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Onset Coding Is Degraded in Auditory Nerve Fibers from Mutant Mice Lacking Synaptic Ribbons

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Introduction

Sensory signals are carried from the cochlea to the brain via ~20,000 fibers in the auditory nerve (AN), comprising a large population (95%) of myelinated neurons contacting inner hair cells (IHCs) and a small population (5%) of unmyelinated fibers contacting outer hair cells (OHCs) (Spoendlin, 1969). The peripheral process of each IHC afferent is unbranched, making synaptic contact with a single IHC via a single terminal swelling (see Fig. 1A). A single ribbon, surrounded by a halo of synaptic vesicles, is anchored to the presynaptic complex opposite the synapse (Spoendlin, 1969, 1972; Liberman, 1980; Spoendlin and Schrott, 1988).

Each ribbon-containing active zone is capable of supporting extremely high rates of exocytosis: a single IHC active zone, with its single synaptic ribbon, can drive the postsynaptic AN fiber at instantaneous rates over 1000 spikes/s at stimulus onset, adapting over a few milliseconds to support sustained rates of up to 400 spikes per second. In addition to encoding stimulus intensity in spike rate, temporal structure is encoded in the fine timing of spikes. Central auditory neurons use this precise timing to resolve temporal features in the signal, such as interaural time differences, on the order of tens of microseconds (Mills, 1958).

In a mouse mutant with partial deletion of Bassoon, the gene coding the presynaptic scaffolding protein Bassoon, ribbons are no longer anchored to the active zones (Dick et al., 2003; Khimich et al., 2005; tom Dieck et al., 2005). This model offers a unique opportunity to study the contribution of synaptic ribbons to neurotransmission. In vitro studies of whole-cell capacitance in IHCs from mutant and wild-type mice suggest that the ribbon may facilitate rapid exocytosis by stabilizing a large readily releasable pool of vesicles (Khimich et al., 2005). However, each IHC is contacted by roughly 20 afferent synapses, which have diverse spontaneous and sound-evoked discharge rates. Thus, in vitro hair-cell recordings reflect the summed activity of a heterogeneous population of synapses. To complement the in vitro measurements, we study here the responses of single AN fibers, in vivo, in mutant and wild-type mice. Since each AN fiber receives input from a single active zone on a single IHC, to which a single ribbon is typically anchored (Spoendlin, 1969, 1972; Liberman, 1980; Spoendlin and Schrott, 1988), single-fiber recordings from the AN offer a sensitive metric of the contribution of a single ribbon to synaptic function.

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Many fundamental aspects of AN response were unaffected by disruption of Bassoon and loss of ribbons including tone-burst thresholds, sharpness of tuning, dynamic range, and accuracy of phase locking to amplitude modulations. The salient abnormalities were a striking reduction in spontaneous and sound-evoked discharge rates. Encoding of stimulus onset time was especially degraded because of the reduced reliability of spike generation. We conclude that the ribbon and/or Bassoon are key to stabilizing a large readily releasable pool of synaptic vesicles, which ensures the reliable coding of stimulus onsets necessary for many key aspects of normal auditory processing.

Materials and Methods
Mice were from a mixed genetic background (C57BL/6 and 129/S6), bred from parents heterozygous for the targeted deletion of exons 4 and 5 of the bassoon gene (Altrock et al., 2003) and genotyped using PCR. Mutant mice and their wild-type littermates were studied at 7–11 weeks of age, before the onset of premature age-related hearing loss that characterizes these strains (Zheng et al., 1999; Hequembourg and Liberman, 2001). Animals with poor cochlear function, as evidenced by high thresholds for distortion product otoacoustic emissions (DPOAEs), were excluded from additional study; these mice comprised 21% of the population, a ratio that was identical for both genotypes. All procedures were approved by the Institutional Animal Care and Use Committee of the Massachusetts Eye and Ear Infirmary.

The sound system, consisting of dual electrostatic sound sources (Tucker-Davis Technologies; ED-1) and a Knowles Electret microphone coupled to a probe tube, was positioned near the tragus of the external ear canal. The sensitivity of the probe tube microphone was measured between 0.1 and 73 kHz using a calibrated quarter-inch Bruel and Kjær condenser microphone in a coupler.

Auditory brainstem responses and DPOAEs
For measurement of auditory brainstem responses (ABRs), mice were anesthetized with ketamine (100 mg/kg) and xylazine (10 mg/kg), and needle electrodes were inserted at the vertex and pinna with a ground near the tail. ABRs were evoked with 4 ms tone pips at 40 per second with a 0.4 ms cosine squared rise–fall envelope and alternating in polarity to remove frequency-following responses. The voltage difference between the pinna and vertex was amplified (100,000×), filtered, digitized at 100 kHz, and averaged across 512 presentations. The sound level was raised in 5 dB steps from 10 dB below threshold to 80 dB sound pressure level (SPL). Waveforms were filtered using a zero-phase first-order Butterworth filter with a pass band from 0.2 to 10 kHz, and wave amplitudes and latencies were extracted using a semiautomated algorithm. Threshold was defined by visual inspection of stacked waveforms.

DPOAEs at 2f1−f2 were recorded in response to primary tones f1 and f2 with f1 spaced logarithmically at frequencies from 5.6 to 45.2 kHz and the f2/f1 ratio fixed at 1.2. With f1 set to the level 10 dB < f1, each frequency pair was swept in 5 dB steps from below threshold to 80 dB SPL. The ear-canal sound–pressure waveform was amplified and digitally sampled at 250 kHz. Fast Fourier transforms were computed and averaged over five consecutive waveform traces before extraction of the 2f1−f2 DPOAE amplitude and surrounding noise floor. Isoresponse contours were interpolated from the 2f1−f2 amplitude versus sound level function, with threshold defined as the f1 level required to produce a DPOAE at 0 dB SPL.

Single-fiber recordings from the auditory nerve
In vivo recording from single fibers in the mouse AN were done as described previously (Taberner and Liberman, 2005).

Surgical approach, inclusion criteria, and preparation stability. Mice were anesthetized with xylazine (5 mg/kg) and urethane (1.32 mg/kg) and placed in a sound-proofed, electrically shielded room. Body temperature was maintained at 37°C. The pinnae were removed, scalp reflected, portions of the lateral interparietal and occipital bone removed, and a partial cerebellar aspiration performed to expose the cochlear nucleus.

Glass electrodes filled with 2.5 KCl and 4% methyl blue were advanced through the cochlear nucleus into the auditory nerve using a stereotactic apparatus to angle the track 24° posterior in the sagittal plane. As defined by Taberner and Liberman (2005), criteria for distinguishing auditory nerve fibers from cochlear nucleus neurons included electrode depth (>1000 μm from brainstem surface) and response properties to tone bursts: primary-like poststimulus time histogram, response latency (mode of the first-spike latency distribution using a 0.1 ms bin) of <5 ms, and coefficient of variation for interspike intervals of >0.5. At the end of the experiment, the cochlear nucleus was aspirated and the position of the electrode tip within the auditory nerve verified by direct inspection.

DPOAE thresholds were measured after recording from each single fiber to monitor preparation stability: data were included only if the DPOAE threshold near the fiber’s characteristic frequency was within 10 dB of the threshold at the beginning of the experiment.

Stimulus and response measures. Noise bursts (50 ms duration, 80 dB SPL) were used as a search stimulus while advancing the electrode. After contact with each new fiber, a tuning curve was measured with a computer-based algorithm that tracks the sound pressure required, as a function of frequency, to evoke a response of 10 spikes/s greater than spontaneous rate (SR) (Kiang et al., 1970). Tone bursts (50 ms duration with 2.5 ms cos−rise–fall envelopes, 10 per second) were used for derivation of the tuning curve and for all other sound-evoked measurements unless otherwise indicated. Characteristic frequency (CF) was defined from the tuning curve as the frequency with lowest threshold. Spontaneous discharge rate was estimated from samples of spike trains collected over durations of 10 to 150 s. Poststimulus onset time and interspike-interval histograms, used for distinguishing AN fibers from cochlear nucleus cells, were computed from responses to tone bursts at CF, presented at 30 dB above threshold.

Rate-level functions were measured with tone bursts at CF. The level was varied in 5 dB steps, presented in random order, with 20–50 tone bursts per level. Functions were fitted using a modified version of a model described previously (Taberner and Liberman, 2005). Dynamic range was defined as the difference between the levels at which the driven rate (average rate minus SR) is 10% and 90% of the model-fit maximum driven rate.

Synchrony was assessed using transposed tones (Bernstein and Trahiotis, 2002), consisting of a carrier tone at the fiber’s CF that was amplitude modulated by a half-wave-rectified sinusoid of 0.125, 0.5, 0.75, or 1 kHz. The level of this modulated tone was varied in 5 dB steps, from below threshold to 80 dB SPL. The synchronization index (SI) for spike times at each modulation frequency and level was defined as the average of a vector sum, where ti is the time of the ith spike in a train of n spikes, and ω is the angular frequency of the modulator:

\[
SI = \frac{1}{n} \sum_{i=1}^{n} e^{i\omega(t_i - t_{i-1})}
\]

Significance of synchronization was quantified using the Rayleigh statistic, which tests the null hypothesis that the time series is uniform throughout the cycle (Buunen and Rhode, 1978; Mardia and Jupp, 1999): r = 2nSI2. Synchrony data not meeting the criterion of p < 0.001 (r ≥ 13.8) were discarded.

Immunohistochemistry. To count synaptic ribbons in hair cells, anesthetized animals were perfused intracardially with 4% paraformaldehyde in PBS. Cochleae were decalified, dissected into half turns, and incubated in 5% normal horse serum with 0.03% Triton X-100 in PBS, followed by incubation in primary antibodies (rabbit α-calretinin from Millipore and mouse α-CtBP2 from Santa Cruz Biotechnology) for 19 h, and secondary antibody (biotinylated donkey α-mouse from Jackson ImmunoResearch and Alexa Fluor-488 chicken α-rabbit from Invitrogen) for 60 min. Cochlear half turns were wet mounted in Vectashield (Vector Laboratories) and placed on glass slides for examination using a Leica confocal microscope with a 100× oil-immersion lens. In seven turns spaced approximately a half octave from each other, focal z-series (0.25 μm step size) were obtained. The frequency of each location was estimated using a modified version of the physiological place-frequency map for mice, as recommended by Taberner and Liberman (2005). Amira, a three-dimensional visualization program (Visage Imaging), was
used to perform three-dimensional Gaussian filtering and transformations. Resulting images were cropped down to the IHC region and passed to Blob3D (University of Texas), a three-dimensional quantitative software, to count the synaptic ribbons.

Results

Synaptic ribbon counts

To quantify the number and distribution of synaptic ribbons in Bassoon-deficient ears, sensory epithelia from four mutants and two wild-type ears were immunostained for a ribbon-specific marker, RIBEYE/CtBP2 (Khimich et al., 2005; Meyer et al., 2009), and an IHC label, calretinin (Fig. 1E, F). In wild types (Fig. 1B), ribbon counts were consistent with IHC innervation patterns and estimates of synapse numbers from electron microscopic data (Francis et al., 2004; Stamatakis et al., 2006), i.e., 12 ribbons/IHC in the basal and apical extremes and 18 ribbons/IHC in midcochlear regions. In mutants, ribbons were reduced in number, ranging from two per IHC in the apex to four per IHC in the base (Fig. 1B). Most of these remaining ribbons were abnormally large (Fig. 1F), reminiscent of the ribbon fields observed in Bassoon-deficient cone photoreceptor terminals (Dick et al., 2003). Only 10% were close to the IHC membrane in subnuclear regions, where AN terminals make contact. Remaining ribbons were floating in the cytosol or in supranuclear regions, consistent with electron microscopic evidence from bassoon mutants (Khimich et al., 2005), indicating that, at most, 1 in 30 AN synapses still had ribbons.

Gross measures of cochlear function

Two minimally invasive measures of cochlear response, DPOAEs, and ABRs, were used to provide an overview of cochlear dysfunction in the mutants.

DPOAEs are acoustic signals that arise from distortions in the hair cell’s mechanoelectric response to two continuous tones. These distortion products, at frequencies not present in the input stimulus, are amplified by OHCs’ biological motors and can be detected with a microphone in the ear canal. DPOAEs are unaffected by loss of IHCs or AN fibers (Liberman et al., 1997). Normal DPOAE thresholds in mutants (Fig. 2A) show that many aspects of cochlear function, including mechanoelectric transduction by OHCs, were normal in the absence of synaptic ribbons.

ABRs, evoked by short tone bursts, represent the summed activity of neurons in the ascending auditory pathway and are measured by averaging the evoked electrical response recorded via subcutaneous electrodes. ABR thresholds in mutants were elevated 10 to 15 dB across most test frequencies (Fig. 2B); the threshold elevation at high frequencies reflects basal-turn OHC degeneration characteristic of the background strain (Zheng et al., 1999; Hequembourg and Liberman, 2001). The amplitude of the first ABR wave (Fig. 2C), which reflects the summed activity of the AN, was reduced by a factor of 5.4 in mutants (Fig. 2D), consistent with dysfunction in synaptic transmission. The plateau just before wave 1 (Fig. 2C, arrow) is similar in wild types and mutants and may represent the summed receptor potentials of IHCs.

Auditory nerve responses

To characterize AN response in the absence of synaptic ribbons, recordings were made from 185 AN fibers obtained from 27 wild-type mice and 78 AN fibers from 19 mutant mice.
Spontaneous rate and discharge irregularity

Mammalian AN fibers fire spontaneously in the absence of sound (Kiang, 1965); in normal mice, SRs range from near zero to over 180 spikes/s, with a distribution skewed toward low rates (Taberner and Liberman, 2005). Many response properties are normally correlated with SR, e.g., threshold and dynamic range (Sachs and Abbas, 1974; Liberman, 1978; Palmer and Evans, 1980; Schalk and Sachs, 1980; Taberner and Liberman, 2005).

In mutant fibers, SRs were significantly lower than normal (Fig. 3A,B), never exceeding 80 spikes/s in mutants, compared with a maximum of 183 spikes/s in wild types. The mean SR across all fibers sampled was reduced by a factor of 4.0.

Spontaneous discharge in AN fibers is highly irregular, with statistics consistent with a Poisson process. Interspike intervals show an exponential distribution with a dead time caused by the absolute refractory period (Young and Barta, 1986; Li and Young, 1993) (but see Heil et al., 2007). This fundamental irregularity of AN response was not altered by loss of ribbons, as shown by the similarity of interspike interval histograms from wild-type and mutant fibers of similar SR (Fig. 3C).

To systematically assess differences in response regularity, we split AN fibers into groups of similar SRs (within two spikes per second), discarded fibers with significant (p ≤ 0.05) fluctuations in rate as described by Heil et al. (2007), and performed a statistical test on each group: out of 10 groups containing at least one wild-type and one mutant fiber, none had interspike interval distributions that differed significantly (p ≤ 0.05) as assessed by the two-sample Kolmogorov–Smirnov test.

Tuning and threshold

AN fibers have a high degree of frequency selectivity. This frequency response is typically measured as a tuning curve (supplemental Fig. S1B, inset, available at www.jneurosci.org as supplemental material), reflecting the tone level required to evoke a response that is 10 spikes/s greater than SR. The sensitive tip of the tuning curve defines the CF, which reflects the fiber’s origin along the mechanically tuned cochlear spiral: high frequencies originate in the base of the cochlea, whereas lower frequencies are from progressively more apical locations (Liberman, 1982).

Since this exquisite frequency selectivity requires the electromechanical feedback of OHCs (Liberman et al., 2002), which amplifies cochlear vibration, it is not surprising that the distribution of thresholds (supplemental Fig. S1A, available at www.jneurosci.org as supplemental material) and tuning (supplemental Fig. S1B, available at www.jneurosci.org as supplemental material) are normal in mutant AN fibers, given the normal DPOAE thresh-
coefficient, SR and threshold remained (Spearman rank-order correlation mean SR was reduced in the mutants, a weak correlation between pooled across many animals, as in the present study. Although (Liberman, 1978). Such correlations are weak when data are high-SR fibers (SR of genotypes.

In normal ears, AN threshold is inversely correlated with SR: high-SR fibers (SR of >10 spikes/s) are, on average, 10–20 dB more sensitive than low-SR fibers (<10 spikes/s) of similar CF (Liberman, 1978). Such correlations are weak when data are pooled across many animals, as in the present study. Although mean SR was reduced in the mutants, a weak correlation between SR and threshold remained (Spearman rank-order correlation coefficient, $r = -0.29$, two-sided $p = 0.05$ in mutants; $r = -0.17$, $p = 0.10$ in wild types; data not shown).

Sound-evoked discharge rates, adaptation, and dynamic range
When stimulated with tones, a normal AN fiber produces a graded response: mean spike rate increases with increasing level, but only over a limited range of levels (Sachs and Abbas, 1974; Schalk and Sachs, 1980). In mouse AN fibers, discharge rate typically saturates within 20 dB of threshold (Taberner and Liberman, 2005) (supplemental Fig. S2A, available at www.jneurosci.org as supplemental material). Since IHC receptor potentials show a larger dynamic range (Russell and Sellick, 1978; Palmer and Russell, 1986), hard saturation in AN fibers is thought to arise in synaptic transmission. When matched for SR, there is no difference in dynamic range between mutant and wild-type fibers, indicating that the presynaptic machinery that controls graded synaptic drive remains intact in the absence of synaptic ribbons (supplemental Fig. S2B, available at www.jneurosci.org as supplemental material).

AN fibers normally respond to tone bursts with a spike rate that declines exponentially from a maximum at stimulus onset (i.e., peak rate) to an adapted rate (Fig. 4A). For 50 ms tone bursts, this adaptation can be described as the sum of a rapid and a slow time constant (Westerman and Smith, 1984) of approximately 0.65 and 10 ms, respectively. Since a similar decrease is not observed in the IHC receptor potential (Russell and Sellick, 1978; Palmer and Russell, 1986), and the reduction in calcium current (Hudspeth and Lewis, 1988; Moser and Beutner, 2000; Yang et al., 2006; Cui et al., 2007) and postsynaptic AMPA receptor desensitization (Goutman and Glowatzki, 2007) are minimal, adaptation is thought to arise mainly in synaptic transmission, e.g., via exhaustion of the readily releasable pool of synaptic vesicles (Furukawa and Matsuura, 1978; Moser and Beutner, 2000; Goutman and Glowatzki, 2007).

In mutant ears, AN response showed clear postonset adaptation (Fig. 4A) in response to saturating CF tone bursts. Adaptation was difficult to quantify for individual fibers because sampling times were insufficient to produce post-stimulus time histograms of the requisite smoothness; thus, average histograms were generated by pooling data from fibers of similar SRs. Time constants of mutant fibers were similar to those of wild types when matched for SR (e.g., for fibers with an SR between 10 and 80 spikes/s, the rapid time constant was 0.64 vs 0.81 ms, and the slow time constant was 9.3 vs 11.4 ms). However, the amplitudes of the rapid and slow components were reduced by factors of 3.8 and 1.9, respectively. Like wild-type, mutant fibers were able to maintain adapted discharge rates for stimulus durations of at least 5 min (data not shown).

Sound-evoked discharge rates in single fibers, both peak (Fig. 4D) and adapted (Fig. 4E), were significantly reduced (independent two-sample, two-tailed Student’s $t$ test; $p < 0.001$) in mutants by factors of 2.5 and 1.8, respectively, when averaged across all fibers. Peak rates are normally correlated with SRs (Fig. 4D). However, even when matched for SR, the peak rates in mutants were reduced (Fig. 4D). This reduction was more pronounced when the stimulus rise time was more abrupt. For example, clicks
(Fig. 4B,C), with a nominally instantaneous onset produced a larger difference in peak rates (factor of 6.5) than tone bursts shaped with a 2.5 ms rise time (Fig. 4A,C). Correspondingly, the tone pips used to measure ABRs (with an intermediate rise time of 0.4 ms) produced an intermediate peak-rate reduction (factor of 4.4) (Fig. 4C), which is close to the 5.4-fold reduction seen in mutant ABR amplitudes (Fig. 2C,D); this large reduction in peak rate likely explains the striking elevation in ABR threshold despite normal single-fiber thresholds in mutants.

First-spike latency and spike-time reliability
Accurate coding of stimulus onsets is critical for many auditory tasks such as localizing sounds in space, requiring precise timing and reliable occurrence of first spikes in AN fibers. Failures to produce a spike, as well as variance in the timing of the first spike relative to stimulus onset, are detrimental when convergence of simultaneous AN inputs onto higher-level neurons is required. The distribution of first-spike latencies, as illustrated by dot raster plots of spike times in response to repeated tone bursts (Fig. 5A), demonstrates why mutant fibers fail to achieve high peak rates: for many stimulus presentations, the mutant fiber fails to produce a spike in response to stimulus onset (Fig. 5B).

One way to capture the difference in the distributions of first-spike latencies is to compute the distribution variance (Fig. 5C). The variance tends to increase with decreasing SR in wild types. When matched for SR, mutant fibers show significantly higher variance by a factor of 4.9, on average. Thus, the spike times are significantly less reliable, even in response to tone bursts at a level high enough to saturate the mean discharge rate.

Phase locking and spike-time accuracy
In response to periodic, amplitude-modulated stimuli, AN fibers tend to fire at a preferred phase of the stimulus cycle (Kiang, 1965; Rose et al., 1967). This phase locking, or synchrony, is essential for key aspects of binaural hearing. For example, small differences in the relative timing of sound between the two ears are the dominant cue for localizing low-frequency sounds (Wightman and Kistler, 1992; Macpherson and Middlebrooks, 2002). Precise timing of IHC exocytosis is required to maintain the fidelity of synaptic transmission required to encode these interaural differences.

Low-frequency pure tones are typically used to assess AN phase locking (Kiang, 1965); however, spike synchronization decreases as tone frequency approaches 4 kHz because IHC membrane capacitance filters out high-frequency components in the receptor potential (Palmer and Russell, 1986). Since few mouse AN fibers are sensitive to frequencies below 4 kHz (Johnson, 1980; Taberner and Liberman, 2005), we used an amplitude-modulated high-frequency carrier known as a transposed tone (Bernstein and Trahiotis, 2002), in which the modulation envelope is a half-wave-rectified, low-frequency sinusoid, and the carrier is set to the fiber’s CF (Fig. 6A, top). Because half-wave rectification is inherent in cochlear mechanolectric transduction, the resulting temporal modulation of IHC receptor potential is similar to the pattern that would be produced by a low-frequency sinusoid (Palmer and Russell, 1986; Dreyer and Delgutte, 2006).

In response to transposed tones, phase locking in mutant AN fibers was as precise as, or more precise than, in wild types (Fig. 6), as can be seen in either dot raster plots (Fig. 6A), period histograms (Fig. 6C), or interspike interval histograms (Fig. 6B). Spikes in both mutant and wild-type fibers clearly lock to the low-frequency amplitude modulation. The SI is a classic metric for assessing the strength of this phase locking (Goldberg and Brown, 1969). The synchronization index varies between 1 (all spikes occur at the same phase of the stimulus cycle) and 0 (spikes occur randomly throughout the cycle). On average, the synchronization indices were greater in mutant than wild-type fibers (Fig. 6D); however, this difference arises from the reductions in SR: spontaneous spikes occur at random times and therefore degrade this measure of synchronization. When matched for SR, the maximum synchrony was comparable in wild-type and mutant fibers across all modulation frequencies tested (data not shown).

The ensemble interspike interval histograms (Fig. 6B) highlight the important difference between spike precision and spike reliability. Wild-type fibers tended to produce a precisely timed

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**Figure 5.** Analysis of first-spike latencies (FSLs) demonstrates the loss of reliable AN response in mutant ears. A. Dot raster plots show spike times (small gray dots) from a representative wild-type and mutant AN fiber for multiple repetitions of a 50 ms tone burst: for each repetition, the time of the first spike is highlighted by the large black (wild type) or red (mutant) symbol. B. Histograms of FSLs for representative wild-type and mutant fibers of comparative spontaneous rate and characteristic frequency as computed from data such as those in A. C, Relationship between SR and FSL variance for all AN fibers sampled.
Available for analysis increased, estimates converged toward 0.61 ms (supplemental Fig. S3B, available at www.jneurosci.org as supplemental material). Although the mean absolute refractory period for mutants is lower than the wild type, values were similar when matched for rate. Estimates for the time constant of the relative refractory period ranged from 2.5 ms at the lowest driven rates (50 spikes/s) to a minimum of 0.45 ms at the highest rates (350 spikes/s); however, no remarkable difference was observed between wild-type and mutant fibers when matched for rate (supplemental Fig. S3C, available at www.jneurosci.org as supplemental material).

**Modeling AN response from inferred vesicle release rates**

The reliability of spike onset times in normal AN fibers is mediated by coordinated release from a pool of readily releasable vesicles maintained by the synaptic ribbon (Khimich et al., 2005; Moser et al., 2006; Goutman and Glowatzki, 2007; Wittig and Parsons, 2008). To test whether the kinetics of presynaptic exocytosis could explain the spike activity observed in wild-type and mutant AN fibers, we modeled synaptic transmission (Fig. 7) using vesicle release rates estimated from depolarization-evoked membrane capacitance changes in IHCs from wild-type and mutant mice (Khimich et al., 2005).

The increase in plasma membrane capacitance, \( \Delta C_{cm}(\Delta t) \), measured after a depolarizing stimulus of duration \( \Delta t \), reflects the surface area added by vesicles exocytosed during the stimulus. Dividing \( \Delta C_{cm}(\Delta t) \) by the average capacitance per vesicle, \( c_v = 44.5 \text{ aF} \) (Neef et al., 2007), and the number of synapses per IHC, \( num_{syn} = 11.5 \) (Khimich et al., 2005), returns the cumulative number of vesicles released with rate \( R(t) \) during \( \Delta t \).

\[
\int_0^{\Delta t} R(t) \, dt = \frac{\Delta C_{\text{cm}}(\Delta t)}{C_v \cdot num_{\text{syn}}}.
\]

Release rate was estimated by fitting an exponential function to the first 2 to 10 ms of the cumulative release, with the data weighted in the fitting algorithm according their standard errors, and accounting for a 1 ms delay in exocytosis (Beutner et al., 2001; Brandt et al., 2005; Neef et al., 2007). The initial release rate, \( R_0 \), is the derivative of the fit function evaluated at the onset of the exocytic response (supplemental Table S1, available at www.jneurosci.org as supplemental material), and the release rate after the first 10 ms is approximated by a linear fit between 10 and 20 ms. Mutant IHCs showed a ~2.5-fold reduction in initial release rate but a comparable release time constant (supplemental Table S1, available at www.jneurosci.org as supplemental material), consistent with a reduced size of the readily releasable pool, but unaltered spike on almost every stimulus cycle: the peak at spike intervals of one period is the highest. Spike discharge in mutant fibers was as precisely locked with the stimulus phase; however, mutant fibers were less reliable in producing a spike on each cycle of the amplitude modulation: spike intervals of 1, 2, 3, or 4 periods were equally probable.

**Absolute and relative refractory periods**

Reduction in spontaneous and sound-evoked activity could arise from a prolonged refractory period. Although refractoriness is a property of the postsynaptic membrane, it is conceivably a downstream effect of this synaptic disruption. To rule out this possibility, refractory periods were estimated from spike trains obtained under conditions of constant synaptic drive (Li and Young, 1993) by computing spike probability as a function of the time since the last spike (supplemental Fig. S3A, available at www.jneurosci.org as supplemental material), i.e., the hazard function. The absolute refractory period is the smallest interspike interval, and the relative refractory period is the time constant for the portion of the hazard function over which probability increases to asymptote. To ensure adequate spike counts, we used data derived from the adapted portion of responses to tone bursts (Fig. 4A).

At the lowest rates, estimates of the absolute refractory period ranged from 0.6 to 10 ms. However, as the number of spikes

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**Figure 6.** Analysis of synchronization index reveals that temporal precision of AN response is not degraded in mutant ears. A. As in Figure 5, dot raster plots show spike times for a representative wild-type (black) and mutant (red) AN fiber in response to multiple repetitions of a transposed tone (modulation frequency set to 500 Hz, carrier frequency set to fiber CF). B. Mean interspike interval histograms for mutant versus wild-type AN fibers responding to transposed tones such as those in A. Intervals are expressed as a fraction of the modulation period. Data from fibers of each genotype are pooled before computing the histogram. Counts are divided by the bin width (0.01 of the period) and number of repetitions to represent the probability of discharge in a given interval. C. Sample post-zero-crossing histograms for representative wild-type (i.e., high SR) and mutant (i.e., low SR) fibers show the degree of synchrony between spike times and the modulation period: histograms such as these are used to compute the synchronization index shown in D. D. Maximum synchronization index as a function of modulation frequency for mutant versus wild-type AN responses to transposed tones with carrier frequency at the CF (box–whisker plots show the first, 25th, 50th, 75th, and 99th quantiles). The maximum SI is determined for each fiber by sweeping transposed tones in 5 dB steps from threshold to ~40 dB from threshold.
vesicular release probability. The difference in steady-state release was smaller (supplementalTableS1, available at www.jneurosci.org as supplemental material), suggesting that vesicle resupply at mutant synapses is less affected by loss of the ribbon and/or Bassoon.

To compare these in vitro IHC recordings to the AN data, we devised a model in which the readily releasable pool (B) consists of vesicles that occupy a fixed number of slots \(N_{\text{slots}}\). Vesicles are released from these slots with a rate constant, \(k_{\text{release}}\), relating release rate to the fill level of the readily releasable pool:

\[
R(t) = B(t) \cdot k_{\text{release}} \tag{3}
\]

Empty slots are refilled from a reserve pool with a rate constant, \(k_{\text{refill}}\), yielding the following differential equation and its solution:

\[
B = -k_{\text{release}} \cdot B(t) + k_{\text{refill}} \cdot \left(N_{\text{slots}} - B(t)\right) \tag{4}
\]

\[
B(t) = N_{\text{slots}} \cdot \left(\frac{k_{\text{refill}}}{k_{\text{release}} + k_{\text{refill}}} \right) \cdot \left(1 - e^{-(k_{\text{release}} + k_{\text{refill}}) t}\right) \tag{5}
\]

In this framework, spike-rate adaptation reflects declining release rate resulting from depletion of the readily releasable pool and its rate-limiting resupply.

To compare vesicle release dynamics with AN responses to tone bursts (Figs. 4, 5), a time-dependent release probability, \(k_{\text{release}}(t)\), was used to mimic the 2.5 ms onset envelope of the tone burst. The dynamic range of an AN synapse was set to 20 dB, with \(k_{\text{release}}(t)\) growing linearly with stimulus intensity within that range. The release rates resulting from Equations 3 and 4 were then used to drive an inhomogeneous Poisson process to estimate first-release-event latencies: as expected, the distribution for mutant synapses was broader than that for wild types (Fig. 7B).

To determine how increased variance of first-release times would degrade onset responses in AN fibers, we extended the model to spike generation (Fig. 7C,D). Spike times were generated using the presynaptic release rate to drive an inhomogeneous Poisson process with refractoriness (Berry and Meister, 1998); i.e., the release rate was convolved with the refractoriness function. After downsampling release rates (factor of 0.137) (Fig. 7A, dashed lines), the modeled spike rate resembles AN response and captures the essential differences in onset rate and postonset adaptation between mutants and wild types (Fig. 7C). Furthermore, the modeled first-spike latency distributions (Fig. 7D) capture the increased variance in mutant AN responses (model standard deviations were 7.4 vs 3.2 ms, compared with observed values of 5.1 vs 2.3 ms for mutants vs wild types, respectively). The downsampling of release rates required to fit the AN data may reflect differences between in vivo and in vitro conditions such as temperature and extracellular calcium concentration as well as the maximization of evoked calcium currents used in vitro (Khimich et al., 2005).

**Discussion**

Mechanisms underlying the degradation of onset coding

Each AN fiber receives synaptic input from a single IHC via a single presynaptic active zone to which a single synaptic ribbon is anchored (Liberman, 1980) (Fig. 1A). A small number of synaptic vesicles (<250) are clustered around each ribbon (Merchan-Perez and Liberman, 1996) (Fig. 1C). Each IHC ribbon synapse normally supports instantaneous AN discharge rates at a stimulus onset of over 1000 spikes/s as well as sustained sound-evoked rates up to 400 spikes/s while mediating the synchronization of spike times with stimulus periodicity at frequencies up to 4 kHz (Johnson, 1980); stimulus intensity is conveyed via discharge rate modulation, whereas timing cues are encoded in the interspike intervals. Data from the present study suggest that the primary function of the synaptic ribbon and/or Bassoon is to maintain a large readily releasable pool, enabling high rates of exocytosis and
The similar dependence of spontaneous and sound-evoked discharge rates on the electrical driving force across the apical hair cell membrane suggests similar mechanisms (Sewell, 1984a,b). Given the steady-state nature of SR measures, it is surprising that the observed (fourfold) SR reduction in mutant AN fibers was larger than that for sustained sound-evoked rates. Because of the lack of spontaneous activity under in vitro conditions, we are unable to draw any conclusions regarding the nature of SR from our model.

Genetic manipulation of Bassoon, one of the largest structural proteins at the active zone (tom Dieck et al., 1998; Richter et al., 1999; Fenster et al., 2000), could conceivably disrupt synaptic transmission through mechanisms unrelated to loss of the synaptic ribbon. Indeed, loss of Bassoon has been reported to “silence” some hippocampal glutamatergic synapses (Altrock et al., 2003). However, if the striking degradation of AN discharge rate, and onset reliability, is attributable to the loss of Bassoon, per se, rather than the absence of the ribbon, this elaborate synaptic structure must be superfluous since all other AN response properties in mutants were indistinguishable from normal.

Auditory performance: predicted effects on high-level processing

Although both spike synchronization to amplitude modulation (Rose et al., 1967; Johnson, 1980) and first-spike variance in response to stimulus onsets (Mainen and Sejnowski, 1995) (for review, see Tiesinga et al., 2008) are used to quantify “temporal precision” in the auditory system, these performance measures have different underlying requirements. Reproducibility of first-spike latency requires both reliability and precision of spiking, whereas synchrony (as it is typically measured) requires only precision. AN fibers lacking ribbons were unreliable in that spikes were not elicited by every cycle of the amplitude modulation, even at very low modulation rates. However, they were precise in that, when spikes occurred, they encoded the temporal envelope with high fidelity. Thus, the synchronization index was not degraded by ribbon loss. On the other hand, the first-spike latency metric was degraded, since decreased reliability means that, on many trials, the first spike was not evoked until long after stimulus onset (Fig. 5).

High onset rates are critical to temporal precision in the auditory periphery (Moser et al., 2006). The decrease in sound-evoked discharge rates and degradation of AN onset response in the absence of the synaptic ribbon should have profound consequences for auditory central processing. Since all mammalian IHCs, including humans’, have ribbon synapses (Liberman et al., 1990; Nadol, 1990), and since mouse AN responses are similar to other mammals’ (Kiang, 1965; Evans, 1972; Taberner and Liberman, 2005), the present results are presumably applicable to human hearing.

Rapid onsets are pervasive in the auditory environment, with many natural sounds and vocalizations characterized by sharp transients and rapid amplitude modulations (Lesica and Grothe, 2008; Elliott and Theunissen, 2009). The ability to resolve temporal structure is key for a number of auditory tasks including sound localization (Wightman and Kistler, 1992; Macpherson and Middlebrooks, 2002) and speech intelligibility (Elliott and Theunissen, 2009). Indeed, certain speech sounds can be discriminated by envelope rise time alone (Cutting and Rosner, 1974), which is encoded in the AN by differences in onset rate (Delgutte, 1980).

Many central auditory circuits rely on the precise coincidence of spikes from converging ascending inputs. For example, in the cochlear nucleus, the first stage of central auditory processing,
octopus cells are designed to respond only to stimulus onset by virtue of their short membrane time constant, which limits the temporal summation of post-synaptic potentials from numerous small AN terminals on their dendrites (Golding et al., 1995). Indeed, a large fraction of these terminals must be active within a restricted time window to produce a postsynaptic spike. The reduced reliability of onset response in bassoon mutants (Fig. 5) reduces the number of synchronous inputs at each onset, likely eliminating octopus cell responses to many rapid-onset stimuli. Onset responses may also be important in processing acoustic cues in reverberant environments (Wallach et al., 1949; Devore et al., 2009) (for review, see Litovsky et al., 1999), and the degradation of onset responses likely decreases the effectiveness of this key neural circuitry.

The neuronal coincidence detectors in the superior olivary complex, a tertiary stage of auditory processing, are also well characterized. These cells compare binaural inputs to compute the location of sounds in space by assessing interaural time differences that arise for stimuli in the azimuthal plane and are sensitive to differences in interaural times as small as 10 μs (Goldberg and Brown, 1969; Yin and Chan, 1990; Spitzer and Semple, 1995; Batra et al., 1997). The decreased reliability of onset responses in AN fibers lacking synaptic ribbons and/or bassoon may significantly compromise the ability to rapidly localize sounds using this coincidence-detection circuitry.

References


