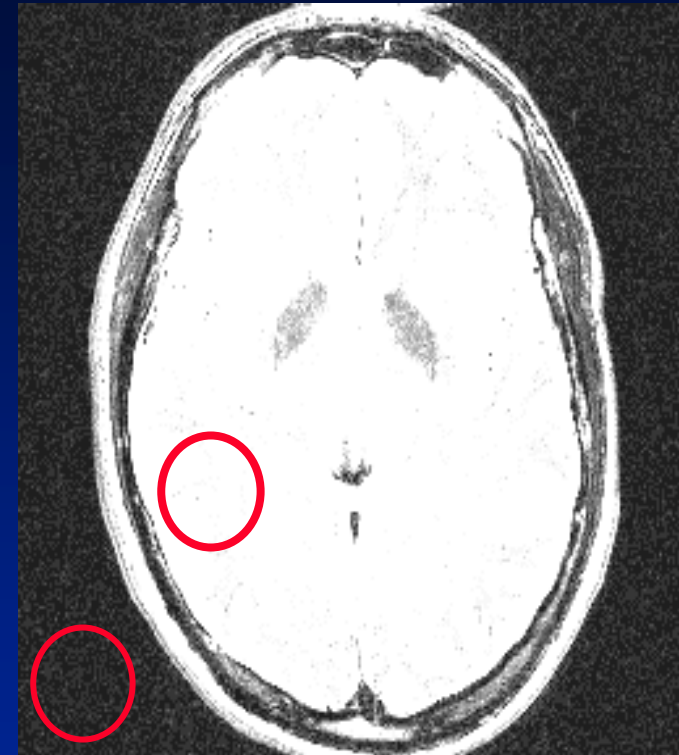
$$P_{\text{noise}} = 4k T R B$$

Bandwidth is set by filter determined by Nyquist condition:

$$B \propto 1 / \text{dwell time}$$

Temporal uncorrelated means:

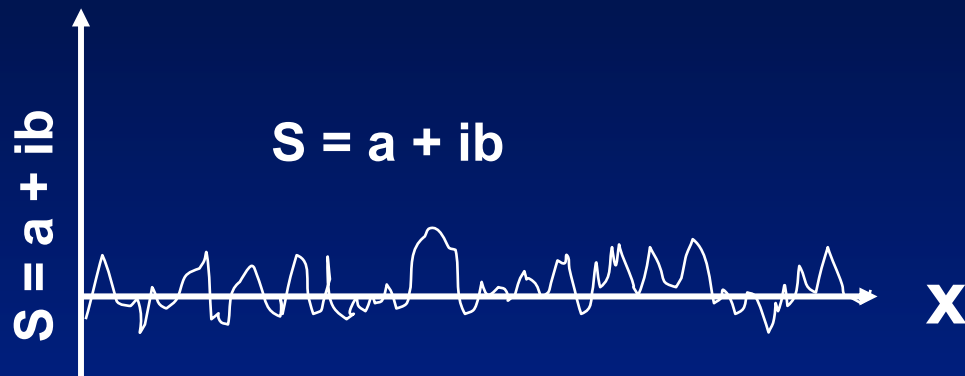
$$\text{SNR} = 1 / \text{SQRT}(\text{averaging time})$$



$$\text{SNR} = \frac{\text{mean}(\text{SignalROI})}{\sigma(\text{noiseROI})}$$

*(Quick and dirty method)*

# Noise in the magnitude image is no longer Gaussian



Gaussian prob. distribution

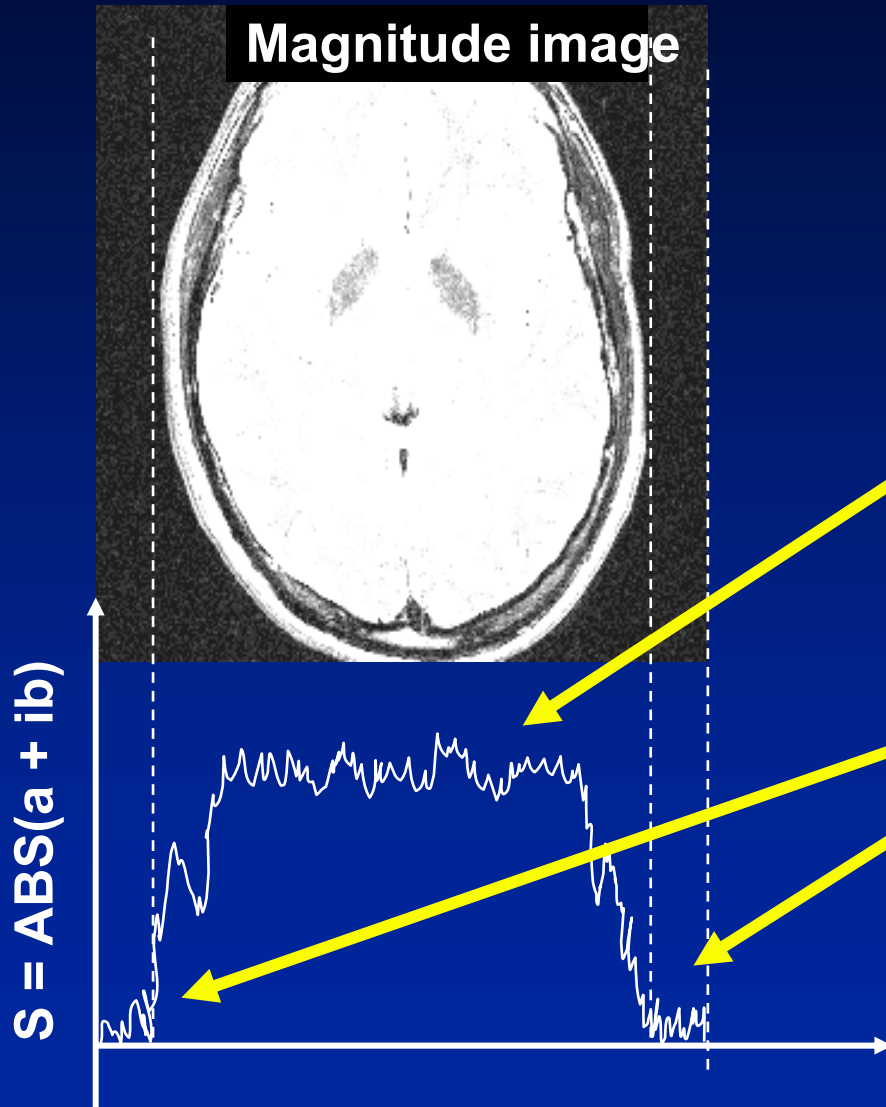
$$f(x) = \frac{1}{\sqrt{2\pi\sigma^2}} \exp\left[-\frac{(x-u)^2}{2\sigma^2}\right]$$



Rayleigh prob. distribution

$$f(z) = \frac{z}{\sigma^2} \exp\left(-\frac{z^2}{2\sigma^2}\right)$$

# In regions of high SNR, dist. Is Gaussian



Gaussian prob. distribution

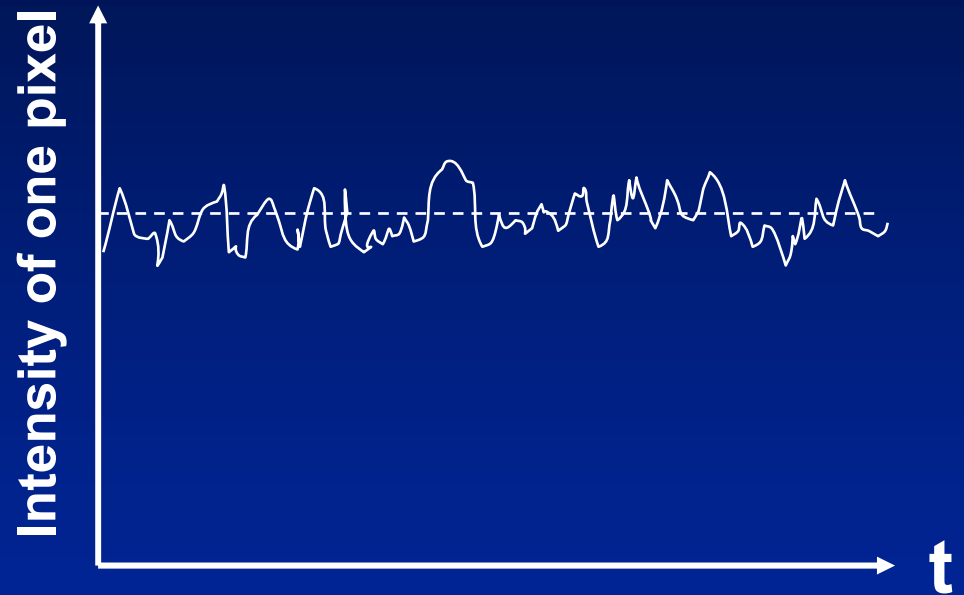
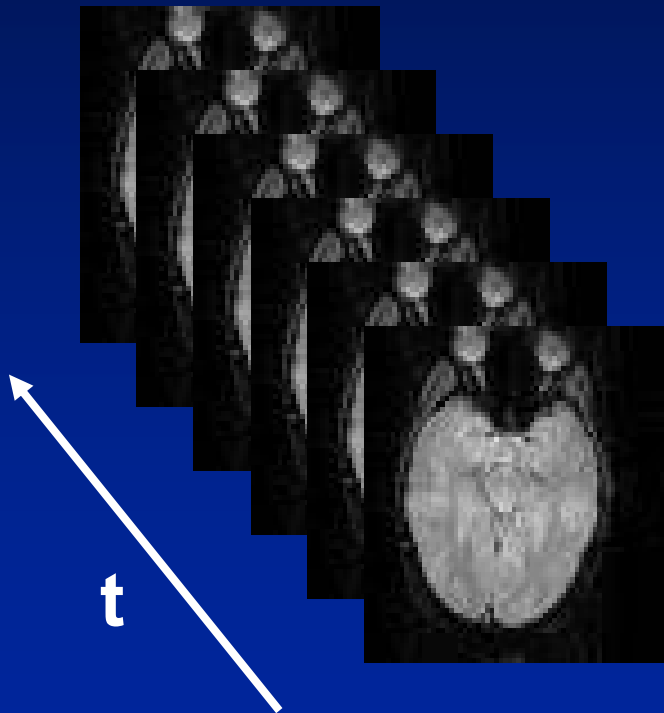
$$f(x) = \frac{1}{\sqrt{2\pi\sigma^2}} \exp\left[-\frac{(x-u)^2}{2\sigma^2}\right]$$

Rayleigh prob. distribution

$$f(z) = \frac{z}{\sigma^2} \exp\left(-\frac{z^2}{2\sigma^2}\right)$$



# fMRI noise means noise in the time series



Gaussian noise characterized by mean and SD ( $\sigma$ )

# Noise sources in fMRI

- Thermal noise from coil and body  $\sigma_T$
- Drift and instabilities in scanner  
 $\sigma_{\text{scanner}}$
- Physiologic modulation of MR signal  
due to non-bold effects  $\sigma_{\text{NB}}$
- Physiologic noise from flux. In basal  
cerebral CBV, CBF, CMRO<sub>2</sub>  $\sigma_B$

# Noise sources in fMRI

- Total system thermal noise  $\sigma_o^2 = \sigma_T^2 + \sigma_{scanner}^2$

- Non-BOLD physiologic noise is modulation of signal from:

respiration

cardiac motion

subject movement

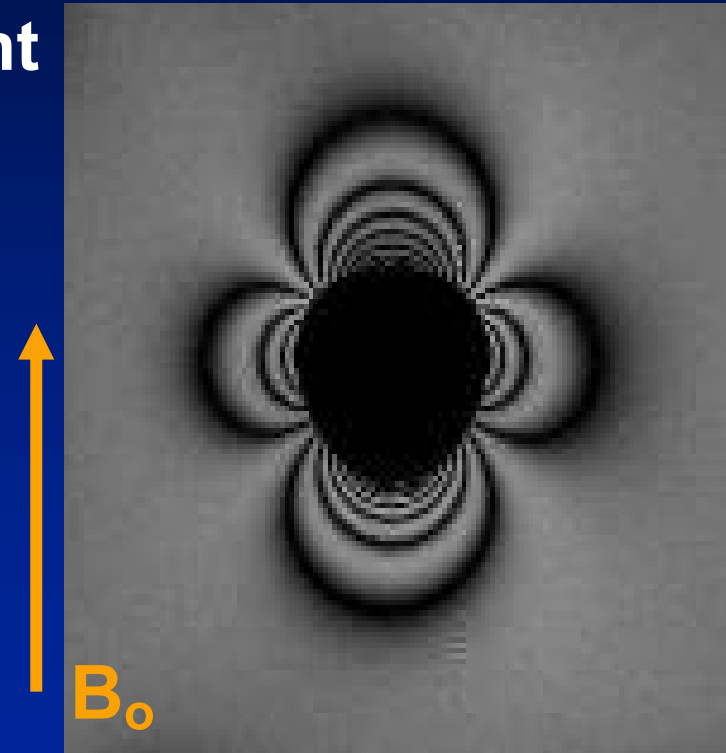
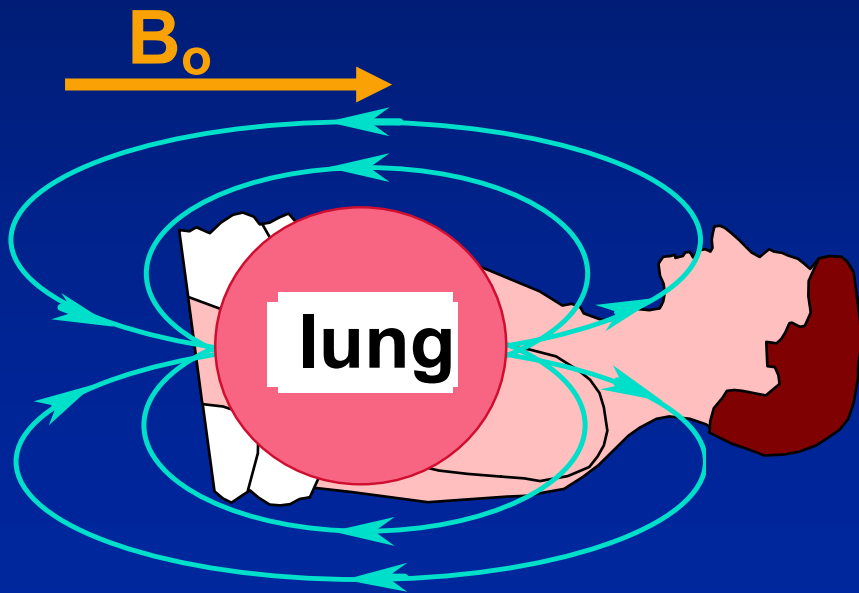
other?

$$\sigma_{NB} \propto S$$

# Respiration: Non-BOLD physiologic noise

(Van de Moortele MRM 47:888 2002)

Inflating lung produces z gradient



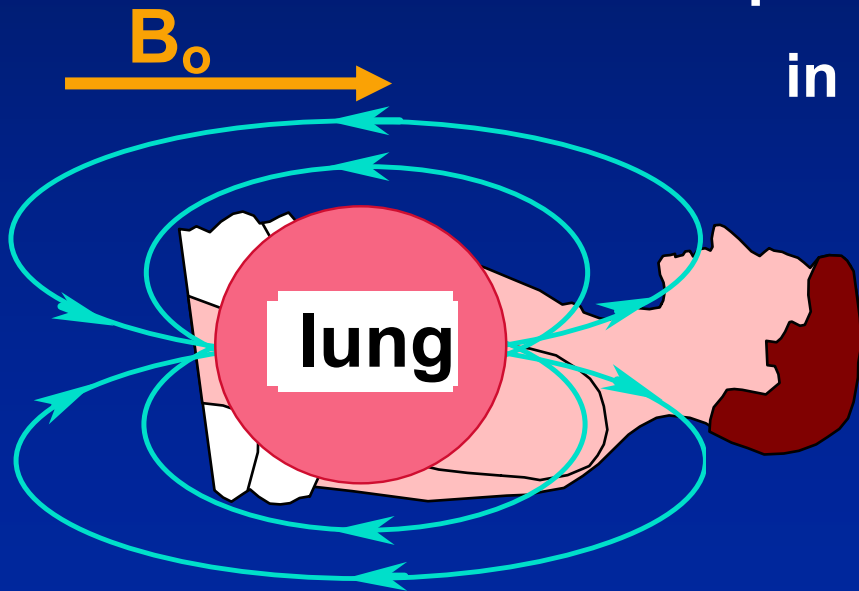
$B_0$  near Ping pong ball in water

# Respiration: Non-BOLD physiologic noise

(Van de Moortele MRM 47:888 2002)

- Inflating lung produces z gradient
- Z grad gives each axial slice a different  $\omega$ .
- Freq shift causes displacement of object

in PE direction



Frequency change is  
as much as 5 Hz.  
Shift of 0.25 pixels

# Noise sources in fMRI

**BOLD noise  $\sigma_B$  Signal modulation from  $\Delta$  in CBV, CBF, CMRO<sub>2</sub> is TE and S dependant.**

$$S = S_o \exp(-TE \cdot R_2^*)$$

$$\frac{dS}{dR_2^*} = -TE \cdot S_o \cdot \exp(-TE \cdot R_2^*)$$

$$\sigma_B = c_1 \cdot S \cdot \Delta R_2^* \cdot TE$$

# Noise sources in fMRI

(Kuger and Glover MRM 46 p631 2001)

Estimate  $\sigma_o$ ,  $\sigma_B$ ,  $\sigma_{NB}$

$\sigma_B$  can be measured by modulating TE

$\sigma_{NB}$  can be measured by modulating S  
by changing flip angle

$\sigma_o$  is the noise independent of TE and  
flip angle

# Noise sources in fMRI

(Kuger and Glover MRM 46 p631 2001)

Relative magnitudes of  $\sigma_o$ ,  $\sigma_B$ ,  $\sigma_{NB}$

	<u>gray matter</u>	<u>white matter</u>	<u>phantom</u>
<b>S</b>	<b>3500</b>	<b>3350</b>	<b>1137</b>
$\sigma_{TOTAL}$	<b>0.63</b>	<b>0.37</b>	<b>0.19</b>
$\sigma_o$	<b>0.21</b>	<b>0.22</b>	<b>0.14</b>
$\sigma_B$	<b>0.53</b>	<b>0.25</b>	<b>0.08</b>
$\sigma_{NB}$	<b>0.21</b>	<b>0.11</b>	<b>0.08</b>



# Noise sources in fMRI

(Kuger and Glover MRM 46 p631 2001)

$\sigma_B$  is maximum for  $TE = T2^*$

Functional SNR:            in gray matter       = 84

   in white matter   = 143

Dominant noise sources  $\propto S$

>> Increasing image SNR thru improved coils and big magnets doesn't help functional SNR after a point...

Elimination of respiration improves fSNR by 10%