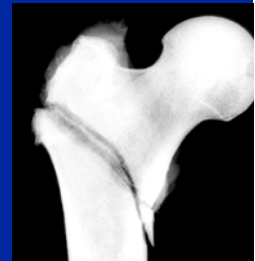


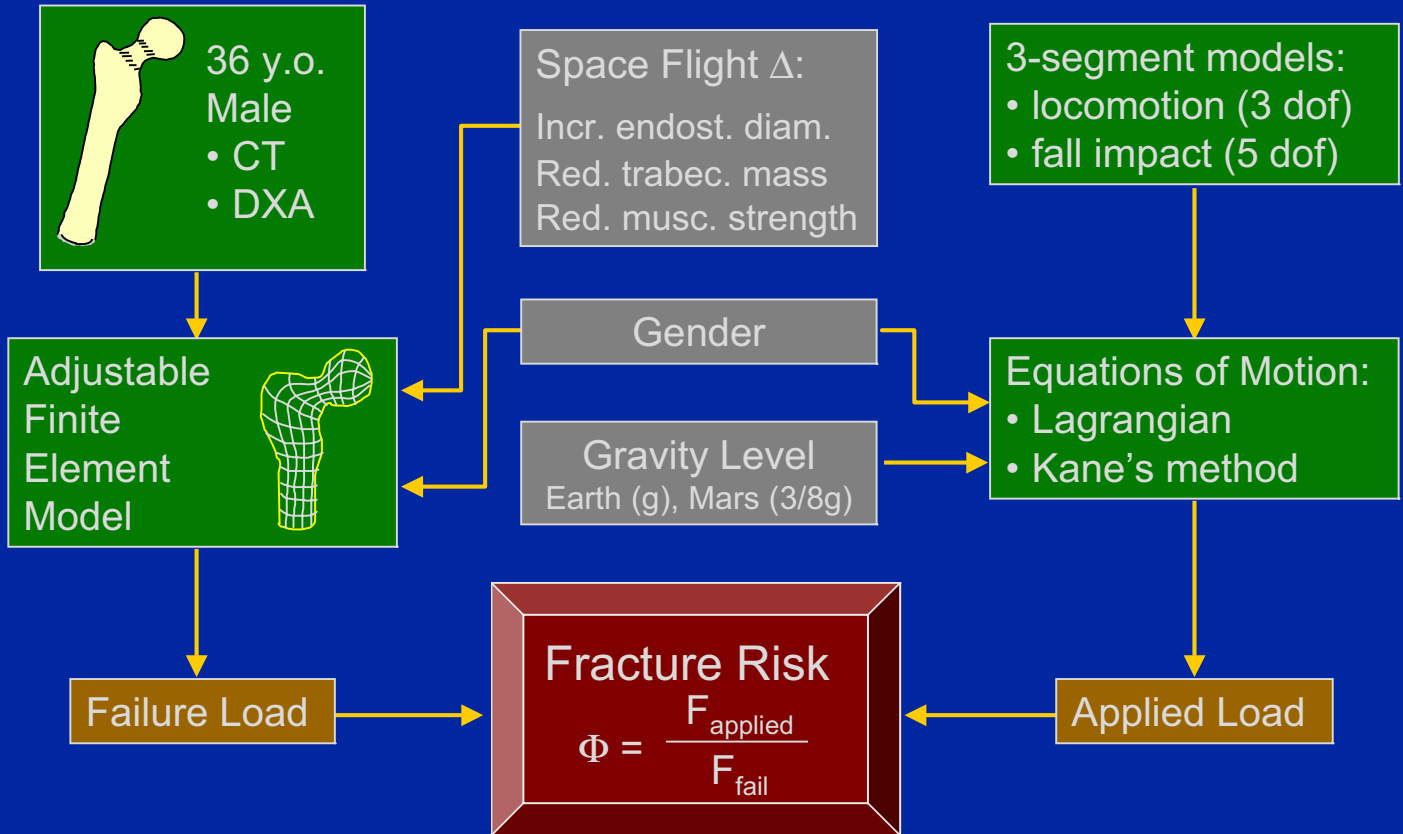
Principal Aim

To assess the strength changes, and associated change in fracture risk, due to structural alterations in the proximal femora of astronauts experiencing long-term weightlessness.

- 3-D FEA has not yet applied to bone loss in astronauts
 - Greatly increased risk of fracture upon return to Earth and possibly even under strenuous loading in space or on the moon or Mars.
- Calculate change in factor of risk (Φ)
 - $\Phi = \text{actual load} / \text{predicted failure load}$
 - hypothesis: $\Phi_{\text{pre}} < \Phi_{\text{post}}$
 - relationship between Φ and duration of weightlessness



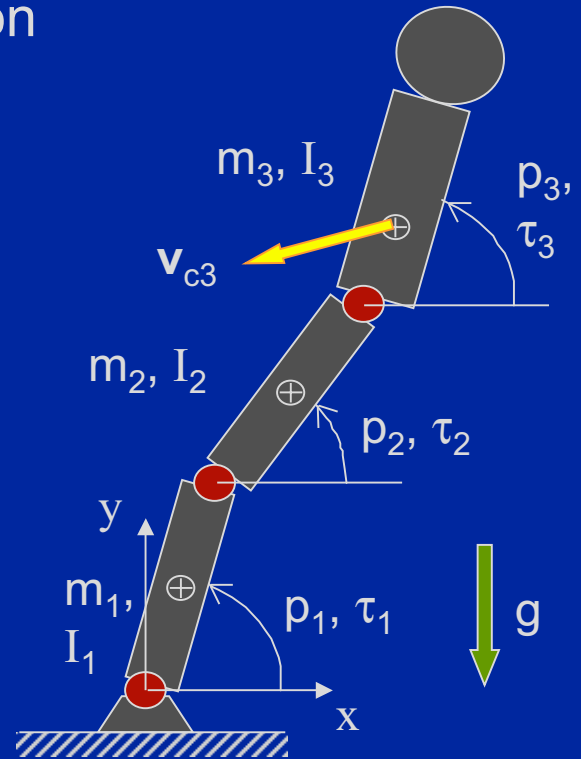
Research Plan



Aim 1: Hip Loading During Locomotion

3-segment model for locomotion

- Lagrangian formulation



Solution of Equations for Locomotion

Initial joint velocity from
hip/seg. 3

Calc. joint acceleration at
each time step

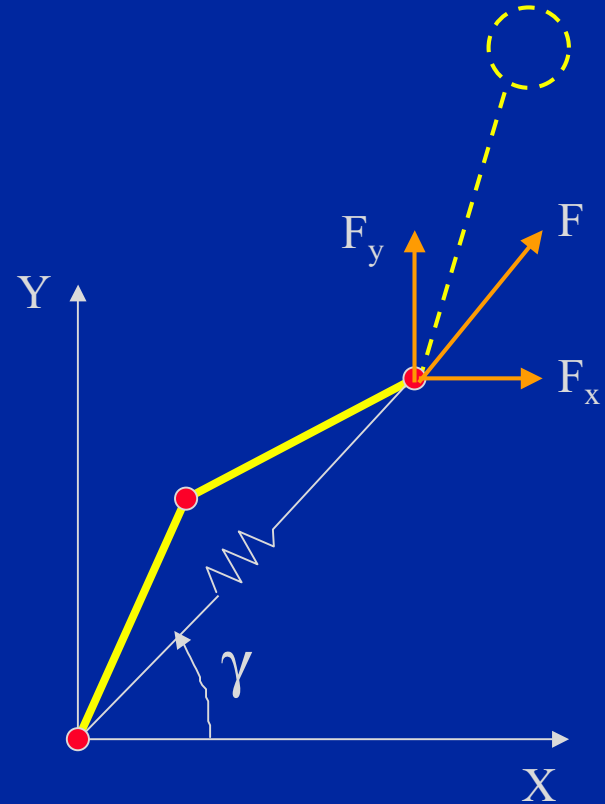
Integrate to get velocity
and position values

Hip force from c.m.
acceleration via Jacobian

Control Scheme (locomotion)

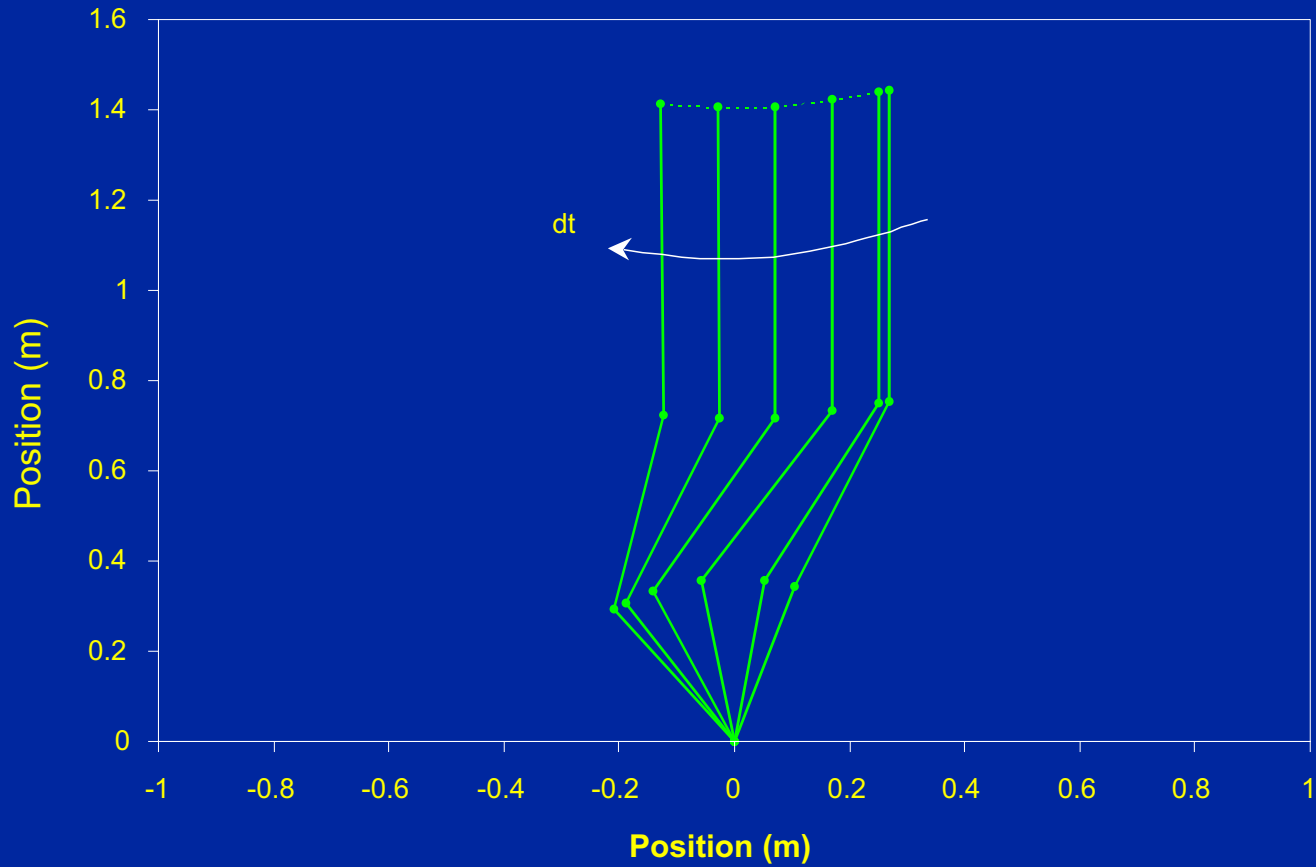
Hip torque:
PPD control

Ankle & knee torque:
Impedance control

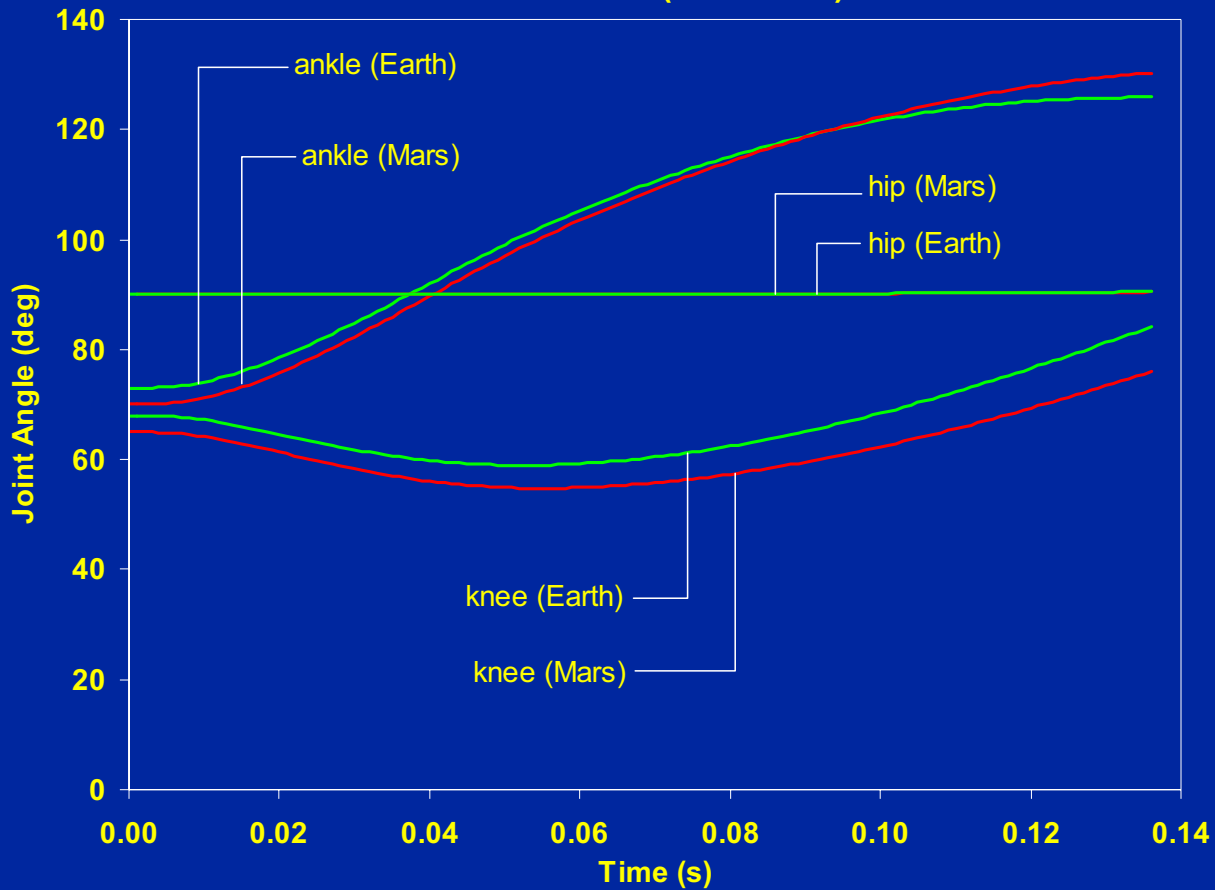


Variation of Parameters (Locomotion)

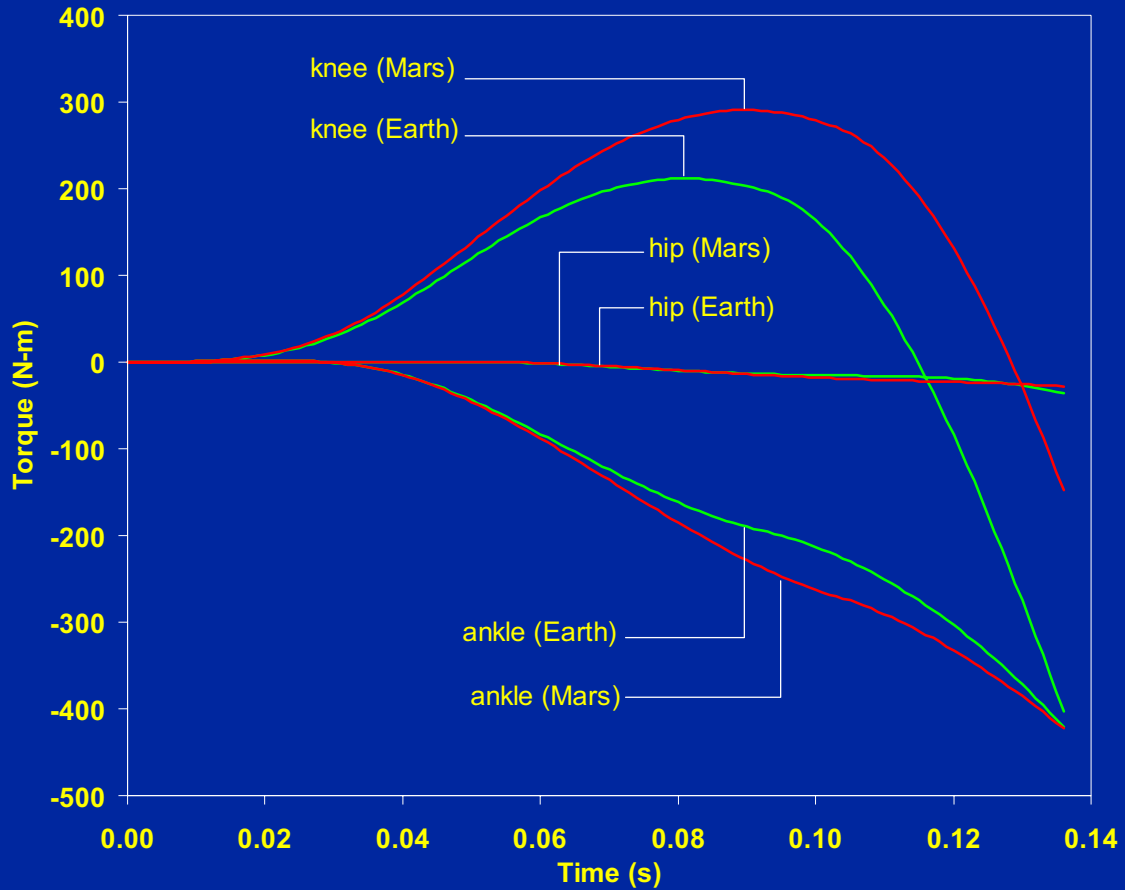
- Body Mass Properties (m , I) and Anthropometrics:
Male and female, 5%, 50%, 95%
Values derived using GEBOD
- Horizontal velocity:
 $u_{\text{Earth}} = 2 - 6 \text{ m/s}$ (He et al., 1991)
 $u_{\text{Mars}} = 2 - 4 \text{ m/s}$ (Newman et al., 1994; Wickman & Luna, 1996)
- Leg stiffness:
 $K_{\text{leg}} = 9 - 15 \text{ kN/m}$ (He et al., 1991; Farley & Gonzalez, 1996; Viale et al., 1998)
- Gravity:
Earth $G = g$, Mars $G = 3/8 g$ ($g = 9.807 \text{ m/s}^2$)
- Initial ankle angle: iteration until lowest point of hip trajectory occurs at $x=0$ (initial knee angle set to 5 deg)



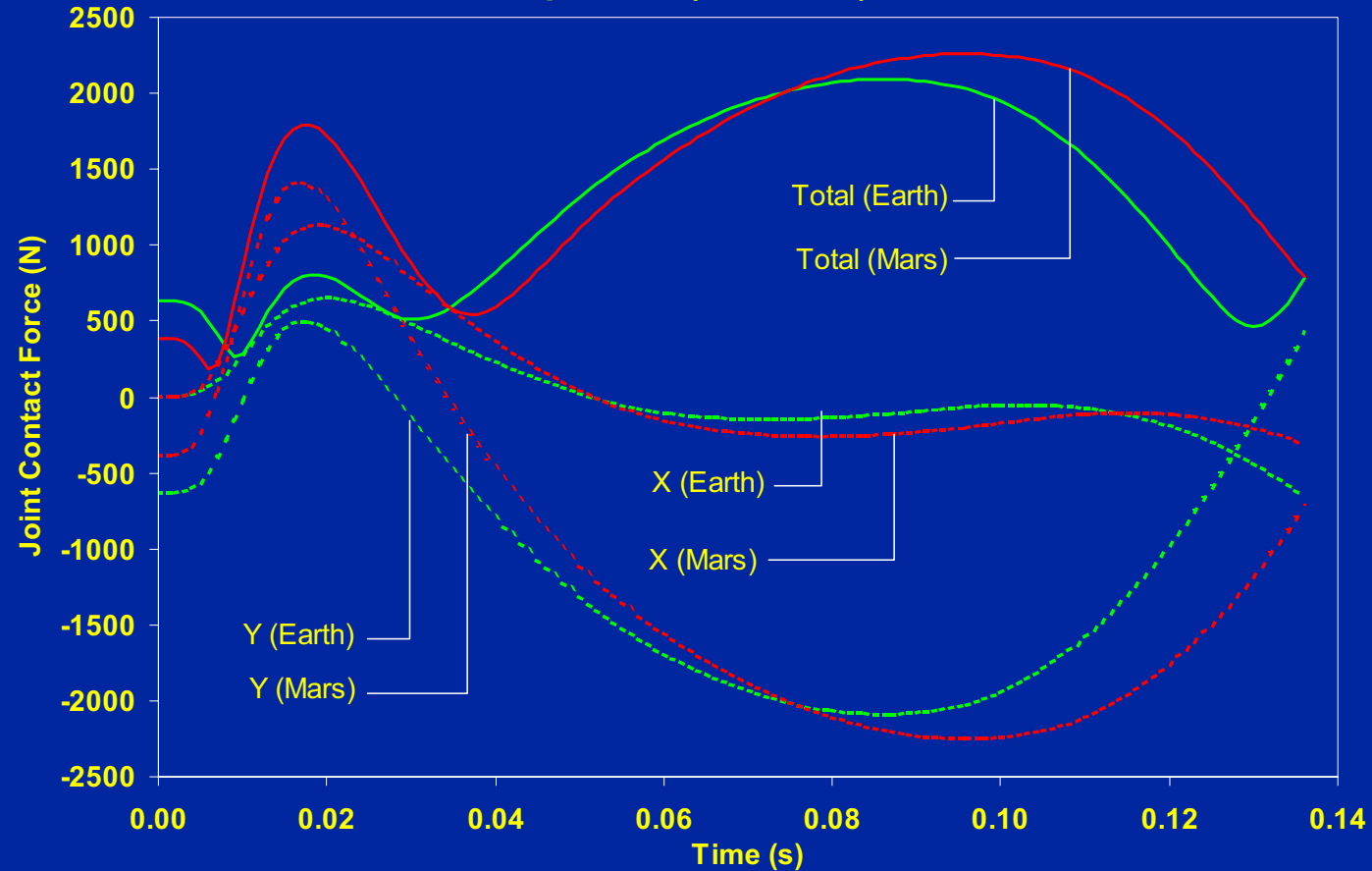
Joint Position (50% Male)



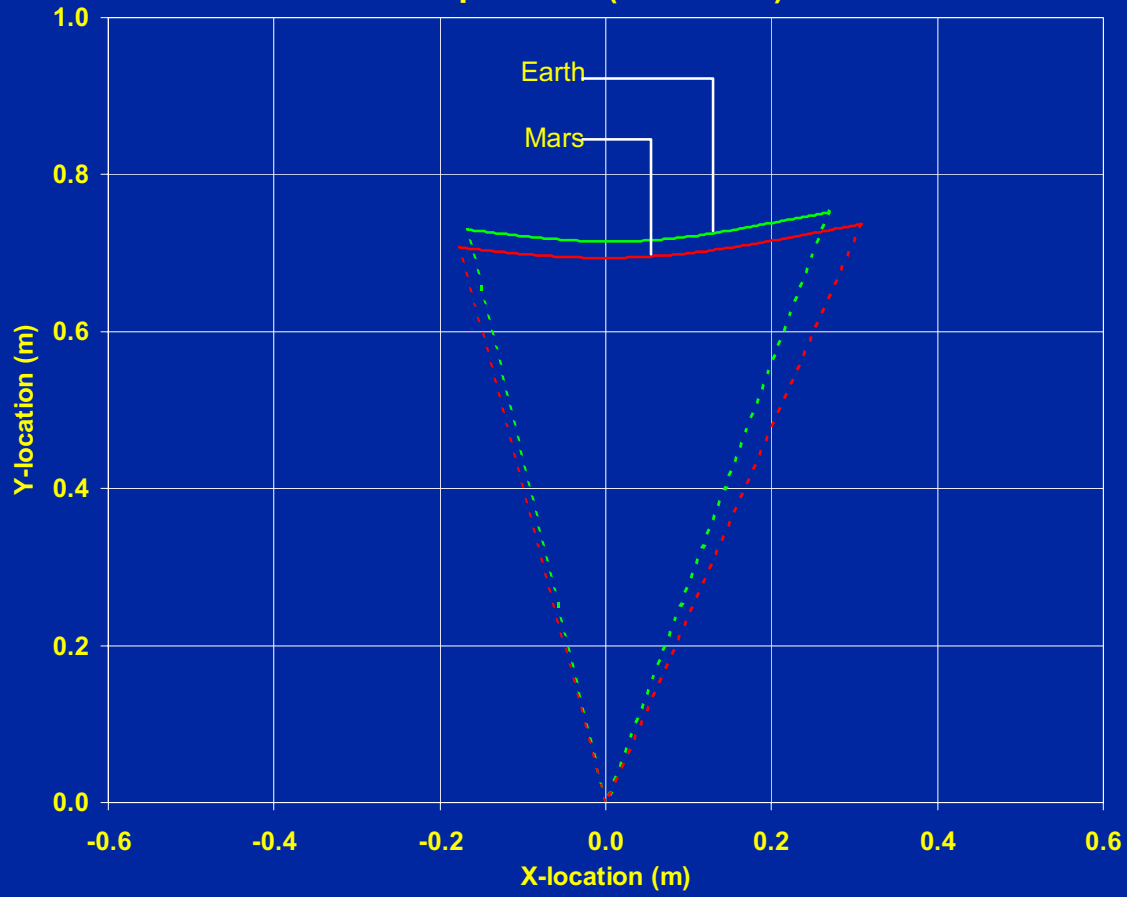
Joint Torque (50% Male)



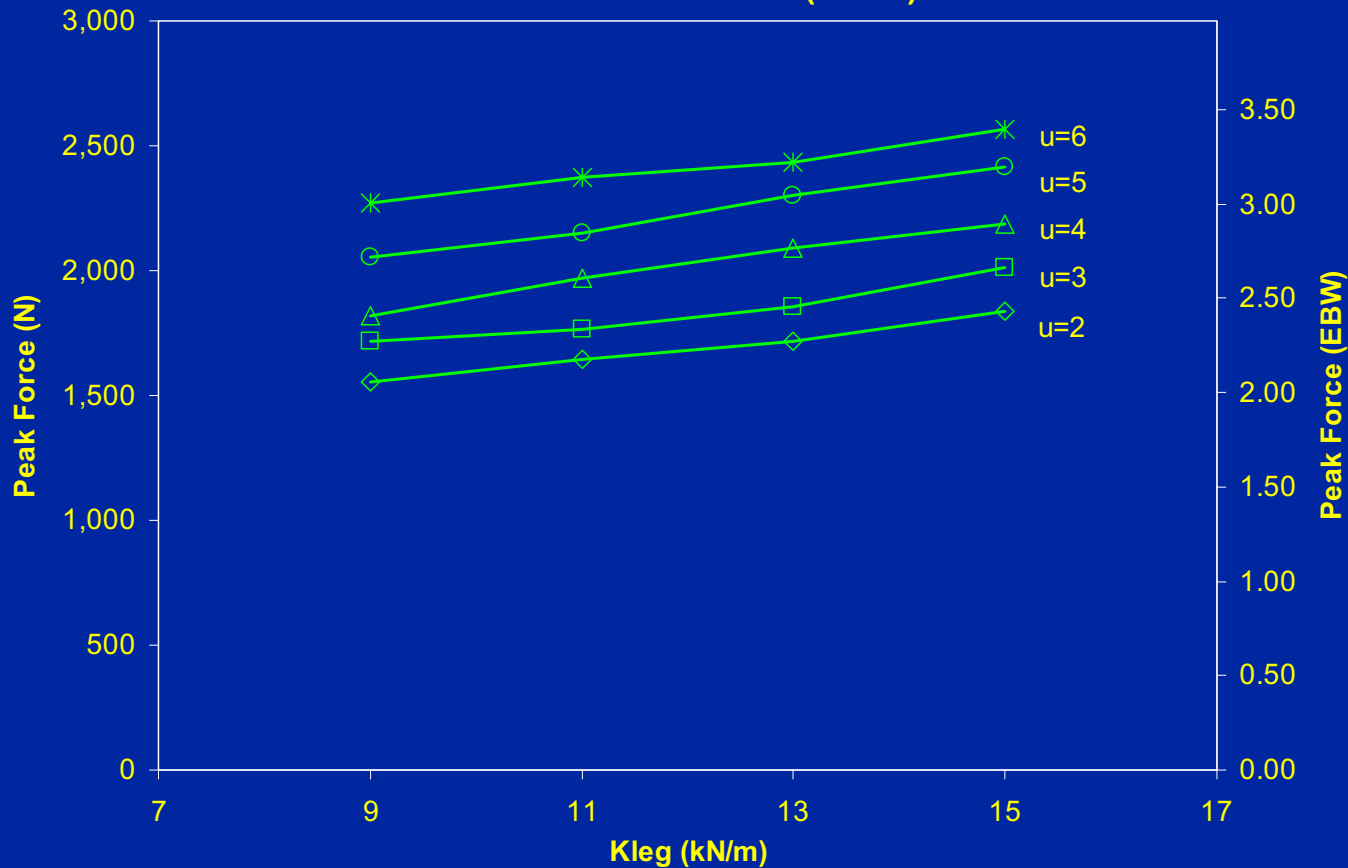
Hip Force (50% Male)



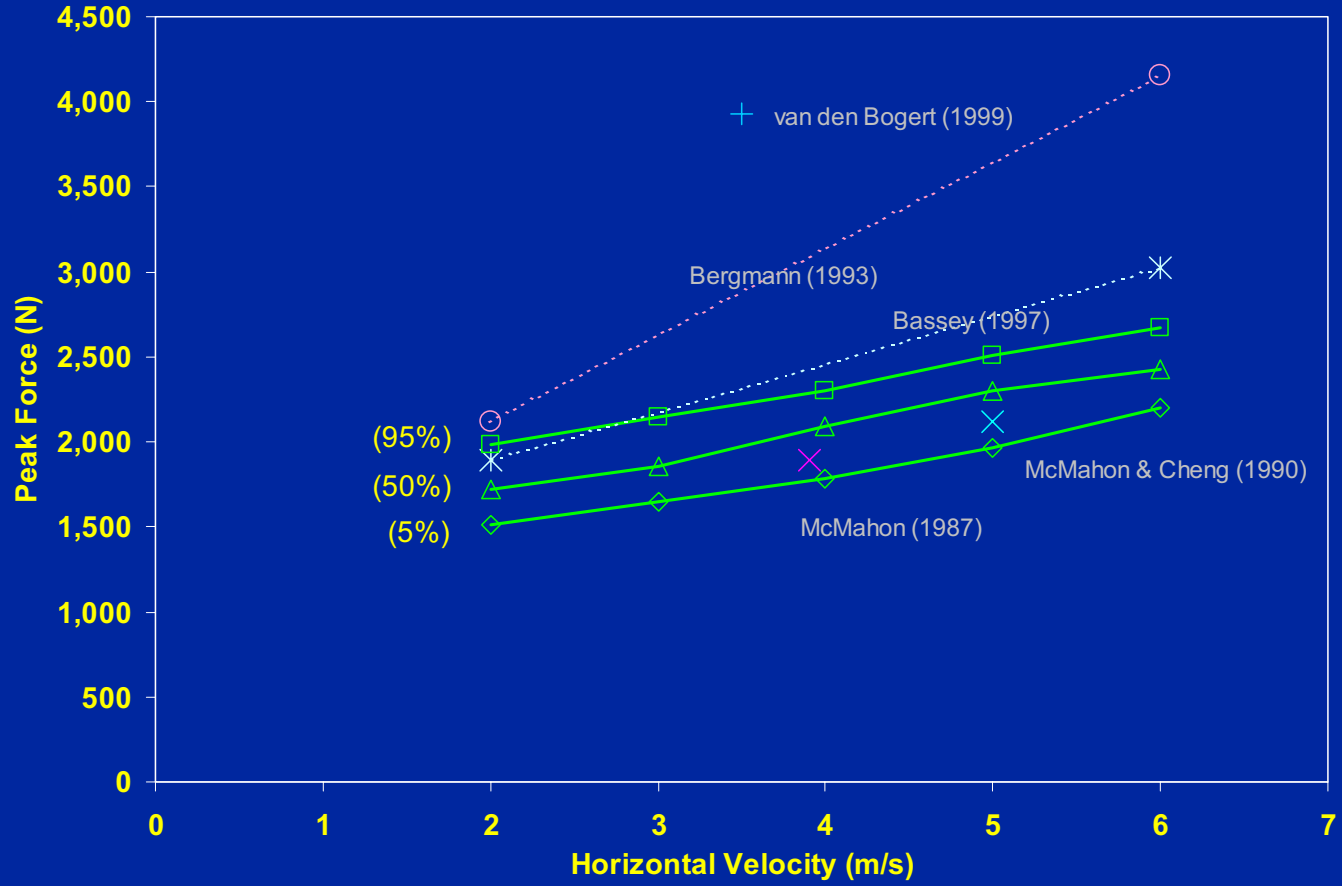
Hip Locus (50% Male)



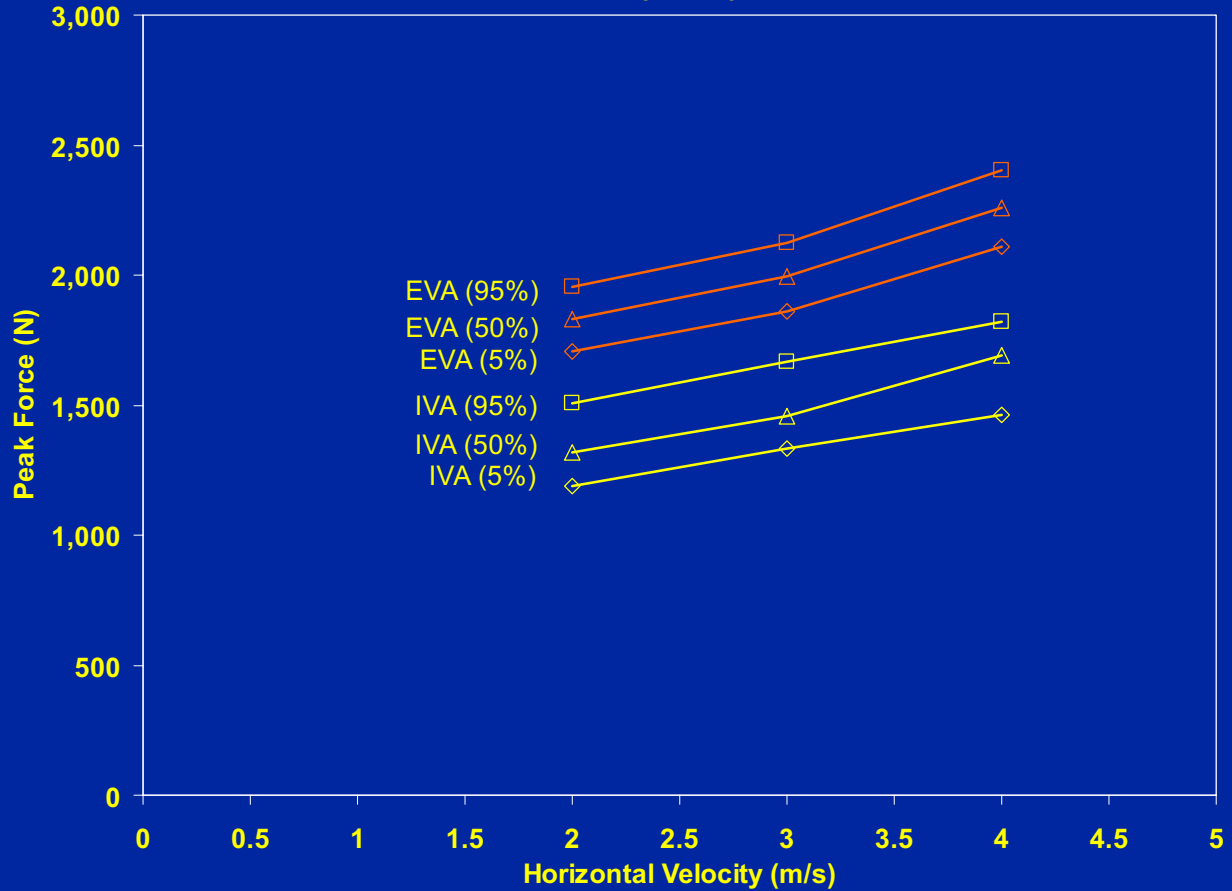
50th Percentile Male (Earth)



Male (Earth)

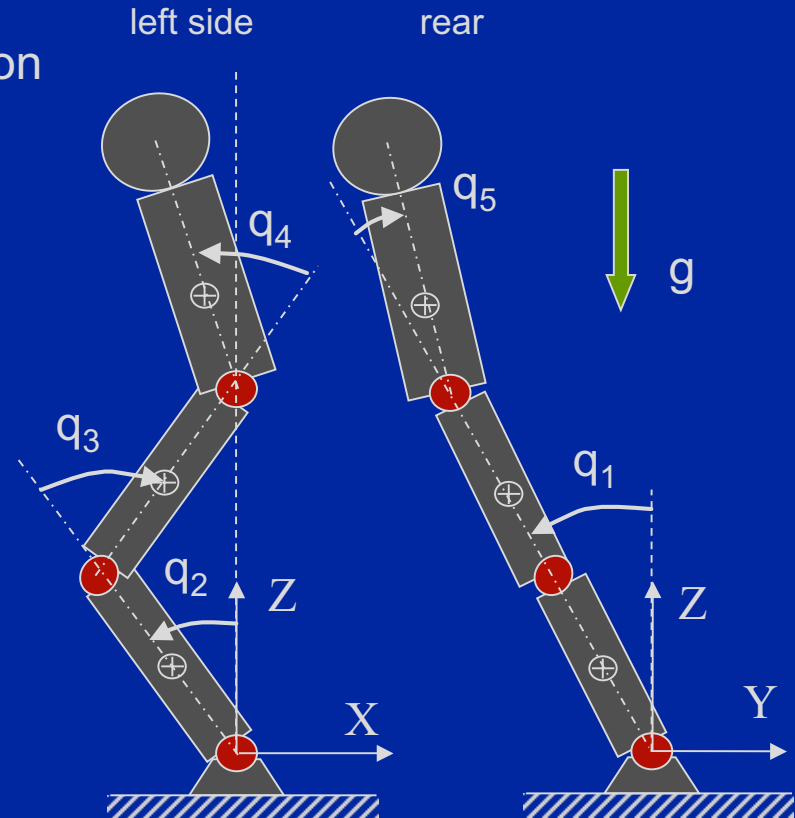


Male (Mars)



Aim 1: Hip Loading During Falls

- 3-segment model based on that derived by van den Kroonenberg (1995)
- 5 degrees-of-freedom



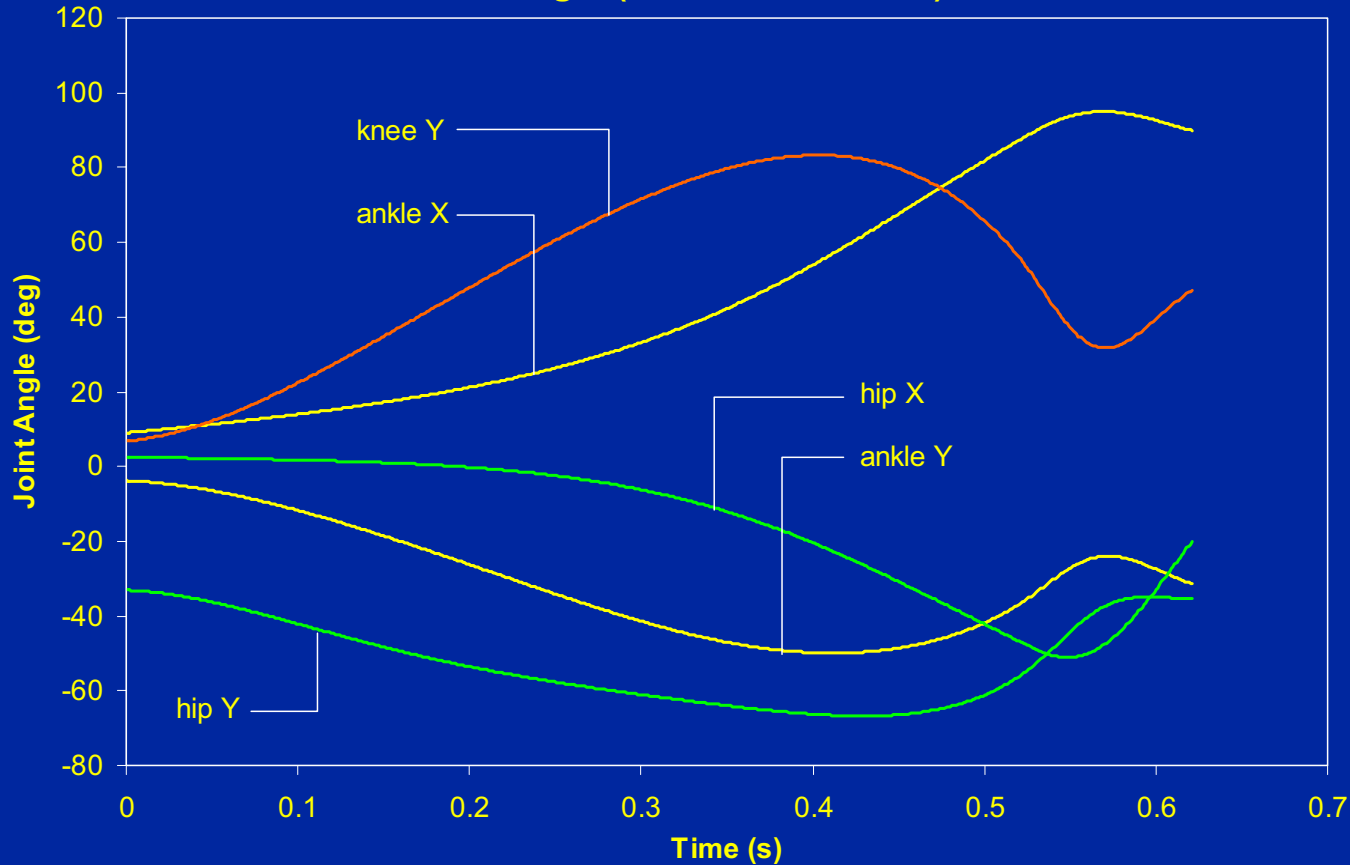
Control Scheme

- Ankle and knee: Impedance Control
 - Adjust $(K_p)_x$ and $(K_d)_x$ so that hip stays close to Y-Z plane
 - Adjust $(K_p)_z$ and $(K_d)_z$ so that body configuration at impact is close to that reported by van den Kroonenberg from kinematic studies
- Hip joints: PPD
 - Adjust control parameters to obtain appropriate trunk orientation at impact

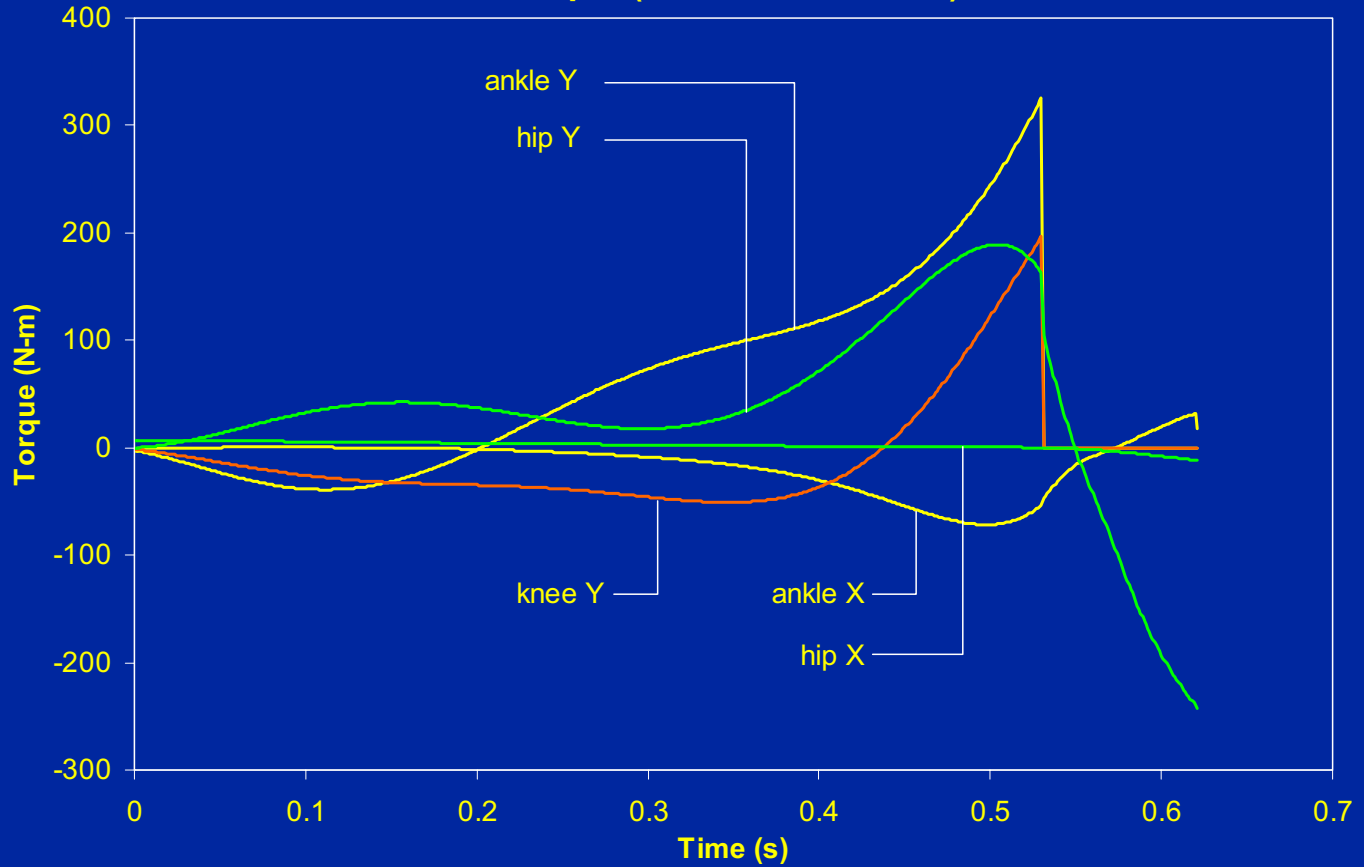
Variation of Parameters (Fall)

- Body Mass Properties (m, I) and Anthropometry:
 - Male and female, 5%, 50%, 95%
 - Values derived using GEBOD
- Gravity: Earth $G = g$, Mars $G = 3/8 g$ ($g = 9.807 \text{ m/s}^2$)
- Initial joint position and velocity values set to correspond with van den Kroonenberg (interpolated to get 50% values)
- Impact model
 - Stiffness: $K_{\text{Earth}} = 71 \text{ kN/m}$ (Robinovitch, et al., 1991)
 $K_{\text{Mars}} = 57 \text{ kN/m}$ (20% less for space suit padding)
 - Damping: $B = 923 \text{ N/m-s}$ (damping ratio = 0.2, Robinovitch, et al., 1991)

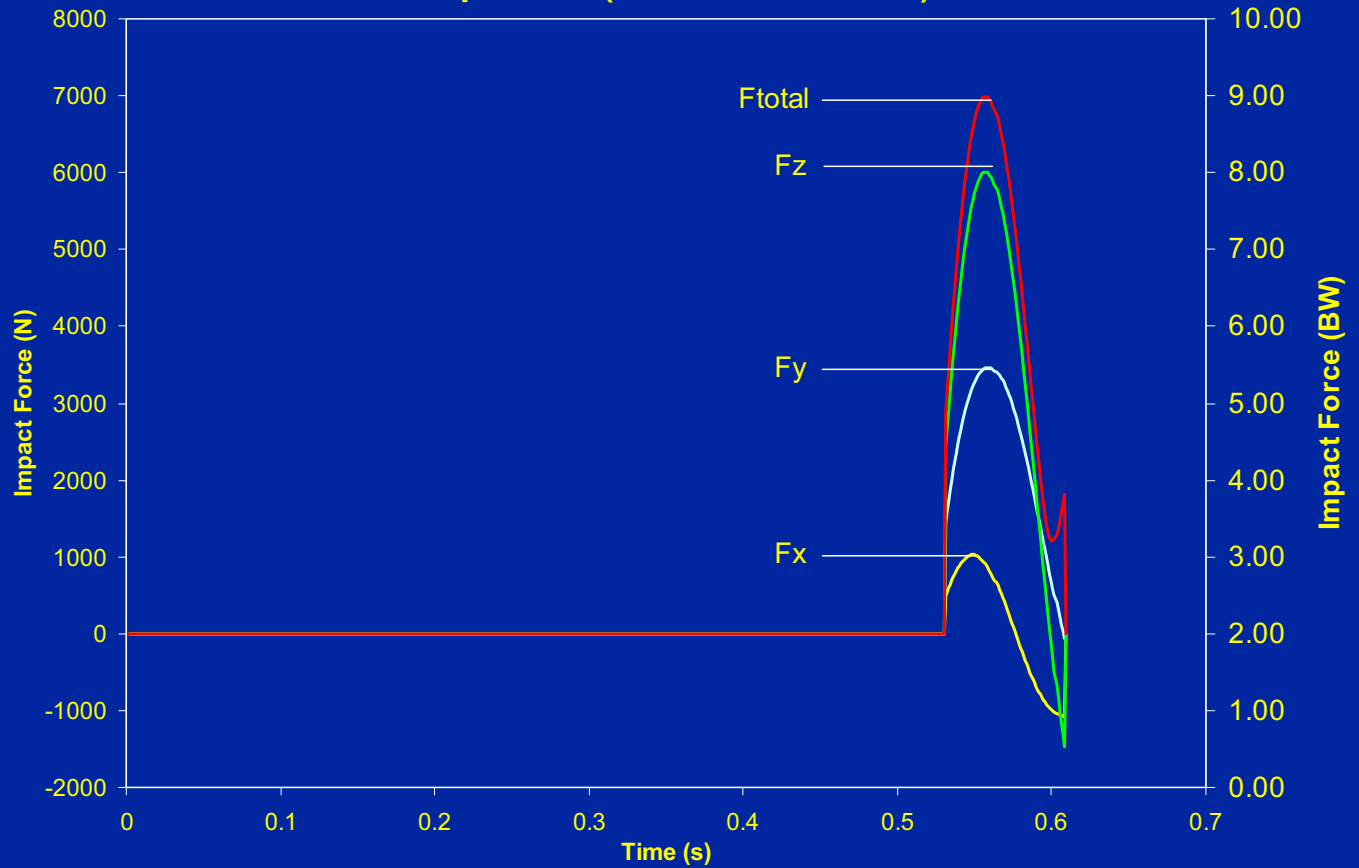
Joint Angle (50% Male — Earth)



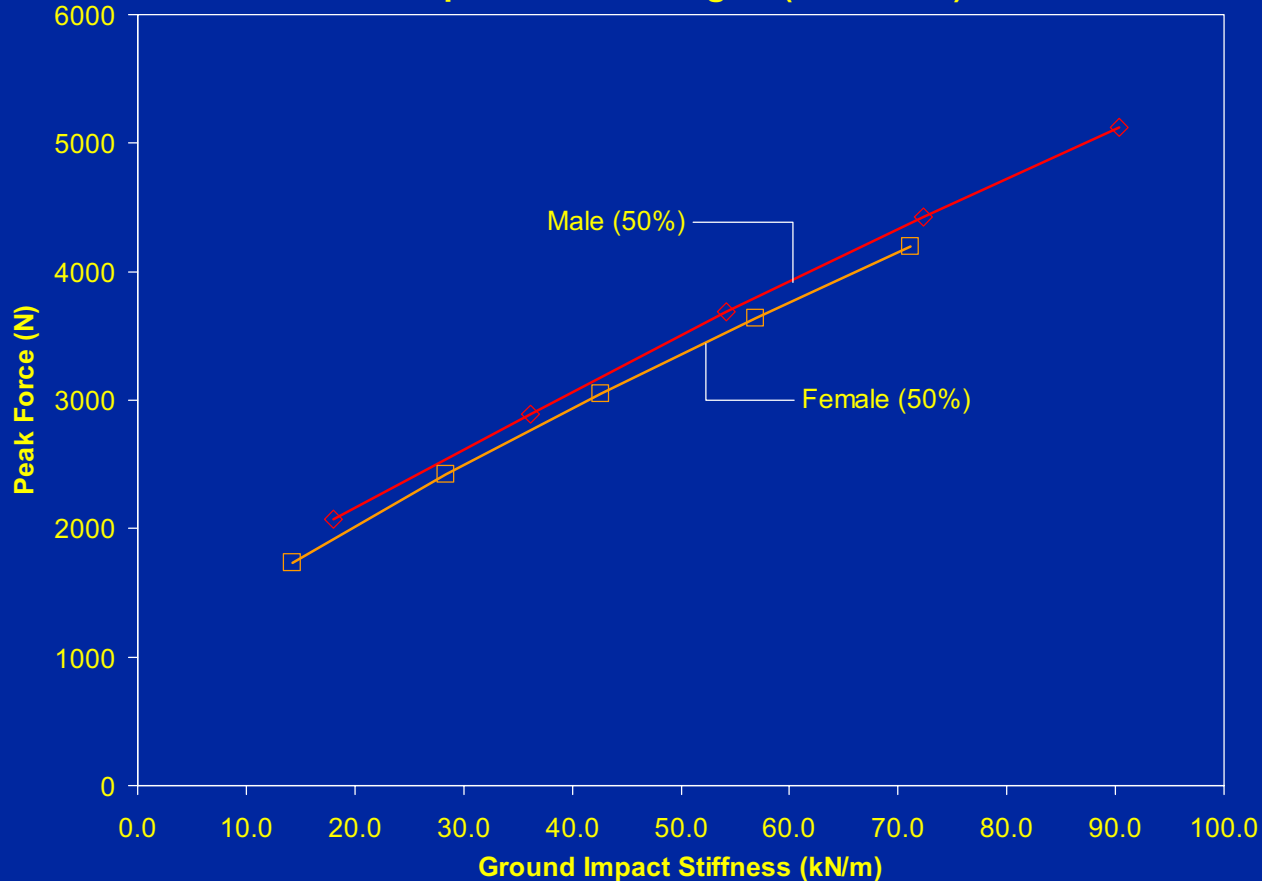
Joint Torque (50% Male — Earth)



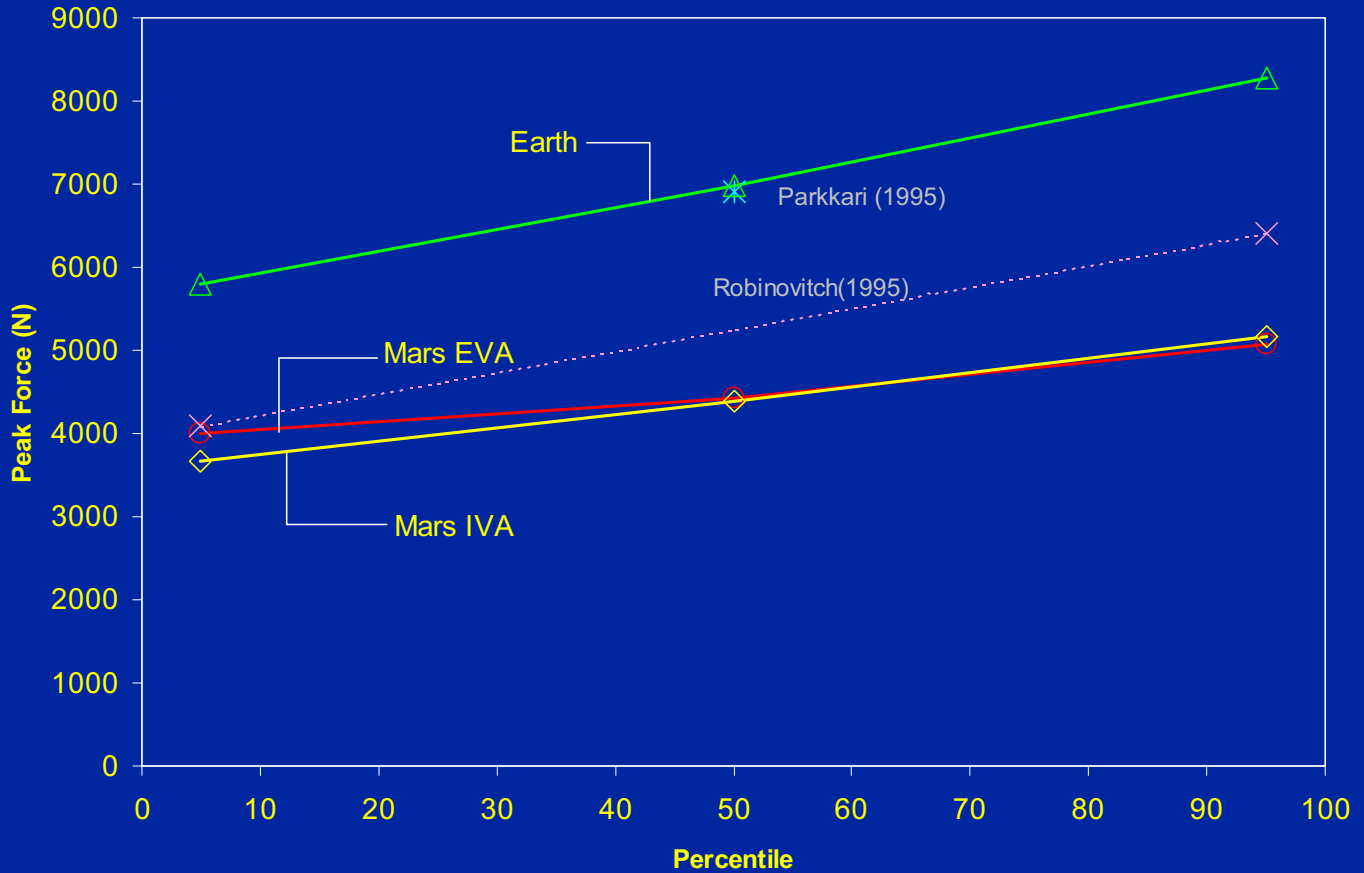
Hip Force (50% Male — Earth)



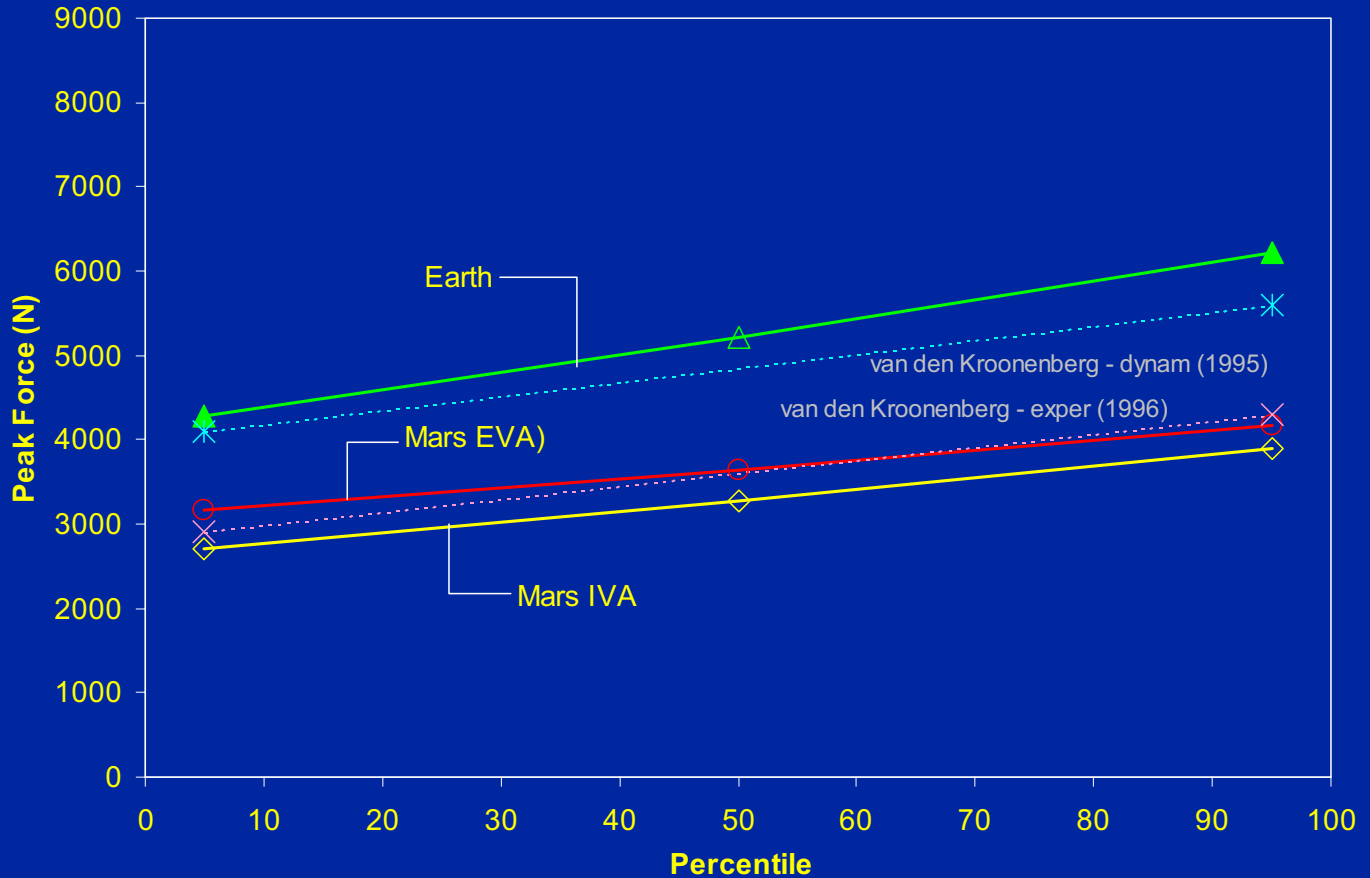
Peak Impact Force vs Kgnd (Mars EVA)



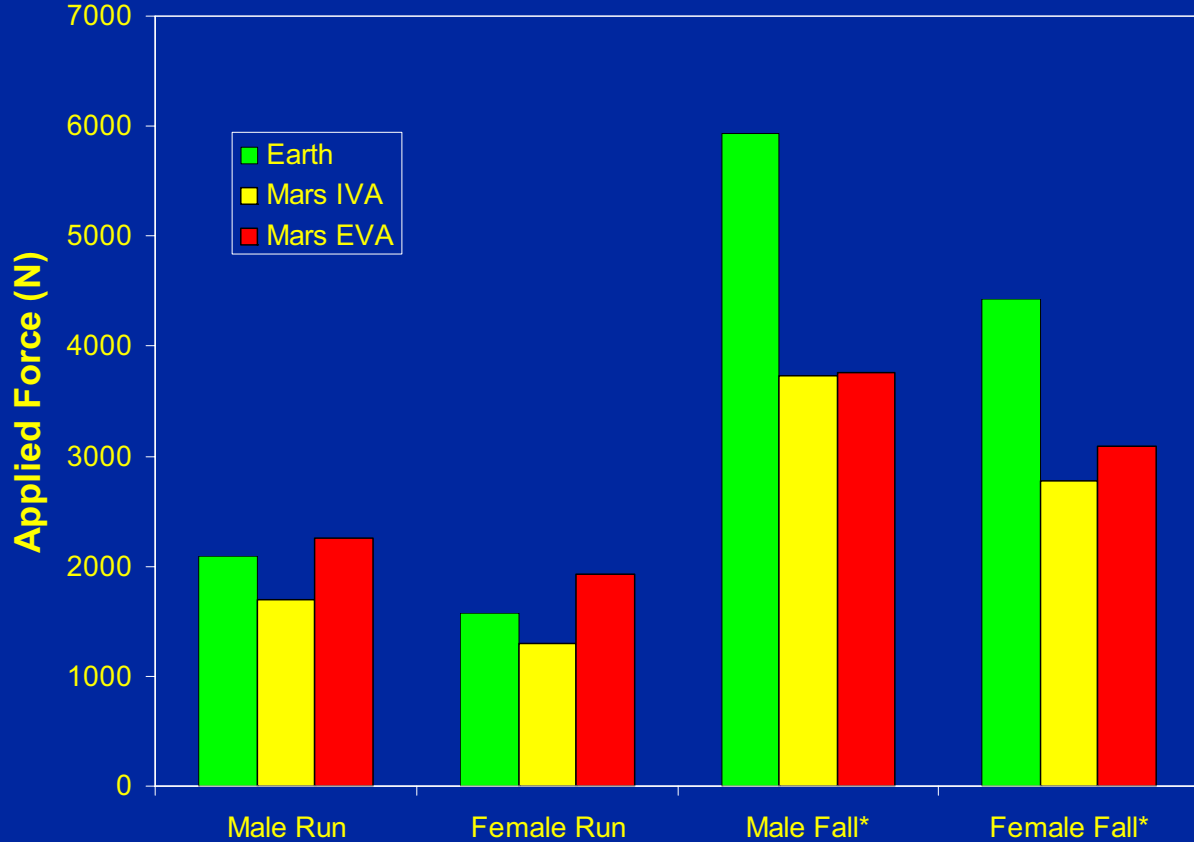
Hip Force during Impact (Male)



Hip Force during Impact (Female)



Applied Force Summary (Male & Female 50%)



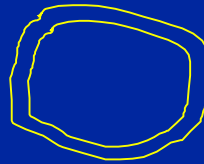
* Fall impact forces reduced by 15% to account for soft tissue attenuation (Robinovitch et al., 1997)

Finite Element Analysis

QCT scans and
NIH Image



Extract
contours

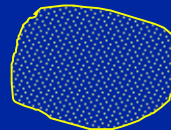


Stack
contours
to define
geometry



3-D Finite
Element
Model

Extract density
distribution
(trabecular area)



Define element
material properties

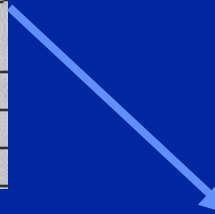
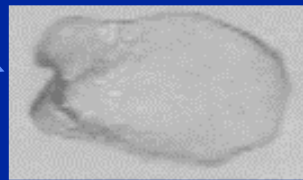
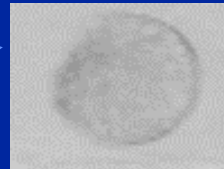
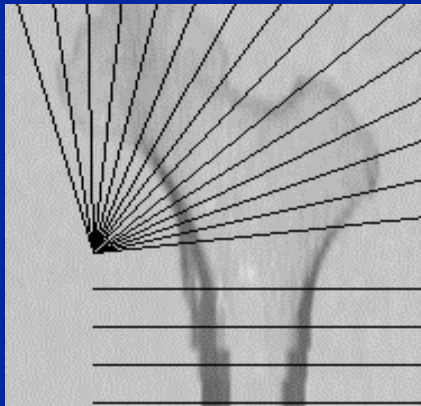


Methods: NIH Image

Resliced Sections

Outlines

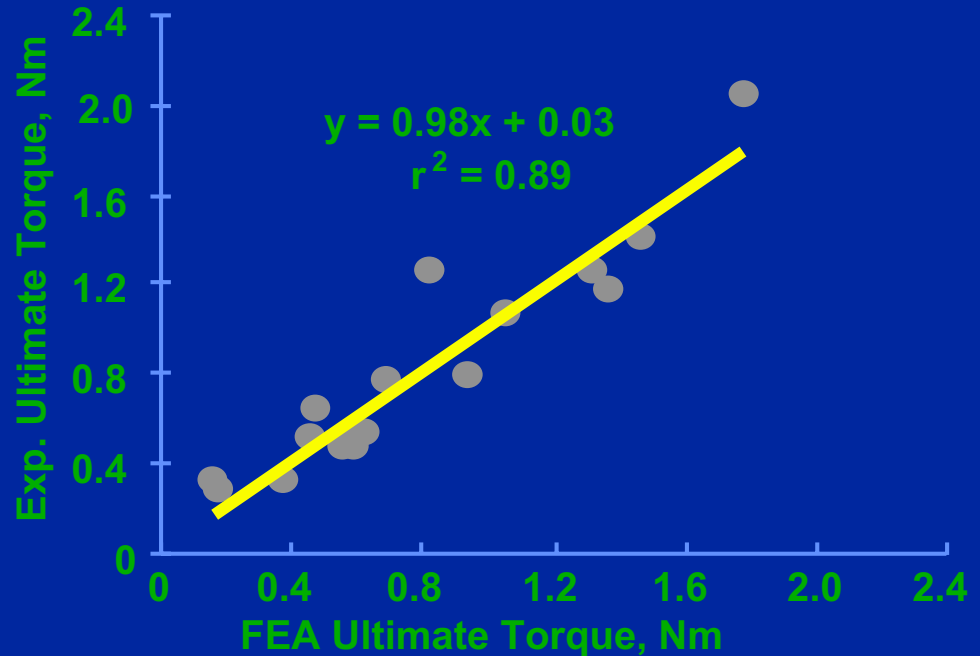
Femur Model

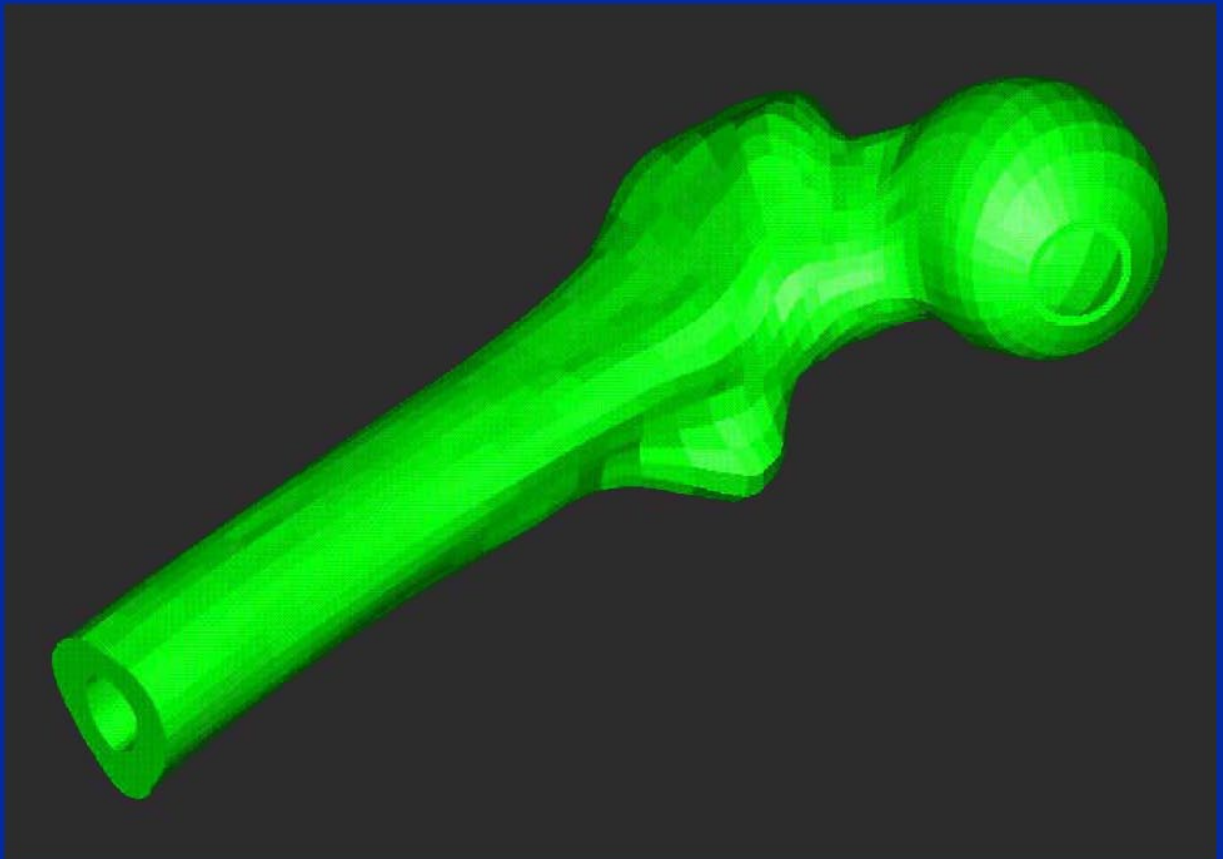
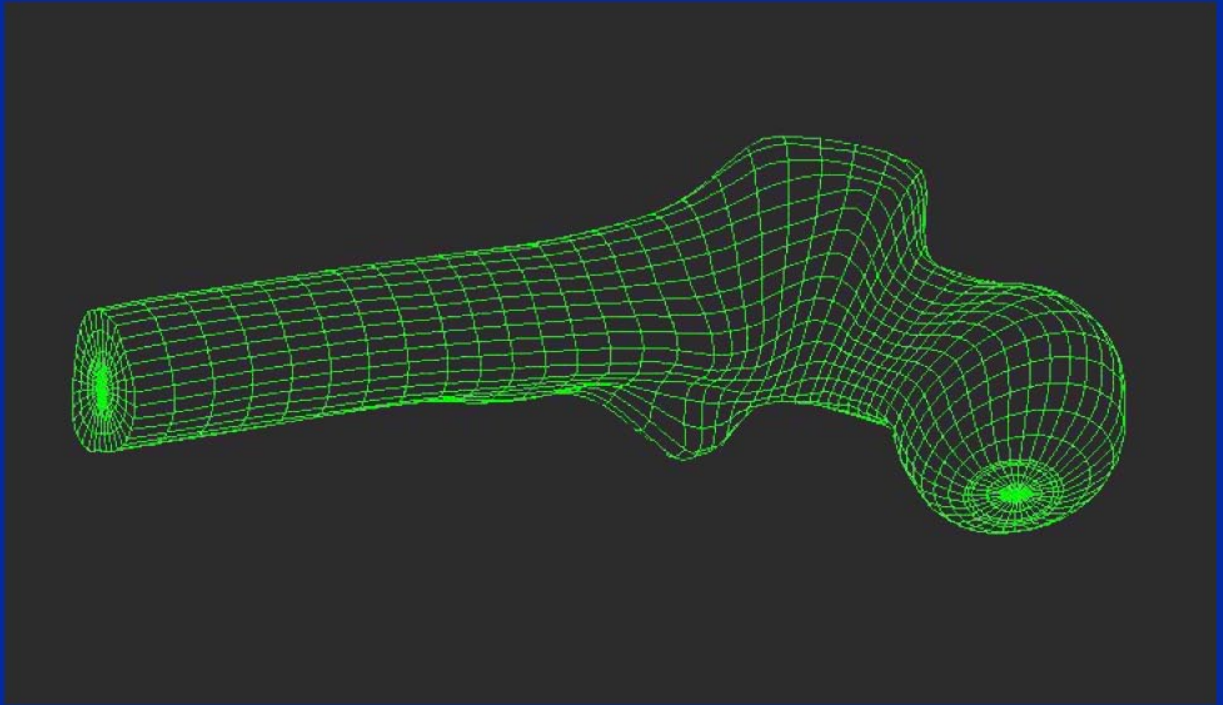


Results: Failure Analysis Validation

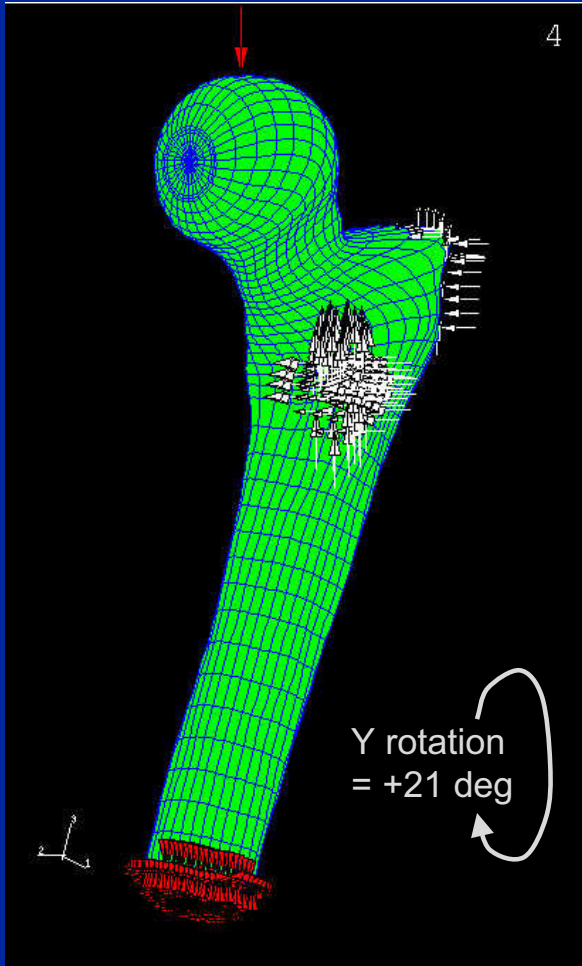
Trabecular bone
specimens in
torsion

Similar results,
 $r^2=0.86$ in
bending

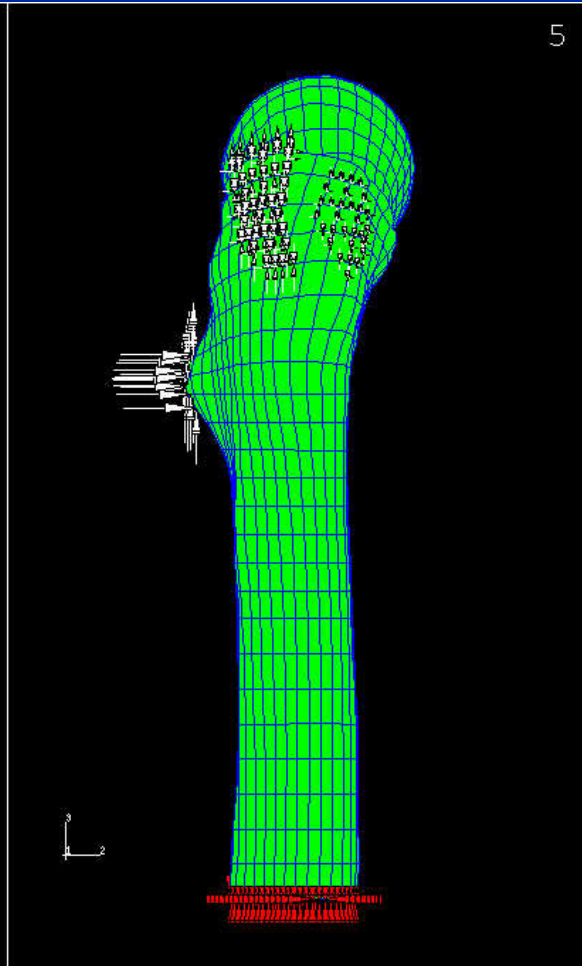


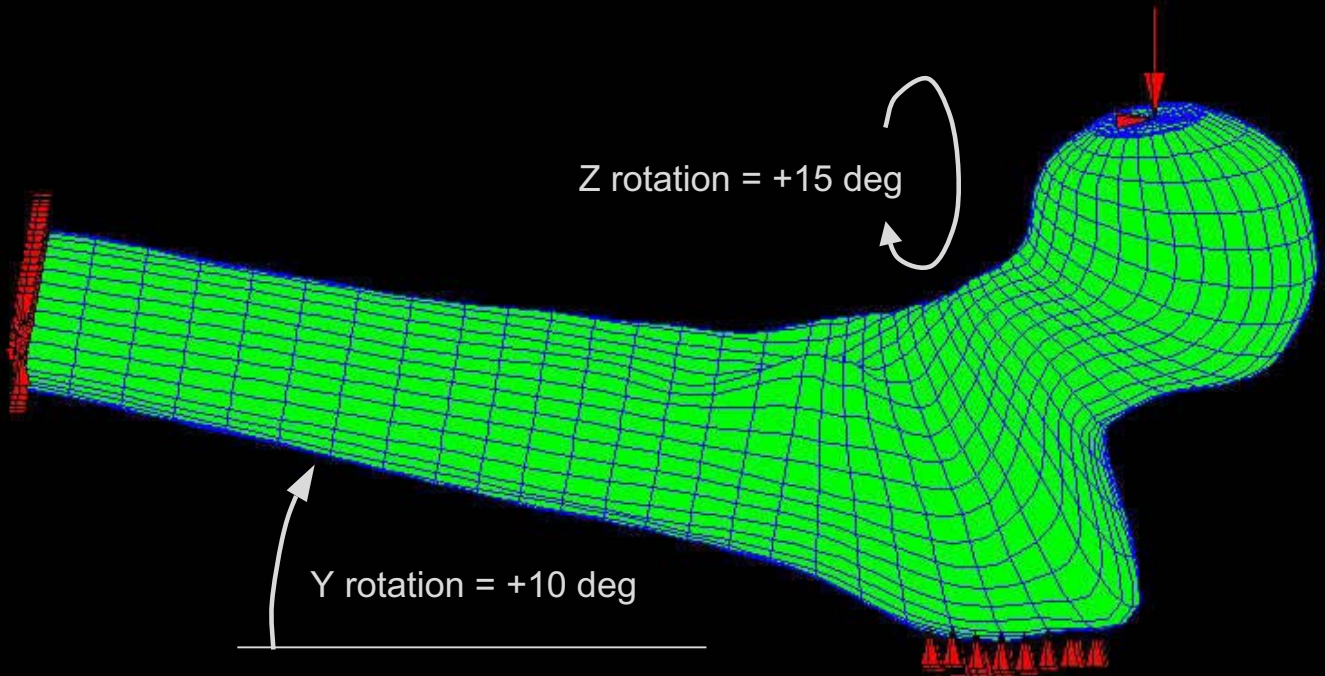


4



5





Element Material Properties

Cancellous elements [Ashman et al., 1989]:

$$E = (2.84 \times 10^3)\rho^{1.07}$$

Cortical elements [Snyder and Schneider, 1991]:

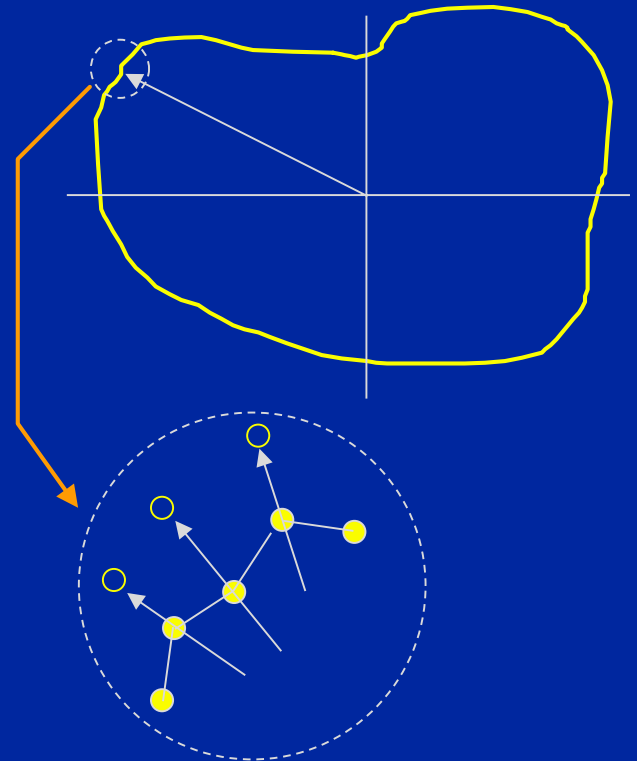
$$E = 21,910\rho - 23,500$$

Poisson's ratio: $\nu = 0.3$ for all elements

Method of Increasing Endosteal Diameter

For each curve defining endosteal boundary:

- Determine centroid
- Calculate average radius
- Calculate magnitude of point displacement (JHU results)
- Direction of displacement found by bisecting angle defined by adjacent points



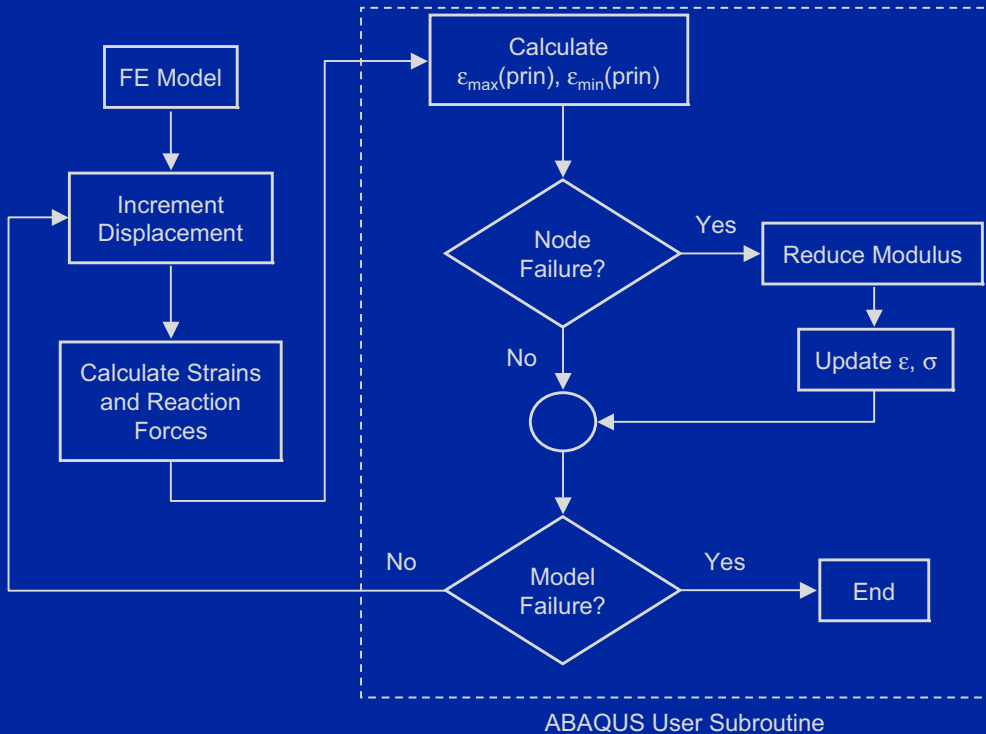
Muscle Strength Loss in Spaceflight

- Start with Earth-normal muscle magnitudes and directions: for mid-stance [Cheal et al.,1992] :

	Mag (BW)	X (med-lat)	Y (post-ant)	Z (dist-prox)
Gluteus medius	0.80	-0.67	0.18	0.72
Gluteus minimus	0.30	-0.78	0.21	0.59
Iliopsoas	1.30	-0.10	0.73	0.68

- Reduce muscle strength with duration of weightlessness:
 - 40% lower at 6 months, 60% lower at 12 months, based on lit.
 - 21% lower peak activated force 17 day flight [Widrick et al., 1999]
 - 120 days of HDT bed rest [Koryak, 1999] :
 - 44% / 33% (M/F) decline in isometric max. voluntary contraction (MVC)
 - 36% / 11% (M/F) decline in isometric twitch contraction (Pt)
 - 34% / 24% (M/F) decline in tetanic contraction force (Po)
 - Maximal explosive power (MEP) reduced to 67% after 31 days, and to 45% after 180 days of space flight [Antonutto et al., 1999]

Failure Analysis Algorithm



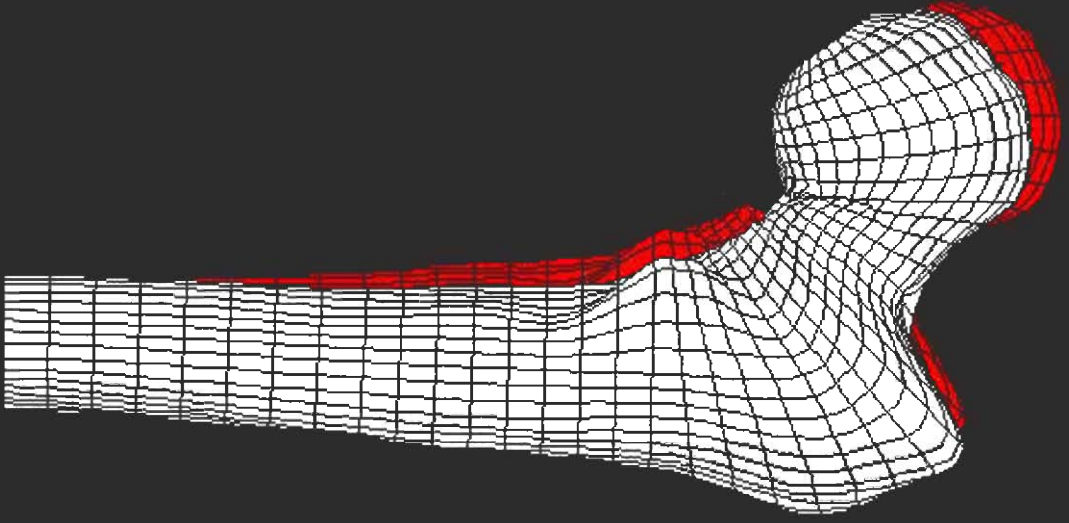
Node Failure:

Maximum Principle Strain
> 0.8% (tension)

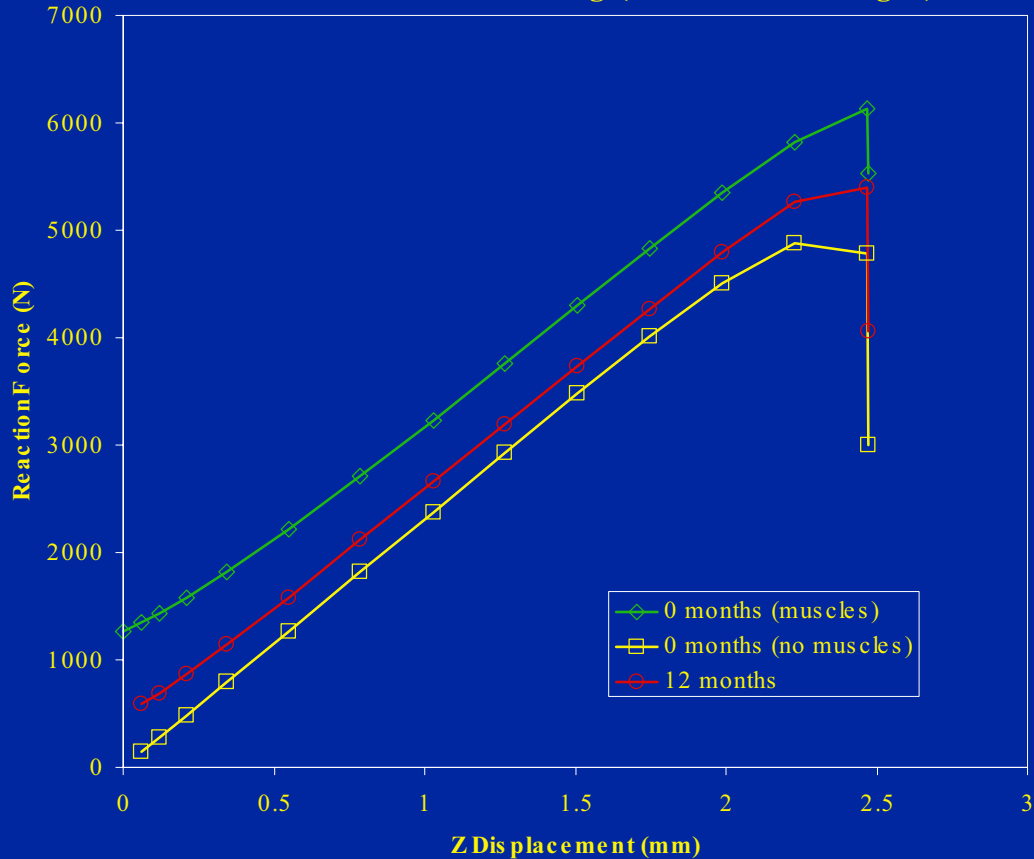
Minimum Principle Strain
< -1.1% (compression)

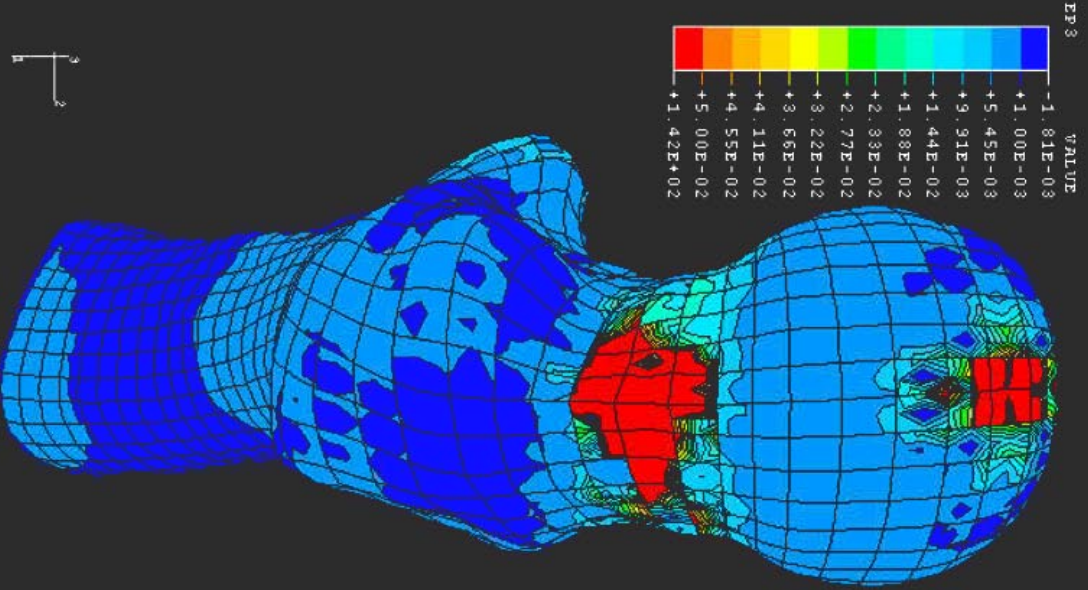
Model Failure:

Reaction Force undergoes
two successive decrements
with increasing displacement

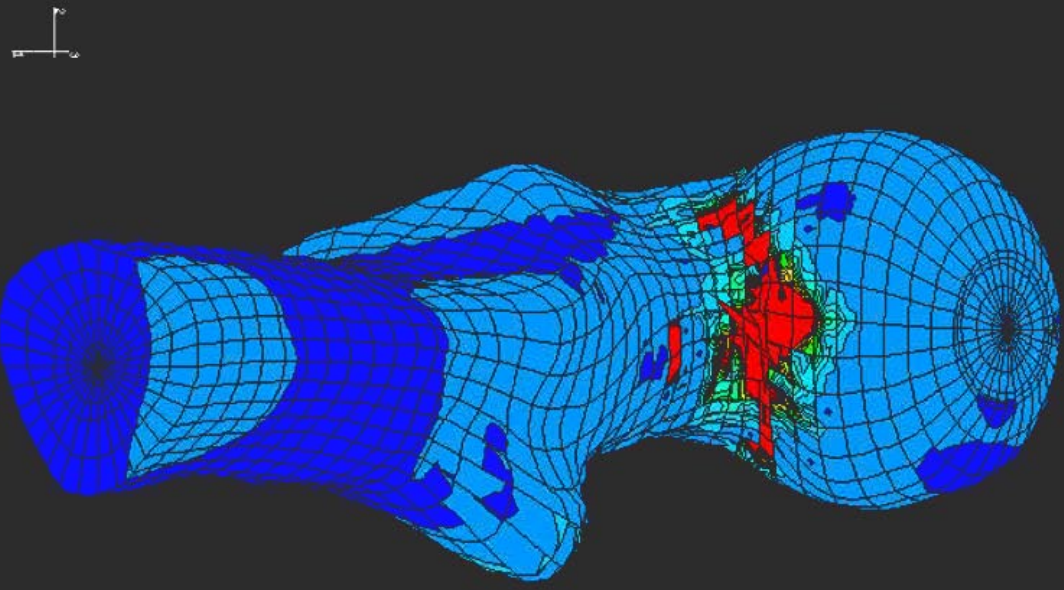


Mid-stance Loading (Pre- and Post-Flight)

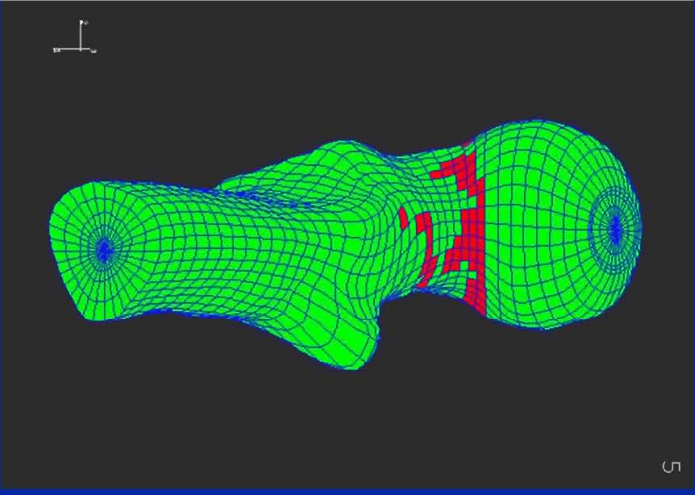
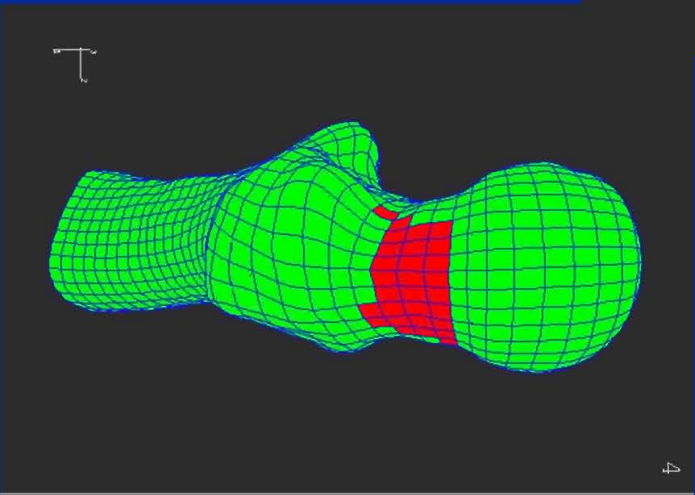
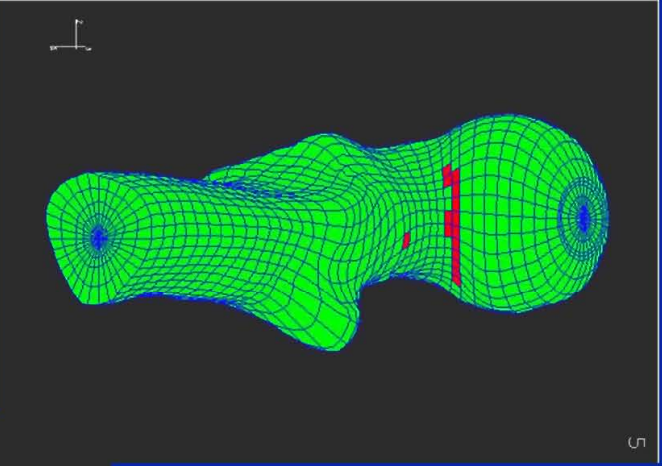
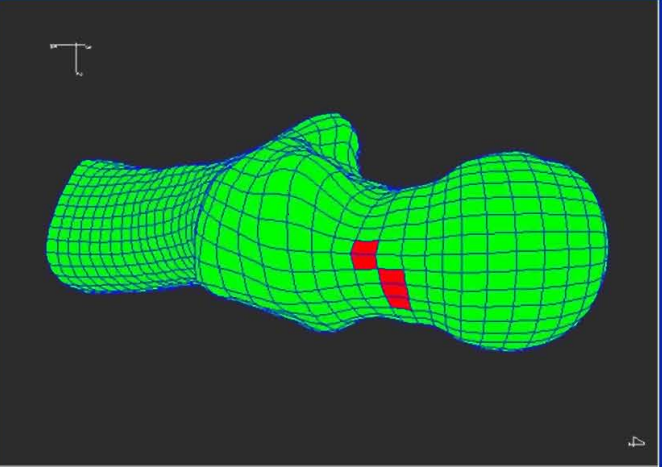


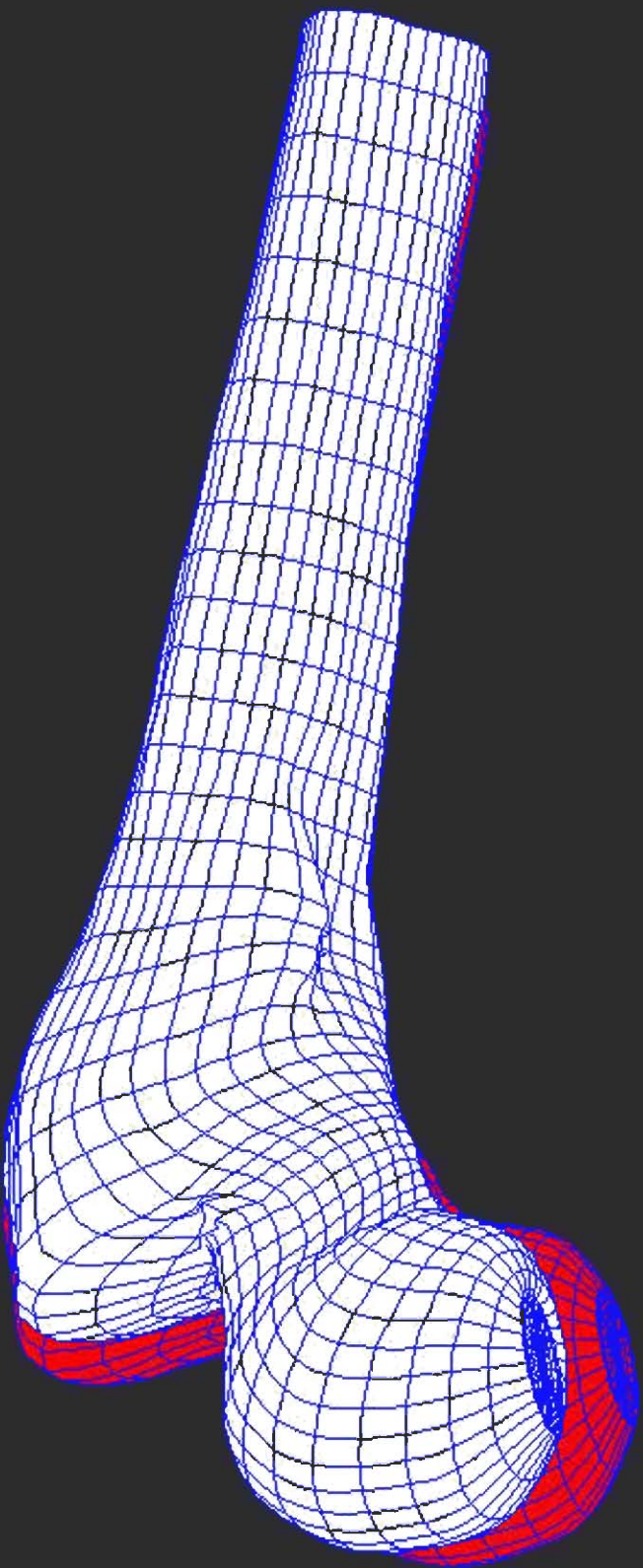


4



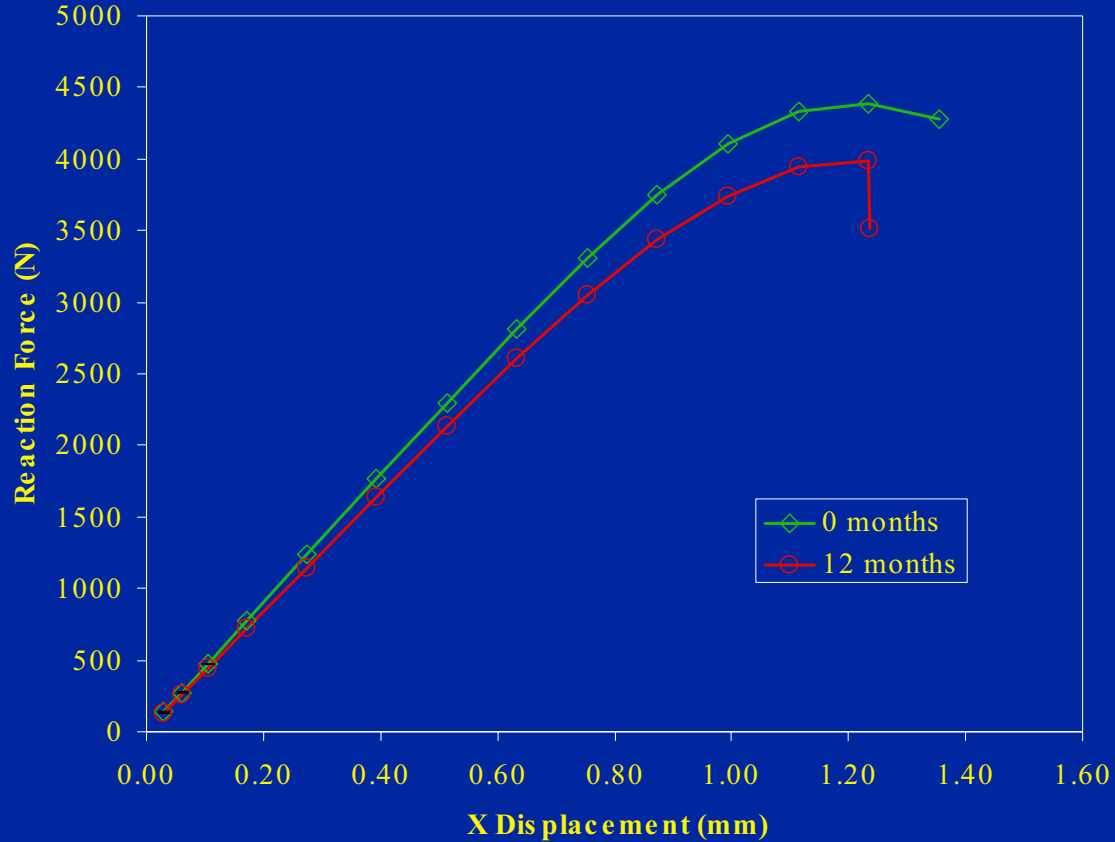
5

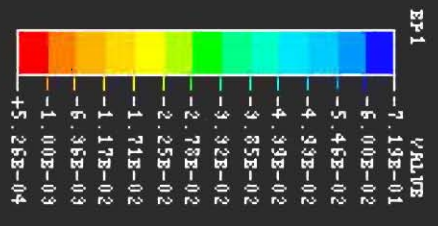
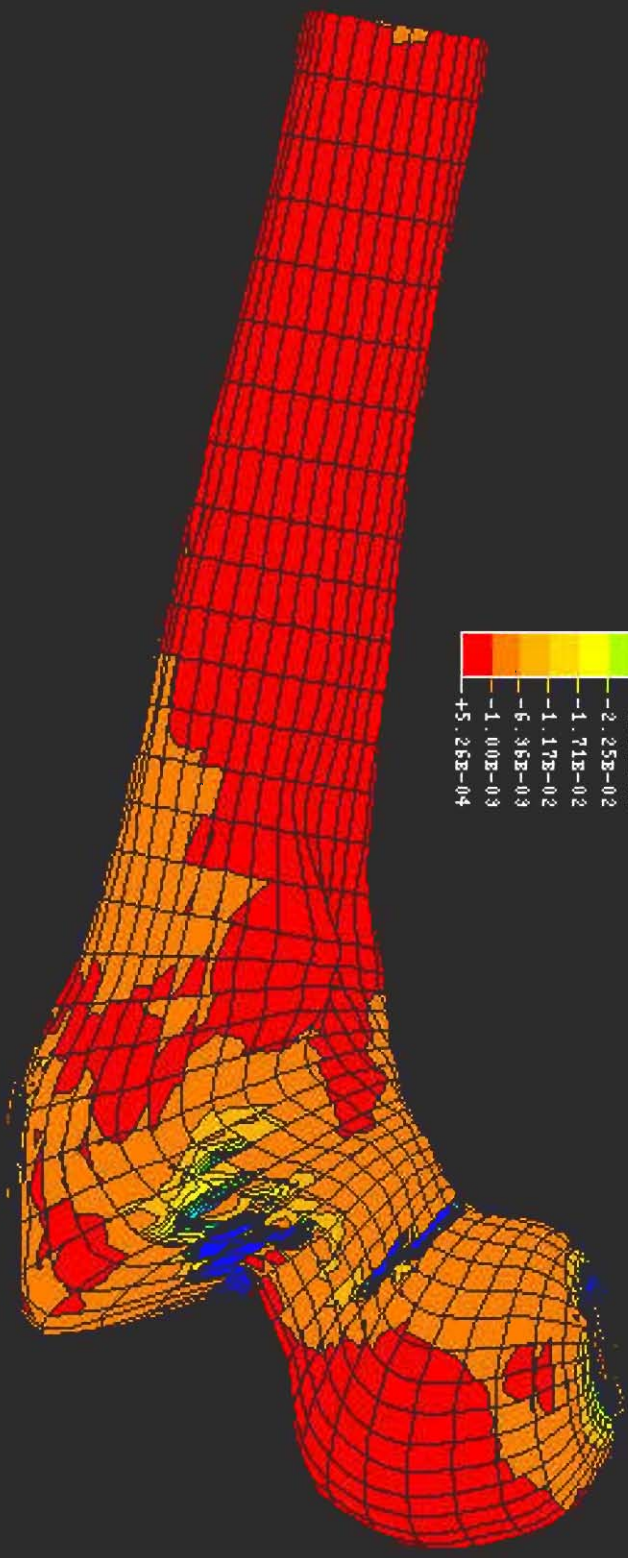


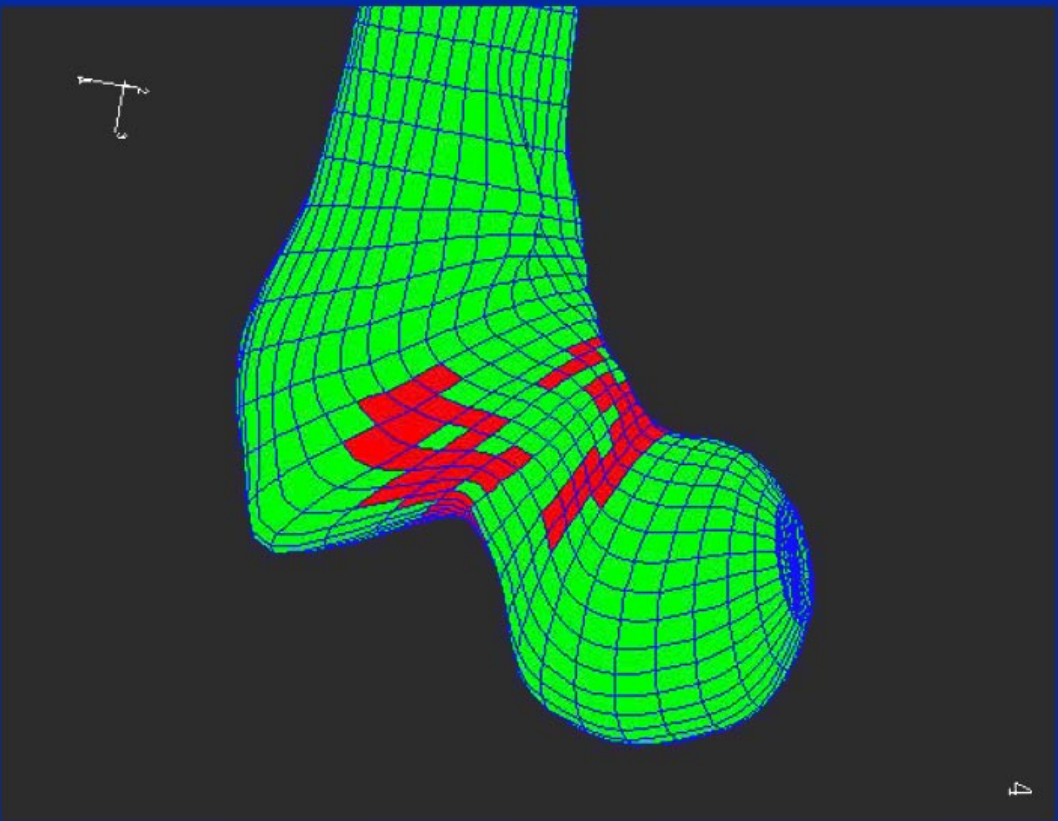
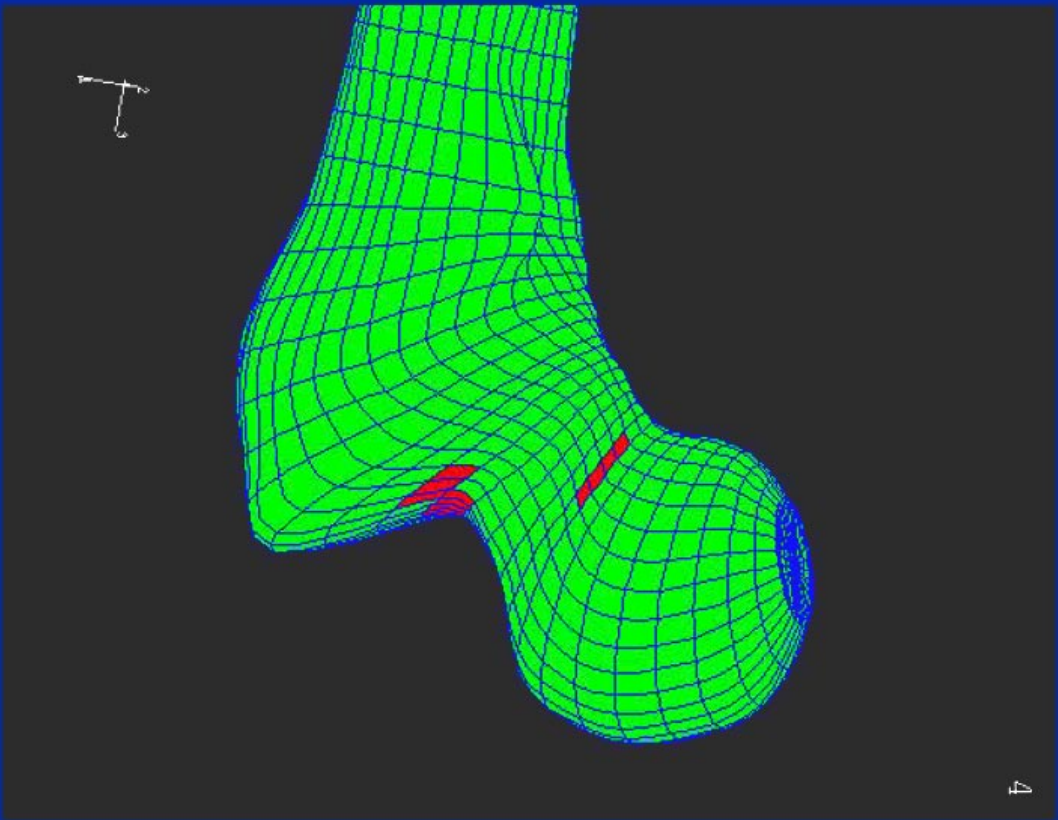


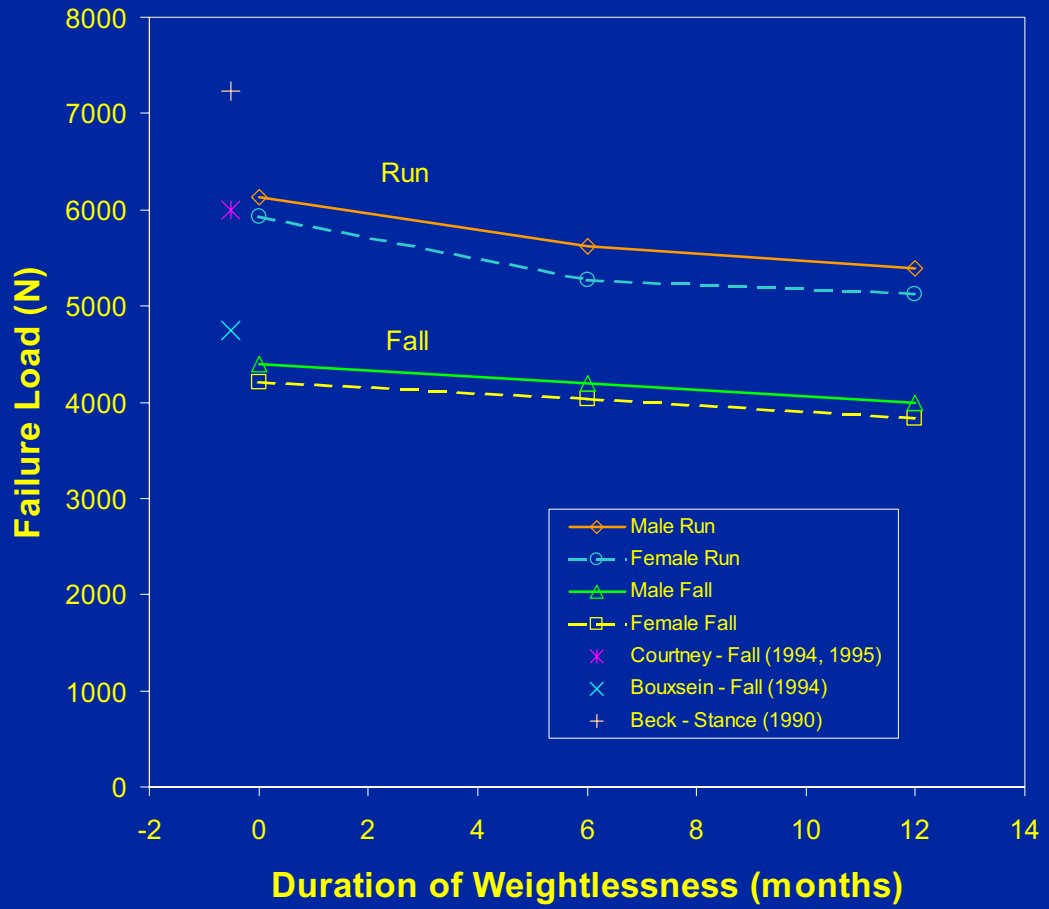
DISPLACEMENT MAGNIFICATION FACTOR = 8.00 ORIGINAL MESH DISPLACED MESH
RESTART FILE = mat_mfo STEP 1 INCREMENT 14
TIME COMPLETED IN THIS STEP 0.451 TOTAL ACCUMULATED TIME 0.451
ABAQUS VERSION: 5.8-1 DATE: 24-JUL-1999 TIME: 15:22:33

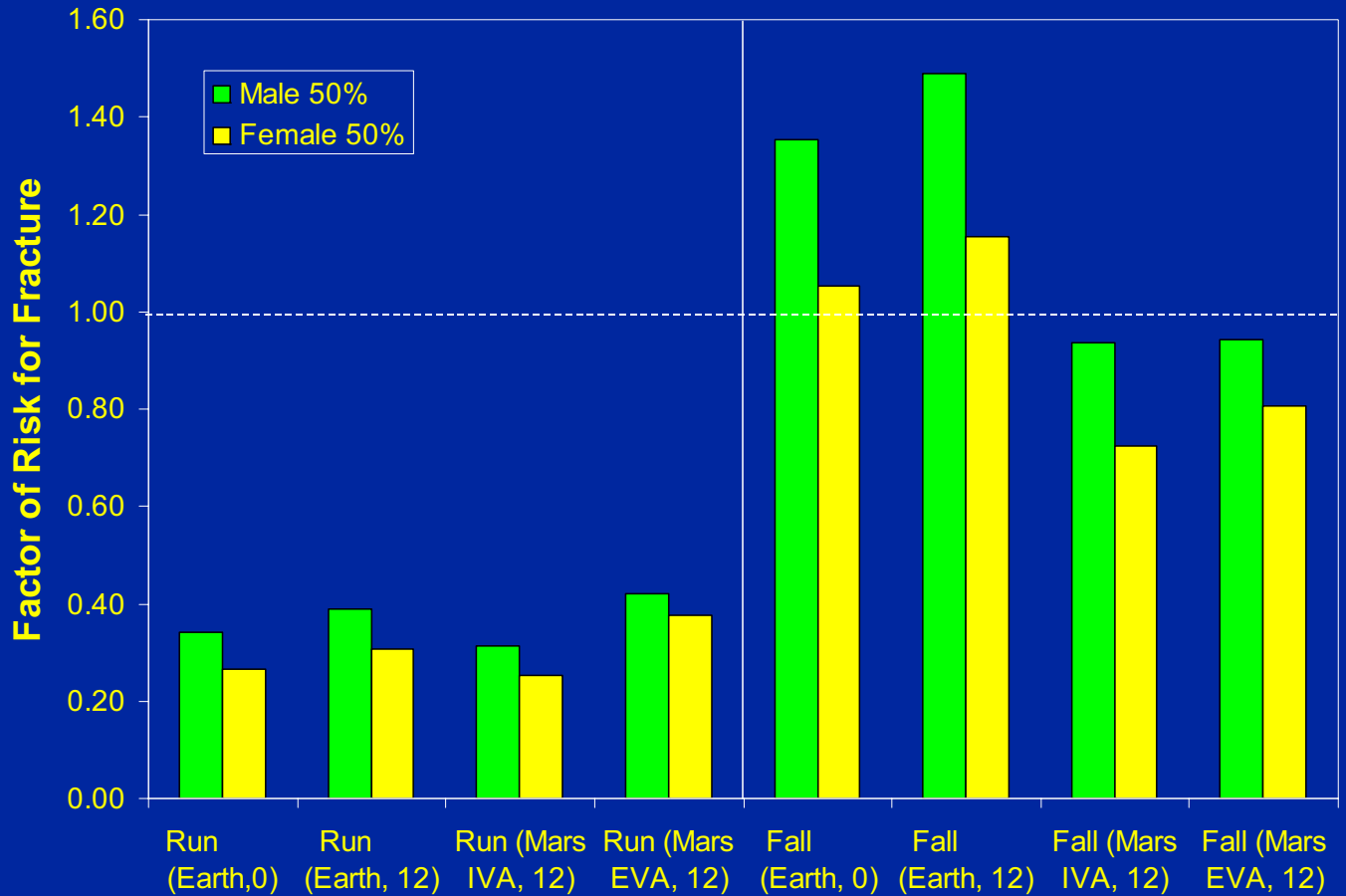
Fall Configuration Loading (Pre- and Post-flight)











Conclusions

- Fall impact carries higher risk of fracture under all circumstances.
- Risk of fracture during locomotion is significantly greater for Mars EVA compared to Earth-normal and Earth-return. Reducing space suit mass is important.
- Muscles contribution during mid-stance is critical.
- Contrary to popular belief, risk of fracture during a fall on Mars (both IVA and EVA) is decreased compared to Earth-normal (lower gravity, spacesuit padding for EVA). FOR values are still close to 1.0, though, especially for males.
- Greatest risk to astronauts is from a fall occurring right after return from a long-duration mission. Use hip pads temporarily?