The Disque Platform for the Investigation of Islet Differentiation to Study, Treat, and Cure Type 1 Diabetes

by

Peter Anthony Jones

B.S. Plastics Engineering University of Massachusetts Lowell, 2014

B.A. International Business Administration American University of Paris, 2006

SUBMITTED TO THE PROGRAM IN HEALTH SCIENCES AND TECHNOLOGY IN PARTIAL FULFILLMENT OF THE REQUIREMENTS FOR THE DEGREE OF

> MASTER OF SCIENCE IN HEALTH SCIENCES AND TECHNOLOGY, CONCENTRATION AREA: MECHANICAL ENGINEERING AT THE

> > MASSACHUSETTS INSTITUTE OF TECHNOLOGY

JUNE 2017



ARCHIVES

© Peter Anthony Jones. All rights reserved.

The author hereby grants to MIT permission to reproduce and to distribute publicly paper and electronic copies of this thesis document in whole or in part in any medium now known or hereafter created.

Signature redacted

Signature of Author:

/ Reogram in Health Sciences and Technology May 22, 2017

Certified by:

Signature redacted Jeffrey M. Karp Associate Professor of Medicine, Brigham and Women's Hospital, Harvard Medical School **Thesis Supervisor**

Signature redacted

Accepted by:

Emery N. Brown, MD, PhD

Director, Harvard-MIT Program in Health Sciences and Technology Professor of Computational Neuroscience and Health Sciences and Technology

The Disque Platform for the Investigation of Islet Differentiation to Study, Treat, and Cure Type 1 Diabetes

by

Peter Anthony Jones

Submitted to the Program in Health Sciences and Technology on May 22, 2017 in Partial Fulfillment of the Requirements for the Degree of Master of Science in Health Sciences and Technology

ABSTRACT

There is a critical health care need to generate large numbers of beta cells for transplantation. In Type 1 Diabetes (T1D), insulin-producing beta cells in the islets of Langerhans within the pancreas, which support glucose homeostasis, are destroyed in an autoimmune attack. The ensuing loss of glycemic control leads to serious complications, requiring life-long insulin injections and close monitoring, while shortening lifespan by 11-13 years. In the face of a three percent annual increase in T1D incidence, there is a grave lack of transplantable material, and very few patients are able to receive an islet transplant each year. Recent advances in stem cell differentiation have enabled the production of large quantities of insulin-producing beta-like cells *in vitro*, bringing hope to the field. However, the efficiency and yield of such production methods remains unacceptably low, with high batch-to-batch variability, and the function of these cells is unstable. Moreover, the ability to probe the conditions that affect differentiation outcomes is limited by the scale, cost, and complexity of existing culture systems.

The present work focuses on the Disque Platform, a biomimetic screening platform for the investigation of islet cell differentiation. The Disque Platform allows for the formation of differentiating 3D micro-tissues within an automation-friendly design, and is capable of systematically manipulating the developing stem cell niche in order to identify chemical and physical cues that enhance beta cell production. Significantly, the Disque Platform consistently differentiates beta-like cells from pancreatic progenitor cells, with similar efficacy to existing high-volume production methods. Furthermore, it achieves superior differentiation outcomes compared to the 2D culture systems tested, and is able to respond to interventions when conventional systems cannot produce a clear signal or readout. Together, these data support the ability of the Disque Platform to investigate specific interventions to enhance beta-cell differentiation. It is hoped that the Disque Platform can serve as a springboard for beta cell and islet study within the diabetes community, and that these advances can contribute towards a cure for Type 1 Diabetes.

Thesis Supervisor: Jeffrey M. Karp

Title: Associate Professor of Medicine, Brigham and Women's Hospital, Harvard Medical School

Table of Contents

BACKGROUND & SIGNIFICANCE	4
Beta Cell Loss in Type 1 and Type 2 Diabetes	4
Beta Cell Replacement Therapy: Promise and Limitations	4
A Device to Interrogate Methods to Enhance Beta Cell Differentiation from Stem Cells	5
SPECIFIC AIM 1: TO CREATE A 3D CULTURE SYSTEM FOR BETA CELL DIFFERENTIATION, WITH CONTROLLED PRESENTATION OF	MICRO-
ENVIRONMENTAL CUES.	5
SPECIFIC AIM 2: TO UTILIZE THE 3D CULTURE SYSTEM AS A SCREENING TOOL TO INTERROGATE VARIOUS MICROENVIRONMEN	1TS
(CHEMICAL AND MECHANICAL CUES) AND CULTURE CONDITIONS TO ENHANCE THE BETA-CELL DIFFERENTIATION EFFICIENCY A	ND YIELD6
	<i>c</i>
	0
SPECIFIC AIM 1: BUILDING A 3D CULTURE SYSTEM FOR BETA CELL DIFFERENTIATION	
The Disque Platform for Beta Cell Differentiation	0
Diffusion Gradients and Suspension Culture Differentiation of Beta-Cell Clusters	
Optimization of 3D Culture Conditions for Beta Cell Differentiation	8
Cell Discs Form Cell-Cell Junctions Critical for Islet Function	10
The Disque Platform Supports High Viability During Multi-Week Culture	
The Disque Platform Replicates Key Outcomes of Spinner Flask Differentiation	
The Disque Platform Shows More Promise for Screening Versus Simpler Culture Methods	
The Disque Platform: A Springboard for the Study of Islet Differentiation	
SPECIFIC AIM 2: IDENTIFYING MICROENVIRONMENTS TO ENHANCE BETA CELL DIFFERENTIATION	15
Mechanical and ECM Microenvironments and Beta Cell Differentiation	15
RADA16-I Oligopeptide Gels Mimic Pancreatic Stiffness	16
DISCUSSION	17
	10
FUTURE WURK	10
Simultaneous Dijjerentiation oj Bela, Alpha, ana Della Cens	10
Oxidative Sterss and Beta Cell Differentiation	
Giucose and Bela Cell Dijjerentiation	
Investigating Developmental Pathways and Cell-Cell Signaling	
Generation of Transplantable Waterial to Cure 11D in Vivo	20
Disease Modeling of Beta Cells in T1D: Redox imbalance and Beta Cell Death	20
METHODS	21
Manufacturing Custom Cell Culture Inserts with Reducing Washer	21
Gel Preparation and ECM Coating	21
Cell Seeding: Forming a Thin Cell Disc within the Disque Platform	21
Cell Disc Removal for Downstream Analysis	21
Cryosectioning and IHC	22
96-Well Multi-Color Flow Cytometry	22
Measurement of Gel Modulus	22
ACKNOWLEDGEMENTS	23
STUDENT'S INVOLVEMENT IN THE RESEARCH	23
	24
JUFFLEIVIEIVIAL DATA Temperature- and Time-Dependent Shear Droperties of DuraMatriv™ and Matriael®	, 24 2 <i>1</i>
Expression of Other Differentiation Markers on the Disque Platform	24 76
Expression of Other Differentiation Warkers on the Disque Platform	20 27
Filot resump of Notich Activator and Innotici Cockluis	,∠/ 27
בוופני טן דומוומוווץ מווע דרמווצףטרגמנוטון טון שבנע כפון שווופרונומנוטון	
REFERENCES	28

BACKGROUND & SIGNIFICANCE

Beta Cell Loss in Type 1 and Type 2 Diabetes

Pancreatic beta cell loss is a common feature of both T1D and advanced T2D¹, leading to the gradual loss of insulin production and of glycemic control². Patients who have lost their insulin-producing β cells live with a constant risk of ketoacidosis and hypoglycemic coma, and often suffer from long-term complications such as heart disease, stroke, kidney failure, foot ulcers, diabetic retinopathy, and shortened lifespan by 11-13 years. Diabetes burdened the U.S. economy at a level equal to 2% of annual GDP in 2012, or \$322 billion, of which \$6.2 billion alone was due to injectable insulin, and this cost increases steadily each year.³

Beta Cell Replacement Therapy: Promise and Limitations

There is currently no durable and effective treatment for β -cell loss⁴, and constant monitoring and insulin injections are mandatory for life. Whole pancreas or islet transplantation can represent a multi-year cure for insulin-dependent patients, however there is an extremely limited supply of transplantable material. This lack of material had held back the promise of β -cell replacement therapy, until the recent development of protocols to differentiate stem cells into β cells, by Melton Lab at Harvard University and other researchers in the field.^{5,6}

Although these β cell protocols are capable of producing large quantities of transplantable material in spinner flasks or bioreactors, they have been faced with several limitations. Notably, there is wide batch-to-batch variability, with final yields between 10% and 30% β -like cells per batch as compared to ~70% β cells on average in native human islets (**Fig.** 1). These stem-cell-derived β -like cells (SC- β cells) lack complete and stable function. Furthermore, the remaining 70% to 90% of non- β -like cells present at the end of the process include unidentified phenotypes that are not controlled by current protocols. Finally, current protocols focus on differentiating one islet cell type at a time and are missing glucagon-producing alpha cells and somatostatin-producing delta cells, which work together with beta cells to control blood sugar in a paracrine feedback system. Such drawbacks severely limit the utility of SC- β cells for transplantation and *in vitro* disease modeling.

There is an urgent need to develop more efficient and effective stem cell differentiation protocols in order to improve the supply of functional β cells for transplantation. Unfortunately, screening for methods to enhance β -cell differentiation directly in spinner flask culture is costly and time-consuming due to its scale. In addition, current 2D culture systems are only capable of measuring immediate effects (due to a dramatic increase in variability after only 3-4 days), while existing 3D culture systems are complex and not amenable to automation and mediumto high-throughput screening. A three-dimensional culture system is a requirement for differentiation, since tissue morphogenesis during development depends on both cell-cell and cell-environment interactions.⁷ In the case of islet differentiation, it has been reported that hESCs cultured within a soft Matrigel-Collagen type I scaffold expressed higher levels of pancreatic and endocrine markers versus 2D culture.⁸



Figure 1. The Melton Lab β -cell differentiation protocol summary and key outcomes. The protocol is organized into stages, and key differentiation markers are assessed at the end of each stage. Stage 4 day 1 (S4d1) corresponds approximately *in vitro* to the beginning of the pancreatic progenitor stage, when nearly all cells are pancreatic in origin (express Pdx1). By Stage 4 Complete (S4-C), on average ~40% of cells express Nkx6.1, an insulin gene promoting transcription factor. Nkx6.1 expression in a cell is a pre-requisite for subsequent insulin expression.

A Device to Interrogate Methods to Enhance Beta Cell Differentiation from Stem Cells

In light of the limitations to studying β -cell differentiation in currently-available cell culture devices, we set out to create a platform to interrogate soluble and mechanical cues within the differentiating stem cell niche that play a central role in determining β cell differentiation outcomes. Since β cells require cell-cell contact to survive and function, and since β -cell differentiation generally occurs more efficiently in 3D versus 2D culture⁹, we identified the need for a 3D biomimetic culture system that would allow us to study the entire course of the differentiation and to develop fully functional β cell micro-tissues.

This automation-friendly, 3D culture platform can be utilized to enhance the function and viability of differentiated SC- β cells *in vitro*. These cells have the potential to transform β cell replacement into a viable therapy for insulin-dependent diabetics. In addition, such a system may be uniquely suited for: the direct generation of transplantable material; disease modeling of immune- β cell interactions in T1D and β -cell death in T1D/T2D; and drug discovery and toxicology.

Specific Aim 1: To create a 3D culture system for Beta cell differentiation, with controlled presentation of micro-environmental cues.

- Culture System Requirements:
 - \circ The system should form β -cell micro-tissues with cell-cell junctions, with the ability to incorporate extracellular matrix components.
 - The system must maintain high cell viability for multi-week differentiations.
 - The system must have reliable and consistent read-outs by imaging and high-throughput phenotypic analysis.
 - The system must be simple and automation-friendly.

- The system should match (gold standard) spinner flask differentiation outcomes in terms of the expression of key pancreatic endocrine markers.
- The system should produce measurable changes in differentiation outcomes in response to changes in the microenvironment.
- Hypothesis 1: Differentiating pancreatic progenitor cells in direct contact will lead to the formation of a 3D micro-tissue with cell-cell junctions.
- Hypothesis 2: A 3D culture system with controlled diffusion distance will enhance cell viability and lead to more better differentiation outcomes.
- Hypothesis 3: A 3D culture system based on these design principles will better predict differentiation outcomes compared to 2D culture systems.

<u>Specific Aim 2</u>: To utilize the 3D culture system as a screening tool to interrogate various microenvironments (chemical and mechanical cues) and culture conditions to enhance the beta-cell differentiation efficiency and yield.

• A wide variety of chemical and mechanical factors within the developing stem cell microenvironment can impact cell fate decisions, including: exogenous cytokines and growth factors, ECM composition, stiffness, juxtacrine and paracrine interactions with neighboring cells such as endothelial cells, temperature, pH, media composition, perfusion, oxygen tension, cell-cell junctions, redox balance, etc.

RESULTS

Specific Aim 1: Building a 3D Culture System for Beta Cell Differentiation

"To create an 3D culture system for beta-cell differentiation, with controlled presentation of microenvironmental cues."

The Disque Platform for Beta Cell Differentiation

The Disque Platform is an in vitro culture system designed to create 3D biomimetic pseudo-islets for improved pancreatic β -cell differentiation. Dispersed pancreatic progenitor cells are re-aggregated into cell discs, which are situated in a custom cell culture insert in a standard 24-well plate, amenable to medium-throughput manipulations. (**Fig. 2**) The thick cell layer allows cell-cell contact, which is essential for juxtacrine (contact-dependent) signaling such as Notch signaling in development, and for gap junction communication for coordinating insulin secretion in mature β cells.



Figure 2. The Disque Platform

The Disque Platform enables the formation of thin cell discs made up of β -like cells for the study of β -cell differentiation. (**Fig. 3**) A custom reducing washer can be set into the bottom of the cell culture insert, which reduces the cell culture area and allows for simple ejection of the disc and the underlying membrane by applying a downward force on the edges of the washer. If desired, extracellular matrix components and gels with defined mechanical properties can be integrated into the cell disc at the time of seeding. Soluble cues can be integrated into the culture medium both above and below the cell disc. The cell discs can be sectioned or left intact for imaging.



Representative sample from n = 1 biological batch.

Figure 3. Cross-section of a thin β cell disc on the Disque Platform, illustrating the expression of key β -cell markers. Pdx-1 expression indicates pancreatic origin; Nkx-6.1 is an insulin gene-promoting transcription factor; and C-peptide is co-expressed with insulin in β cells. The image was generated by confocal microscopy of a 15- μ m cross section of a cell disc, stained by immunohistochemistry.

Diffusion Gradients and Suspension Culture Differentiation of Beta-Cell Clusters

Gradients in morphogen concentrations and central hypoxia are inherent challenges to cultured embryoid bodies and cell spheroids, since gradients over length scales of just 100 to 200 μ m are known to drive cell specification in development.^{10–12} Indeed, attempts by others to

reduce the effects of morphogen gradients have led to more uniform differentiation of other cell types.^{13,14} We hypothesize that cytokine and oxygen gradients drive inhomogeneous cell specification in cell clusters *in vitro*. Such a phenomenon may become especially problematic when feeding high molecular weight growth factors to cell clusters with the goal of activating surface receptors that affect cell fate, since such factors may not diffuse readily between cells, and may form a morphogen gradient from the periphery to the core of each cluster.¹⁵ Three such molecules, Activin A, KGF and betacellulin, each on the order of 20 kDa, are added to the media during β -cell differentiation.

In a pilot study to model the diffusion of large molecules such as growth factors, a diffusible 10-kDa dextran probe was used to investigate gradients within SC- β cell clusters. This study found that the probe formed a gradient within the first 50 μ m from the periphery of SC- β cell clusters that had been differentiated in spinner flask culture. (Fig. 4) This result is consistent with other findings in the literature for the diffusion of growth factors such as EGF.¹⁶



Figure 4. Dextran diffusion within SC- β cell clusters taken from spinner flask suspension culture, after a 4-hour incubation in 0.125 mg/ml 10-kDa Texas Red dextran. Clusters were fixed, cryosectioned, imaged by confocal microscopy, and then analyzed using mean gray value along concentric circles in ImageJ. Three representative clusters were used to generate the data.

Optimization of 3D Culture Conditions for Beta Cell Differentiation

In suspension culture in a spinner flask or bioreactor, convection helps with oxygenation and mass transport. However, there are inherent viability issues with static 3D cultures. Therefore, it was necessary to identify conditions to maximize their viability.

The Disque Platform enables the formation of thin 3D cell discs with a defined thickness and diffusion distance for the controlled presentation of soluble cues, such as oxygen, nutrients, and cytokines. Since the cell disc is suspended on a permeable membrane within a custom cell culture insert, diffusion can occur from both above and below. The thickness of the 3D cell disc in the Disque Platform can be precisely regulated by changing the seeding density. (**Fig. 5A/B**) The reduced diffusion distance in thin cell discs is hypothesized to result in enhanced viability, minimized phenotypic heterogeneity and enrichment for the β cell phenotype. A coreshell structure forms in many spinner flask-cultured clusters, although it does not appear consistently in all batches, which may be a result of necrosis due to central hypoxia from O₂ diffusion limits¹⁷, or perhaps from the development of a blastocoel-like structure during *in vitro* differentiation. In the Disque Platform, a thin cell disc approximately 50 µm in thickness was shown to have high viability throughout the cell layer, while retaining expression of key β -cell markers. (**Fig. 5C**)



of Melton Lab.

Figure 5. (A) Seeding density precisely controls the final thickness of the 3D cell disc on the Disque Platform, and (B) this can be fit to a linear model with a coefficient of determination of $R^2 = 0.99$. (C) Cell clusters cultured in suspension (spinner flask) sometimes exhibit a core-shell structure. This structure is not observed on the Disque Platform. Immunostaining of representative cryosectioned cell discs and clusters shows live (fluorescein diacetate), dead cells (propidium iodide), nuclei (DAPI), Nkx-6.1, and C-peptide. Representative images of spinner flask clusters were taken from n > 50 clusters across ≥ 3 biological batches, and representative images of cell discs were taken from $n \ge 3$ differentiated cell discs.

Oxygen forms a gradient from the air-liquid interface to the surface of the cultured cells.¹⁵ Due to this fact, we hypothesized that a shorter media height would improve viability of the cell disc. Therefore, we set out to determine the optimum media height above the 3D cell discs. In a pilot study, it was found that reducing the media column height to 4.5 mm ensured sufficiently high cell disc viability, and the media did not excessively evaporate between media changes. (**Fig. 6A**) Future studies will determine whether reducing the media height further

could provide benefits beyond enhanced viability, such as enhanced Neurogenin3 expression due to repression of HIF1 α , as has been found in the example of air-liquid interface differentiation of β cells.^{6,18}

Oxygen and other soluble factors also form a gradient from the periphery to the core of any 3D culture construct.¹⁵ In a second pilot study, it was found that setting the cell disc thickness to 50 μ m maximized the cell disc viability, however the effect of reducing disc thickness on improving viability was not large in the range studied, likely because oxygen diffuses readily into tissue at all the thicknesses tested. (**Fig. 6B**)

We then hypothesized that limiting the disc thickness would also improve key differentiation outcomes, such as the expression of key endocrine progenitor markers. In a third pilot study carried out twice in separate biological batches, minimizing the cell disc thickness to 50 μ m (and thus the maximum diffusion distance to 25 μ m) maximized Pdx1 and Nkx6.1 co-expression in Disque Culture. This may be due to gradients of soluble cues that contribute toward driving the differentiation. (**Fig. 6C**)



Figure 6. Correlation between diffusion-related cell culture parameters, viability, and differentiation outcomes. Each experiment was carried out on a different biological batch of differentiating cells. (A) Correlation between media height above the cell disc and viability. A linear model provides a coefficient of determination equal to 0.98. (B) Estimated disc thickness and the percentage of viable cells in the disc. (C) Correlation between the estimated diffusion distance (half of the thickness) and the percentage of cells that became pancreatic endocrine progenitors after 5-day differentiations from two biological batches (co-expression of Pdx-1 and Nkx-6.1). A one-phase exponential fit gives R² = 0.80 for both differentiations.

Cell Discs Form Cell-Cell Junctions Critical for Islet Function

Cell-cell junctions play a role in contact-dependent signaling in development and mediate glucose-dependent insulin secretion in mature islets.¹⁹ We hypothesized that differentiating pancreatic progenitor cells in direct contact will lead to the formation of a 3D micro-tissue with cell-cell junctions. The preserved 3D architecture of the Disque Platform is a key requirement for β -cell differentiation and disease modeling, since dispersed β cells quickly lose their function *in vitro*. It was found that dispersed pancreatic progenitor clusters initially grown in suspension culture can successfully re-form a differentiating micro-tissue within the Disque Platform. (**Fig. 7**) In addition, confocal imaging can be performed directly on 50-µm cell discs without the need for sectioning.



Figure 7. Representative image of a cell disc on the Disque Platform cultured on a thin layer of laminin and collagen IV, taken at the pancreatic endocrine progenitor stage after 5 days in culture. Taken by confocal microscopy through the disc without sectioning. Background corrected by comparison to unstained controls. Adherens junctions (E-cadherin) indicate the initiation of cell-cell contacts. Tight junctions (ZO-1) indicate the potential for polarity and the gating of ions and solutes between cells. Gap junctions (Connexin-36, not shown) play a role in the synchronization of insulin secretion through the exchange of current-carrying ions between cells.

The Disque Platform Supports High Viability During Multi-Week Culture

We hypothesized that the optimized cell culture parameters would promote high viability despite moving from suspension culture (spinner flask) to static 3D culture (Disque Platform). Indeed, the Disque Platform (with optimized culture parameters) achieves comparable high viability to Spinner Flask culture during pancreatic progenitor differentiation to endocrine progenitors. (**Fig. 8A**) The ability to recapitulate suspension culture in a 3D static culture format suggests its utility for studying β -cell differentiation. After optimizing the 3D culture conditions, the Disque Platform maintains the high viability required for multi-week differentiations. (**Fig. 8B**)



Figure 8. The percentage of viable cells in the 3D cell disc versus same-batch spinner flask clusters during differentiation from pancreatic progenitors, assessed by Zombie UV dye exclusion and flow cytometry. (A) Viability at the endocrine progenitor stage (S4-Complete, S4-C) after a 5-day differentiation from pancreatic progenitors (Stage4 day1, S4d1), shown as an average of 5 experimental repeats with $n \ge 3$ differentiations per repeat. (B) Viability during the course of an 18-day differentiation from pancreatic progenitors (S4d1) to SC- β cells (Stage6 day7, S6d7).

The Disque Platform Replicates Key Outcomes of Spinner Flask Differentiation

In the Disque Platform, Nkx-6.1 expression levels increased synchronously with the spinner flask. Nkx-6.1 is a critical transcription factor that promotes insulin gene expression. This is a baseline result that suggests the platform's potential utility to predict the response of Spinner Flask-cultured cell clusters to conditions and signals. (**Fig. 9**)





The Disque Platform with optimized baseline culture parameters is able to achieve comparable differentiation outcomes to spinner flask cultures for stem cell-derived pancreatic progenitors. This result confirms that the cell discs on the Disque Platform recapitulate key outcomes of spinner flask-cultured clusters in suspension. (**Fig. 10A**) In addition, the Disque Platform can produce C-peptide-expressing β -like cells if allowed to differentiate for longer periods of time. (**Fig. 10B**) See the Supplemental Data for additional information on expression of key differentiation markers in both culture systems.



Figure 10. Key transcription factor expression after differentiation on the Disque Platform. (A) Six nonsimultaneous experimental repeats of side-by-side 5-day differentiations from pancreatic progenitors (S4d1 to S4-C, six experiments with $n \ge 4$ Disque Platform differentiations per experiment). Each experimental repeat was started from a matched batch pancreatic progenitor cells. Shows the percentage of cells expressing each marker on the final day of each experiment. (B) The Disque Platform generated 6.8% β -like cells after a 12-day differentiation from pancreatic progenitors (S4d1 to S6d1, n = 3 differentiations seeded from a single batch of pancreatic progenitors), defined as cells which co-express Pdx1, Nkx6.1, Chromogranin-A, and C-peptide/proinsulin.

The Disque Platform Shows More Promise for Screening Versus Simpler Culture Methods

Although the Disque Platform is relatively straightforward to set up, it is still more complex and costly compared to traditional screening assays such as 96-well or 384-well planar culture or monolayer culture on Matrigel. Therefore, we set out to determine whether a simpler culture system could effectively measure the effects of microenvironmental manipulations on β -cell differentiation. We hypothesized that a thick cell layer with cell-cell contact would promote a more effective differentiation. We also hypothesized that placing the cell layer on a cell culture insert surrounded by media on the top and bottom would enable improved differentiation outcomes. Finally, we hypothesized that the Disque Platform would more effectively sense the effects of changes in chemical and physical cues, and that this would be reflected by the ability to detect significant changes in differentiation outcomes.

Various cell culture systems were compared to evaluate their ability to differentiate endocrine cells from pancreatic progenitors over the course of five days. A differentiation cocktail consisting of cytokines and growth factors was added to the media, and each cell culture system was analyzed to determine whether these chemical signals could produce a detectable change in differentiation outcomes. Although all the cell culture systems exhibited high viability (**Fig. 11A**), the percentages of Nkx6.1 Pdx1 co-positive cells varied significantly. Monolayer culture generally had poor differentiation outcomes, whereas culture on the Disque Platform led to expression levels similar to those obtained in the matched spinner flask. (**Fig. 11B**) Moreover, the multi-layer cell culture systems were able to reflect changes soluble cues that the monolayer systems could not. Also, a chemically-defined Matrigel-free system is sufficient to produce this effect. (**Fig. 11C**) Future investigations will determine whether a collagen IV/laminin coating is required, and whether a monolayer on a cell culture insert could produce an effective differentiation. Overall, this data suggests that a system such as the Disque Platform is better able to predict changes in β -cell differentiation based on the addition of soluble cues compared to the other methods tested. This data also suggests that the presence of a multilayer cell aggregate is a pre-requisite for endocrine differentiation.



Figure 11. Culture method comparison. The Disque Platform is comprised of a 50-µm thick cell layer on a collagen IV and laminin-coated custom cell culture insert. (A) All cell culture systems supported high viability, as determined by Zombie UV dye exclusion by flow cytometry. (B) Nkx6.1 Pdx1 co-expression by culture method after a 5-day differentiation from pancreatic progenitors. Cells in a monolayer on either tissue culture polystyrene (TCPS) or Matrigel showed poor differentiation outcomes compared to culture of a thick cell layer on a custom cell culture insert. (C) The effect of a differentiation cocktail on differentiation outcomes within each cell culture platform. (N = 5 Disque Platform differentiations per condition from a single batch of pancreatic progenitors.)

The Disque Platform: A Springboard for the Study of Islet Differentiation

Together, these data support the ability of the Disque Platform to investigate specific interventions to enhance the β -cell differentiation from pancreatic progenitors, for disease modeling, drug screening, and transplantation. Due to its innovative format, the Disque Platform is uniquely suited for medium- to high-throughput studies: all steps have been designed in a format amenable to automation. Furthermore, its ability to support long-term multi-week viability raises the possibility of using the Disque Platform to sustain native islets in preparation for transplantation. We believe that the Disque 3D Islet Culture Platform can serve as a springboard for β cell and islet study within the diabetes community.

Specific Aim 2: Identifying Microenvironments to Enhance Beta Cell Differentiation

"To utilize the 3D culture system as a screening tool to interrogate various microenvironments (chemical and mechanical cues) and culture conditions to enhance the 6 cell differentiation efficiency and yield."

Mechanical and ECM Microenvironments and Beta Cell Differentiation

The Disque Platform is distinct from monolayer or spinner-flask suspension culture, as the 3D cell disc may be cultured directly on ECM or may have ECM components incorporated, allowing for the investigation of mechanical cues critical for β -cell development. The simplicity and automation-friendliness of our platform show greater promise for ECM composition and general screening purposes in comparison to 3D culture with matrigel, alginate encapsulation, and other common 3D culture methods²⁰. The Disque Platform is well suited for the manipulation of the developmental niche, including tissue architecture (stiffness and ECM composition), paracrine and juxtacrine signaling, morphogen gradients, oxygen tension, and coculture with other islet, endothelial, nerve, or immune cells, among other factors.

A key feature of the islet microenvironment is tissue stiffness. The pancreas is known to be a soft organ, with an elastic modulus in the range of ~1-2 kPa.^{21,22} Cells sense and respond to the stiffness of their surroundings by mechanotransduction, and their mechanical microenvironment serves as a physical cue that plays a role in driving differentiation or dedifferentiation.^{23,24} In addition, cells have a memory of past physical environments that conditions their future fate even after changing to a new physical environment.²⁵

In the case of islet differentiation, a more efficient pancreatic progenitor differentiation has been achieved within alginate gel capsules of ~4-7 kPa versus those of ~22-73 kPa (elastic modulus). (However, all of the capsules tested in that case were harder than native pancreas.) The harder capsules were found to upregulate the sonic hedgehog pathway as measured by downstream expression of the transcription factor GL11, which suppressed PDX1 expression.²⁶ Sonic hedgehog (Shh) is excluded from pancreatic tissue in several species, and elevated SHH expression is known to impair pancreas organogenesis while promoting liver bud formation. It has been proposed that Shh plays different roles at different stages of development, restricting pancreatic growth early on yet supporting β -cell differentiation and function during islet formation.²⁷ We therefore hypothesized that softer substrates in the range of 1-2 kPa would help to maintain Pdx1 expression during the differentiation from PDX1-expressing pancreatic progenitors to NKX6.1-expressing endocrine progenitors. In addition, we reasoned that SHH pathway activation may affect cells differently when they have already acquired PDX1 expression. We also reckoned that softer substrates would inhibit SHH activation, and that the molecule KAAD-cyclopamine (CYC), which inhibits the SHH pathway through the receptor smoothened, would accentuate any SHH inhibition provided by a softer substrate, and this would be seen through lower GLI1 expression.

We identified a commercially-available, chemically-defined, transparent hydrogel with tunable mechanical properties called PuraMatrix[™]. PuraMatrix[™] is an aqueous solution of the 16-residue peptide RADA16-I, which contains four repeats of the amino acid sequence RADA (arginine-alanine-aspartate-alanine). When exposed to millimolar quantities of monovalent cations, it self-assembles into a transparent hydrogel made up of β sheets with a fibril size on the order of ~10 nm and pore diameter of ~5-200 nm, analogous to native ECM.^{28,29} When used in concentrations from 0.1% to 3%, PuraMatrix[™] has tunable mechanical properties in the range of ~0.2-10 kPa (shear storage modulus)^{30–32} and a Poisson's ratio of 0.47 similar to other hydrogels.³³ We thus reasoned that it would be possible to mimic the islet mechanical microenvironment by controlling the concentration of RADA16 in solution.

RADA16-I Oligopeptide Gels Mimic Pancreatic Stiffness

Rheological testing confirmed that the storage modulus of PuraMatrix gels increased in a concentration-dependent manner, and that concentrations of PuraMatrix between 0.2% and 0.3% mimicked the stiffness of native healthy pancreatic tissue. PuraMatrix exhibited a mean modulus of elasticity of 1.3 \pm 0.3 kPa at 0.2%, 1.7 \pm 0.5 kPa at 0.25%, 2.5 \pm 0.8 kPa at 0.3%, 2.8 \pm 0.5 kPa at 0.4%, and 6.3 \pm 2.0 kPa at 0.5%. (**Fig. 12**)

Upcoming studies will determine whether softer gels can aid in Pdx1 retention and whether gel stiffness influences the acquisition of Nkx6.1 expression. In addition, future studies will evaluate whether changes in the differentiation due to the modulation of stiffness occur through the sonic hedgehog pathway, and whether these effects could be mimicked or amplified through the use of a sonic hedgehog pathway inhibitor such as KAAD-cyclopamine (CYC).



Figure 12. Modulating the mechanical microenvironment for β -cell differentiation with an oligopeptide hydrogel on the Disque Platform. (A) Changing the concentration of PuraMatrixTM in solution controlled the stiffness of the hydrogel ($n \ge 3$ gels per condition, except n = 2 gels for 0.5% PuraMatrix). (B) Modulating the concentration of PuraMatrixTM allowed for matching the pancreatic stiffness. Reference data adapted from Sugimoto 2014²¹, Shi 2015²², and the Technical Datasheet for INEOS Styrolution 1300/1301 polystyrene for medical labware³⁴. (C) Storage modulus (G') greater than loss modulus (G'') indicates gel formation, and parallel G' vs. G'' across a wide frequency range indicates gel stability. A frequency-dependent complex viscosity (shear thinning) indicated that the gels behave more like a fluid at higher shear rates.

DISCUSSION

Performing the differentiation process in a multi-well format on the Disque Platform enables the preservation of 3D tissue architecture and the investigation of variables that play a role in cell specification, and in particular, the enrichment of pancreatic β -cells *in vitro*, in a higher-throughput manner. In addition, the Disque Platform enables the detection of changes in differentiation outcomes in response to soluble cues, which simpler culture systems could not detect.

With the characterization and optimization of the Disque Platform, we now have a powerful tool in hand to address interesting and critical questions regarding β -cell biology, and to ascertain 3D microenvironments that best support maturation of pancreatic progenitor cells into functional insulin-producing β cells.

The Disque Platform can easily accommodate 3D culture of a different cell type, and it is also amenable to use as a co-culture system. The preserved 3D architecture is an important aspect for the Disque Platform to be used in diabetes disease modeling as well as drug screening purposes. Finally, thin cell discs hold promise as a novel transplantation strategy requiring further testing to transition from *in vitro* cultures to *in vivo* implementations.

Despite its advantages for studying β -cell differentiation, the Disque Platform in its current form does have limitations. First, it requires 800,000 cells per well to form a 50-µm thick cell disc, which means that a reliable high-volume cell source must be available. We are fortunate to collaborate with Melton Lab at Harvard, which has extensive experience in scaling up differentiation from stem cells. Efforts are underway to optimize culture conditions to enable moving from a 24- to a 96-well format for high-throughput screening. Second, setting up cell discs within the Disque Platform requires significantly more time and practice than a 2D culture system. Nevertheless, all the steps can be performed in sequence using common laboratory techniques and equipment, and are automation-friendly for scale-up to higher-throughput screening.

FUTURE WORK

Simultaneous Differentiation of Beta, Alpha, and Delta Cells

Current differentiation protocols are designed to differentiate one islet cell type at a time, however all islet cell types develop together in the context of *in vivo* human development. Both glucagon-producing alpha cells and somatostatin-producing delta cells work together with beta cells to control blood sugar in a paracrine feedback system. Wang et al. demonstrated in 2017 that human embryonic stem cell organoids within soft Matrigel-Collagen type I hybrid gels can differentiate into insulin-expressing cells alongside somatostatin and glucagon-expressing cells, indicating that simultaneous differentiation in vitro is possible.⁸ Unfortunately, Matrigel is not suitable for the culture of cells destined for human transplantation due to its animal origin, and the authors were not able to demonstrate effective differentiation in Collagen type I alone. Moreover, Collagen I is not the only component of islet extracellular matrix, whose basement membranes are mainly composed of Collagen IV and Iaminin.^{35,36} We hypothesize that reproducing key islet physical and biochemical cues on the Disgue Platform using chemicallydefined xeno-free materials, will enable the simultaneous differentiation of functional islet endocrine cell types. Its multi-well format and simple, automation-friendly configuration facilitates the study of a wide variety of microenvironmental cues in a medium- to highthroughput manner.

Oxidative Sterss and Beta Cell Differentiation

It is well-known that *in vitro* cell culture can generate large numbers of reactive oxygen species.^{37–39} In addition, β cells have lower levels of the cellular antioxidant enzymes catalase and glutathione peroxidase than any other tissue tested^{40,41}, while overexpression and addition of cellular antioxidants have been shown to protect β cells from oxidative stress.^{42–44} Furthermore, oxidative stress reduces Nkx-6.1, Pdx-1, MafA, and MafB expression, transcription factors that play key roles in β -cell differentiation and maturation.^{45–48} (Pdx-1 binds to the promoter region of the insulin gene. Nkx-6.1 promotes insulin gene expression in Pdx-1 expressing cells.^{49,50} MafA binds to the promoter region of the insulin gene. MafB, which is also required for β -cell maturation, binds within the insulin and glucagon transcriptional control regions of endocrine cells as well as stimulates MAFA transcription.⁵¹)

We hypothesize that the addition of antioxidants to the culture medium will improve the expression of insulin-promoting transcription factors that are sensitive to oxidative stress. In addition, we hypothesize that increasing serum levels in the culture medium will improve the expression of insulin-promoting transcription factors that are sensitive to oxidative stress due to antioxidants present in non-heat-deactivated serum.³⁷

Glucose and Beta Cell Differentiation

It is well known that supra-physiological glucose levels in culture media causes mitochondria to produce large numbers of reactive oxygen intermediates.³⁷ We hypothesize that reducing glucose levels in the culture medium will improve the expression of insulin-promoting transcription factors that are sensitive to glucose-induced oxidative stress.

Investigating Developmental Pathways and Cell-Cell Signaling

The cell-cell contact provided by our platform enables the probing of juxtacrine signaling pathways critical for β -cell differentiation, such as the Notch signaling pathway. Similarly, cell junctions re-formed in our platform allow us to investigate the role of cell junctions in cadherin-mediated β -cell communication and islet structure cohesiveness. In future studies of multiple islet cell type co-culture, the Disque Platform's precise control over diffusion gradients can be applied to activate and explore paracrine signaling between α - and β -cells in insulin secretion⁵².

Studies of human and rodent foetal islets reveal the role of the Notch pathway in patterning and cell specification during pancreas and β -cell development.^{53–57} Notch activation during trunk/tip specification leads to pro-ductal or pro-endocrine cell types. Subsequent Notch inhibition of trunk progenitors during endocrine/ductal specification leads to an endocrine fate and subsequent transient Neurogenin-3 (Ngn3) expression, which is a requirement for endocrine development. Specifically, Notch activation up-regulates Hes1, and Hes1 inhibits Ngn3 expression. Therefore, Notch inhibition during endocrine/ductal specification is a requirement for Ngn3 expression and endocrine specification. Then, expression of MafA and other factors leads to the β -cell phenotype. To that end, pilot studies have begun to test cocktails of Notch inhibitors and activators for β -cell differentiation (**Supplemental Figure 3**).

We hypothesize that Notch inhibition during the differentiation from pancreatic progenitors to pancreatic endocrine progenitors will promote Ngn3 expression and subsequent endocrine (but not ductal) fate through repression of Hes1.

Generation of Transplantable Material to Cure T1D In Vivo

It is thought that over half of transplanted islets or β -cells die within the first few weeks following transplantation.^{58–60} A major contributor to impaired function and necrosis is acute ischemia. Even mild hypoxia is severely detrimental to function, with a 50% reduction in insulin release at 27 mmHg oxygen tension and a 98% reduction at a pO_2 of 5 mmHg.⁶¹ To complicate matters, macroencapsulation devices used in islet transplantation can have thicknesses exceeding oxygen diffusion limits.¹⁵ Such devices also lead to delayed glucose sensing and insulin release, reducing their ability to provide complete glycemic control.

The β -cell discs grown on the Disque Platform represent an attractive transplantation option due to their reduced thickness, which we hypothesize would result in better viability and insulin dynamics, while reducing the number of cells required to achieve a therapeutic effect. We hypothesize that transplantable cell discs generated on the Disque Platform can restore normoglycemia in an immunodeficient diabetic mouse model of T1D. Specifically, a large cell disc with 5 million HUES8 pancreatic endocrine progenitor (S4-C) cells will restore normoglycemia after transplantation into an immunocompromised diabetic mouse model (by differentiating *in vivo* into insulin-secreting cells).

Disease Modeling of Beta Cells in T1D: Redox Imbalance and Beta Cell Death

In Type 1 Diabetes, necrosis is thought to be a major contributor to β cell death.⁶² Two phenomena contribute to necrosis: insulitis and auto-immune attack. Insulitis is characterized by the presence of activated macrophages and cytokine-stimulated capillary endothelial cells in islets, which release toxic amounts of nitric oxide. Infiltrating immune cells release reactive oxygen intermediates as well as inflammatory cytokines such as IL-1 β , TNF α , and IFN γ . Together, these phenomena cause damage in several compartments, including to key enzymes present in mitochondria, and to nuclear DNA. Single-strand DNA breaks lead to PARP-mediated repair, which requires NAD+. High levels of DNA damage from this inflammatory environment therefore lead to depletion of NAD+ pools, depletion of cellular ATP, and necrotic β cell death. A loss of more than 65% of β cell mass ultimately leads to a loss of glycemic control.²

Attempts to prevent β cell death with the PARP inhibitor nicotinamide have shown mitigated results in a series clinical trials on patients with Type 1 Diabetes risk factors and newly diagnosed patients. Although PARP inhibition helped preserve baseline C-peptide (insulin secretory capacity) versus untreated controls, there was no difference insulin injection requirement. In addition, PARP inhibition impedes DNA repair.

Recent studies have shown that oral nicotinamide riboside (NR) supplementation raises blood and tissue NAD+ levels *in vivo*.⁶³ Therefore, we propose the following hypotheses:

- Hypothesis 1 (in vitro): Replenishment of cellular NAD+ (by media supplementation with NR) will prevent PARP-mediated necrotic death of SC-β cells (from damage by ROI, NO, and inflammatory cytokines), by preventing the depletion of ATP stores.
- Hypothesis 2 (in vivo): Direct replenishment of cellular NAD+ by oral NR supplementation will protect against β cell death while allowing PARP to initiate DNA repair.

METHODS

Manufacturing Custom Cell Culture Inserts with Reducing Washer

Custom reducing washers were cut from 1/16-in. (1.6-mm) thick cast poly(methyl methacrylate) (PMMA) sheets (McMaster-Carr) by laser machining with a 10- μ m CO₂ laser (Universal Laser Systems PLS6MW). The washers were then soaked in 70% ethanol and shaken for 15 minutes, rinsed briefly in 10% bleach, and then rinsed in sterile PBS. Then they were sprayed with 70% ethanol, which was allowed to evaporate, and finally they were washed twice in sterile PBS and stored in a sterile container. Washers were placed on the permeable membrane within a cell culture insert before cell seeding. The cell culture insert had a polyester (PETE) membrane and a 3- μ m pore size (Corning 3472). At this stage, the cell culture insert could optionally be coated with a gel or ECM coating within the reducing washer.

Gel Preparation and ECM Coating

PuraMatrixTM gels and Reduced Growth Factor Matrigel[®] (Corning 354230) were fabricated within cell culture inserts on a polyester membrane with a pore size of 3 µm, according to the manufacturers' protocols. Where applicable, a thin coating of collagen IV and laminin (each at 100 µg/mL) was applied to the surface of the gel, incubated for 2 h, and then washed.

Cell Seeding: Forming a Thin Cell Disc within the Disque Platform

Pancreatic progenitor cell clusters in their medium were obtained from Melton Lab at Harvard, and transported from Melton Lab at Harvard to Karp Lab at Brigham and Women's hospital via ground transportation (30-45 min) at ambient temperature in a sterile tube or bottle. There was no evidence that such handling affected the differentiation outcome. (Fig. 10A and Supp. Fig. 4)

The clusters were dispersed into a single cell solution in TrypLE Express, pre-warmed to 37 °C (8-12 min). Cells were then concentrated by centrifugation at $200 \times g$ for 4 minutes to obtain the required number of cells per well in a seeding volume of 20 µl. At this stage, ECM or gel could optionally be integrated into the cells. For a 50-µm thick cell disc, single cells were seeded within the washer onto the cell culture insert at a density of 110,000 viable cells / mm². The cell disc was then formed by centrifugation at $200 \times g$ for 4 minutes. Pre-warmed media containing 10 µM rho-kinase inhibitor Y-27632 (R&D Systems) was then slowly added to the bottom and top of the cell culture insert, taking care not to disrupt the cell disc by adding media along the side of the well or onto the reducing washer. Consistent results have been obtained with 80 µl of media above and 600-900 µl of media below the cell culture insert.

Cell discs were incubated at 37 °C, with media changes every 48 hours. Media composition and growth factor formulas followed the β cell differentiation protocol published by Melton Lab.⁵

Cell Disc Removal for Downstream Analysis

Cell discs were removed from cell culture inserts for further analysis. First the cell culture insert was removed from its well and any excess media was carefully discarded. Then,

the insert was placed flat onto a clean surface and the membrane was separated from the bottom of the cell culture insert by simultaneously applying a downward force on the washer with tweezers and pulling upward on the insert's outer edge. The washer could then be removed from atop the membrane, and the cell disc could be sectioned or dispersed into single cells for downstream analysis. Effective single cell dispersal was achieved by submerging the cells still on their permeable membrane support in pre-warmed 37 °C TrypLE Express for 8-12 minutes.

Cryosectioning and IHC

Cell discs were either stained directly or sectioned and then stained. For sectioning, cell discs (still on their membrane) or whole cell clusters were embedded in optimal cutting temperature (OCT) compound and flash frozen above liquid nitrogen. They were then sectioned at a thickness of 10 µm on a cryostat at -20 °C and transferred to glass slides. Samples were then blocked for 1 h at R.T. in 1% Triton X100 + 5% donkey serum + 1% BSA in PBS. Then they were incubated in primary antibody solution in 5% donkey serum + 1% BSA in PBS for 1 h at R.T. or overnight at 4 °C. Samples were stained with secondary antibody solution for 30 min, and mounted in ProLong Gold antifade reagent with DAPI. Finally, samples were imaged on a Zeiss LSM 800 with Airyscan confocal system on a Zeiss Axio Observer Z1 Inverted Microscope.

96-Well Multi-Color Flow Cytometry

Cell discs were removed from each well, as described above, transferred to microcentrifuge tubes, and submerged in pre-warmed 37 °C TrypLE, to disperse them into a single cell solution (8-12 min). A P200 air displacement pipette was used to mechanically disrupt the cell disc by pipetting solution down onto the permeable membrane support. Single cells were then stained with 1:200 Zombie UV dye in PBS for 10 minutes. The cells were then fixed in 4% paraformaldehyde for 12 minutes and stored in PBS at 4 °C until staining.

Fixed single cells were transferred to 96-well ultra-low attachment U-bottom plates for staining (Corning Costar 7007). Blocking and permeabilization was performed with 5% donkey serum + 0.1% saponin in PBS (blocking solution) for 30 minutes at 4 °C. Cells were incubated in primary antibodies in blocking solution for 60-90 minutes at R.T., then washed, and incubated in secondary antibodies in blocking solution for 30 minutes at 4 °C. Washing between steps was performed in 5% donkey serum in PBS, and following each centrifugation the supernatant from all wells was decanted by inverting the plate.

Stained cells in 96-well plates were run in high-throughput mode on a BD[™] LSR II Flow Cytometer with a high-throughput sample (HTS) attachment. Compensation was applied based on unstained and single-color controls, as well as fluorescence minus one controls in instances where more than 6 fluorophores were present in the same sample. Population and gating analysis was performed in accordance with validated methods provided by Melton Lab.

Measurement of Gel Modulus

A Discovery HR-3 hybrid rheometer (TA Instruments, P/N 533003.901, S/N 5333-0209) was set up for parallel plate rheometry and programmed to record storage modulus (G') and loss modulus (G'') in response to oscillatory shearing of the gel surface. A 20-mm round flat

plate geometry was zeroed to a gap height equal to the thickness of the permeable membrane gel backing on top of a layer of paraffin wax (which was meant to prevent slippage during testing). Each gel was hydrated within a moat of PBS and conditioned at 37 °C on the temperature-controlled Peltier plate prior to measurement (15 minutes for PuraMatrix[™] and 120 minutes for Matrigel[®]). In order to reduce sample-to-sample measurement error due to relaxation or flowing of the gel, the geometry was programmed to first lower onto the sample to achieve a force of 2.75 g, followed by a 30-s relaxation, then 2.50 g followed by another 30-s relaxation, then 2.25 g followed by a 60-s relaxation. Oscillatory frequency sweep tests were performed at 1% shear strain from 0.01 Hz to 10 Hz with five points recorded per frequency decade. Storage modulus (G') was related to the Young's modulus (E) by the formula E=2G'(1+v). The Poisson's ratio (v) for an 8-residue self-assembling oligopeptide matrix similar to PuraMatrix[™] has been reported as 0.47.³³

ACKNOWLEDGEMENTS

- This work was supported by a grant from the NIH NIDDK (UC4DK104165), and is part of a collaboration between Melton Lab (Harvard), Karp Lab (BWH), and Parker Lab (Wyss Institute).
- Thank you to Prof. Douglas Melton and Quinn Peterson, PhD at Melton Lab for providing key insights and feedback. Thank you also to Elise Engquist and Yi Yu at the Beta Cell Foundry at Melton Lab for providing pancreatic progenitor and SC-β cell clusters.
- Thank you to the Koch Institute Flow Cytometry Core at MIT for the use of their flow cytometry analysis facility, which receives support from NCI Grant P30-CA14051.
- Thank you to the Confocal Microscopy Core Facility at Brigham and Women's Hospital for the use of their microscope.

Thank you to the Harvard MRSEC (DMR-1420570) for the use of their rheometry equipment. Thank you to the Neurogenomics Laboratory led by Clemens R. Scherzer, M.D. at Brigham and Women's Hospital, for the use of their qRT-PCR equipment.

STUDENT'S INVOLVEMENT IN THE RESEARCH

This project has been a collaborative effort between Karp Lab (BWH), Melton Lab (HSCI), and Parker Lab (Wyss Institute), funded by the NIH under RFA-DK-13-016 UC4. Post-doctoral researcher Quinn Peterson and Prof. Douglas Melton from Melton Lab provided valuable expertise on the subjects of beta cell biology and differentiation, and have generated embryonic stem-cell derived pancreatic progenitor cells for our platform. Parker Lab is developing an islet-on-a-chip for the evaluation of beta cell physiology, disease modeling, and drug testing, that will house stem-cell-derived beta cells developed by Melton Lab and Karp Lab.

Our three-laboratory team represents a larger effort within the Consortium on Human Islet Biomimetics (CHIB) and the NIH Human Islet Research Network (HIRN). I have participated in the leadership of this project at Karp Lab since December of 2014, becoming the project leader at Karp Lab in late 2015. During that time, four post-doctoral researchers and three undergraduate researchers have contributed to the project at Karp Lab. Other than myself, the project contributors included: Professor Jeffrey M. Karp, Girish Chitnis, PhD, Liu Yi 'Jamie' Wu, Lillian Vo, and Kisuk Yang, PhD. Dr. Chitnis led the project during its first year and was responsible for writing a section of the grant application that funded this work.

I was responsible for inventing the Disque Platform itself, including the design requirements, concept, drawings, manufacturing processes, and culture techniques, with helpful feedback from Karp Lab members, and key contributions from Liu Yi Wu, Girish Chitnis, and Prof. Karp. The culture conditions were optimized with the help of the project team members Liu Yi Wu and Lillian Vo, who also aided in performing many of the experiments presented in this thesis. As project leader (under Dr. Karp), I was responsible for experimental planning and design, coordinating with our collaborators, and determining the project vision and direction, with expert guidance provided by Dr. Karp. I wish to thank Dr. Karp for the wonderful opportunity he has provided me to grow as a scientist and engineer within his laboratory.

SUPPLEMENTAL DATA

Temperature- and Time-Dependent Shear Properties of PuraMatrix™ and Matrigel®

Hydrogels should retain their mechanical properties during cell culture experiments, which occur over time and involve transitions from 37 °C to room temperature during media changes. To assess time and temperature dependency of shear properties, a Matrigel[®] gel and a PuraMatrix[™] gel were prepared. The time dependency of modulus was assessed at 37 °C for 20 minutes at a constant shear strain of 1% and constant frequency of 1 Hz. Temperature dependency was assessed from 20 °C to 50 °C, at 1% strain and 1 Hz, with a 10 °C temperature step between measurements and a 10-min soak time after each temperature adjustment. Minimal temperature-dependency was identified for 1% PuraMatrix[™] in the tested range, however the length of testing did influence modulus. The storage modulus, loss modulus, and complex viscosity of PuraMatrix[™] declined gradually over the course of the 20-minute test. Time-dependent shear thinning (thixotropic) behavior is a common characteristic of weak gels, and is due to a breakdown of the gel's internal structure over time. It is not expected that the static culture of cells on or within PuraMatrix would have such an effect. Also, Matrigel[®] exhibited minimal temperature- or time-sensitivity in the tested range.



Supplemental Figure 1. Time- and temperature-dependent mechanical properties of Matrigel[®] and PuraMatrix[™] gels.



Expression of Other Differentiation Markers on the Disque Platform

*Relative expression level based on correlation to fluorescence intensity measured by flow cytometry.

Supplemental Figure 2. The prevalence and relative expression level of key differentiation markers after a 9-day differentiation from pancreatic progenitors on the Disque Platform ($n \ge 3$ differentiations / condition seeded from a single batch of pancreatic progenitors). Matched to the expression data for the spinner flask from which the cells originated. (A) The percentage of cells expressing key markers is high in both the spinner flask and on the Disque Platform, with induction of Nkx6.1 expression in a portion of the cells by the last day of the experiment. (B) The expression level per cell (relative to less differentiated cells on experimental day 0) is higher for Pdx1, Hes1, and Sox9 on the Disque Platform compared to in the spinner flask.

Pilot Testing of Notch Activator and Inhibitor Cocktails



Notch Activation Level

Supplemental Figure 3. Development of Notch activation and Notch inhibition cocktails to study developmental pathways during β -cell differentiation (n = 6 differentiations per condition, seeded from a single batch of pancreatic progenitors). The Notch inhibitory cocktail consisting of DAPT and gamma secretase inhibitor XXI was found to decrease Hes1 expression after a 6-day differentiation from pancreatic progenitors. KGF is normally administered in Stage 4 medium, and it was removed from the Notch inhibitory cocktail since it may play some role in sustaining Notch activity.

Effect of Handling and Transportation on Beta Cell Differentiation



Supplemental Figure 4. Effect of handling and transportation on spinner flask-differentiated cells (n = 1 differentiation per flask, 5-day differentiation from pancreatic progenitors, S4d1 \rightarrow S4C). Cells were removed from a 500-ml spinner flask at Melton Lab, placed into a sterile container, and transported 30-45 minutes by ground transportation at ambient temperature to Karp Lab, where they were seeded into a 125-ml spinner flask. Rotational frequency was adjusted from 70-to 100 rpm to correct for the change in shear force moving to the smaller diameter spinner flask. Clusters tend to move along the outer periphery of the flask, thus the outer diameter was used to calculate the angular velocity.

REFERENCES

- 1. Matveyenko, A. V & Butler, P. C. Relationship between beta-cell mass and diabetes onset. *Diabetes. Obes. Metab.* **10 Suppl 4,** 23–31 (2008).
- 2. Meier, J. J. *et al.* Pancreatic diabetes manifests when beta cell area declines by approximately 65% in humans. *Diabetologia* **55**, 1346–54 (2012).
- 3. Dall, T. M. *et al.* The Economic Burden of Elevated Blood Glucose Levels in 2012: Diagnosed and Undiagnosed Diabetes, Gestational Diabetes Mellitus, and Prediabetes. *Diabetes Care* **37**, 3172–3179 (2014).
- 4. Ryan, E. A. *et al.* Five-year follow-up after clinical islet transplantation. *Diabetes* **54**, 2060–9 (2005).
- 5. Pagliuca, F. W. *et al.* Generation of functional human pancreatic β cells in vitro. *Cell* **159**, 428–39 (2014).
- 6. Rezania, A. *et al.* Reversal of diabetes with insulin-producing cells derived in vitro from human pluripotent stem cells. *Nat. Biotechnol.* **32**, 1121–33 (2014).
- 7. Pampaloni, F., Reynaud, E. G. & Stelzer, E. H. K. The third dimension bridges the gap between cell culture and live tissue. *Nat. Rev. Mol. Cell Biol.* **8**, 839–845 (2007).
- 8. Wang, W., Jin, S. & Ye, K. Development of Islet Organoids from H9 Human Embryonic Stem Cells in Biomimetic 3D Scaffolds. *Stem Cells Dev.* **0**, scd.2016.0115 (2017).
- 9. Bose, B. & Sudheer, P. S. in *Methods in molecular biology (Clifton, N.J.)* **1341,** 257–84 (2016).
- 10. Gurdon, J. B., Mitchell, A. & Mahony, D. Direct and continuous assessment by cells of their position in a morphogen gradient. *Nature* **376**, 520–1 (1995).
- 11. Gurdon, J. B., Harger, P., Mitchell, A. & Lemaire, P. Activin signalling and response to a morphogen gradient. *Nature* **371**, 487–92 (1994).
- 12. Fraker, C. A. *et al.* Enhanced oxygenation promotes beta-cell differentiation in vitro. *Stem Cells* **25**, 3155–64 (2007).
- 13. Bratt-Leal, A. M., Nguyen, A. H., Hammersmith, K. A., Singh, A. & McDevitt, T. C. A microparticle approach to morphogen delivery within pluripotent stem cell aggregates. *Biomaterials* **34**, 7227–35 (2013).
- 14. Carpenedo, R. L. *et al.* Homogeneous and organized differentiation within embryoid bodies induced by microsphere-mediated delivery of small molecules. *Biomaterials* **30**, 2507–15 (2009).
- 15. Van Winkle, A. P., Gates, I. D. & Kallos, M. S. Mass transfer limitations in embryoid bodies during human embryonic stem cell differentiation. *Cells. Tissues. Organs* **196**, 34–47 (2012).
- 16. Lindström, A. & Carlsson, J. Penetration and binding of epidermal growth factor-dextran conjugates in spheroids of human glioma origin. *Cancer Biother.* **8**, 145–58 (1993).
- 17. Schrezenmeir, J. *et al.* Effect of microencapsulation on oxygen distribution in islets organs. *Transplantation* **57**, 1308–14 (1994).
- 18. Heinis, M. *et al.* Oxygen Tension Regulates Pancreatic B-cell Differentiation Through Hypoxia-Inducible Factor 1a. *Diabetes* **59**, 662–669 (2010).
- 19. Cirulli, V. Cadherins in islet β -cells: more than meets the eye. *Diabetes* **64**, 709–11 (2015).

- 20. Amer, L. D., Mahoney, M. J. & Bryant, S. J. Tissue engineering approaches to cell-based type 1 diabetes therapy. *Tissue Eng. Part B. Rev.* **20**, 455–67 (2014).
- 21. Sugimoto, M. *et al.* What is the nature of pancreatic consistency? Assessment of the elastic modulus of the pancreas and comparison with tactile sensation, histology, and occurrence of postoperative pancreatic fistula after pancreaticoduodenectomy. *Surgery* **156**, 1204–11 (2014).
- Shi, Y., Glaser, K. J., Venkatesh, S. K., Ben-Abraham, E. I. & Ehman, R. L. Feasibility of using 3D MR elastography to determine pancreatic stiffness in healthy volunteers. *J. Magn. Reson. Imaging* 41, 369–75 (2015).
- 23. Engler, A. J., Sen, S., Sweeney, H. L. & Discher, D. E. Matrix elasticity directs stem cell lineage specification. *Cell* **126**, 677–89 (2006).
- 24. Caiazzo, M. *et al.* Defined three-dimensional microenvironments boost induction of pluripotency. *Nat. Mater.* (2016). doi:10.1038/nmat4536
- 25. Yang, C., Tibbitt, M. W., Basta, L. & Anseth, K. S. Mechanical memory and dosing influence stem cell fate. *Nat. Mater.* **13**, 645–52 (2014).
- 26. Richardson, T., Barner, S., Candiello, J., Kumta, P. N. & Banerjee, I. Capsule stiffness regulates the efficiency of pancreatic differentiation of human embryonic stem cells. *Acta Biomater.* **35**, 153–65 (2016).
- 27. Lau, J., Kawahira, H. & Hebrok, M. Hedgehog signaling in pancreas development and disease. *Cell. Mol. Life Sci.* **63**, 642–52 (2006).
- 28. Zhang, S., Ellis-Behnke, R. & Zhao, X. in *Scaffolding in Tissue Engineering* (eds. Ma, P. X. & Elisseeff, J.) 217–240 (Taylor & Francis, 2006). doi:10.1201/9781420027563.ch15
- Cormier, A. R., Pang, X., Zimmerman, M. I., Zhou, H. & Paravastu, A. K. Molecular structure of RADA16-I designer self-assembling peptide nanofibers. *ACS Nano* 7, 7562–72 (2013).
- 30. Allen, P., Melero-Martin, J. & Bischoff, J. Type I collagen, fibrin and PuraMatrix matrices provide permissive environments for human endothelial and mesenchymal progenitor cells to form neovascular networks. *J. Tissue Eng. Regen. Med.* **5**, e74-86 (2011).
- 31. Soofi, S. S., Last, J. A., Liliensiek, S. J., Nealey, P. F. & Murphy, C. J. The elastic modulus of Matrigel as determined by atomic force microscopy. *J. Struct. Biol.* **167**, 216–9 (2009).
- 32. Reed, J., Walczak, W. J., Petzold, O. N. & Gimzewski, J. K. In situ mechanical interferometry of matrigel films. *Langmuir* **25**, 36–39 (2009).
- 33. Leon, E. J., Verma, N., Zhang, S., Lauffenburger, D. a & Kamm, R. D. Mechanical properties of a self-assembling oligopeptide matrix. *J. Biomater. Sci. Polym. Ed.* **9**, 297–312 (1998).
- 34. INEOS Styrolution PS 1300/1301 Technical Datasheet. (2016). at <http://ineosstyrolution.com/>
- 35. Otonkoski, T., Banerjee, M., Korsgren, O., Thornell, L.-E. & Virtanen, I. Unique basement membrane structure of human pancreatic islets: implications for beta-cell growth and differentiation. *Diabetes. Obes. Metab.* **10 Suppl 4,** 119–27 (2008).
- 36. Goh, S.-K. *et al.* Perfusion-decellularized pancreas as a natural 3D scaffold for pancreatic tissue and whole organ engineering. *Biomaterials* **34**, 6760–72 (2013).
- Halliwell, B. Cell culture, oxidative stress, and antioxidants: avoiding pitfalls. *Biomed. J.* 37, 99–105 (2014).

- 38. Halliwell, B. Oxidative stress in cell culture: An under-appreciated problem? *FEBS Lett.*540, 3–6 (2003).
- 39. Gülden, M., Jess, A., Kammann, J., Maser, E. & Seibert, H. Cytotoxic potency of H2O2 in cell cultures: impact of cell concentration and exposure time. *Free Radic. Biol. Med.* **49**, 1298–305 (2010).
- 40. Tonooka, N., Oseid, E., Zhou, H., Harmon, J. S. & Robertson, R. P. Glutathione peroxidase protein expression and activity in human islets isolated for transplantation. *Clin. Transplant.* **21**, 767–72 (2007).
- 41. Lenzen, S., Drinkgern, J. & Tiedge, M. Low antioxidant enzyme gene expression in pancreatic islets compared with various other mouse tissues. *Free Radic. Biol. Med.* **20**, 463–6 (1996).
- 42. Harmon, J. S. *et al.* beta-Cell-specific overexpression of glutathione peroxidase preserves intranuclear MafA and reverses diabetes in db/db mice. *Endocrinology* **150**, 4855–62 (2009).
- 43. Kaneto, H. *et al.* Beneficial effects of antioxidants in diabetes: possible protection of pancreatic beta-cells against glucose toxicity. *Diabetes* **48**, 2398–406 (1999).
- 44. Wang, X., Yun, J.-W. & Lei, X. G. Glutathione peroxidase mimic ebselen improves glucosestimulated insulin secretion in murine islets. *Antioxid: Redox Signal.* **20**, 191–203 (2014).
- 45. Dai, C. *et al.* Stress-impaired transcription factor expression and insulin secretion in transplanted human islets. *J. Clin. Invest.* **126**, 1857–70 (2016).
- 46. Harmon, J. S., Stein, R. & Robertson, R. P. Oxidative stress-mediated, post-translational loss of MafA protein as a contributing mechanism to loss of insulin gene expression in glucotoxic beta cells. *J. Biol. Chem.* **280**, 11107–11113 (2005).
- 47. Guo, S. *et al.* Inactivation of specific β cell transcription factors in type 2 diabetes. *J. Clin. Invest.* **123**, 3305–16 (2013).
- Liang, J. *et al.* NADPH Oxidase-Dependent Reactive Oxygen Species Stimulate β-Cell Regeneration Through Differentiation of Endocrine Progenitors in Murine Pancreas. *Antioxid. Redox Signal.* 24, 419–33 (2016).
- 49. Gefen-Halevi, S. *et al.* NKX6.1 promotes PDX-1-induced liver to pancreatic β-cells reprogramming. *Cell. Reprogram.* **12**, 655–64 (2010).
- 50. Rezania, A. *et al.* Enrichment of human embryonic stem cell-derived NKX6.1-expressing pancreatic progenitor cells accelerates the maturation of insulin-secreting cells in vivo. *Stem Cells* **31**, 2432–42 (2013).
- 51. Artner, I. *et al.* MafB is required for islet beta cell maturation. *Proc. Natl. Acad. Sci. U. S. A.* **104,** 3853–8 (2007).
- 52. Meda, P. Protein-mediated interactions of pancreatic islet cells. *Scientifica (Cairo).* **2013**, 621249 (2013).
- 53. Li, X.-Y., Zhai, W.-J. & Teng, C.-B. Notch Signaling in Pancreatic Development. *Int. J. Mol. Sci.* **17**, 1–19 (2015).
- 54. Jennings, R. E., Berry, A. A., Strutt, J. P., Gerrard, D. T. & Hanley, N. A. Human pancreas development. *Development* **142**, 3126–37 (2015).
- 55. Afelik, S. & Jensen, J. Notch signaling in the pancreas: patterning and cell fate specification. *Wiley Interdiscip. Rev. Dev. Biol.* **2**, 531–44 (2013).
- 56. Shih, H. P. *et al.* A Notch-dependent molecular circuitry initiates pancreatic endocrine

and ductal cell differentiation. *Development* **139**, 2488–99 (2012).

- 57. Ninov, N., Borius, M. & Stainier, D. Y. R. Different levels of Notch signaling regulate quiescence, renewal and differentiation in pancreatic endocrine progenitors. *Development* **139**, 1557–67 (2012).
- 58. Biarnés, M. *et al.* Beta-cell death and mass in syngeneically transplanted islets exposed to short- and long-term hyperglycemia. *Diabetes* **51**, 66–72 (2002).
- 59. Davalli, A. M. *et al.* Vulnerability of islets in the immediate posttransplantation period. Dynamic changes in structure and function. *Diabetes* **45**, 1161–7 (1996).
- 60. Barshes, N. R., Wyllie, S. & Goss, J. A. Inflammation-mediated dysfunction and apoptosis in pancreatic islet transplantation: implications for intrahepatic grafts. *J. Leukoc. Biol.* **77**, 587–97 (2005).
- 61. Molnár, C. *et al.* Islet engraftment and revascularization in clinical and experimental transplantation. *Cell Transplant*. **22**, 243–51 (2013).
- 62. Burkart, V. in *Cell Death: The Role of Poly (ADP-ribose) polymerase* (ed. Szabó, C.) 103–130 (CRC Press, 2000).
- 63. Cantó, C. *et al.* The NAD(+) precursor nicotinamide riboside enhances oxidative metabolism and protects against high-fat diet-induced obesity. *Cell Metab.* 15, 838–47 (2012).