

# PHYSICS OF MRI ACQUISITION

- **Quick Review**
- **Alternatives to BOLD for fMRI**

*HST-583, Fall 2002*

# Quick Review of Concepts

- NMR Signal
- MR Imaging
- MRI Contrast
- Brain Functional MRI
  - Goal: Detect neural activation
  - BOLD method

# Physiology during Neural Activation: Quick Review

- **Neural Firing: Electromagnetic Activity**  
Detection: EEG, MEG
- **Biochemical Reaction: Metabolic Activity**  
Detection: PET, MRS
  - cerebral metabolic rate of oxygen utilization (CMRO<sub>2</sub>)
- **Vascular Response: Hemodynamic Activity**  
Detection: PET, Optical Imaging, *fMRI*
  - cerebral blood flow (CBF)
  - cerebral blood volume (CBV)

# Alternatives to BOLD: Motivation

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- What does BOLD detect?
- Changes in [deoxy-Hgb]:
  - changes in: CBF + CBV + CMRO<sub>2</sub>
- Strong effects but limited physiological interpretation
- Independent measures of:  
CBF, CBV and CMRO<sub>2</sub> would be better

# Alternative to BOLD: Perfusion MRI

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- **Techniques that measure vascular parameters:**
  - **CBF:** rate at which blood flows through the microvasculature of a region of tissue.  
Unit: ml / g tissue / sec  
(~50 in gray matter, ~20 white matter)  
Independent of MRI technique.
  - **CBV:** fraction of volume of tissue occupied by blood (~3%).  
Dependent of MRI technique (sensitivity to vessel size)
  - **MTT:** Mean transit time, average time that blood spends passing through the blood volume with a region of tissue before it exits through the venous system.

# Perfusion MRI

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- **Fundamental Principle**

- A paramagnetic tracer goes through a capillary network
- Transient changes in local magnetic fields of surrounding tissue
- Transient changes in the MR signal
- MR signal changes vary rapidly: **need fast MRI**
- MR signal time course
  - ➔ concentration-time course (of tracer in tissue)
  - ➔ tissue hemodynamic parameters

# Perfusion MRI

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- **Mainstream Approaches**
    - Bolus injection of magnetic contrast agent
    - *Arterial Spin Labeling (ASL): blood as tracer*
  - **Potential Applications in Brain**
    - Blood flow in resting state:
      - Cerebrovascular disease, tumor characterization, monitoring drug effects, etc.
    - *Blood flow during activation:*
      - quantification, complements BOLD
- } **Area of research**

# Strengths of ASL

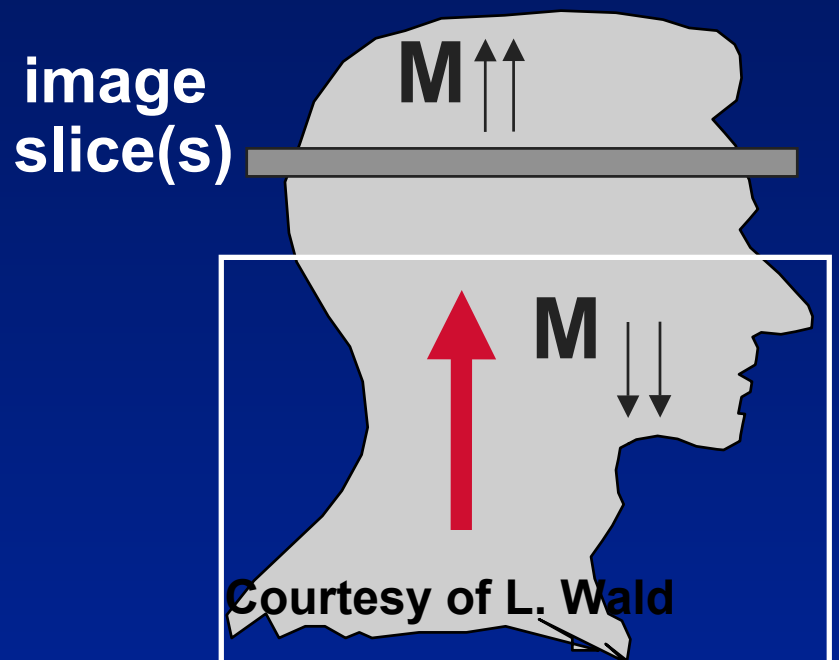
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- **Relative to bolus method**
  - no contrast agent required
  - reduced cost, discomfort
  - no limit to number of scans
  - temporal resolution of seconds
- **Relative to BOLD**
  - provide absolute measure of blood flow
  - more statistical power for low frequencies\*
  - less variability across subjects\*
  - less sensitive to susceptibility



# Arterial Spin Labeling in Brief

↑  $B_0$  magnetic field



**in flowing blood**

- **Tracer:** water in blood
- **Labeling:** invert inflowing magnetization
- **Life time:**  $T_1$  of blood water ( $\sim 1$ s)
- Labeled water flows into capillaries and exchanges with tissue water
- Inverted arterial inflow reduces total tissue magnetization in slice ( $\sim 1\%$ )
- Subtraction from a control image gives image proportional to CBF
- Theory can relate the ASL signal with absolute blood flow

# Arterial Spin Labeling Strategies

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- **Pulsed ASL**
  - Labeling is achieved by a short RF pulse that inverts the magnetization in a slab of tissue
- **Continuous ASL**
  - Labeling is achieved continuously as water spins flow past a plane defined by the location where a continuous RF B1 field is resonant

# Pulsed ASL: The Label

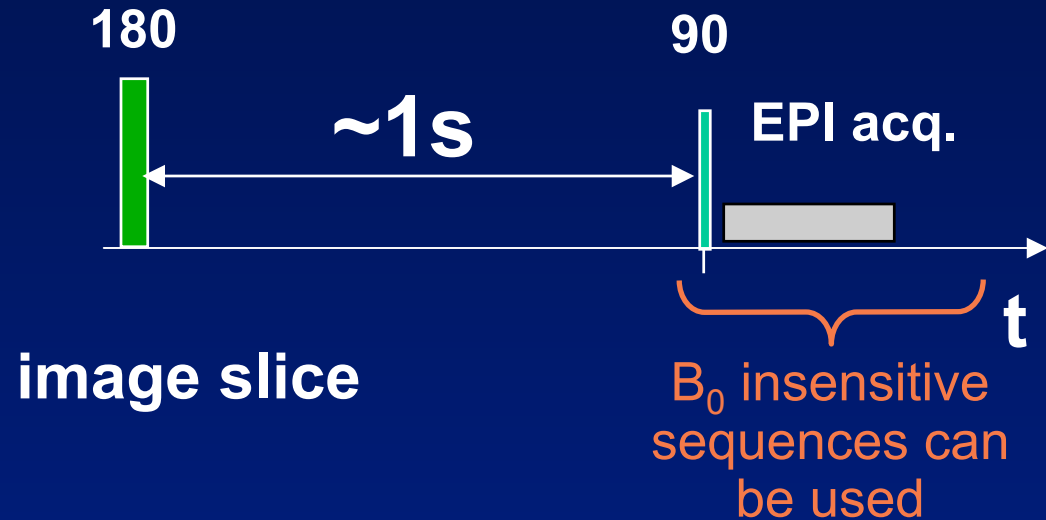
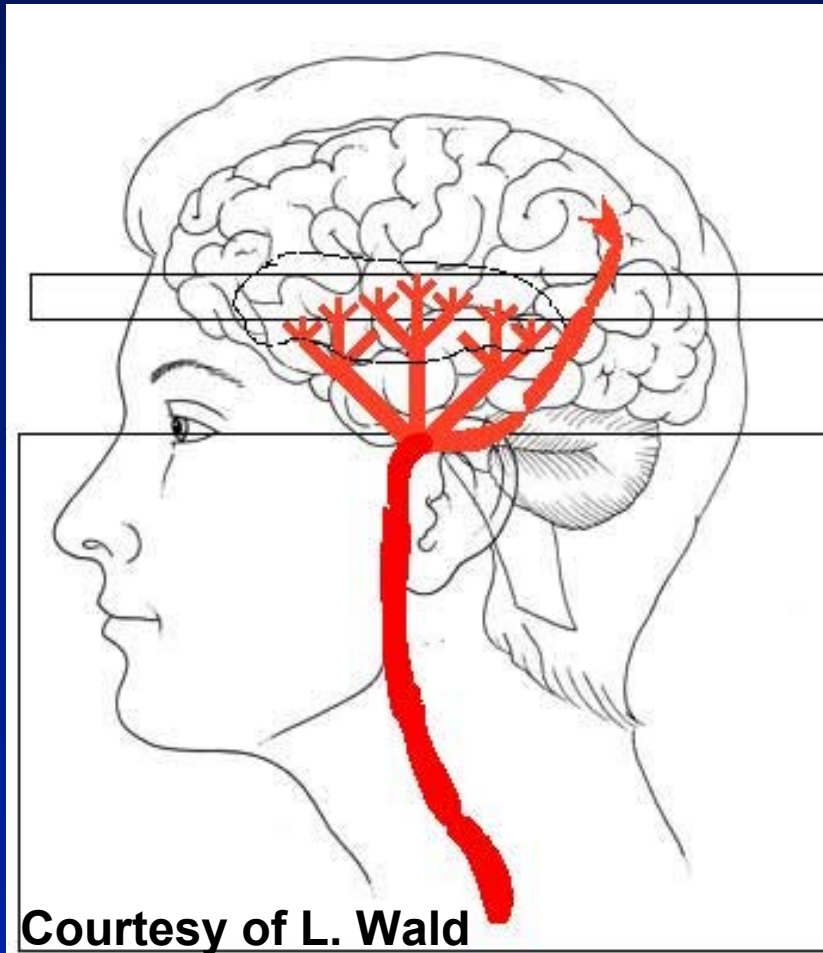


image slice

inversion slab

- T1 is important
- Thru slice arteries relatively dark
- Large inversion slab is important

Simultaneous BOLD + perfusion fMRI possible

# Arterial Spin Labeling

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- Perfusion image = **control image** - **labeled image**
- Perfusion signal changes < 3% intensity reduction
- Averaging to improve SNR:  
**control - label - control - label - control - label - ...**  
⇒ lower temporal resolution than BOLD
- Motion: big problem (subtraction errors)

# BOLD and Perfusion fMRI: Temporal Stability

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Estimated SNR vs stimulus frequency

See Aguirre et al., *NeuroImage* 2002

Within subject  
experimental design:

- BOLD greater SNR for most stimuli frequencies
- Due to low noise at low low frequencies, perfusion might be better for experimental designs in which low frequencies predominate

# ASL Sensitivity Across Subjects

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## *Average t-values*

*See Aguirre et al., NeuroImage 2002*

- **Small signal changes**
  - But better than BOLD for long time scales
  - But maybe better across subjects (more consistent)
- **SNR increases more rapidly with field strength than BOLD**
  - BOLD TE's must be shortened
  - T1 lengthening increases ASL signal

# ASL: Limitations

- Short life time of label due to T1
  - Low SNR: limits spatial resolution
- Dependence on arrival times and exchange times
- Oblique flowing blood vs assumption of upwards flow
- Accurate measurements of arterial blood  $T_1$  and  $M_0$  for absolute quantification
- No CBV obtained

# Direct measurement of CBV for fMRI

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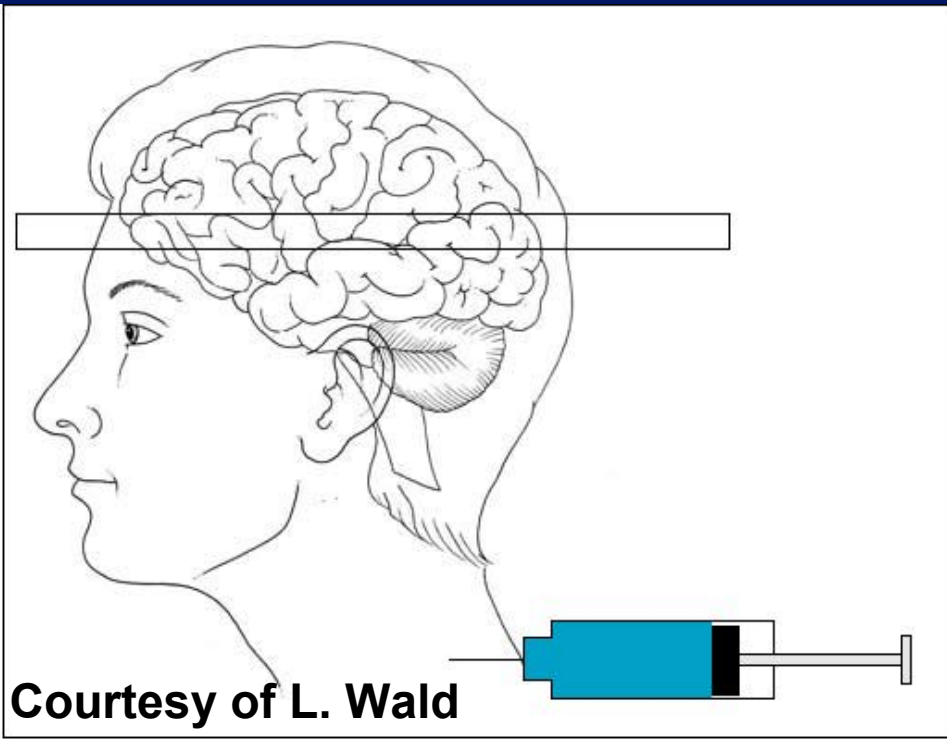
- **MOTIVATION:**

If CBF and CBV measured independently

⇒ estimation of  $CMRO_2$



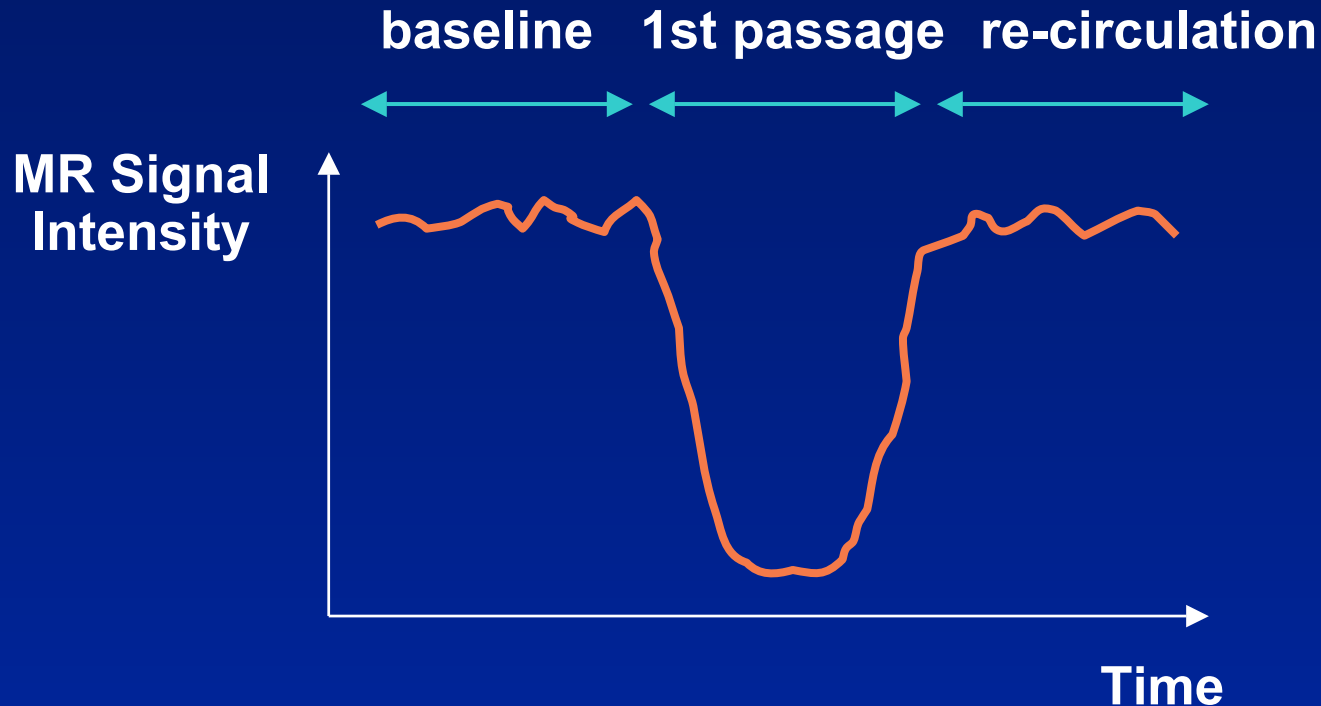
# Bolus Gd(DTPA) MR CBV (Intravascular T2\* agent)



- Agent stays in brain vessels
- Susceptibility effects  
⇒  $\downarrow T_2^*$  ⇒ signal drop
- Signal drop  
⇒ concentration agent
- Integral of concentration  
time course proportional to  
rCBV

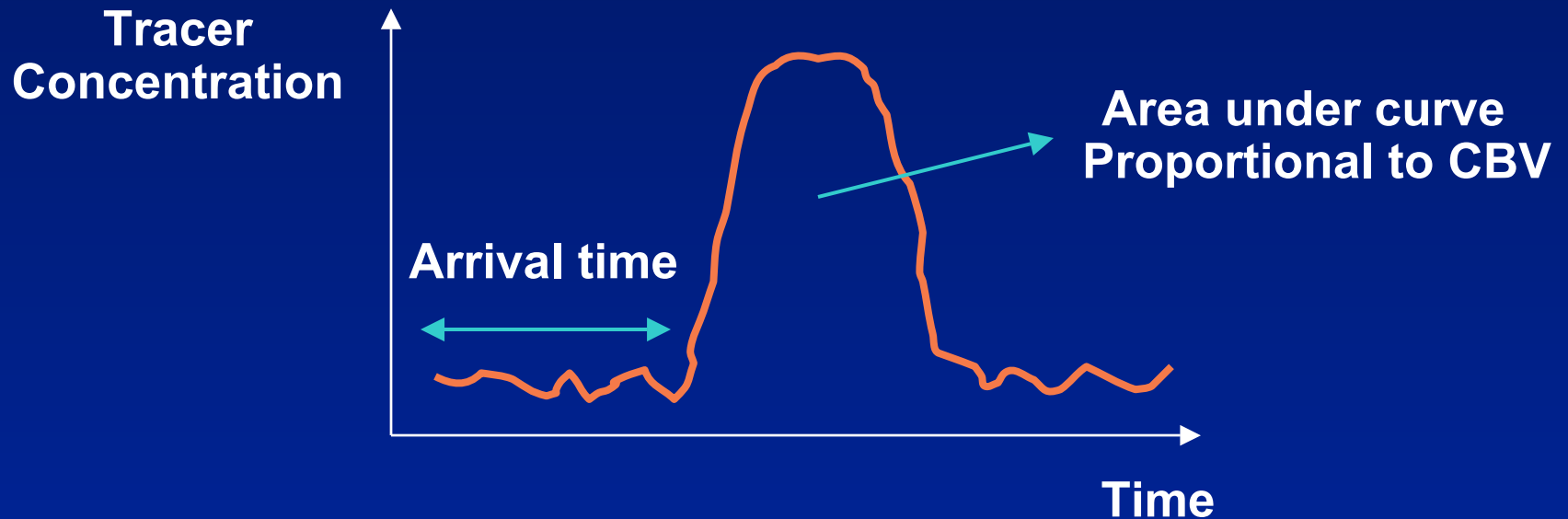
# CBV: Bolus tracking

Signal time course in perfused voxel



# CBV: Bolus tracking

## Concentration time curve in perfused voxel



# Summary: Brain fMRI Contrasts

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- **BOLD:** The most sensitive, but complex link to sources of neural activation
- **Alternatives to BOLD:**
  - CBF, CBV, CMRO<sub>2</sub>
  - Used for better understanding and complement BOLD
  - More direct assessment of vascular response
  - Less sensitive, under active development
- **Hopes for the future:**
  - Perfusion quantification improvements
  - Less motion sensitivity
  - Wider availability

*More in: <http://www.ujf-grenoble.fr/ismrm/ASL/outline.htm>*