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α v and β 1 integrins regulate dynamic compression–induced proteoglycan synthesis in 3D gel culture by distinct complementary pathways

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Abstract

Objective: Our goal was to test the hypothesis that specific integrin receptors regulate chondrocyte biosynthetic response to dynamic compression at early times in 3D gel culture, during initial evolution of the pericellular matrix, but prior to significant accumulation of further-removed matrix. The study was motivated by increased use of dynamic loading, *in vitro*, for early stimulation of tissue engineered cartilage, and the need to understand the effects of loading, *in vivo*, at early times after implantation of constructs.

Methods: Bovine articular chondrocytes were seeded in 2% agarose gels (15×10^6 cells/mL) and incubated for 18 hours with and without the presence of specific integrin blockers (small-molecule peptidomimetics, function-blocking antibodies, and RGD-containing disintegrins). Samples were then subjected to a 24-hour dynamic compression regime found previously to stimulate chondrocyte biosynthesis in 3D gel as well as cartilage explant culture (1 Hz, 2.5% dynamic strain amplitude, 7% static offset strain). At the end of loading, proteoglycan synthesis (^{35}S -sulfate incorporation), protein synthesis (^3H -proline incorporation), DNA content (Hoechst dye 33258) and total GAG content (DMMB dye binding) were assessed.

Results: Consistent with previous studies, dynamic compression increased proteoglycan synthesis and total GAG accumulation compared to free-swelling controls. Blocking $\alpha\beta$ 3 abolished this response, independent of effects on controls, while blocking β 1 abolished the relative changes in synthesis when changes in free-swelling synthesis rates were observed.

Conclusions: This study suggests that both $\alpha\beta$ 3 and β 1 play a role in pathways that regulate stimulation of proteoglycan synthesis and accumulation by dynamic compression, but through distinct complementary mechanisms.

Keywords

Integrin; Mechanical stimulation; Dynamic Compression; Chondrocyte; Proteoglycan synthesis; Agarose culture; Mechanotransduction

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Conflict of interest statement

E.C.A. is a former employee and stockholder of Pfizer, Inc.; D.W.G. is an employee and stockholder of Pfizer, Inc.

Introduction

In vivo, articular cartilage experiences a combination of compressive, tensile, and shear forces, both dynamic and static in nature¹⁻³. These mechanical forces can induce a variety of macroscopic signals including changes in intratissue pH and osmotic pressure, hydrostatic pressure gradients, fluid flow, streaming potentials and current, and mechanical deformation⁴⁻⁶, which are sensed by chondrocytes and can regulate cell behavior. *In vivo*, static immobilization or reduced joint-loading leads to a loss of glycosaminoglycan (GAG) content and decreased proteoglycan (PG) synthesis, which can be partially rescued by remobilization^{7, 8}. *In vitro*, radially unconfined dynamic compression at frequencies greater than 0.001 Hz has been shown to increase chondrocyte biosynthesis of PG and protein in both explant and 3-D agarose gel culture models⁹⁻¹², while static compressive loading can lead to decreases in biosynthesis¹³⁻¹⁶. *In vitro*, static and dynamic loading cause activation of mitogen-activated protein (MAP) kinase pathway and ion channel signaling cascades, which result in time-varying changes in gene transcription of matrix proteins, catabolic enzymes, and transcription factors¹⁷⁻²⁰.

Recent research on the transduction of mechanical signals into changes in cell behavior has begun to elucidate the role of integrin interactions with the extracellular matrix (ECM). Chondrocytes express $\alpha 1\beta 1$, $\alpha 2\beta 1$, $\alpha 3\beta 1$, $\alpha 5\beta 1$, $\alpha v\beta 3$ and $\alpha v\beta 5$ ²¹⁻²³. This expression can change with local microenvironment, mechanical stimulation, and during osteoarthritis²⁴⁻²⁶. Integrins play a role in adhesion, cell survival, regulating matrix metabolism, and in chondrocyte response to mechanical stimuli *see 27-29 for reviews*. $\beta 1$, $\alpha 5\beta 1$, $\alpha v\beta 5$ integrins have been shown to mediate chondrocyte adhesion to cut cartilage surfaces²¹⁻³⁰. In monolayer studies, blocking $\alpha 5\beta 1$ integrin interactions led to increased matrix metalloproteinase-13 (MMP-13) activation and cellular apoptosis²³⁻³¹. Upregulation of aggrecan mRNA and suppression of matrix metalloproteinase-3 (MMP-3) mRNA levels by dynamic stretching of monolayer chondrocytes was shown to involve a $\beta 1$ -integrin-dependent pathway as well as stretch-activated ion channels and autocrine/paracrine stimulation by interleukin-4 (IL-4)³²⁻³³. Other studies have also identified a $\beta 1$ -integrin-dependent translocation of protein kinase C alpha (PKC α) to the cell membrane, increased association of intracellular receptor for activated C-kinase1 (RACK1) and PKC α with $\beta 1$ -integrin after mechanical stimulation³⁴, and interactions between the integrin associated protein (CD47/IAP) and $\alpha 5$ -integrin³⁵, as possible downstream signaling mechanisms. More recently, monolayer studies demonstrated that blocking with anti- $\alpha v\beta 5$ antibody could also abolish chondrocyte responses to dynamic stretching³⁶.

The use of physiologic dynamic compression as a stimulant for cartilage regeneration in tissue engineering has been demonstrated by several groups^{10,11,19,37-41} and has prompted studies of the mechanisms by which cells in tissue engineered constructs transduce signals under physiological loading conditions. While some studies suggest a role for ion channels, especially calcium channels, in regulating sGAG synthesis in response to dynamic compression^{42,43}, studies in 3-D culture models have suggested that the roles are more complicated than that elucidated in monolayer culture models⁴². Monolayer studies have provided insights into signaling pathways involved in chondrocyte mechanotransduction, but the role of cell interactions with newly-synthesized and assembled matrix macromolecules in 3-D geometries is less well understood.

The goal of this study was to examine the role of integrins in chondrocyte response to dynamic compression by cells in 3D agarose gel culture at early times in culture, during initial evolution of the pericellular matrix, but prior to significant accumulation of further removed extracellular matrix. Chondrocyte cultures in agarose at early times, with little pericellular matrix present, can respond to dynamic compression with increased sulfate incorporation and sGAG

accumulation^{10,11,39}. They also have the added benefit of permitting the use of multiple methods for perturbing integrin-matrix interactions, including the use of blocking antibodies similar to those used in monolayer studies, which have diffusive limitations in native cartilage tissue.

Methods

CELL HARVEST AND CULTURE

Chondrocytes were isolated from the femoral condyle cartilage of 2- to 3- week old bovine calves (Research 87, Marlborough, MA) by sequential digestion in 0.2% pronase (Protease type XIV, Sigma) and 0.025% Collagenase-P (Roche), as described previously⁴⁴. Cells were seeded in 2% agarose (low melting-temperature, Invitrogen) at concentrations of 15 million cells/mL using a stainless steel casting frame^{38,45}, in a slab geometry approximately 1.6 mm thick. 4 mm diameter disks were cored from the slab using a dermal punch and cultured in 1% ITS-supplemented feed medium (high glucose DMEM, 0.1 mM nonessential amino acids, 0.4 mM proline, 100 U/mL PSA – penicillin, streptomycin, amphotericin, 10 µg/mL ascorbate).

INTEGRIN-BLOCKING COMPOUNDS

An array of integrin-blocking compounds was used including small-molecule peptidomimetics, function-blocking antibodies, and RGD-containing disintegrins. Small-molecule compounds have the advantage of rapid diffusion times, which allow for more spatial uniformity of treatment. PF001 (previously referenced as S247 46), PF002, PF003 are synthetic peptidomimetics (obtained from Pfizer; Fig. 1) of the conserved amino acid motif RGD (arginine-glycine-aspartic acid) and are potent *in vitro* antagonists (with IC₅₀s on the order of nM) of ligand interaction with specific integrins. Their molecular weights and potencies against selected integrins as measured in integrin-overexpressing cell-adhesion assays are summarized in Table 1. PF001 is a relatively broad spectrum blocker while PF002 and PF003 are more specific blockers of $\alpha 5\beta 1$ and $\alpha v\beta 3$ integrins, respectively.

To test activity and toxicity of the peptidomimetic compounds, a cell-adhesion assay was performed using an RGD-conjugated comb copolymer surface which promotes integrin-mediated adhesion and prevents non-specific adhesion⁴⁷⁻⁴⁹. Prepared surfaces were obtained⁵⁰ in which cover slips were spin-coated with a poly(methyl methacrylate)-*graft*-poly(ethylene oxide), PMMA-g-PEO, a comb copolymer with a fraction of PEO side chains functionalized with maleimide groups using N-(p-maleimidophenyl) isocyanate (PMPI), and conjugated with a PHSRN-K-GRGDSP peptide (RGD peptide + fibronectin synergy site). The RGD-containing peptide was presented in dispersed and clustered conformations. Further details of polymer synthesis, peptide synthesis, and surface preparation are described in Kuhlman et al.⁴⁸. Cover slips were placed at the bottom of a 24-well plate and held in place by silicon rings. After isolation, 25,000 chondrocytes were seeded per well and given 2 hours to attach. PF001, PF002, PF003 were then added at concentrations of 0, 50, 100, or 200 µM. Cells were cultured for 7 days, with medium changes every other day. Cells were imaged daily using an inverted microscope to qualitatively observe adhesion and spreading. After 7 days, cells were stained with FDA/EtBR (live/dead assessment) and imaged using an inverted UV microscope.

Echistatin (Sigma) is a 5.4 kDa disintegrin peptide that non-selectively blocks the activities of several integrins including $\alpha v\beta 3$, $\alpha 5\beta 1$, and $\alpha I\text{Ib}\beta 3$ with IC₅₀s on the order of 10nM⁵¹. Function blocking antibodies to $\alpha v\beta 3$ (MAB1976, clone LM609), αv (MAB1953, clone P3G8), $\alpha 5$ (MAB1956, clone P1D6), and $\beta 1$ (MAB1965, clone JB1A) integrins were obtained from Chemicon. Cross-reactivity of blocking antibodies MAB1976, MAB1956, and MAB1965 to bovine integrins have been previously demonstrated⁵²⁻⁵⁴ and are supported by dot-blot

analysis (Figure 1S). Echistatin³¹ and the blocking antibodies^{21,23,34,55,56} have been previously used on chondrocytes with no reported cell death. All antibody preps had endotoxin levels below 0.5 EU/mL (LAL method, Lonza QCL-1000 test kit).

MECHANICAL LOADING

On day of casting, 3-4 chondrocyte-seeded agarose disks maintained in free-swelling culture were pre-incubated for 18 hours in one of the following conditions: (1) untreated control (feed medium), (2) 200 μ M PF001, PF002, or PF003, (3) 5 μ g/mL integrin-blocking antibody (each antibody used in separate experiments), (4) 1 μ M echistatin. Parallel sets of disks from treatment conditions (1) – (4) were subjected to dynamic compression. Immediately prior to loading, 5 μ Ci/mL of ³⁵S-sulfate and 10 μ Ci/mL of ³H-proline were added to the medium. Disks were then subjected to a 24-hour, 1 Hz continuous, sinusoidal unconfined dynamic compression at 2.5% dynamic strain amplitude (in displacement feedback control) superimposed on a 7% static offset strain, using a non-porous polysulfone loading chamber and platens in an incubator-housed loading apparatus⁵⁷. Free-swelling cultures over the same 24-hour incubation period served as controls. Throughout the applied compression, the total harmonic distortion of the resulting continuously measured dynamic load signal was < 25%. The applied cyclic displacement waveform and resulting load waveform were similar to that shown in ref. 37. Upon completion of loading, plugs were washed 3 \times 20 minutes in PBS with 142 μ g/mL sodium sulfate and 50 μ g/mL L-proline to remove free radiolabel, and digested in 1mL Proteinase K (0.1 mg/mL, Roche) at 60°C overnight (~16 hours). Experiments were repeated using chondrocytes isolated from 1-6 animals (as noted below).

BIOCHEMICAL MEASUREMENTS

Radiolabel incorporation rates were measured by scintillation counting^{58,59}. sGAG content in the proteinase K digests and collected medium was assayed by DMMB dye binding⁹. DNA was quantified by Hoechst 33258 dye-binding assay⁶⁰.

DATA ANALYSIS

Radiolabel incorporation and sGAG content data were normalized to DNA content to account for disk-to-disk variations in cell number. Data were further normalized to averaged free-swell controls for each animal to account for baseline animal-to-animal variability. All data are shown as mean \pm 95% confidence interval (CI). The number of observations varied with treatment, as detailed in the figure legends. A Shapiro-Wilk test was used to test for normality of data. 1-way and 2-way ANOVA was used to test for the effect of treatment (mechanical and/or pharmacological) followed by post-hoc Bonferoni pairwise comparisons to correct for multiple comparisons from multiple treatments. A p-value < 0.05 was considered significant. Statistical analysis was performed using Systat 12 software (Richmond, CA).

Results

ACTIVITY AND TOXICITY OF PF001, PF002, PF003

RGD-conjugated comb copolymer surfaces that can promote binding by the α v β 3 or α 5 β 1 integrins were used to confirm activity of PF001, PF002, and PF003 on chondrocytes. By day 6 in culture, untreated cells seeded onto RGD-conjugated surfaces showed a spread morphology, while cells treated with 100 μ M PF001, PF002, or PF003 remained rounded on the RGD-conjugated surfaces throughout the 7-day treatment (Supplementary Fig. 2S). Treatment with 1 μ M echistatin served as an assay control. At concentrations up to 200 μ M of each compound over 7 days, there was no qualitative increase in ethidium bromide-stained cells (approximately 10%) (Fig. 2S) compared to untreated controls or quantitative changes in DNA content (Fig. 3S), suggesting no adverse effects on cell viability.

EFFECTS OF SMALL-MOLECULE BLOCKERS ON GAG BIOSYNTHESIS AND ACCUMULATION WITH DYNAMIC COMPRESSION OF AGAROSE GEL CULTURES

To test the role of integrin-ECM interactions in chondrocyte biosynthetic response to dynamic compression, agarose cultures were incubated with small-molecule peptidomimetics of the RGD binding sequence recognized by integrins such as $\alpha v\beta 3$ and $\alpha 5\beta 1$ to block these interactions and subjected to a 24-hour continuous, unconfined dynamic compression. At the end of the loading period, untreated free-swelling cultures incorporated an average of 192 pmol sulfate/ μg DNA/hr and accumulated 7.38 μg GAG/ μg DNA. Treatment with PF001, PF002, or PF003 did not alter DNA content (Supplementary Fig. 3S). DNA content was used to normalize data for all subsequent analyses. *In free-swelling controls*, PF001 and PF002 did not significantly change sulfate incorporation or sulfated GAG content, while PF003 (200 μM) resulted in a 27% decrease in sulfate incorporation ($p < 0.0005$ compared to untreated control using post-hoc Bonferoni pairwise comparison) and 17% decrease GAG content ($p < 0.0005$ vs. untreated control) (Fig. 2). Free-swell levels for sulfate incorporation and GAG content under all treatment conditions can be found in Supplementary Materials (Figure 5S).

Consistent with previous studies^{10,11,39}, low amplitude ($< 10\%$ strain amplitude) dynamic compression at 1Hz frequency increased sulfate incorporation rates by approximately 25% (to 243 pmol sulfate/ μg DNA/hr, $p < 0.0005$ vs. free-swell control) after 24 hours of compression in untreated agarose gel plugs (Fig. 2). GAG loss to the medium was minimal: $< 10\%$ of the total GAG content (i.e., agarose disk plus medium combined) or approximately 0.7 μg GAG/ μg DNA, was lost to the medium over 24 hours in free-swell culture. While GAG loss to medium increased by $\sim 75\%$ to 1.2 μg GAG/ μg DNA with dynamic compression, possibly due to increased transport, enhanced synthesis caused a net increase in GAG accumulation within the disks after 24 hours of dynamic compression by $\sim 14\%$ (to 8.51 μg GAG/ μg DNA, $p < 0.0005$ vs. free-swell control) (Fig. 2). Since the experiment was conducted during early times in culture and GAG loss was minimal, the majority of the GAG content was newly synthesized and GAG accumulation mirrored sulfate incorporation trends.

PF001-treated samples responded to dynamic compression with similar increases in sulfate incorporation (27%, $p < 0.0005$ compared to treated free-swell control in post-hoc Bonferoni comparison) and GAG accumulation (15%, $p = 0.089$ vs. treated free-swell control, $p = 0.017$ uncorrected) (Fig. 2). PF002-treated samples responded to dynamic compression with slight increases in sulfate incorporation (12%, $p = 0.16$ vs. treated free-swell control, $p = 0.03$ uncorrected) and GAG accumulation (6%). In contrast, PF003-treated samples showed no stimulation of sulfate incorporation or GAG accumulation with dynamic compression (Fig. 2). None of the treatments (PF001, PF002, or PF003) affected GAG loss to the medium. Taken together, markers of PG synthesis (sulfate incorporation and GAG content) were responsive to dynamic compression and sensitive to the integrin blocker PF003, the most selective inhibitor of $\alpha v\beta 3$ function. A dose response experiment up to the efficacious concentration of 200 μM with PF003 was then conducted: PG synthesis response to dynamic compression was measured at 0, 100, 150, 200 μM PF003. Free-swelling disks showed a graded decrease in sulfate incorporation and GAG accumulation with increasing concentrations of PF003 (Fig. 4SA,B). Stimulation of PG synthesis (sulfate incorporation and GAG accumulation) by dynamic compression relative to free-swell also varied with increasing concentrations of PF003, with a slight (10%, $p = 0.8$ compared to treated free-swell in Bonferoni post-hoc pairwise comparison, $p = 0.15$ uncorrected) increase in sulfate incorporation and GAG accumulation at 100 μM , and no stimulation by 150 μM PF003 (Fig. 4S).

BROAD-SPECTRUM BLOCKERS PF001 AND ECHISTATIN SHOWED LITTLE EFFECT ON RESPONSE TO DYNAMIC COMPRESSION

Echistatin is a disintegrin containing the RGD-motif that has broad specificity to integrins⁵¹. In free swelling controls, echistatin decreased sulfate incorporation by 43% ($p < 0.0005$ compared to untreated control in Bonferoni post-hoc pairwise comparison) and GAG content by 21% ($p < 0.0005$ vs. untreated control) (Fig. 3A), and increased GAG loss to medium by 77%. In contrast, PF001 had no effect on radiolabel incorporation or GAG accumulation in free swelling conditions. With PF001 treatment, dynamic compression increased sulfate incorporation by ~20% ($p < 0.0005$ compared to treated free-swell) and slightly increased GAG content ($p = 0.071$ vs. treated free-swell, $p = 0.02$ uncorrected). In contrast, with echistatin treatment, dynamic compression increased sulfate incorporation in treated samples by ~20% ($p = 0.125$, $p = 0.032$ uncorrected), and dynamic compression did not stimulate GAG accumulation (Fig. 3B). This may be due to GAG loss to medium, not seen in PF001-treated samples, since the total GAG content (agarose disk + medium) increased by ~9% after 24 hours dynamic compression in the presence of echistatin.

DIFFERENTIAL EFFECTS OF INTEGRIN BLOCKERS IN FREE-SWELLING CULTURE

To further test the hypothesis that blocking specific integrin-ECM interactions can disrupt chondrocyte response to dynamic compression, a series of blocking antibodies were used in parallel experiments. Antibodies are larger in size (~150 kDa), but in agarose culture at early times before much accumulation of ECM, antibodies can still diffuse in relatively easily^{61, 62}. $\alpha v \beta 3$ blocker PF003 decreased sulfate incorporation by approximately 30% ($p < 0.0005$ compared to untreated control by Bonferoni pairwise comparisons) and GAG accumulation by 18% ($p < 0.0005$ vs. untreated control) in free-swelling culture (Fig. 4A). $\alpha v \beta 3$ blocking antibody clone LM609 showed a slight but non-significant decrease in sulfate incorporation at 5 $\mu\text{g}/\text{mL}$ (Fig. 4A). αv blocking antibodies showed no effects on sulfate incorporation, GAG accumulation, or GAG loss in free-swelling culture (Fig. 4A). In contrast, $\alpha 5 \beta 1$ blocker PF002 showed a slight increase in sulfate incorporation (9%) and GAG accumulation (6%) under free swelling conditions (Fig. 5), and blocking antibodies to $\beta 1$ (5 $\mu\text{g}/\text{mL}$, 10 $\mu\text{g}/\text{mL}$) integrins increased sulfate incorporation rates, and GAG accumulation by 20%-40% ($p < 0.0005$, vs. untreated control) (Fig. 5A). None of the blocking antibodies had significant affects on GAG loss to the medium.

$\alpha v \beta 3$ AND $\beta 1$ BLOCKING ANTIBODIES, NOT PF002 OR $\alpha 5$ BLOCKING ANTIBODIES, ABOLISHED PG-SYNTHESIS RESPONSE TO COMPRESSION

In untreated samples, dynamic compression increased sulfate incorporation rates by approximately 20% ($p < 0.0005$ compared to free-swelling control by Bonferoni post-hoc comparison) and GAG accumulation by 14% ($p < 0.0005$ vs. free-swelling control). Treatment with PF003, $\alpha v \beta 3$ blocking antibodies, and αv blocking antibodies abrogated this response to dynamic compression ($p < 0.0005$ by ANOVA) (Fig. 4B). In separate experiments with PF002 and $\alpha 5$ blocking antibody-treated samples, dynamic compression resulted in a 12-15% increase in sulfate incorporation ($p = 0.079$, 0.023 , respectively vs. treated free-swelling controls, $p = 0.011$, 0.006 uncorrected), while GAG accumulation increased by only 5-10% (Fig. 5B). $\beta 1$ blocking antibody-treated samples showed no stimulation of sulfate incorporation or GAG accumulation by dynamic compression (Fig. 5B). None of these effects described were due to changes in GAG loss to medium. While blockers of $\alpha v \beta 3$ and $\beta 1$ integrins both appear to abrogate the response to dynamic compression, they appear to be acting through distinct pathways considering their opposing effects in free-swelling culture.

Discussion

Dynamic compression and other mechanical stimuli have been increasingly used in tissue engineering to promote development of cartilage constructs through increasing extracellular matrix content and mechanical properties^{37,38}, and the use of immature chondrocytes in tissue engineering and cartilage repair has been shown to be an effective cell source for tissue engineering, with greater activity than adult chondrocytes⁶³⁻⁶⁵. Even at early times in culture, when little pericellular matrix is present, chondrocyte cultures in agarose can respond to dynamic compression with increased sulfate incorporation and sGAG accumulation^{10,11,39}. This response to 24 hours of continuous dynamic compression increased with number of days in free-swell culture¹⁰. In long-term studies of the effects of dynamic loading, the presence of a pre-elaborated pericellular matrix (either by seeding chondrons initially or culturing for 2 weeks prior to loading) did not alter the stimulatory effects of extended dynamic loading, which increased with loading duration³⁷. This suggests that interactions between the cell and its surrounding matrix developed *during* dynamic compression may play a greater role than pre-existing interactions. The goal of this study was to examine the role of integrin-ECM interactions in the response of chondrocytes to dynamic compression at early times in culture using a 3D agarose culture of immature bovine chondrocytes as a model system. An added benefit of studying such interactions at early times is the ability to compare multiple integrin blockers, including antibodies, without the complicating issue of diffusion and penetration of antibodies into a dense tissue matrix. The results of this study suggest that multiple integrins ($\beta 1$, $\alpha v\beta 3$) appear to play a role in mechanotransduction and the chondrocyte's ability to sense its local microenvironment; however these integrins appear to play opposing or complementary roles.

In the present study, blocking $\beta 1$ integrin function with blocking antibodies, or blocking $\alpha v\beta 3$ integrins with either small-molecule antagonists or blocking antibodies, abolished proteoglycan stimulation by dynamic compression (as measured by sulfate incorporation or sGAG accumulation). While the concentration of the small-molecule antagonists used in these functional assays were much higher than the IC50s reported in Table 1, previous studies have confirmed the observation that higher concentrations are necessary to see functional response, especially in 3-D culture models⁶⁶. Our results using blocking antibodies support the specificity of these small-molecules as well. As previously shown^{10,11,39}, 24 hour continuous unconfined dynamic compression stimulated proteoglycan synthesis at days 1-2 in culture. Measurable amounts of sGAG were accumulated in constructs by the end of culture. Previous studies have also shown that a pericellular matrix begins developing within 4 hours after isolation⁶⁷ and can be visualized at the cell surface on day 2 in agarose culture⁶⁸. The $\beta 1$ integrin subunit can associate with a large number of differentially expressed alpha subunits to form integrins with distinct ligand binding and cell signaling characteristics. Echistatin and the RGD peptidomimetics used in this study are expected to inhibit only the subset of $\beta 1$ -containing integrins that interact with their ligands via the RGD sequence. $\alpha v\beta 3$ and $\alpha 5\beta 1$ are both RGD-recognizing integrins. While the main binding partners for $\alpha v\beta 3$ and $\alpha 5\beta 1$ are vitronectin and fibronectin, respectively, $\alpha v\beta 3$ has also been shown to bind to fibronectin, fibrinogen, osteopontin, and collagen⁶⁹. Blocking $\alpha 5\beta 1$ specifically using the RGD peptidomimetic PF002 or $\alpha 5$ blocking antibodies may partially decrease proteoglycan stimulation by dynamic compression, but this effect was not significant. Other potential $\beta 1$ integrins include collagen receptors $\alpha 1\beta 1$ and $\alpha 2\beta 1$, as well as $\alpha 3\beta 1$ and $\alpha 10\beta 1$.

While blocking both $\alpha v\beta 3$ and $\beta 1$ integrins prevented stimulation of proteoglycan synthesis by dynamic compression, these results appeared to be acting through independent mechanisms. In this study, blocking $\beta 1$ integrins in free-swelling culture with blocking antibodies resulted in a significant upregulation of sulfate incorporation, while blocking $\alpha v\beta 3$ integrins with small-molecule compounds resulted in a down regulation. Blocking $\alpha v\beta 3$ integrins with antibodies

resulted in no detectable change in basal sulfate incorporation. Previous studies have suggested that $\alpha\text{v}\beta 3$ and $\alpha 5\beta 1$ have modulating roles in articular chondrocytes⁵⁶. In those studies, treatment with anti- $\alpha 5\beta 1$ antibody JBS5 induced a pro-inflammatory response (upregulation of NO, PGE2, IL-6, IL-8, and IL-1 β) in both normal and osteoarthritic cartilage as well as bovine articular chondrocytes, while treatment with $\alpha\text{v}\beta 3$ blocking antibody LM609 decreased these pro-inflammatory signals and could regulate the $\alpha 5\beta 1$ response in a dominant-negative fashion⁵⁶. Other studies demonstrated similar responses when blocking with anti- $\alpha 5\beta 1$ antibodies or treating with fibronectin fragments²³. In addition, studies have shown that blocking $\alpha 1\beta 1$ and $\alpha 2\beta 1$ with blocking antibodies can stimulate MMP-13 production through the MAP kinase pathway similar to treatment with $\alpha 5\beta 1$ blocking antibodies or fibronectin fragments^{23,70}, although their roles in mechanotransduction had not previously been investigated to our knowledge. These studies demonstrate that the use of blocking antibodies can induce cellular responses by disrupting integrin signaling or causing abnormal signaling. While the stimulation of PG synthesis by blocking $\beta 1$ integrins in agarose culture might appear to be in contradiction to these previous studies, it is possible that the stimulation observed, here, is part of increased turnover that has been described previously with hyaluronan (HA) oligosaccharide treatment of cartilage⁷¹. In addition, only blockers of $\beta 1$ integrins that induced an increase in biosynthesis in free-swelling controls resulted in abolishment of the response to dynamic compression, and the effects of blocking antibodies were distinct from that of small-molecule antagonists, which likely block integrin interactions through different mechanisms. Taken together, these studies suggest that blocking $\beta 1$ integrins with blocking antibodies may decrease response to dynamic compression through a pro-inflammatory pathway or an analogous pathway resulting from abnormal integrin signaling.

Consistent with previous studies, we observed that treatment with different types of $\alpha\text{v}\beta 3$ blockers can result in distinctly different free-swelling responses⁵⁶. However, all specific blockers of $\alpha\text{v}\beta 3$ integrins affected stimulation of proteoglycan synthesis by dynamic compression. Thus, blocking $\alpha\text{v}\beta 3$ appears to be inhibiting a signaling response directly resulting from dynamic compression, independent of effects in free-swelling culture. Finally, our observation that treatment with relatively broad-spectrum blockers (PF001 and echistatin) that target RGD-binding integrins, and which bind to $\alpha 5\beta 1$ and $\alpha\text{v}\beta 3$ with similar affinities, did not affect stimulation of proteoglycan synthesis by dynamic compression, suggests a modulatory role for $\alpha 5\beta 1$ and $\alpha\text{v}\beta 3$ as seen in previous studies⁵⁶.

It is important to note that previous studies of the role of $\alpha 5\beta 1$ integrins in chondrocyte mechanotransduction focused on chondrocyte monolayer cultures^{23, 31-35}. The present study utilizes 3D gel culture, and the results in 3D suggest a more complex view in which multiple integrins may be playing a role in regulating chondrocyte response to compression within the gel construct. This hypothesis is consistent with research on the role of ion channel signaling, where more complex interactions were observed in 3D compared to 2D culture⁴³. A variety of mechanical signals are present during physiological (3D) dynamic compression (e.g., fluid flow, pressure gradients, streaming potentials, deformation)⁴⁻⁶. Even at early times in culture, the presence of proteoglycans would contribute to streaming potentials and osmotic gradients, while cell and pericellular matrix deformation⁷² and fluid flow may affect receptor-extracellular matrix (ECM) interactions. With the multitude of signals, it is conceivable that individual ligand-surface receptor interactions may be sensing different mechanical signals, mechanisms for which are beginning to be elucidated⁷³. Finally, further studies on downstream signaling events may shed light on how upstream mechanical signals may interact, and allow for better understanding as to how mechanical stimulation may be utilized to optimize ECM development in cartilage tissue engineering applications.

Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

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References

- Li G, Van de Velde SK, Bingham JT. Validation of a non-invasive fluoroscopic imaging technique for the measurement of dynamic knee joint motion. *J Biomech* 2008;41(7):1616–22. [PubMed: 18394629]
- Hodge WA, Fijan RS, Carlson KL, Burgess RG, Harris WH, Mann RW. Contact pressures in the human hip joint measured in vivo. *Proc Natl Acad Sci U S A* May;1986 83(9):2879–83. [PubMed: 3458248]
- Herberhold C, Faber S, Stammberger T, Steinlechner M, Putz R, Englmeier KH, et al. In situ measurement of articular cartilage deformation in intact femoropatellar joints under static loading. *J Biomech* Dec;1999 32(12):1287–95. [PubMed: 10569707]
- Frank EH, Grodzinsky AJ. Cartilage electromechanics--II. A continuum model of cartilage electrokinetics and correlation with experiments. *J Biomech* 1987;20(6):629–39. [PubMed: 3611138]
- Mak AF. Unconfined Compression of Hydrated Viscoelastic Tissues - a Biphasic Poroviscoelastic Analysis. *Biorheology* 1986;23(4):371–83. [PubMed: 3779062]
- Mow VC, Holmes MH, Lai WM. Fluid transport and mechanical properties of articular cartilage: a review. *J Biomech* 1984;17(5):377–94. [PubMed: 6376512]
- Jurvelin J, Kiviranta I, Saamanen AM, Tammi M, Helminen HJ. Partial restoration of immobilization-induced softening of canine articular cartilage after remobilization of the knee (stifle) joint. *J Orthop Res* 1989;7(3):352–8. [PubMed: 2703928]
- Behrens F, Kraft EL, Oegema TR Jr. Biochemical changes in articular cartilage after joint immobilization by casting or external fixation. *J Orthop Res* 1989;7(3):335–43. [PubMed: 2703926]
- Sah RLY, Kim YJ, Doong JYH, Grodzinsky AJ, Plaas AHK, Sandy JD. Biosynthetic Response of Cartilage Explants to Dynamic Compression. *J Orthopaed Res SEP*;1989 7(5):619–36.
- Buschmann MD, Gluzband YA, Grodzinsky AJ, Hunziker EB. Mechanical compression modulates matrix biosynthesis in chondrocyte/agarose culture. *J Cell Sci Apr*;1995 108(Pt 4):1497–508. [PubMed: 7615670]
- Lee DA, Bader DL. Compressive strains at physiological frequencies influence the metabolism of chondrocytes seeded in agarose. *J Orthop Res Mar*;1997 15(2):181–8. [PubMed: 9167619]
- Kelly TA, Ng KW, Wang CC, Ateshian GA, Hung CT. Spatial and temporal development of chondrocyte-seeded agarose constructs in free-swelling and dynamically loaded cultures. *J Biomech* 2006;39(8):1489–97. [PubMed: 15990101]
- Kiviranta I, Jurvelin J, Tammi M, Saamanen AM, Helminen HJ. Weight bearing controls glycosaminoglycan concentration and articular cartilage thickness in the knee joints of young beagle dogs. *Arthritis Rheum Jul*;1987 30(7):801–9. [PubMed: 3619962]
- Gray ML, Pizzanelli AM, Grodzinsky AJ, Lee RC. Mechanical and physiochemical determinants of the chondrocyte biosynthetic response. *J Orthop Res* 1988;6(6):777–92. [PubMed: 3171760]
- Caterson B, Lowther DA. Changes in Metabolism of Proteoglycans from Sheep Articular-Cartilage in Response to Mechanical-Stress. *Biochim Biophys Acta* 1978;540(3):412–22.
- Kim YJ, Sah RL, Grodzinsky AJ, Plaas AH, Sandy JD. Mechanical regulation of cartilage biosynthetic behavior: physical stimuli. *Arch Biochem Biophys* May 15;1994 311(1):1–12. [PubMed: 8185305]
- Fanning PJ, Emkey G, Smith RJ, Grodzinsky AJ, Szasz N, Trippel SB. Mechanical regulation of mitogen-activated protein kinase signaling in articular cartilage. *J Biol Chem Dec 19*;2003 278(51):50940–8. [PubMed: 12952976]

18. Fitzgerald JB, Jin M, Dean D, Wood DJ, Zheng MH, Grodzinsky AJ. Mechanical compression of cartilage explants induces multiple time-dependent gene expression patterns and involves intracellular calcium and cyclic AMP. *J Biol Chem* May 7;2004 279(19):19502–11. [PubMed: 14960571]
19. De Croos JN, Dhaliwal SS, Grynepas MD, Pilliar RM, Kandel RA. Cyclic compressive mechanical stimulation induces sequential catabolic and anabolic gene changes in chondrocytes resulting in increased extracellular matrix accumulation. *Matrix Biol* Aug;2006 25(6):323–31. [PubMed: 16697175]
20. Fitzgerald JB, Jin M, Chai DH, Siparsky P, Fanning P, Grodzinsky AJ. Shear- and Compression-induced Chondrocyte Transcription Requires MAPK Activation in Cartilage Explants. *J Biol Chem* Mar 14;2008 283(11):6735–43. [PubMed: 18086670]
21. Kurtis MS, Schmidt TA, Bugbee WD, Loeser RF, Sah RL. Integrin-mediated adhesion of human articular chondrocytes to cartilage. *Arthritis Rheum* Jan;2003 48(1):110–8. [PubMed: 12528111]
22. Salter DM, Hughes DE, Simpson R, Gardner DL. Integrin expression by human articular chondrocytes. *Br J Rheumatol* Apr;1992 31(4):231–4. [PubMed: 1372838]
23. Forsyth CB, Pulai J, Loeser RF. Fibronectin fragments and blocking antibodies to alpha2beta1 and alpha5beta1 integrins stimulate mitogen-activated protein kinase signaling and increase collagenase 3 (matrix metalloproteinase 13) production by human articular chondrocytes. *Arthritis Rheum Sep; 2002 46(9):2368–76. [PubMed: 12355484]*
24. Lucchinetti E, Bhargava MM, Torzilli PA. The effect of mechanical load on integrin subunits alpha5 and beta1 in chondrocytes from mature and immature cartilage explants. *Cell Tissue Res* Mar;2004 315(3):385–91. [PubMed: 14673641]
25. Kim SJ, Kim EJ, Kim YH, Hahn SB, Lee JW. The modulation of integrin expression by the extracellular matrix in articular chondrocytes. *Yonsei Med J* Jun 30;2003 44(3):493–501. [PubMed: 12833588]
26. Lapadula G, Iannone F, Zuccaro C, Grattagliano V, Covelli M, Patella V, et al. Integrin expression on chondrocytes: correlations with the degree of cartilage damage in human osteoarthritis. *Clin Exp Rheumatol* May-Jun;1997 15(3):247–54. [PubMed: 9177918]
27. Millward-Sadler SJ, Salter DM. Integrin-dependent signal cascades in chondrocyte mechanotransduction. *Ann Biomed Eng* Mar;2004 32(3):435–46. [PubMed: 15095818]
28. Knudson W, Loeser RF. CD44 and integrin matrix receptors participate in cartilage homeostasis. *Cell Mol Life Sci* Jan;2002 59(1):36–44. [PubMed: 11846031]
29. Mobasheri A, Carter SD, Martin-Vasallo P, Shakibaei M. Integrins and stretch activated ion channels; putative components of functional cell surface mechanoreceptors in articular chondrocytes. *Cell Biol Int* 2002;26(1):1–18. [PubMed: 11779216]
30. Kurtis MS, Tu BP, Gaya OA, Mollenhauer J, Knudson W, Loeser RF, et al. Mechanisms of chondrocyte adhesion to cartilage: role of beta1-integrins, CD44, and annexin V. *J Orthop Res* Nov; 2001 19(6):1122–30. [PubMed: 11781014]
31. Pulai JI, Del Carlo M Jr. Loeser RF. The alpha5beta1 integrin provides matrix survival signals for normal and osteoarthritic human articular chondrocytes in vitro. *Arthritis Rheum* Jun;2002 46(6): 1528–35. [PubMed: 12115183]
32. Millward-Sadler SJ, Wright MO, Lee H, Nishida K, Caldwell H, Nuki G, et al. Integrin-regulated secretion of interleukin 4: A novel pathway of mechanotransduction in human articular chondrocytes. *J Cell Biol* Apr 5;1999 145(1):183–9. [PubMed: 10189377]
33. Millward-Sadler SJ, Wright MO, Davies LW, Nuki G, Salter DM. Mechanotransduction via integrins and interleukin-4 results in altered aggrecan and matrix metalloproteinase 3 gene expression in normal, but not osteoarthritic, human articular chondrocytes. *Arthritis Rheum Sep;2000 43(9):2091–9. [PubMed: 11014361]*
34. Lee HS, Millward-Sadler SJ, Wright MO, Nuki G, Al-Jamal R, Salter DM. Activation of Integrin-RACK1/PKCalpha signalling in human articular chondrocyte mechanotransduction. *Osteoarthritis Cartilage* Nov;2002 10(11):890–7. [PubMed: 12435334]
35. Orazizadeh M, Lee HS, Groenendijk B, Sadler SJ, Wright MO, Lindberg FP, et al. CD47 associates with alpha 5 integrin and regulates responses of human articular chondrocytes to mechanical stimulation in an in vitro model. *Arthritis Res Ther* Jan 10;2008 10(1):R4. [PubMed: 18186923]

36. Holledge MM, Millward-Sadler SJ, Nuki G, Salter DM. Mechanical regulation of proteoglycan synthesis in normal and osteoarthritic human articular chondrocytes--roles for alpha5 and alphaVbeta5 integrins. *Biorheology* 2008;45(34):275–88. [PubMed: 18836230]
37. Kelly TA, Wang CC, Mauck RL, Ateshian GA, Hung CT. Role of cell-associated matrix in the development of free-swelling and dynamically loaded chondrocyte-seeded agarose gels. *Biorheology* 2004;41(34):223–37. [PubMed: 15299255]
38. Kisiday JD, Jin M, DiMicco MA, Kurz B, Grodzinsky AJ. Effects of dynamic compressive loading on chondrocyte biosynthesis in self-assembling peptide scaffolds. *J Biomech* May;2004 37(5):595–604. [PubMed: 15046988]
39. Chowdhury TT, Bader DL, Shelton JC, Lee DA. Temporal regulation of chondrocyte metabolism in agarose constructs subjected to dynamic compression. *Arch Biochem Biophys* Sep 1;2003 417(1):105–11. [PubMed: 12921786]
40. Demartean O, Wendt D, Braccini A, Jakob M, Schafer D, Heberer M, et al. Dynamic compression of cartilage constructs engineered from expanded human articular chondrocytes. *Biochem Biophys Res Commun* Oct 17;2003 310(2):580–8. [PubMed: 14521950]
41. Mauck RL, Byers BA, Yuan X, Tuan RS. Regulation of Cartilaginous ECM Gene Transcription by Chondrocytes and MSCs in 3D Culture in Response to Dynamic Loading. *Biomech Model Mechanobiol.* May 12;2006
42. Pingguan-Murphy B, Lee DA, Bader DL, Knight MM. Activation of chondrocytes calcium signalling by dynamic compression is independent of number of cycles. *Arch Biochem Biophys* Dec 1;2005 444(1):45–51. [PubMed: 16289021]
43. Mouw JK, Imler SM, Levenston ME. Ion-channel Regulation of Chondrocyte Matrix Synthesis in 3D Culture Under Static and Dynamic Compression. *Biomech Model Mechanobiol.* Jun 10;2006
44. Ragan PM, Chin VI, Hung HH, Masuda K, Thonar EJ, Arner EC, et al. Chondrocyte extracellular matrix synthesis and turnover are influenced by static compression in a new alginate disk culture system. *Arch Biochem Biophys* Nov 15;2000 383(2):256–64. [PubMed: 11185561]
45. Kisiday J, Jin M, Kurz B, Hung H, Semino C, Zhang S, et al. Self-assembling peptide hydrogel fosters chondrocyte extracellular matrix production and cell division: implications for cartilage tissue repair. *Proc Natl Acad Sci U S A* Jul 23;2002 99(15):9996–10001. [PubMed: 12119393]
46. Shannon KE, Keene JL, Settle SL, Duffin TD, Nickols MA, Westlin M, et al. Anti-metastatic properties of RGD-peptidomimetic agents S137 and S247. *Clin Exp Metastasis* 2004;21(2):129–38. [PubMed: 15168730]
47. Irvine DJ, Mayes AM, Griffith LG. Nanoscale clustering of RGD peptides at surfaces using Comb polymers. 1. Synthesis and characterization of Comb thin films. *Biomacromolecules* Spring;2001 2(1):85–94. [PubMed: 11749159]
48. Kuhlman W, Taniguchi I, Griffith LG, Mayes AM. Interplay between PEO tether length and ligand spacing governs cell spreading on RGD-modified PMMA-g-PEO comb copolymers. *Biomacromolecules* Oct;2007 8(10):3206–13. [PubMed: 17877394]
49. Koo LY, Irvine DJ, Mayes AM, Lauffenburger DA, Griffith LG. Co-regulation of cell adhesion by nanoscale RGD organization and mechanical stimulus. *J Cell Sci* Apr 1;2002 115(Pt 7):1423–33. [PubMed: 11896190]
50. kindly provided by Maria Ufret from the Griffith Lab at MIT
51. Pfaff M, McLane MA, Beviglia L, Niewiarowski S, Timpl R. Comparison of disintegrins with limited variation in the RGD loop in their binding to purified integrins alpha IIb beta 3, alpha V beta 3 and alpha 5 beta 1 and in cell adhesion inhibition. *Cell Adhes Commun* Dec;1994 2(6):491–501. [PubMed: 7538018]
52. Duque H, LaRocco M, Golde WT, Baxt B. Interactions of foot-and-mouth disease virus with soluble bovine alphaVbeta3 and alphaVbeta6 integrins. *J Virol* Sep;2004 78(18):9773–81. [PubMed: 15331710]
53. Radel C, Rizzo V. Integrin mechanotransduction stimulates caveolin-1 phosphorylation and recruitment of Csk to mediate actin reorganization. *Am J Physiol Heart Circ Physiol* Feb;2005 288(2):H936–45. [PubMed: 15471980]

54. Funderburgh JL, Funderburgh ML, Mann MM, Corpuz L, Roth MR. Proteoglycan expression during transforming growth factor beta -induced keratocyte-myofibroblast transdifferentiation. *J Biol Chem* Nov 23;2001 276(47):44173–8. [PubMed: 11555658]
55. Genes NG, Rowley JA, Mooney DJ, Bonassar LJ. Effect of substrate mechanics on chondrocyte adhesion to modified alginate surfaces. *Archives of Biochemistry and Biophysics* FEB 15;2004 422(2):161–7. [PubMed: 14759603]
56. Attur MG, Dave MN, Clancy RM, Patel IR, Abramson SB, Amin AR. Functional genomic analysis in arthritis-affected cartilage: yin-yang regulation of inflammatory mediators by alpha 5 beta 1 and alpha V beta 3 integrins. *J Immunol* Mar 1;2000 164(5):2684–91. [PubMed: 10679109]
57. Frank EH, Jin M, Loening AM, Levenston ME, Grodzinsky AJ. A versatile shear and compression apparatus for mechanical stimulation of tissue culture explants. *J Biomech* Nov;2000 33(11):1523–7. [PubMed: 10940414]
58. Hascall VC, Handley CJ, McQuillan DJ, Hascall GK, Robinson HC, Lowther DA. The effect of serum on biosynthesis of proteoglycans by bovine articular cartilage in culture. *Arch Biochem Biophys* Jul 1;1983 224(1):206–23. [PubMed: 6870254]
59. Sah RL, Doong JY, Grodzinsky AJ, Plaas AH, Sandy JD. Effects of compression on the loss of newly synthesized proteoglycans and proteins from cartilage explants. *Arch Biochem Biophys* Apr;1991 286(1):20–9. [PubMed: 1897947]
60. Kim YJ, Sah RL, Doong JY, Grodzinsky AJ. Fluorometric assay of DNA in cartilage explants using Hoechst 33258. *Anal Biochem* Oct;1988 174(1):168–76. [PubMed: 2464289]
61. Leddy HA, Awad HA, Guilak F. Molecular diffusion in tissue-engineered cartilage constructs: effects of scaffold material, time, and culture conditions. *J Biomed Mater Res B Appl Biomater* Aug 15;2004 70(2):397–406. [PubMed: 15264325]
62. De Rosa E, Urciuolo F, Borselli C, Gerbasio D, Imparato G, Netti PA. Time and space evolution of transport properties in agarose-chondrocyte constructs. *Tissue Eng* Aug;2006 12(8):2193–201. [PubMed: 16968160]
63. Hidaka C, Cheng C, Alexandre D, Bhargava M, Torzilli PA. Maturation differences in superficial and deep zone articular chondrocytes. *Cell Tissue Res* Jan;2006 323(1):127–35. [PubMed: 16133144]
64. Lu Y, Adkisson HD, Bogdanske J, Kalscheur V, Maloney W, Cheung R, et al. In vivo transplantation of neonatal ovine neocartilage allografts: determining the effectiveness of tissue transglutaminase. *J Knee Surg* Jan;2005 18(1):31–42. [PubMed: 15742595]
65. Feder, J.; Adkisson, H.; Kizer, N.; Hruska, K.; Cheugn, R.; Grodzinsky, A., et al. The promise of chondral repair using neocartilage. In: Sandell, L.; Grodzinsky, A., editors. *Tissue Engineering in Musculoskeletal Clinical Practice*. Amer Acad Orthop Surg; Rosemont: 2004. p. 219-26.
66. Engleman VW, Nickols GA, Ross FP, Horton MA, Griggs DW, Settle SL, et al. A peptidomimetic antagonist of the alpha(v)beta3 integrin inhibits bone resorption in vitro and prevents osteoporosis in vivo. *J Clin Invest* May 1;1997 99(9):2284–92. [PubMed: 9151803]
67. Goldberg RL, Toole BP. Pericellular coat of chick embryo chondrocytes: structural role of hyaluronate. *J Cell Biol* Dec;1984 99(6):2114–22. [PubMed: 6501414]
68. Dimicco MA, Kisiday JD, Gong H, Grodzinsky AJ. Structure of pericellular matrix around agarose-embedded chondrocytes. *Osteoarthritis Cartilage* Oct;2007 15(10):1207–16. [PubMed: 17524677]
69. Hynes RO. Integrins: versatility, modulation, and signaling in cell adhesion. *Cell* Apr 3;1992 69(1):11–25. [PubMed: 1555235]
70. Ronziere MC, Aubert-Foucher E, Gouttenoire J, Bernaud J, Herbage D, Mallein-Gerin F. Integrin alpha1beta1 mediates collagen induction of MMP-13 expression in MC615 chondrocytes. *Biochim Biophys Acta* Oct 30;2005 1746(1):55–64. [PubMed: 16198011]
71. Knudson W, Casey B, Nishida Y, Eger W, Kuettner KE, Knudson CB. Hyaluronan oligosaccharides perturb cartilage matrix homeostasis and induce chondrocytic chondrolysis. *Arthritis Rheum* May; 2000 43(5):1165–74. [PubMed: 10817571]
72. Knight MM, Ghori SA, Lee DA, Bader DL. Measurement of the deformation of isolated chondrocytes in agarose subjected to cyclic compression. *Med Eng Phys* Nov-Dec;1998 20(9):684–8. [PubMed: 10098613]

73. Jalali S, del Pozo MA, Chen K, Miao H, Li Y, Schwartz MA, et al. Integrin-mediated mechanotransduction requires its dynamic interaction with specific extracellular matrix (ECM) ligands. *Proc Natl Acad Sci U S A* Jan 30;2001 98(3):1042–6. [PubMed: 11158591]

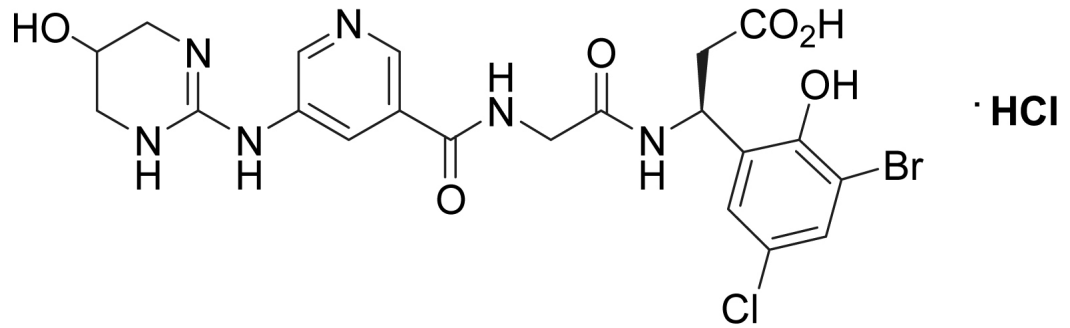


Figure 1. Chemical structure for PF001 (previously cited as S247 [40]). PF001 is a synthetic RGD peptidomimetic that acts as an integrin binding antagonist with broad specificity to αv and α5 integrins.

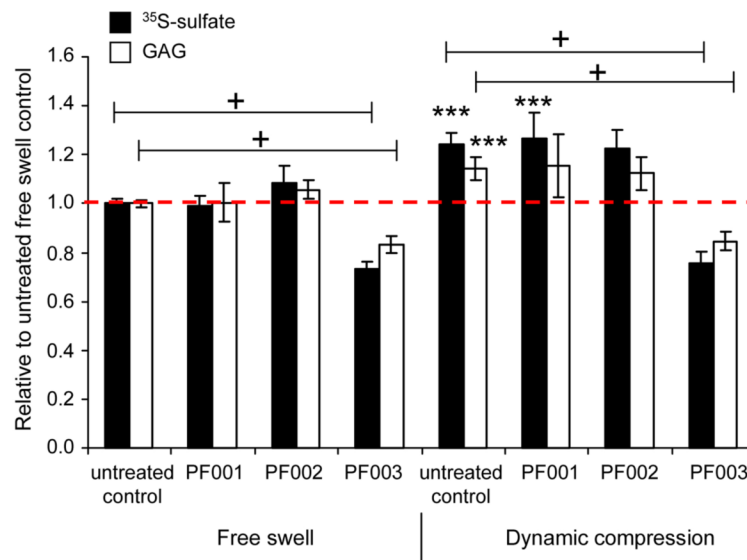


Figure 2. Biosynthetic response of chondrocytes in agarose culture to 24 hours of dynamic compression (1.0 Hz, 2.5% amplitude) in the presence of small-molecule integrin blockers PF001, PF002, PF003 (200uM). Data were normalized by the averaged untreated free-swell control for each animal. Data shown as mean \pm 95% confidence interval (CI), n = 6-19 disks from 2-6 animals (PF001 n=6, PF002 n=6, PF003 n=19). Sulfate incorporation as measured by radiolabel incorporation. Glycosaminoglycan (GAG) accumulation as measured by DMMB dye binding assay. *** p<0.0005 relative to free-swell, + p<0.0005 relative to untreated controls.

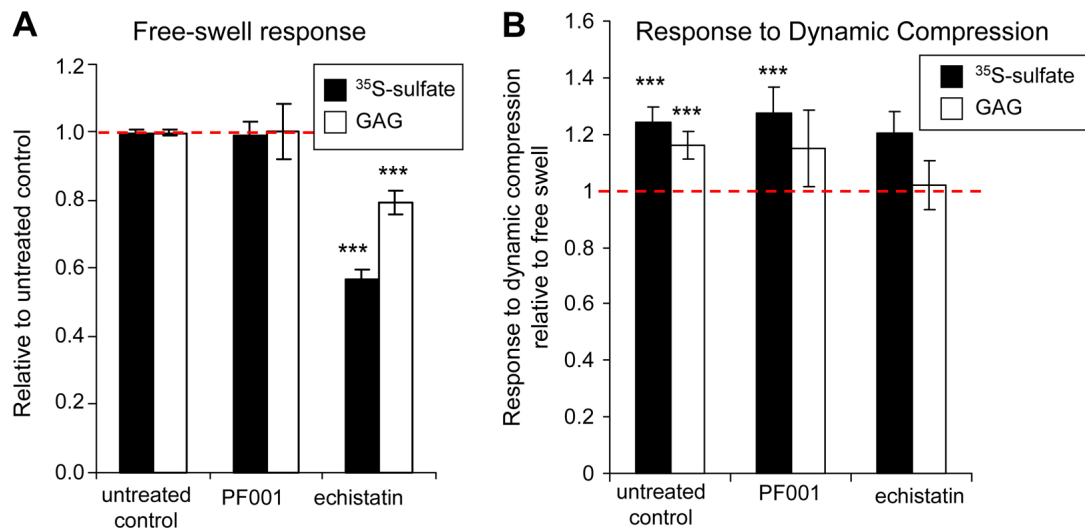


Figure 3.

Effects of broad spectrum integrin antagonists PF001 and echistatin in free-swelling culture (A) and on dynamic compression stimulation of agarose cultures (B). Data shown as mean \pm 95% CI. (A) Sulfate incorporation and GAG content in free-swell relative to untreated controls. n = 6-51 samples from 2-11 animals (control n=51, PF001 n=6, echistatin n=7), ***p<0.0005 relative to untreated control. (B) Proteoglycan synthesis as indicated by sulfate incorporation and GAG content with dynamic compression relative to treated free-swell controls. n = 6-13 samples from 2-4 animals (control n=13, PF001 n=6, echistatin n=7), ***p<0.0005 relative to 1 (no change relative to free-swell).

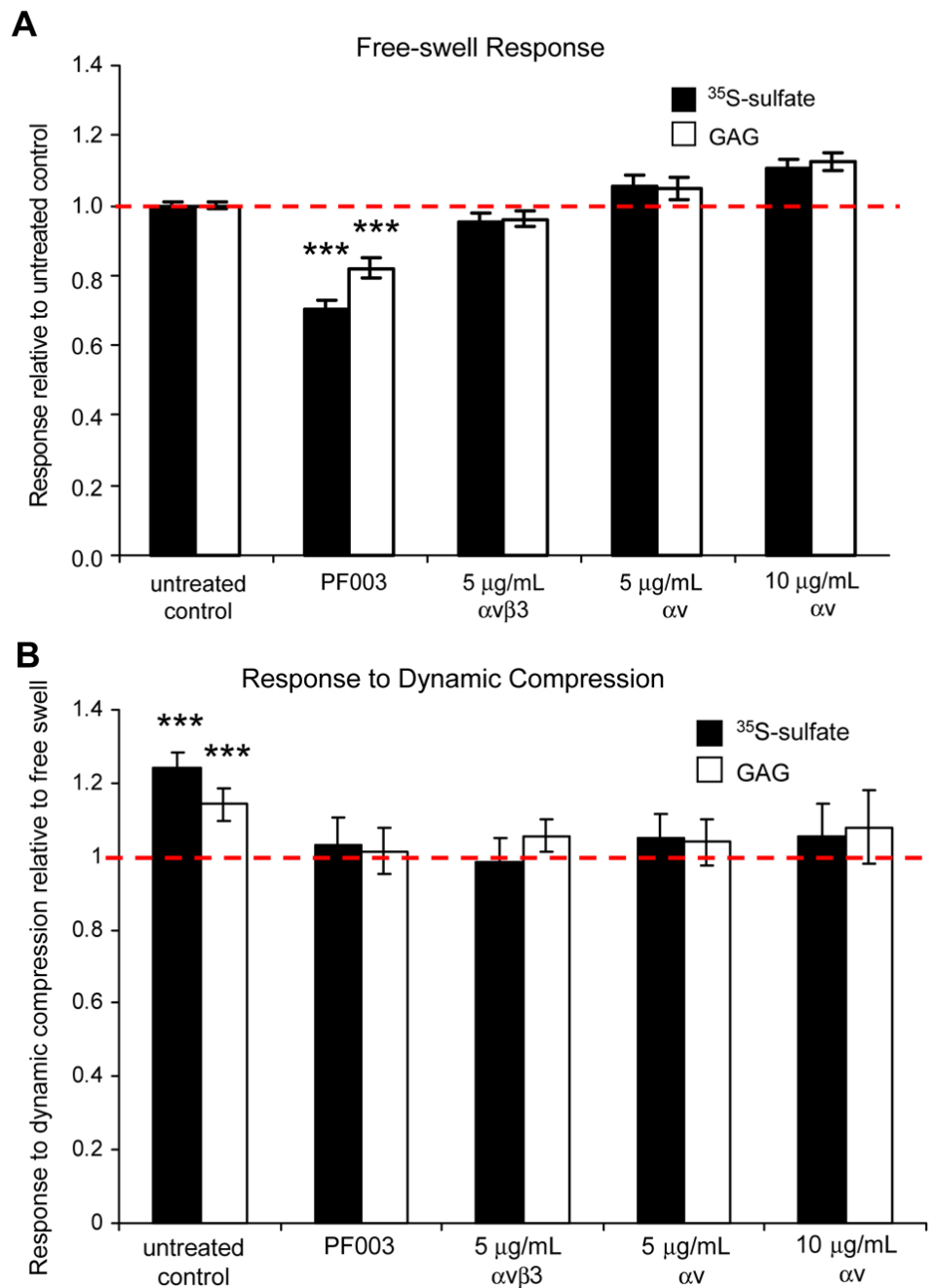


Figure 4. Effects of blocking $\alpha v\beta 3$ integrins on biosynthetic behavior in free-swelling culture and in response to dynamic compression. Data shown as mean \pm 95% CI. (A) Sulfate incorporation and GAG content in free-swelling agarose cultures relative to untreated controls. $n = 3$ -51 samples from 1-11 animals (control $n=51$, PF003 $n=29$, $\alpha v\beta 3$ $n=16$, 5 $\mu\text{g}/\text{mL}$ αv $n=12$, 10 $\mu\text{g}/\text{mL}$ αv $n=3$), *** $p < 0.0005$ relative to untreated control. (B) Proteoglycan synthesis (sulfate incorporation and GAG accumulation) after 24 hours of dynamic compression relative to respective treated free-swelling controls. $n = 3$ -19 samples from 1-6 animals (control $n=19$, PF003 $n=19$, $\alpha v\beta 3$ $n=3$, 5 $\mu\text{g}/\text{mL}$ αv $n=9$, 10 $\mu\text{g}/\text{mL}$ αv $n=3$), *** $p < 0.0005$ relative to 1 (no change compared to free-swelling).

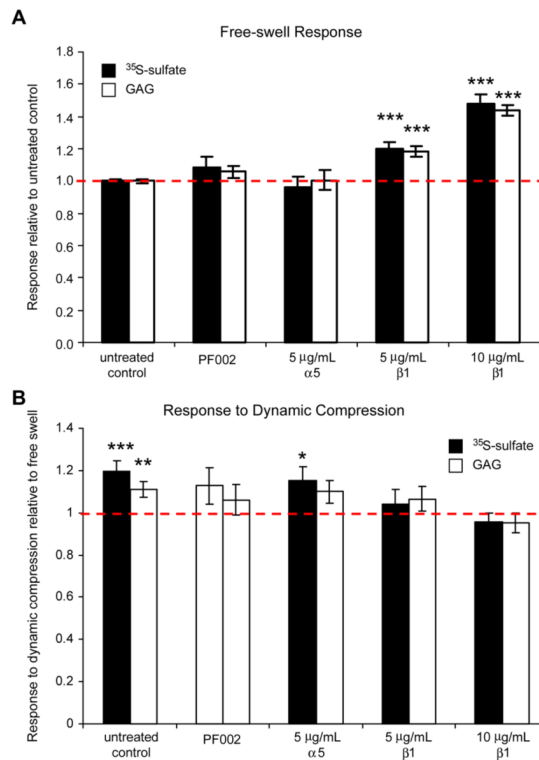


Figure 5.

Effects of blocking $\alpha 5\beta 1$ integrins on agarose cultures in free-swelling culture and in response to dynamic compression. Data shown as mean \pm 95% CI. (A) Sulfate incorporation and GAG content in free-swelling agarose cultures relative to untreated controls. $n = 3-51$ samples from 1-11 animals (control $n=51$, PF002 $n=6$, $\alpha 5$ $n=6$, 5 $\mu\text{g/mL}$ $\beta 1$ $n=6$, 10 $\mu\text{g/mL}$ $\beta 1$ $n=3$), $***p < 0.0005$ relative to untreated controls. (B) Proteoglycan synthesis (sulfate incorporation and GAG content) response after 24 hours of dynamic compression relative to respective treated free-swell controls. $n = 3-12$ samples from 1-4 animals (control $n=12$, PF002 $n=6$, $\alpha 5$ $n=6$, 5 $\mu\text{g/mL}$ $\beta 1$ $n=6$, 10 $\mu\text{g/mL}$ $\beta 1$ $n=3$). $***p < 0.0005$, $**p = 0.001$, $*p = 0.023$ relative to 1 (no change compared to free-swell).

Table 1

Molecular weight and relative specificities for PF001, PF002, PF003. IC50s were measured using specific integrin-transfected HEK 293 cell adhesion assays as in [46]. Data obtained from Pfizer, Inc. PF001 was previously cited as S247 46.

	Mol Wt	IC50 (nM)		
		$\alpha v \beta 3$	$\alpha v \beta 5$	$\alpha 5 \beta 1$
PF001 (S247)	569.8	0.40	1.50	64
PF002	388.9	179	1660	1.23
PF003	681.7	0.627	1.38	8940