State-space analysis on time-varying correlations in parallel spike sequences

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STATE-SPACE ANALYSIS ON TIME-VARYING CORRELATIONS IN PARALLEL SPIKE SEQUENCES

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ABSTRACT

A state-space method for simultaneously estimating time-dependent rate and higher-order correlation underlying parallel spike sequences is proposed. Discretized parallel spike sequences are modeled by a conditionally independent multivariate Bernoulli process using a log-linear link function, which contains a state of higher-order interaction factors. A nonlinear recursive filtering formula is derived from a log-quadratic approximation to the posterior distribution of the state. Together with a fixed-interval smoothing algorithm, time-dependent log-linear parameters are estimated. The smoothed estimates are optimized via EM-algorithm such that their prior covariance matrix maximizes the expected complete data log-likelihood. In addition, we perform model selection on the hierarchical log-linear state-space models to avoid over-fitting. Application of the method to simultaneously recorded neuronal spike sequences is expected to contribute to uncover dynamic cooperative activities of neurons in relation to behavior.

Index Terms— State space methods, Point processes, Generalized linear model, Correlation, Information geometry

1. INTRODUCTION

Classical studies in neurophysiology are based on the idea that stimulus information is encoded in the firing rates of single neurons. Alternatively, precise spike coordination is discussed as an indication of coordinated network activity in form of a cell assembly [1] relevant for information processing. Activation of a cell assembly predicts higher-order correlation (HOC) between the spiking activities of its member neurons [2]. Supportive evidence for this concept was provided by existence of excess synchrony among neuronal spiking activities occurring dynamically in relation to behavioral context [3, 4, 5]. However, available approaches for correlation analysis do not allow for identifying time-dependent HOCs to trace active assemblies.

To characterize higher-order interaction, the log-linear model is an useful tool because it provides a well-defined measure of correlation based on information geometry [6]. Although its natural (canonical) parameters are not orthogonal, HOCs can be extracted in a quasi-orthogonal manner from a mixture of dually affine Riemannian coordinates [7, 8]. Former studies performed a regression analysis on parallel spike trains using either a log-linear model [7, 8, 9], or the log-linear model considering up to pairwise interaction only (maximum entropy model) [10] to characterize neuronal data. The existing approaches, however, assume stationarity, a condition that is typically not fulfilled in neuronal spike data from awake behaving animals.

The state-space method [11] was suggested as a framework to model a time-dependent system by representing its parameters (states) as a Markov process. It allows to estimate a filtered/smoothed posterior distribution of the time-dependent state conditional on observed data. The approximation method for non-Gaussian point process observation in a recursive filtering algorithm was successfully applied to neuronal spike data [12, 13, 14]. Existing state-space models incorporated ensembles of spike histories into the univariate spike response model [14, 15], however, without considering correlations between the spike sequences.

In this contribution, we provide a method for estimating the dynamics of HOCs by combining the log-linear model with a state-space analysis. For that estimation, we combined a fixed-interval smoother [11] with a nonlinear recursive filtering algorithm which we derived from a log-quadratic approximation of the posterior distribution. To obtain the most predictive model, we compared goodness-of-fit of hierarchical log-linear state-space models with different order of interactions by using the Akaike’s Bayesian information criterion (ABIC) [16]. While inclusion of increasingly higher-order interaction terms improves the model accuracy, the estimation of higher-order parameters may suffer large variance due to the paucity of synchronous spikes in the data. This trade-off is optimally resolved with the model that minimizes the ABIC. The model complexity is thus selected based on the sample size as well as the prominence of higher-order structure.

An earlier version of this paper was presented in abstract form [Shimazaki, Brown, Grün, Statistical Analysis of Neuronal Data 4, Pittsburgh, May 2008].
2. METHODS

2.1. Log-linear model of higher-order interactions

We model \( N \) simultaneous spike sequences as a multivariate Bernoulli process. The processes, repeated over \( n \) trials, are discretized into \( T \) bins of bin size \( \Delta \). Let \( X^{(l)} = (X_1^{(l)}, X_2^{(l)}, \ldots, X_N^{(l)}) \) be \( N \)-tuple binary variables at \( t \)-th bin of \( l \)-th trial, where \( 1 \) denotes a bin filled with one or more spikes, and \( 0 \) denotes no spike. Let \( x = (x_1, x_2, \ldots, x_N) \) represent \( 2^N \) spike patterns, and \( \Omega_k \) be a \( k \)-subset of \( N \) elements: \( \Omega_1 = \{1, 2, \ldots, N\} \), \( \Omega_2 = \{12, 13, \ldots\} \), \( \Omega_3 = \{123, 124, \ldots\} \), etc. We define the interaction terms across the variables as \( F_i(x) = x_1 \cdot F_{ij} = x_i x_j \cdot F_{ijk} = x_i x_j x_k \) \((1 \leq i < j < k \leq N)\), etc. The log-linear model up to the \( r \)-th order interaction \( (r \leq N) \) is defined as [6]

\[
\log p_t^{(r)}(x) = -\psi_t + \sum_{i \in \Omega_1, \ldots, \Omega_r} \theta_i^t F_i(x) \tag{1}
\]

with \( \psi_t \) being a normalization parameter. \( \theta_i^t \) is a natural parameter referring to an interaction among variables indexed in the index \( i \). Let \( \theta_t = [\theta_1^t, \ldots, \theta_{12}^t, \ldots, \theta_1^t, \ldots, \theta_r^t, \ldots] \) be a \( d = \sum_{r=1}^r \binom{N}{r} \) dimensional vector. Our goal is to obtain the estimate of \( \theta_t \) from the observed parallel spike sequences.

The log-linear model belongs to the exponential family which defines a doubly flat space [6]. Its c-affine coordinate is given as the natural parameter \( \theta_t \), its m-affine coordinates as the expectation parameter \( \eta_t = [\eta_1^t, \ldots, \eta_{12}^t, \ldots, \eta_1^t, \ldots, \eta_r^t, \ldots]^t \), where

\[
\eta_i^t = E[F_i(X) \vert \theta_t] \tag{2}
\]

for \( i \in \{\Omega_1, \ldots, \Omega_r\} \). An efficient estimator of \( \eta_i^t \) is the synchrony rate defined for the \( t \)-th bin as

\[
y_i^t = \frac{1}{n} \sum_{l=1}^n F_i(X^{(l)}) \tag{3}
\]

for \( i \in \{\Omega_1, \ldots, \Omega_r\} \). Synchrony rates up to the \( r \)-th order, \( y_t = [y_1^t, \ldots, y_{12}^t, \ldots, y_1^t, \ldots, y_r^t, \ldots]^t \), constitute sufficient statistics of the log-linear model up to the \( r \)-th order interaction.

2.2. State-space analysis on the log-linear model

Assuming conditionally independent observations, the likelihood of observed spike sequences is given as

\[
p(y_{1:T} \vert \theta_{1:T}) = \prod_{t=1}^T \exp[n \cdot (y_t \theta_t - \psi_t)], \tag{4}
\]

with \( y_{1:T} = \{y_1, y_2, \ldots, y_T\} \) and \( \theta_{1:T} = \{\theta_1, \theta_2, \ldots, \theta_T\} \).

Our prior assumption is the following state equation

\[
\theta_t = F \theta_{t-1} + \xi_t, \tag{5}
\]

for \( t = 2, \ldots, T \). A random vector \( \xi_t \) \((d \times 1 \) matrix\) is drawn from a zero-mean multivariate normal distribution with a covariance matrix \( Q \) \((d \times d \) matrix\). A matrix \( F \) \((d \times d \) matrix\) is the first order autoregressive parameters. The initial value obeys \( \theta_1 \sim \mathcal{N}(\mu, \Sigma) \); \( \mu \) \((d \times 1 \) matrix\) and \( \Sigma \) \((d \times d \) matrix\). We denote the set of hyper-parameters \( w = [F, Q, \mu, \Sigma] \).

The joint probability distribution is obtained by combining the observation equation (Eq. 4) and the state equation (Eq. 5). The optimization principle for \( w \) is chosen as the maximization of the marginal log-likelihood,

\[
l(w) = \log \int p(y_{1:T}, \theta_{1:T} \vert w) d\theta_{1:T}. \tag{6}
\]

We make use of the expectation-maximization (EM) algorithm known to efficiently combining the estimation of the posterior density and the optimization of the hyper-parameter. Instead of Eq. 6, the method maximizes its lower bound,

\[
Q(w,w^*) = \mathbb{E}[\log p(y_{1:T}, \theta_{1:T} \vert w)] \mid y_{1:T}, w^*
\]

by alternating expectation (E) and maximization (M) steps. In the E-step, we obtain the expected values with respect to \( \theta_t \) in Eq. 7 using \( w^* \). In the M-step, the hyper-parameter \( w \) that maximizes Eq. 7 is obtained. The obtained \( w \) is then used for \( w^* \) in the next E-step. The details of each step are given as follows.

**E-step** Mean and covariance of the one-step prediction density \( p(\theta_t \mid y_{1:t-1}) \) for the Gaussian state transition is given as [11, 12, 13]

\[
\theta_{t|t-1} = F \theta_{t-1|t-1}, \tag{8}
\]

\[
W_{t|t-1} = F W_{t-1|t-1} F^T + Q. \tag{9}
\]

Here \( \theta_{t|s} \) and \( W_{t|s} \) are the conditional mean \( E[\theta_t \mid y_{1:s}] \) and covariance \( E[(\theta_t - \theta_{t|s})(\theta_t - \theta_{t|s})] \mid y_{1:s} \). The filter distribution is given by the Bayes’ theorem as

\[
p(\theta_t \mid y_{1:t}) = \frac{p(\theta_t \mid y_{1:t}) \cdot p(\theta_t \mid y_{1:t-1})}{p(y_{1:t} \mid y_{1:t-1})} \approx \exp[n \cdot (y_t \theta_t - \psi_t)]
\]

\[
-\frac{1}{2} (\theta_t - \theta_{t|t-1})^T W_{t|t-1}^{-1} (\theta_t - \theta_{t|t-1}). \tag{10}
\]

Here we make a Gaussian approximation to the posterior by Laplace’s method: the posterior mean, \( \theta_{t|t} \), obtained from \( \frac{\partial}{\partial \theta_t} \log p(\theta_t \mid y_{1:t}) = 0 \); the covariance is given as \(-[\frac{\partial^2}{\partial \theta_t \partial \theta_t}] \log p(\theta_t \mid y_{1:t}) \mid \theta_t = \theta_{t|t})^{-1} \). Note that the first
The mean of the initial distribution is updated with \( \mu = \theta_{1|T} \). The covariance matrix \( \Sigma \) is not updated. Instead, we use a nominal diagonal matrix as \( \Sigma \).

\begin{align*}
W_{t-1,t|T} & = E[ (\theta_{t-1} - \theta_{t-1|T})(\theta_{t} - \theta_{t|T})' | y_{1:T}] \\
& = A_{t-1} W_{t|T}. \quad (16)
\end{align*}

**M-step** Given \( \theta_{t|T}, W_{t|T}, W_{t-1,t|T} \), the update of \( w \) is given by the following equations. The covariance matrix \( Q \) and the auto-regressive parameter \( F \) are updated according to

\begin{align*}
Q & = \frac{1}{T-1} \sum_{t=2}^{T} (W_{t|T} - W_{t-1,t|T}F') \\
& \quad - FW'_{t-1,t|T} + FW_{t-1|T}F' \\
& + \frac{1}{T-1} \sum_{t=2}^{T} (\theta_{t|T} - F\theta_{t-1|T})(\theta_{t|T} - F\theta_{t-1|T})' \quad (17)
\end{align*}

and

\begin{align*}
F & = \left[ \sum_{t=2}^{T} (W_{t-1,t|T} + \theta_{t|T}\theta'_{t-1|T}) \right]^{-1} \\
& \cdot \left[ \sum_{t=2}^{T} (W_{t-1|T} + \theta_{t-1|T}\theta'_{t-1|T}) \right]. \quad (18)
\end{align*}

The mean of the initial distribution is updated with \( \mu = \theta_{1|T} \).

The covariance matrix \( \Sigma \) is not updated. Instead, we use a nominal diagonal matrix as \( \Sigma \).
Table 1. The ABIC of the r-th order log-linear model applied to data of different number of trials n (data shown in Fig.1-A). The asterisk indicates the model that minimizes the ABIC.

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2.3. Model Selection

Let us define a log-linear space-state model with up to the r-th order interaction by $E_r$. Since $E_r$ is a submanifold of $E_{r+1}$, the log-linear models naturally form hierarchical structure, $E_1 \subset E_2 \subset \cdots \subset E_N$. Comparison of the hierarchical models is performed by computing the ABIC [16]:

$$\text{ABIC} = -2l(w) + 2 \dim w. \quad (19)$$

The marginal log-likelihood is computed by using the one-step prediction formula for the mean Eq. 8 as $l(w) = \sum_{t=1}^{T} \log p(y_{it}|y_{1:t-1}, w) \approx n \sum_{t=1}^{T} (y_{it}\theta_{i1t-1} + \psi_{t-1})$.

3. RESULTS

We applied the method to $N = 3$ parallel spike sequences with $n = 100$ repetitions (Fig.1-A), generated by a time-dependent log-linear model (Fig.1-B, dashed lines). Figure 1-B (solid lines) shows the estimates of the log-linear parameters from the data in Figure 1-A. The gray band is the 99% credible interval of the marginalized posterior distribution $p(\theta_i^t | y_{1:T})$ for $i \in \{\Omega_1, \Omega_2, \Omega_3\}$. Note that parameter $\theta_{i123}^t$ indicates triplewise correlation, i.e. excess synchrony compared to expectation given pairwise correlations.

While the full model ($E_3$) is an unbiased model for the triple binary sequences, the fitted parameter for the triplewise correlation $\theta_{i123}^t$ may suffer large variance (over-fitting) due to the paucity of triplet synchrony. Thus a submodel with $r < 3$ can be close to the generative model in terms of the Kullback-Leibler risk. To validate that the inclusion of the triplewise correlation improves the goodness-of-fit, we computed the ABICs for the hierarchical models ($r = 1, 2, 3$) as shown in Table 1. To test the influence of the sample size of the data upon the model selection, we varied the number of trials $n$ used to fit the hierarchical log-linear models. For small number of trials ($n = 5$), the model without correlation structure was selected. With increasing trial numbers, models with increasing correlation orders were selected. For $n = 50, 100, \text{and} 200$, the full model predicts best.

4. CONCLUSION

We developed a method for identifying the time-varying higher-order correlation structure in parallel spike sequences. Its application to simultaneous recordings of neuronal activity is expected to provide us with new insights into the dynamics of assembly activities, their composition and behavioral relevance.

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5. REFERENCES